

# Supplementary Material

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Title: *“Human Purkinje in silico model enables mechanistic investigations into automaticity and pro-arrhythmic abnormalities”*

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# 1 - Supplementary Methods

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## 1.1 The Calibrated Trovato2020 Model

Figure 1B illustrates the structure of the new human Purkinje model, the Trovato2020 model, with 6 cellular compartments, 18 trans-membrane ionic currents, 3 intracellular concentrations ( $\text{Na}^+$ ,  $\text{K}^+$  and  $\text{Ca}^{2+}$ ) for each of the 3 cellular compartments,  $\text{Ca}^{2+}$  buffers and CaMKII kinetics as in the ORd model (O'Hara et al. 2011), and  $\text{Ca}^{2+}$  subsystem as in the PRd model (Li and Rudy 2011). Overall, the Trovato2020 model has 46 state variables.

*Cellular compartments:* the intracellular compartmentalisation was defined as in the PRd model, based on a triple-layer structure suggested by (Stuyvers et al. 2005). The cell, represented as a cylinder, is divided into 3 cytoplasmic compartments: i) peripheral coupling subspace (SS), where sarcolemmal  $\text{Ca}^{2+}$  entry (via  $I_{\text{CaL}}$ ) interacts with the sarcoplasmic reticulum (SR); ii) sub-sarcolemmal region (SL), representing the layer of cytoplasm underneath the membrane; iii) bulk myoplasm, that represents the innermost region of the cell.

The SR is also divided into 3 compartments:

- i) junctional SR, with two  $\text{Ca}^{2+}$ -release units (RyR3 and  $\text{IP}_3\text{R}$ ), which respond to  $\text{Ca}^{2+}$  changes in the SS;
- ii) corbular SR, representing the SR portion close to the cell membrane, and with  $\text{Ca}^{2+}$ -release units (RyR2) which respond to  $\text{Ca}^{2+}$  changes into the bulk myoplasm only;
- iii) network SR, representing a region between JSR and CSR with no expression of  $\text{Ca}^{2+}$ -release units (Li and Rudy 2011).

*Potassium Currents:*  $I_{\text{to}}$ ,  $I_{\text{Sus}}$  and  $I_{\text{K1}}$  formulations were constructed using Dataset I (Han et al., 2002) as follows.  $I_{\text{to}}$  formulation includes one activation gate and two inactivation gates (fast and slow) with steady state activation/inactivation curves and inactivation time constants, larger in PCs than in VCs, based on experiments by Han et al., 2002, and activation time constant as in the ORd model (no experimental data available). Thus, the Trovato2020 representation of  $I_{\text{to}}$  differs both from the ventricular formulation used by ten Tusscher and Panfilov 2008 and from the one implemented in Stewart et al. 2009. In particular, the latter describes  $I_{\text{to}}$  inactivation using only one gate, using experimental data for the slow inactivation time constant published by (Han et al. 2002), whereas, the activation time constant is fitted on the experimental data for  $I_{\text{to}}$  fast inactivation. The small ORd background  $\text{K}^+$  current was replaced with a single instantaneous voltage-dependent current, based on the experimental I-V curve for  $I_{\text{Sus}}$ . The  $I_{\text{K1}}$  formulation was modified by fitting the instantaneous voltage-dependent

rectification gate to the experimental I-V curve, shifted by -14 mV to account for the liquid junction potential and to match the reversal potential to the potassium Nernst potential computed from the intra and extra-cellular concentrations. The maximum conductances of these three currents were also set based on the experimental I-V curves, after correcting the data for heart failure (+25% and +56% for  $I_{K1}$  and  $I_{to}$ , respectively), as described in (Stewart et al. 2009).  $I_{Kr}$  and  $I_{Ks}$  formulations were left as in the ORd model, since no human Purkinje data are available in literature (Nagy et al. 2015) and gene expression levels for these proteins in humans (hERG and KvLQT1) were found to be similar in PCs and VCs (Gaborit et al. 2007). Based on the sensitivity analysis, some changes were made to  $I_{Kr}$  kinetics: activation time constants were shifted by +15 mV and the time-independent inactivation gate was scaled by a factor of 0.3 (Table S1).

