Online supplement

Deep Learning Detection of Penumbral Tissue on Arterial Spin Labeling in Stroke

| Sex | 8 | |
|----------------------|--|--|
| | Female | 89/167 (53.3%) |
| | Male | 78/167 (46.7%) |
| Age, years | | 70.7 (14.7) |
| Clinical features | | |
| | NIHSS score* | 14 (5-19) |
| | Systolic blood pressure, mmHg | 152.0 (28.3) |
| | Diastolic blood pressure, mm Hg | 85.0 (17.6) |
| | Large Vessel Occlusion | 105/137 (76.6%) |
| Field strength | | |
| | 1.5 T | 93/167 (55.7%) |
| | 3.0 T | 74/167 (44.3%) |
| Scan Time Point | | |
| | Baseline | 121/167 (72.5%) |
| | Time point 2 | 38/167 (22.8%) |
| | Time point 3 | 8/167 (4.8%) |
| Coord times from the | | |
| Scan time from the | Whole group | |
| onset of symptoms, n | Receipe | 11.7 (0.0-20.2) |
| | Time point 2 | 0.2 (4.0-22.0) 25 5 (13 0-33 0) |
| | Time point 2 | 23.3 (13.0-33.0) |
| | | J7.2 (JU.0 ⁻ 04.0) |
| Affected Territory* | Internal Constid Antony | 22/126/26/20/ |
| | Internal Carotid Artery | 33/126 (26.2%) |
| | Middle Cerebral Artery | /6/126 (60.3%) |
| | Antonior Cerebral Artery | 11/12b (10.3%) |
| | Anterior Cerebral Artery | //120 (5.0%) 1/126 (0.7%) |
| | Common Carotid Artony | 1/120 (U.7%) 2/126 (2.4%) |
| | Vortobral Artony | 5/120 (2.4%) 4/126 (2.2%) |
| | Normal appearance | 4/ 120 (3.2 <i>%</i>) 21/126 (16.7%) |
| | Multiple hilateral | 5/126 (10.7%) |
| | Normal appearance Multiple, bilateral | 21/126 (16.7%) 5/126 (4.0%) |

Table I. Demographics of Training Dataset

Data are in n (%), mean (SD), or median (IQR). NIHSS = National Institutes of Health Stroke Scale. *Scores range from 0 to 42, with higher scores indicating more severe neurological deficit. †Affected territory (territories) designation according to the clinician's interpretation of MRA, if available, at baseline.

| Sex | | |
|-----------------------------|--|---|
| | Female Male | 8/12 (66.7%) 4/12 (33.3%) |
| Age, years | | 68.3 (11.3) |
| Clinical features | | |
| | NIHSS score* Systolic blood pressure, mmHg Diastolic blood pressure, mm Hg Large Vessel Occlusion | 14 (9 - 18) 132(30) 69 (18) 12/12 (100%) |
| Field strength | | |
| | 1.5 T 3.0 T | 1/12 (8.3%) 11/12 (92.7%) |
| Scan Time Point | | |
| | Baseline | 12/12 (100%) |
| Scan time from the onset of | | |
| symptoms, h | Whole group | 5.8 (3.4-9.9) |
| Affected Territory† | | |
| | Middle Cerebral Artery | 11/12 (92.7%) |
| | Internal Carotid Artery | 1/12 (8.3) |

Table II. Demographics of Stanford Validation Dataset

Data are in n (%), mean (SD), or median (IQR). NIHSS = National Institutes of Health Stroke Scale. *Scores range from 0 to 42, with higher scores indicating more severe neurological deficit. †Affected territory (territories) designation according to the clinician's interpretation of MRA, if available, at baseline.

Table III Confusion Matrix of treatment decision of DL model in the UCLA cohort

| | | DSC | | |
|-----------|----------|----------|----------|--|
| | | Positive | Negative | |
| Informa | Positive | 17 | 1 | |
| interence | Negative | 2 | 18 | |

Of the total 38 subjects, 35 were correctly classified, leading to an accuracy of 0.92 (95% CI: [0.79, 0.98]).

| | Accuracy | Sensitivity | Specificity | Positive Predictive Value | Negative Predictive Value | AUC | Cohen's Kappa |
|-------------------------------|----------|-------------|-------------|---------------------------------|---------------------------------|-------|------------------|
| DL model | 0.92 | 0.89 | 0.95 | 0.94 | 0.90 | 0.95 | 0.84 |
| Linear Regression | 0.84 | 0.68 | 1.00 | 1.00 | 0.76 | 0.947 | 0.68 |
| Ridge Regression | 0.79 | 0.58 | 1.00 | 1.00 | 0.70 | 0.915 | 0.58 |
| Kernel Ridge Regression | 0.79 | 0.58 | 1.00 | 1.00 | 0.70 | 0.931 | 0.58 |
| Neural Network | 0.66 | 0.37 | 0.95 | 0.88 | 0.60 | 0.94 | 0.31 |
| SVM with RBF Kernel | 0.82 | 0.63 | 1.00 | 1.00 | 0.73 | 0.949 | 0.63 |
| Random Forests | 0.74 | 0.53 | 0.95 | 0.91 | 0.67 | 0.924 | 0.47 |

Table IV. Summary of classification indices of the DL model and 6 ML algorithms.

When the cut-off determined by voxel-wise training was applied, our DL model achieved significantly higher accuracy for treatment eligibility, compared with ML algorithms. When the cutoff threshold was varied to generate a ROC curve, the DL model still yielded the highest AUC of 0.950, while the AUC of the ML algorithms ranged from 0.915 to 0.949. Cohen's Kappa coefficient also supported that the DL model has the most consistent output with Tmax label compared with ML algorithms.

Table V Confusion Matrix of treatment decision of DL model in the Stanford cohort.

| | | DSC | | |
|-----------|----------|----------|----------|---|
| | | Positive | Negative | |
| Inference | Positive | 3 | | 0 |
| | Negative | 1 | | 8 |

Of the total 12 subjects, only 1 subject was misclassified, yielding an accuracy of 0.92 (95% CI: [0.62, 0.99]).

| CBF (ml/100g/min) | ASL 1.5T | ASL 3T |
|-------------------|-----------|-----------|
| Infarct CBF | 11.8±13.4 | 9.9±9.7 |
| Penumbral CBF | 15.4±16.6 | 12.7±11.1 |
| Contralateral CBF | 38.9±26.9 | 34.5±15.4 |
| | | |

Table VI Mean CBF \pm SD of infarct core, penumbral tissue and contralateral region at 1.5T and 3T

Although no specific CBF threshold are required for the DL model to learn, the mean CBF values increase from the infarct core, to penumbral tissue (based on DL inference), and to the contralateral region at both 1.5 and 3T.