Dissociable Neural Correlates of Uncertainty Underlie Different Exploration Strategies: Supplementary Information

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Supplementary Information

771 Variance inflation factors

Since the parametric modulators of the trial_onset regressor are correlated (e.g. V and V/TU), we computed variance 772 inflation factors (VIFs) for all four parametric modulators on all runs for all subjects (Supplementary Figure 8). 773 Overall, only 5% of VIFs for RU were above the threshold of 10 (12 out of 240), however we found that around 774 20% of VIFs for TU and V/TU were above 10 (53 and 47 out of 240, respectively), and more than half of VIFs for V 775 were above 10 (128 out of 240). Note that inferences are valid even for regressors with a high VIF since the estimate 776 of the beta coefficients is still unbiased and thus the type I error rate is preserved [1]. However, the inflated variance 777 of the beta estimates might reduce the power of the analysis. To investigate this possibility, we re-analyzed the data 778 using four new GLMs that were nearly identical to GLM 1, with the only difference that each new GLM had a single 779 parametric modulator at trial onset rather than four. Thus there was one GLM with RU, one with TU, one with V, and 780 one with V/TU. As before, we thresholded single voxels at p < 0.001. Since we are not using these results for ROI 781 selection, we report uncorrected whole-brain contrasts. 782

⁷⁸³ We found the same network of brain regions for RU and TU (Supplementary Figure 9A and B, respectively) and ⁷⁸⁴ no regions for V/TU. For V, we found clusters in medial PFC (Supplementary Figure 9C), which is consistent with ⁷⁸⁵ previous reports of value coding in this region [2, 3]. ROI analysis using an anatomically defined vmPFC region (as a ⁷⁸⁶ conjunction of Superior frontal gyrus, medial orbital; Superior frontal gyrus, medial; and Gyrus rectus from the AAL2 ⁷⁸⁷ atlas [4, 5]) showed a significant positive effect of V in left vmPFC (t(30) = 2.14, p = 0.04, t-test of ROI-averaged ⁷⁸⁸ betas across subjects). Since the value-coding function of this region has been characterized extensively [6, 7] and ⁷⁸⁹ since our primary interest was in the role of uncertainty in guiding exploration, we chose not to pursue this finding.

790 Reaction times and decision value

One potential confound of our decision value result (GLM 2) in motor cortex is reaction time (RT). When including RT's as a parametric modulator in addition to DV (GLM 2A), we found no effect of DV in motor cortex (no voxels ⁷⁹³ survived cluster FWE correction). Note, however, that the sequential sampling framework predicts a strong relationship ⁷⁹⁴ between DV and RT's: when DV is close to zero, the two options are similar to each other and hence it takes longer ⁷⁹⁵ for the evidence accumulator to reach a decision bound. This prediction was manifested in our data (coefficient ⁷⁹⁶ = -0.006, F(1,9717) = 23.8, p = 0.000001, mixed effects linear regression: RT ~ 1 + DV + (1 + DV | SubjectID)), ⁷⁹⁷ indicating that the negative result could be due to RT's capturing some of the shared variance in the BOLD signal.

To account for this possibility, we performed random effects Bayesian model comparison [8] between the GLM with 798 DV alone (GLM 2), the GLM with both DV and RT (GLM 2A), and a GLM with RT alone (GLM 2B) in the left 799 motor cortex ROI identified by GLM 2 (Figure 5A). Specifically, following our previous work [9], we approximated 800 the log model evidence as -0.5 * BIC, where the BIC was computed based on the residual variance of the GLM fits 801 within a 10 mm sphere around the peak voxel in left M1 from GLM 2. To prevent circularity [10], we performed 802 this using leave-one-subject-out cross-validation: for each subject, we computed the BIC in the peak ROI from the 803 group-level DV contrast computed using all other subjects. Since SPM fits each subject separately, this means that 804 we used independent data for ROI selection and model comparison, resulting in an unbiased analysis. To ensure the 805 validity of our inference, we confirmed that the resulting ROIs were highly overlapping (Supplementary Figure 10), 806 with all but one subject having the same left M1 ROI as the contrast using all subjects (Figure 5A, MNI [-38 -8 62]). 807 This analysis strongly favored GLM 2A (PXP = 0.96) over GLM 2 (PXP = 0) and GLM 2B (PXP = 0.04). This 808 indicates that the BOLD signal in left M1 is best explained by combination of DV and RT, rather than RT or DV alone, 809 pointing to decision value coding in motor cortex above and beyond RT's. 810



Supplementary Figure 1. Learning curves for human (A) and model (B) data. The better option is defined as the option with the greater expected reward $\mu(k)$. Error bars are cross-subject standard errors.



Supplementary Figure 2. Choice probability functions (A) and probit regression results (B) for human (left) and model (right) data. Error bars are cross-subject standard errors.



Supplementary Figure 3. **Performance comparison** of different exploration strategies. Simulation results from running different models generatively with subject-specific fitted coefficients. Error bars indicate s.e.m. across simulations.