*Sodium Currents:* The Trovato2020 model includes the modified ORd formulation of  $I_{Na}$  described in (Dutta et al. 2017; Passini et al. 2016) which supports AP propagation also in 3D simulations. Several studies in PCs (Haissaguerre et al. 2016; Nagy et al. 2015) highlighted the role of non-cardiac isoforms of the sodium channel, which have slower inactivation kinetics and a different sensitivity to tetrodotoxin. In order to account for the sodium current characteristics and functional role experimentally shown in PCs, the original ORd formulation of  $I_{NaL}$  was kept in the Trovato2020, though its conductance was increased 2.5 folds, based on experimental evidence by (Iyer et al. 2015; Haufe et al. 2005). However, we did not split the formulation into cardiac and non-cardiac isoform contributions, which might be a possible future development when data from human PCs become available. Background  $Na^+$  current was increased by the same amount as  $I_{NaL}$ , as in (Passini et al. 2016).

*Calcium Currents:*  $I_{CaL}$  formulation was left as in the ORd model, since no human Purkinje data are available in literature (Nagy et al. 2015). Based on the sensitivity analysis, some changes were made to the current kinetics: both inactivation and activation gates were shifted by +2 mV, and inactivation time constants were scaled of 30% and shifted by +15 mV (Table S1).  $I_{CaT}$  was incorporated into the model, using the formulation proposed in the PRd model. Background  $Ca^{2+}$  current ( $I_{Cab}$ ) and the sarcolemmal  $Ca^{2+}$  pump ( $I_{pCa}$ ) were left as in the ORd model.

*Other currents:*  $I_f$  was included in the model, using the formulation proposed in the PRd model.  $I_{NCX}$  and  $I_{NaK}$  were kept as in the ORd model.

## 1.2 Sensitivity Analysis

A sensitivity analysis was conducted on the initial model to investigate how the 6 criteria for

model calibration are affected by variations in the conductances of all the ionic currents ( $I_{Na}$ ,  $I_{NaL}$ ,  $I_{CaL}$ ,  $I_{CaT}$ ,  $I_{to}$ ,  $I_{sus}$ ,  $I_{Kr}$ ,  $I_{Ks}$ ,  $I_f$ ,  $I_{K1}$ ,  $I_{NCX}$ ,  $I_{NaK}$ ) and in the kinetics of  $I_{CaL}$  and  $I_{Kr}$  ( $I_{CaL}$ : steady state activation and inactivation, fast and slow inactivation time constants;  $I_{Kr}$ : fast and slow activation time constants, steady state inactivation). Each current conductance was varied from 10% to 200% of its nominal values, while specific variation ranges were defined for each current kinetics parameter (Table S1). For each value of each parameter, the protocols 1-6 were simulated to evaluate the effects of the current modulation on each of the 6 criteria used for the model design. A sensitivity analysis was also performed for the optimised model (see below, Section 1.3), varying only the current conductances. Correlation coefficients between ionic currents and AP biomarkers were computed at 1 Hz, similarly to (Romero et al. 2009). For each biomarker  $b_i$ , current conductance  $g_j$  and conductance scaling factor  $x$  the changes in respect to control ( $\Delta B_{i,j,x}$ ) and the sensitivity coefficient ( $S_{i,j}$ ) were computed as follows:

$$\Delta B_{i,j,x} = b_{i,j,x} - b_{i,j,1} \quad \begin{cases} 1 \leq i \leq 9 & AP \text{ biomarkers} \\ 1 \leq j \leq 12 & \text{conductances} \\ 0.1 \leq x \leq 2 & \text{scaling factors} \end{cases}$$

