

## **Ketamine, but not the NMDA Receptor Antagonist Lanicemine, Increases Prefrontal Connectivity in Depressed Patients**

### ***Image Processing***

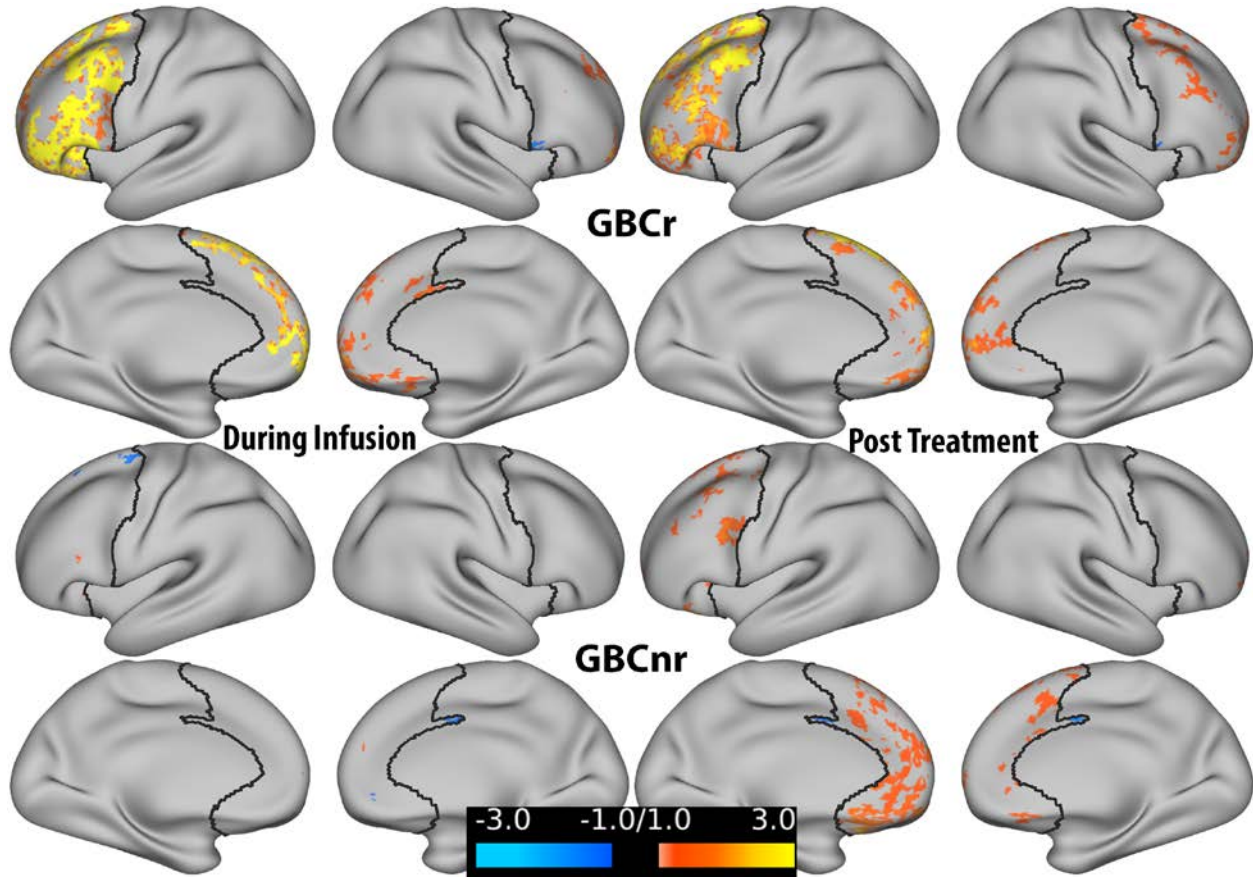
The Human Connectome Project (HCP) Pipelines ([github.com/Washington-University/Pipelines](https://github.com/Washington-University/Pipelines)) were adapted to process the imaging data <sup>1</sup>. Briefly, the adapted minimal preprocessing included FreeSurfer automatic segmentation and parcellation of high resolution T1 MRI scans, deletion of first 5 volumes, slice timing correction, motion correction, intensity normalization, brain masking, and registration of fMRI images to structural MRI and standard template, while minimizing smoothing from interpolation. Then, the cortical gray matter ribbon voxels and each subcortical parcel were projected to a standard Connectivity Informatics Technology Initiative (CIFTI) 2mm grayordinate space. ICA-FIX was run to identify and remove artifacts <sup>2,3</sup>, followed by mean grayordinate time series regression (MGTR; which is comparable to global signal regression in volume data). The latter two processing steps (FIX+MGTR) have been found to significantly reduce motion-correlated artifacts <sup>4</sup>. In addition, there were no differences in head motion during fMRI session between groups at any study time point (see Table S1).