Supplementary Figure 4. **Performance comparison** of simulations of the UCB/Thompson hybrid model (Eq. 4) with different parameter settings **w**. Color scale indicates P(better option), averaged across simulations. Red circle denotes the fitted fixed effects coefficients.



Supplementary Figure 5. Subject performance based on exploration strategy. Correlation between subject performance and fitted subject-specific coefficients (Eq. 4), indicating greater reliance on the corresponding strategy.



Supplementary Figure 6. Parameter recoverability.

- (A) Correlation between simulated and fitted parameters.
- (B) Correlation between fitted parameters.



Supplementary Figure 7. Corrected GLM 1 contrasts with single voxels thresholded at p < 0.001 and cluster FWE

correction applied at significance level $\alpha = 0.05$.

- (A) Relative uncertainty ($|RU_t|$) contrast. See Supplementary Table 3.
- (B) Total uncertainty (TU_t) contrast. See Supplementary Table 4.



Supplementary Figure 8. Variance inflation factors (VIFs) for parametric modulators of the trial onset regressor in GLM 1. Each plot shows the VIFs for all runs of a given subject. Green circles correspond to runs with VIF ≤ 10 , red circles correspond to runs with VIF > 10. A red horizontal line denotes the cutoff at 10.

- (A) relative uncertainty (RU),
- (B) total uncertainty (TU),
- (C) value difference (V),
- (D) value difference scaled by total uncertainty (V/TU).



Supplementary Figure 9. Contrasts from GLMs with a single parametric modulator.

(A) Uncorrected whole-brain RU contrast when only RU was included as a parametric modulator. Compare with

Figure 3A.

(B) Uncorrected whole-brain TU contrast when only TU was included as a parametric modulator. Compare with

Figure 4A.

(C) Uncorrected whole-brain V contrast when only V was included as a parametric modulator.



Supplementary Figure 10. Heatmap of ROIs from leave-one-subject-out GLM 2 DV contrasts.

Overlay of spherical ROIs around the peak voxel from the group-level DV contrast from GLM 2 using leave-one-subject-out cross-validation. Colorbar indicates how many folds each voxel was part of.

Model	Regressors	AIC	BIC	LL	Deviance
Softmax	V	8414.73	8400.37	-4198.18	8396.37
UCB	V + RU	7982.34	7953.62	-3972.81	7945.62
Thompson sampling	V/TU	8315.20	8300.84	-4148.42	8296.84
UCB/Thompson hybrid	V + RU + V/TU	6655.89	6612.80	-3300.40	6600.80

Supplementary Table 1. **Model comparison** between different exploration strategies, which can be thought of as lesioned versions of the UCB/Thompson hybrid model (Eq. 4). Lower AIC, BIC, and deviance indicate better fit. AIC = Akaike information criterion; BIC = Bayesian information criterion; LL = maximized log likelihood.

Regressor	Event	Duration	Pmods	Which trials	
GLM 1: RU, TU, V, V/TU					
trial_onset	trial onset	0 s	$ \mathrm{RU}_t , \mathrm{TU}_t, \mathrm{V}_t , \mathrm{V}_t /\mathrm{TU}_t$	non-timeout	
trial_onset_timeout	trial onset	0 s		timeout	
trial_onset_chose_1	trial onset	0 s		chose arm 1	
button_press	reaction time	0 s		all	
feedback_onset	feedback onset	0 s		all	
GLM 2: DV					
trial_onset	trial onset	0 s	$ \mathrm{DV}_t $	non-timeout	
trial_onset_timeout	trial onset	0 s		timeout	
trial_onset_chose_1	trial onset	0 s		chose arm 1	
button_press	reaction time	0 s		all	
feedback_onset	feedback onset	0 s		all	

Supplementary Table 2. GLM definitions. GLMs used to analyze the fMRI data in the main text.

Sign	Brain region	BA	Extent	<i>t</i> -value	MNI coord.
Negative	Middle occipital gyrus (L)	18	27153	-9.164	-30 -92 6
	Cerebellum (L)	37	27153	-8.433	-46 -52 -30
	Inferior occipital gyrus (R)	19	27153	-8.398	40 -84 -8
	Precentral gyrus (L)	6	1066	-6.702	-38 -16 68
	Superior frontal gyrus, dorsolateral (L)	6	1066	-4.582	-24 -6 48
	Superior frontal gyrus, dorsolateral (L)	6	1066	-4.075	-20 -10 76
	Supplementary motor area (L)	32	860	-6.231	-10 8 46
	Middle cingulate & paracingulate gyri (R)	32	860	-5.291	10 14 38
	Posterior cingulate gyrus (R)		530	-5.550	4 -22 28
	Left cerebral white matter (L)		530	-5.380	-16 -28 38
	Posterior cingulate gyrus (L)	26	530	-4.700	-6 -42 24
	Middle frontal gyrus (R)		732	-5.197	38 -4 68
	Supplementary motor area (R)	6	732	-5.169	16 2 62

Supplementary Table 3. **GLM 1 results: relative uncertainty**. Brain regions in which the BOLD signal tracks $|RU_t|$ from GLM 1 (corresponding to Supplementary Figure 7A). Anatomical labels and MNI coordinates are based on peak voxels (maximum *t*-statistic), with up to three peaks extracted per cluster (minimum separation of 20 voxels). Single voxels were thresholded at *p* < 0.001 and whole-brain cluster FWE correction was applied at significance level $\alpha = 0.05$. Regions were labeled using the Automated Anatomical Labeling (AAL2) atlas, the SPM Anatomy Toolbox, and the CMA Harvard-Oxford atlas. MNI = Montreal Neurological Institute; BA = Brodmann area.