$$\Delta B_{i,MAX} = \max_{j,x} \Delta B_{i,j,x}; \quad \Delta B_{i,MIN} = \min_{j,x} \Delta B_{i,j,x};$$

$$S_{i,j} = \frac{\Delta B_{i,j,2} - \Delta B_{i,j,0.1}}{\max\{|\Delta B_{i,MAX}|; |\Delta B_{i,MIN}|\}}$$

where  $b_{i,j,x}$  is the value of biomarker  $b_i$  when  $g_j = x$ ;  $b_{i,j,1}$  is the value of biomarker  $b_i$  using the baseline model;  $\Delta B_{i,MAX}$  and  $\Delta B_{i,MIN}$  are the maximum and the minimum changes for each biomarker  $b_i$ , respectively.

### 1.3 Optimisation with a Multi-Objective Genetic Algorithm

A multi-objective genetic algorithm (Matlab function *gamultiobj*) was used for automated multi-object optimisation (Deb 2001) of the calibrated model described above. All the ionic current conductances (except for the background currents) were allowed to vary in the range [50-150]% of their nominal values, to exclude extreme up/down-regulations. The 7 kinetic parameters of  $I_{CaL}$  and  $I_{Kr}$  were allowed to vary in the ranges reported in Table S1, based on the sensitivity analysis results. The algorithm was run for 30 generations, with 300 models each. The multi-object cost function was computed as a weighted sum of 2 error functions: i) distance from the experimental mean of the AP biomarkers in control condition at 1 Hz (Dataset II, Section 2.1 in the main text); ii) a linear combination of errors, based on the criteria 2-5 described in the main text (Section 2.2) for the APD<sub>90</sub> rate-dependence, AP response to  $I_{CaL}$  and  $I_{Kr}$  modulations and EADs inducibility. At the end of each generation, the Pareto front

(Deb 2001) was computed, to identify the 35% of local minima of the cost function, i.e., the models with the best performances, then combined to create the following generation. After 30 generations, the model with best performance was chosen as the final optimised Trovato2020 model.

#### **1.4 1D Purkinje Fibre**

In order to evaluate the effects of intracellular coupling on the protocols tested (Section 2.5 in the main text), a 1D Purkinje fibre model was constructed using the Trovato2020 model to represent membrane kinetics. The 5 cm fibre was discretised in 100 nodes to obtain a spatial resolution of 500  $\mu\text{m}$ . Temporal integration step was set to 500  $\mu\text{s}$ . Both spatial and temporal resolutions were determined to guarantee the best compromise between spatial and temporal convergence errors (<10%) (Bueno-Orovio et al. 2014) and computational time for simulations. The monodomain formulation was used to simulate propagation along the fibre (Keener and Sneyd 2009) and was solved using the Fourier spectral method for fractional diffusion (Bueno-Orovio et al. 2014). The Rush-Larsen method (Rush and Larsen 1978) was implemented for the integration of the gating variables to speed up the simulations. Stimulus duration was set to 2.2 ms, i.e. twice the minimum value to achieve propagation in the fibre. The fibre was stimulated on one side for 1 mm. For each protocol tested, three beats were simulated in the fibre, to allow relaxation from the initial conditions (all the nodes were initialised to the SS computed at cellular level). APD<sub>90</sub> and CV were computed for the last beat. CV was computed at the centre of the fibre, to avoid border effects, as the distance between the 17 central nodes (set to 0.26 cm), divided by the difference of activation times (identified as the instant with maximum  $dV/dt$ ) at the border nodes.

Diffusion coefficient was set to 9  $\text{cm}^2/\text{s}$  to match the CV of 1.6 m/s computed from observations at sinus rhythm in human Purkinje fibres (Kupersmith et al. 1973, Durrer et al. 1970). Protocols 1, 5, 6 and 8 (Section 2.5) were simulated in fibre. In addition, effects of  $I_{\text{Na}}$  blocks on the CV were considered, modifying the protocol used for hERG-blocks.  $I_{\text{Na}}$  was reduced up to 100%, or until propagation failure was observed.

