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Table S1: Comparison of aneurysm epidemiology, morphology, clinical treatments, intervention criteria, simulation considerations, and types of clinical studies. Abbreviations: D, Diameter; KD, Kawasaki disease

Table S2: Modeling parameters and inputs commonly used in computational modeling of aneurysms⁵¹

hemodynamic parameter	nomenclature/equation	common units	hemodynamic considerations
wall shear stress (WSS)	$\overrightarrow{t_{w}} = \mu \frac{\partial v}{\partial r}$, evaluated at the wall	Dynes/cm ² , Pa	measure of hemodynamic stress on vessel wall - related to thrombosis risk and endothelial function; low levels
time-averaged wall shear stress (TAWSS)	$TANSS = \frac{1}{t} \int_{0}^{t} WSS dt$	Dynes/cm ² , Pa	associated with proinflammatory and prothrombotic and high levels associated with vascular disease pathogenesis ^{93,94}
wall shear stress gradient (WSSG)	WSSG $=\sqrt{\left(\left \frac{\partial \vec{\tau}_w}{\partial x}\right \right)^2+\left(\left \frac{\partial \vec{\tau}_w}{\partial y}\right \right)^2+\left(\left \frac{\partial \vec{\tau}_w}{\partial z}\right \right)^2}$	Dynes/cm ³ , Pa/mm	magnitude of spatial gradient of WSS, positive WSSG (i.e. accelerating flow) associated with cerebral aneurysm growth and remodeling 93
oscillatory shear index (OSI)	$OSI = 0.5\left(1 - \frac{ \int_0^t WSSdt }{\int_0^t WSS dt}\right)$	dimensionless	measure of flow directionality and disturbed flow, associated with proinflammatory changes ⁹³ minimum $OSI = 0$: unidirectional flow; maximum $OSI = 0.5$: equal flow in both directions ⁹²
residence time (RT) measures	quantifiable via Lagrangian or Eulerian methods 95	s, $1/Pa$, dimensionless	measure of flow stagnation, related to thrombosis and wall inflammation ^{95,96} there is no globally appropriate RT method; approach should be selected based on the context of the simulation and quantities of interest ⁹⁵

Table S3: Hemodynamic parameters commonly used in computational modeling of aneurysm⁹²

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