Details of global brain connectivity with global signal regression (GBCr) methods were previously described <sup>5-16</sup>. Briefly, time series were demeaned and normalized, followed by generating dense connectomes correlating each vertex/voxel with all other vertices/voxels in the CIFTI grayordinates, and then transformed to Fisher z values. For each vertex/voxel, GBCr is calculated as the standardized average (z-scored) across those Fisher z values, which generates a map for each fMRI session where each vertex/voxel value represents the functional connectivity strength of that grayordinate with the rest of the brain. In graph theory terms, GBCr (also known as Functional Connectivity Strength; FCS <sup>17</sup>) is considered a weighted measure of nodal strength of a voxel in the whole brain network – determining brain hubs and examining the coherence between a local region and the rest of the brain <sup>18</sup>.

Similar to previous studies <sup>5</sup>, we have limited our investigation to the prefrontal cortex (PFC), 1<sup>st</sup> because of its critical role in depression, 2<sup>nd</sup> because previous findings of reduced GBCr were limited to the PFC, and 3<sup>rd</sup> to limit Type I & Type II errors and facilitate the interpretation of the findings. GBCr maps were smoothed ( $\sigma = 4$ ) prior to vertex-wise analyses. The HCP multi-modal parcellation (MMP) <sup>19</sup> was used to create the PFC mask (delineated in Fig. 2 & 3). Each PFC mask included the following regions: R\_FEF\_ROI, R\_PEF\_ROI, R\_55b\_ROI, R\_SFL\_ROI, R\_SCEF\_ROI, R\_6ma\_ROI, R\_33pr\_ROI, R\_a24pr\_ROI, R\_p32pr\_ROI, R\_a24\_ROI, R\_d32\_ROI, R\_8BM\_ROI, R\_p32\_ROI, R\_10r\_ROI, R\_47m\_ROI, R\_8Av\_ROI, R\_8Ad\_ROI, R\_9m\_ROI, R\_8BL\_ROI, R\_9p\_ROI, R\_10d\_ROI, R\_8C\_ROI, R\_44\_ROI, R\_45\_ROI, R\_47l\_ROI, R\_a47r\_ROI, R\_6r\_ROI, R\_IFJa\_ROI, R\_IFJp\_ROI, R\_IFSp\_ROI, R\_IFSa\_ROI, R\_p9-46v\_ROI, R\_46\_ROI, R\_a9-46v\_ROI, R\_9-46d\_ROI, R\_9a\_ROI, R\_10v\_ROI, R\_a10p\_ROI, R\_10pp\_ROI, R\_11l\_ROI, R\_13l\_ROI, R\_OFC\_ROI, R\_47s\_ROI, R\_6a\_ROI, R\_i6-8\_ROI, R\_s6-8\_ROI, R\_FOP4\_ROI, R\_AVI\_ROI, R\_FOP1\_ROI, R\_25\_ROI, R\_s32\_ROI, R\_pOFC\_ROI, R\_FOP5\_ROI, R\_p10p\_ROI, R\_p47r\_ROI, R\_a32pr\_ROI, R\_p24\_ROI, L\_FEF\_ROI, L\_PEF\_ROI, L\_55b\_ROI, L\_SFL\_ROI, L\_SCEF\_ROI, L\_6ma\_ROI, L\_33pr\_ROI, L\_a24pr\_ROI, L\_p32pr\_ROI, L\_a24\_ROI, L\_d32\_ROI, L\_8BM\_ROI, L\_p32\_ROI, L\_10r\_ROI, L\_47m\_ROI,