## 2 - Supplementary Tables

**Table S1.** Parameters and ranges to perform the sensitivity analysis and to optimise the calibrated model through multi-object genetic algorithm

	Sensitivity analysis range		Calibrated model Pre-optimisation Coefficients	Optimisation Range		Final Model Post-optimisation Coefficients
	Min	Max		Min	Max	
<i>Conductances</i>						
<b>G<sub>Na</sub></b>	[10 ; 200] %		1	[50 ; 150] %		<b>0.75</b>
<b>G<sub>NaL</sub></b>			2.5*			<b>1</b>
<b>G<sub>CaL</sub></b>			1			<b>0.75</b>
<b>G<sub>CaT</sub></b>			1			<b>0.96</b>
<b>G<sub>to</sub></b>			1			<b>0.93</b>
<b>G<sub>sus</sub></b>			1			<b>1.28</b>
<b>G<sub>Kr</sub></b>			1			<b>0.93</b>
<b>G<sub>Ks</sub></b>			1			<b>0.84</b>
<b>G<sub>f</sub></b>			1			<b>0.97</b>
<b>G<sub>K1</sub></b>			1			<b>0.67</b>
<b>G<sub>NCX</sub></b>			1			<b>1.2</b>
<b>G<sub>NaK</sub></b>			1			<b>1.1</b>
<i>I<sub>CaL</sub> Kinetics</i>						
<b>Activation/ Inactivation V shift (mV)</b>	-4	4	2	0	4	<b>3.3</b>
<b>Time constants V shift (mV)</b>	-10	30	15	10	20	<b>15.2</b>
<b>Slow time constants scales</b>	0.1	3	0.7	0.4	1	<b>0.49</b>
<b>Fast time constants scales</b>	0.1	3	0.7	0.4	1	<b>0.72</b>
<i>I<sub>Kr</sub> Kinetics</i>						
<b>Fast time constant V shift (mV)</b>	[-10 ; 30] mV		15	10	20	<b>17.6</b>
<b>Slow time constant V shift (mV)</b>	[-10 ; 30] mV		15	10	20	<b>17.2</b>
<b>Inactivation slope</b>	[0.3 ; 3]]		0.3	0.1	0.5	<b>0.32</b>

Varied parameters (1<sup>st</sup> column). Ranges investigated via sensitivity analysis (2<sup>nd</sup> & 3<sup>rd</sup> columns). Conductances scaling factors and kinetics coefficients for the calibrated model (4<sup>th</sup> column). Optimisation ranges for the multi-object genetic algorithm (5<sup>th</sup> & 6<sup>th</sup> columns). Conductances scaling factors and kinetics coefficients for the final model are reported in bold (7<sup>th</sup> column). \*from (Iyer et al., 2015).



**Table S2.** Normalised relative correlation coefficients for each ionic current and simulated AP biomarker at 1 Hz.

	$I_{Na}$	$I_{NaL}$	$I_{CaL}$	$I_{CaT}$	$I_{to}$	$I_{sus}$	$I_{Kr}$	$I_{Ks}$	$I_f$	$I_{K1}$	$I_{NCX}$	$I_{NaK}$
$\frac{dV}{dt}$ (V/s)	<b>1.0</b>								-0.1	0.1		0.2
APD <sub>90</sub>		0.4				<b>-0.6</b>	<b>-1.0</b>			-0.1	0.3	
APD <sub>75</sub>		0.4				<b>-0.6</b>	<b>-1.0</b>				0.3	
APD <sub>50</sub>	-0.1	0.5	0.1			<b>-0.8</b>	<b>-1.0</b>				0.4	
APD <sub>25</sub>	-0.2	0.4	0.3			<b>-1.0</b>	-0.3				0.4	0.1
APD <sub>10</sub>	-0.5	0.3	0.4		-0.2	<b>-1.0</b>						
APA	<b>1.0</b>	0.1	0.4		-0.4	<b>-0.9</b>	-0.2		-0.3	0.3	0.1	0.4
TOP		-0.1	-0.2			0.2	0.5		<b>1.0</b>	<b>-1.0</b>	-0.5	<b>-0.8</b>
EOP		-0.1	-0.2			0.3	0.4		<b>1.0</b>	<b>-1.0</b>	-0.5	<b>-0.8</b>