Sign	Brain region	BA	Extent	t-value	MNI coord.
Positive	Inferior parietal gyrus, excluding supramarginal and angular gyri (L)	40	25346	9.793	-42 -40 52
	Inferior parietal gyrus, excluding supramarginal and angular gyri (R)	40	25346	9.362	38 -42 44
	Middle occipital gyrus (R)	19	25346	9.111	32 -66 36
	Precentral gyrus (L)	44	785	7.353	-44 4 30
	Insula (L)	48	614	7.054	-28 20 2
	Precentral gyrus (R)	44	709	7.018	48 8 30
	Thalamus (L)		294	6.099	-4 -16 14
	Insula (R)	47	307	5.369	36 18 0
	Middle frontal gyrus (L)	46	704	5.152	-42 36 36
	Middle frontal gyrus (L)	46	704	4.405	-44 48 14
Negative	Superior frontal gyrus, dorsolateral (L)	10	1650	-6.957	-4 62 30
	Superior frontal gyrus, medial orbital (L)	11	1650	-6.448	-2 58 -8
	Gyrus rectus (L)	11	1650	-5.884	-4 36 -16
	Precuneus (L)	30	436	-5.904	-10 -54 16
	Precuneus (L)	30	436	-5.196	-10 -50 38

Supplementary Table 4. **GLM 1 results: total uncertainty**. Brain regions in which the BOLD signal tracks TU_t (corresponding to Supplementary Figure 7B). Notation and procedures as in Supplementary Table 3.

Sign	Brain region	BA	Extent	<i>t</i> -value	MNI coord.
Negative	Precentral gyrus (L)	6	721	-6.851	-38 -8 62
	Postcentral gyrus (L)	2	721	-4.303	-48 -38 56
	Superior frontal gyrus (L)		721	-4.014	-14 6 74

Supplementary Table 5. **GLM 2 results: decision value**. Brain regions in which the BOLD signal tracks $|DV_t|$ (corresponding to Figure 5A). Notation and procedures as in Supplementary Table 3.

Supplementary References

[1] Jeanette Mumford, Jean-Baptiste Poline, and Russell Poldrack. "Orthogonalization of Regressors in fMRI

Models". In: PLoS ONE 10 (Apr. 2015), e0126255.

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813

814	[2]	William H Alexander and Joshua W Brown. "Medial prefrontal cortex as an action-outcome predictor". In:
815		<i>Nature neuroscience</i> 14.10 (2011), p. 1338.
816	[3]	Fabian Grabenhorst and Edmund T Rolls. "Value, pleasure and choice in the ventral prefrontal cortex". In:
817		Trends in cognitive sciences 15.2 (2011), pp. 56–67.
818	[4]	N. Tzourio-Mazoyer et al. "Automated Anatomical Labeling of Activations in SPM Using a Macroscopic
819		Anatomical Parcellation of the MNI MRI Single-Subject Brain". In: NeuroImage 15.1 (2002), pp. 273–289.
820		ISSN: 1053-8119. DOI: http://dx.doi.org/10.1006/nimg.2001.0978. URL: http://www.
821		sciencedirect.com/science/article/pii/S1053811901909784.
822	[5]	Edmund T. Rolls, Marc Joliot, and Nathalie Tzourio-Mazoyer. "Implementation of a new parcellation of the
823		orbitofrontal cortex in the automated anatomical labeling atlas". In: NeuroImage 122 (2015), pp. 1-5. ISSN:
824		1053-8119. DOI: http://dx.doi.org/10.1016/j.neuroimage.2015.07.075. URL: http:
825		//www.sciencedirect.com/science/article/pii/S1053811915006953.
826	[6]	Nathaniel D Daw et al. "Cortical substrates for exploratory decisions in humans". In: Nature 441.7095 (2006),
827		p. 876.
828	[7]	Seung-Lark Lim, John P O'Doherty, and Antonio Rangel. "The decision value computations in the vmPFC and
829		striatum use a relative value code that is guided by visual attention". In: Journal of Neuroscience 31.37 (2011),
830		pp. 13214–13223.
831	[8]	Lionel Rigoux et al. "Bayesian model selection for group studies-revisited". In: Neuroimage 84 (2014), pp. 971–985.
832	[9]	Momchil S Tomov, Hayley M Dorfman, and Samuel J Gershman. "Neural computations underlying causal
833		structure learning". In: Journal of Neuroscience 38.32 (2018), pp. 7143–7157.

60

- [10] Nikolaus Kriegeskorte et al. "Circular analysis in systems neuroscience: the dangers of double dipping". In:
- ⁸³⁵ *Nature neuroscience* 12.5 (2009), p. 535.