L\_8Av\_ROI, L\_8Ad\_ROI, L\_9m\_ROI, L\_8BL\_ROI, L\_9p\_ROI, L\_10d\_ROI, L\_8C\_ROI, L\_44\_ROI, L\_45\_ROI, L\_47l\_ROI, L\_a47r\_ROI, L\_6r\_ROI, L\_IFJa\_ROI, L\_IFJp\_ROI, L\_IFSp\_ROI, L\_IFSa\_ROI, L\_p9-46v\_ROI, L\_46\_ROI, L\_a9-46v\_ROI, L\_9-46d\_ROI, L\_9a\_ROI, L\_10v\_ROI, L\_a10p\_ROI, L\_10pp\_ROI, L\_11l\_ROI, L\_13l\_ROI, L\_OFC\_ROI, L\_47s\_ROI, L\_6a\_ROI, L\_i6-8\_ROI, L\_s6-8\_ROI, L\_FOP4\_ROI, L\_AVI\_ROI, L\_FOP1\_ROI, L\_25\_ROI, L\_s32\_ROI, L\_pOFC\_ROI, L\_FOP5\_ROI, L\_p10p\_ROI, L\_p47r\_ROI, L\_a32pr\_ROI.

We have used GBCr, instead of GBC without global signal regression (GBCnr), because the study hypotheses were based on previous GBCr findings<sup>5-11, 13, 17</sup>, which provided the rationale for the current report and will facilitate the interpretation of the study findings. Of note, in previous studies we found no GBCnr alteration in TRD and ketamine had no effects on GBCnr levels<sup>6</sup>. For completion, we have repeated the vertex-wise analyses in the current study using PFC GBCnr (i.e., without MGTR), which showed no significant effects of ketamine on PFC GBCnr during infusion or 24h post-treatment. The patterns of uncorrected PFC GBCr and GBCnr changes following ketamine are shown in Fig. S1. It is noticeable that 24h post-treatment the PFC GBCnr clusters (mostly increased) appears to largely follow the same pattern of PFC GBCr changes.



**Figure S1. Statistical maps comparing delta PFC GBCr (top) and GBCnr (bottom) between ketamine and placebo.** These maps were not corrected for multiple comparisons. None of the clusters in the GBCnr maps will survive correction. Although there were no large GBCnr clusters during infusion (left), it is noticeable that 24h post-treatment the PFC GBCnr clusters (mostly increased) appeared to largely follow the same pattern of PFC GBCr changes (right). The latter observation raises the question whether the higher sensitivity of GBCr is due to its resistance to artifacts.

**Table S1. Demographics and Clinical Characteristics**

	Placebo	Ketamine	Lanicemine	<i>p</i> <sup>a</sup>
	Mean ± <i>SEM</i>	Mean ± <i>SEM</i>	Mean ± <i>SEM</i>	
Subjects (N)	18	19	19	
Female (N; %)	10 (56%)	12 (63%)	12 (63 %)	0.86
Manchester site (N; %)	10 (56%)	9 (47%)	8 (42%)	0.71
Oxford site (N; %)	8 (44%)	10 (53%)	11 (58%)	0.71
Baseline - BDI	26 ± 1.9	31 ± 1.6	34 ± 2.3	0.02
Post-treatment - BDI	18 ± 2.5	22 ± 1.9	26 ± 2.7	0.06
Improvement (%) - BDI	27 ± 8	29 ± 6	20 ± 5	0.49
Baseline – Motion <sup>b</sup>	0.11 ± 0.01	0.12 ± 0.02	0.09 ± 0.01	0.41
During Infusion - Motion <sup>b</sup>	0.18 ± 0.03	0.14 ± 0.01	0.14 ± 0.02	0.46
Post-treatment - Motion <sup>b</sup>	0.12 ± 0.02	0.13 ± 0.02	0.11 ± 0.02	0.52

a. ANOVA or Chi square test (significance set at  $p \leq .05$ ); b. frame to frame motion; **Abbreviations:** BDI: Beck Depression Inventory;

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