Values bigger than 0.60 are highlighted in bold. Values smaller than 0.1 are not shown. The upstroke velocity is set by the  $I_{Na}$  and, to a lesser extent, by  $I_f$ ,  $I_{K1}$ , and  $I_{NaK}$ . The APD at late stages of repolarisation, 50-75-90%, is determined by the contribution of different currents:  $I_{NaL}$  and the  $I_{NCX}$  prolong the AP;  $I_{sus}$  and  $I_{Kr}$  shorten it. At the early phase of repolarisation, APD at 10-25%, the effects of  $I_{NaL}$  and  $I_{Kr}$  are reduced, whereas,  $I_{Na}$  and  $I_{CaL}$  play a more relevant role in setting the APD. Both  $I_{Na}$  and  $I_{CaL}$  increase the AP amplitude whereas  $I_{to}$  and  $I_{sus}$  reduce it.  $I_{NaK}$  and, to a lesser extent,  $I_{K1}$  and  $I_f$  affect the APA indirectly, since they affect the membrane resting potential. The major currents responsible for the membrane repolarisation are,  $I_{K1}$  and  $I_{NaK}$ , whereas  $I_f$  depolarises the cell during the diastolic interval. No relevant changes were induced by the modulation of  $I_{Ks}$  and  $I_{CaT}$ .

**Table S3.** Comparison between experimental and simulated AP biomarkers with different cardiac models at 1Hz

BIOMARKER	EXPERIMENTS	TROVATO 2020	STW	TT08	ORD	PRD
$\frac{dV}{dt}$ (V/s)	387 ± 143	381	522	742	264	527
APD <sub>90</sub> (ms)	294 ± 76	306	285	374	268	527
APD <sub>75</sub> (ms)	261 ± 67	280	254	364	248	328
APD <sub>50</sub> (ms)	210 ± 52	224	197	330	208	208
APD <sub>25</sub> (ms)	117 ± 46	143	13	209	167	31
APD <sub>10</sub> (ms)	33 ± 35	34	4	3	74	2
APA (mV)	106 ± 7	110	120	146	128	134
TOP (mV)	-85 ± 2.4	-86.5	-74.0	-86.0	-87.8	-84.1
EOP (mV)	-86 ± 2	-87.3	-77.3	-86.0	-88.0	-84.9

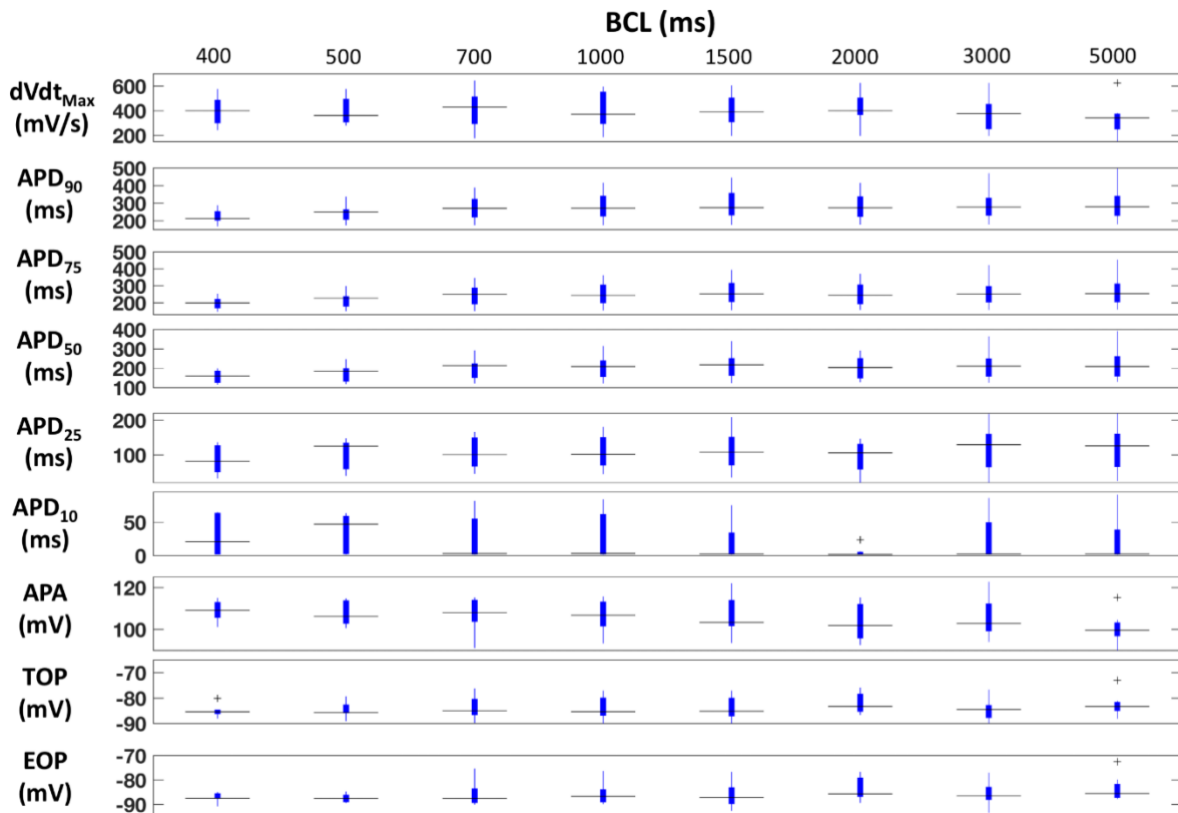
**dV/dt<sub>MAX</sub>**: maximum depolarisation rate; **APD<sub>x</sub>**: AP Duration at X% of repolarisation; **APA**: action potential amplitude; **TOP**: take-off potential, voltage level before depolarisation; **EOP**: end of potential, voltage level at the end of repolarisation. **STW**: Stewarts et al. 2009 model; **TT08**: ten Tusscher et al 2008 model; **ORD**: O’Hara et al 2011 model; **PRd**: Pan Li & Rudy 2011 model.

**Table S4.** Effects of simulated  $I_{Na}$  block on the maximum depolarisation velocity and conduction velocity in Purkinje cell and fibre using the Trovato2020 model.

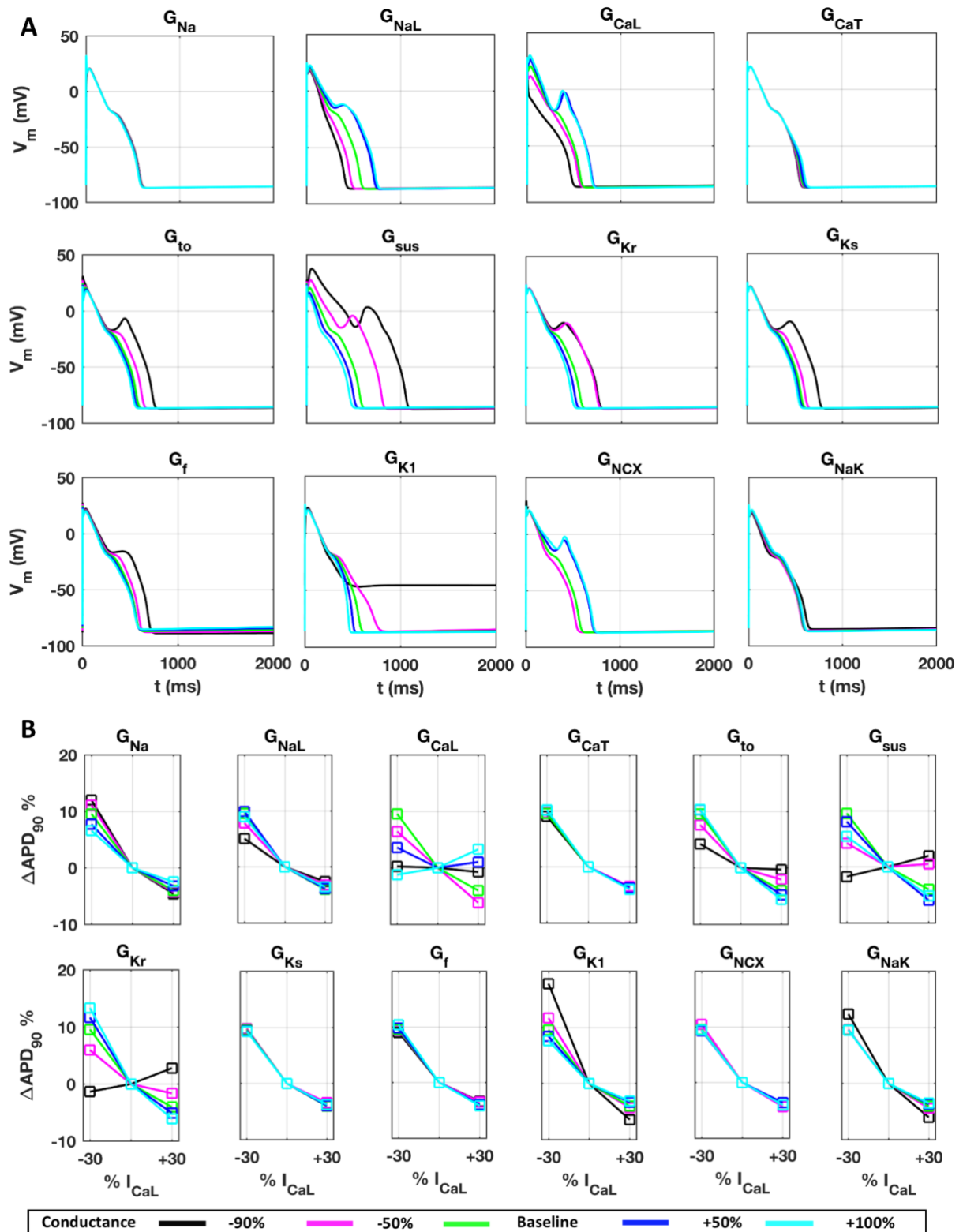
	SINGLE CELL		FIBRE	
$I_{Na}$ block	$\frac{dV}{dt}_{Max}$ (V/s)	AP Inducibility	CV (cm/s)	AP propagation
<b>Control (No Block)</b>	380	Yes, Na <sup>+</sup> driven	160	Yes
<b>30%</b>	315	Yes, Na <sup>+</sup> driven	147	Yes
<b>50%</b>	260	Yes, Na <sup>+</sup> driven	136	Yes
<b>90%</b>	92	Yes, Na <sup>+</sup> driven	88	Yes
<b>95%</b>	44	Yes, Na <sup>+</sup> driven	69	Yes
<b>100%</b>	40	Yes, Ca <sup>2+</sup> driven	-	No

$\frac{dV}{dt}_{Max}$ : maximum depolarisation rate computed in single cell; CV: conduction velocity computed in a 5 cm 1D fibre.

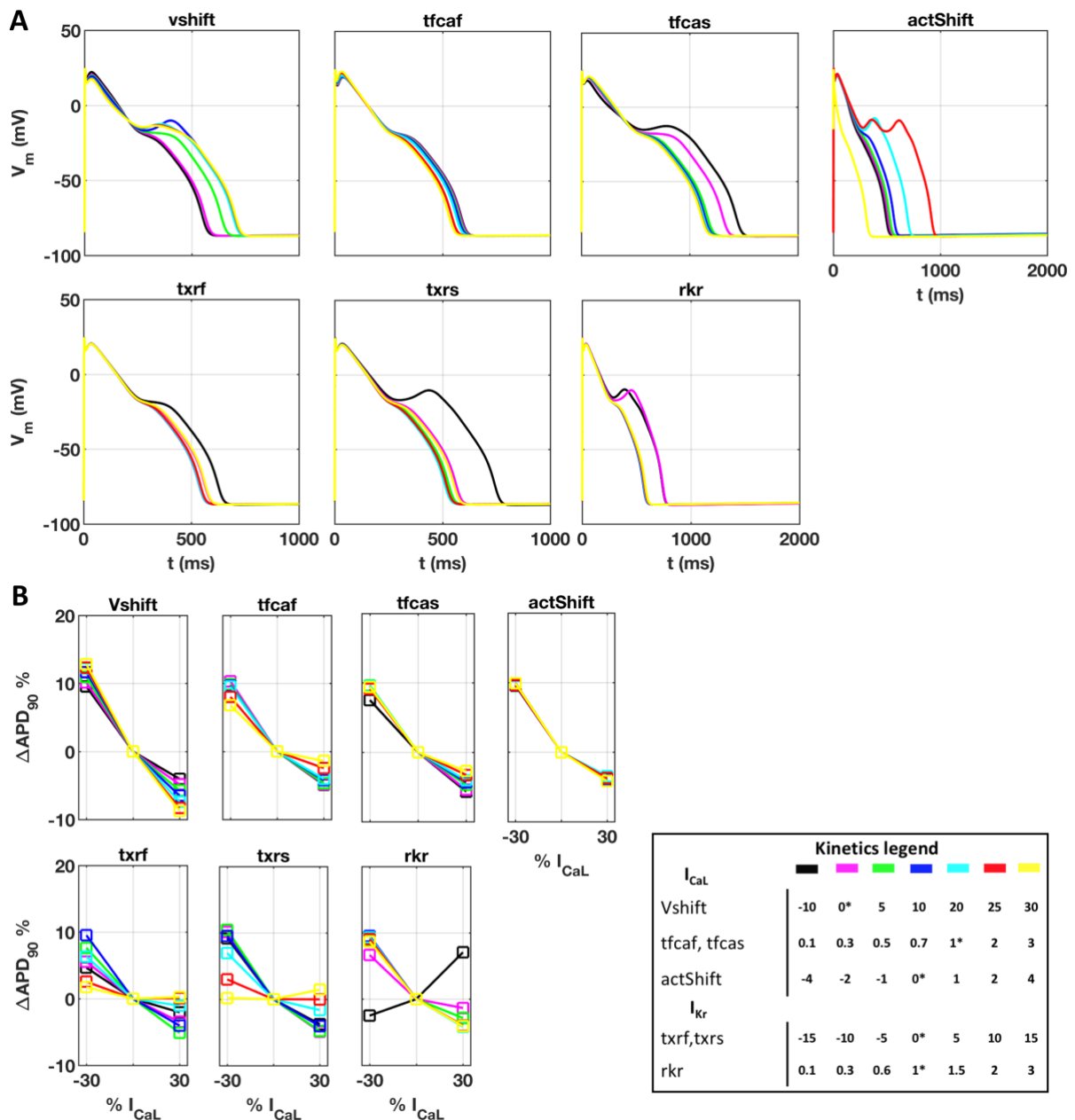
### 3 - Supplementary Figures



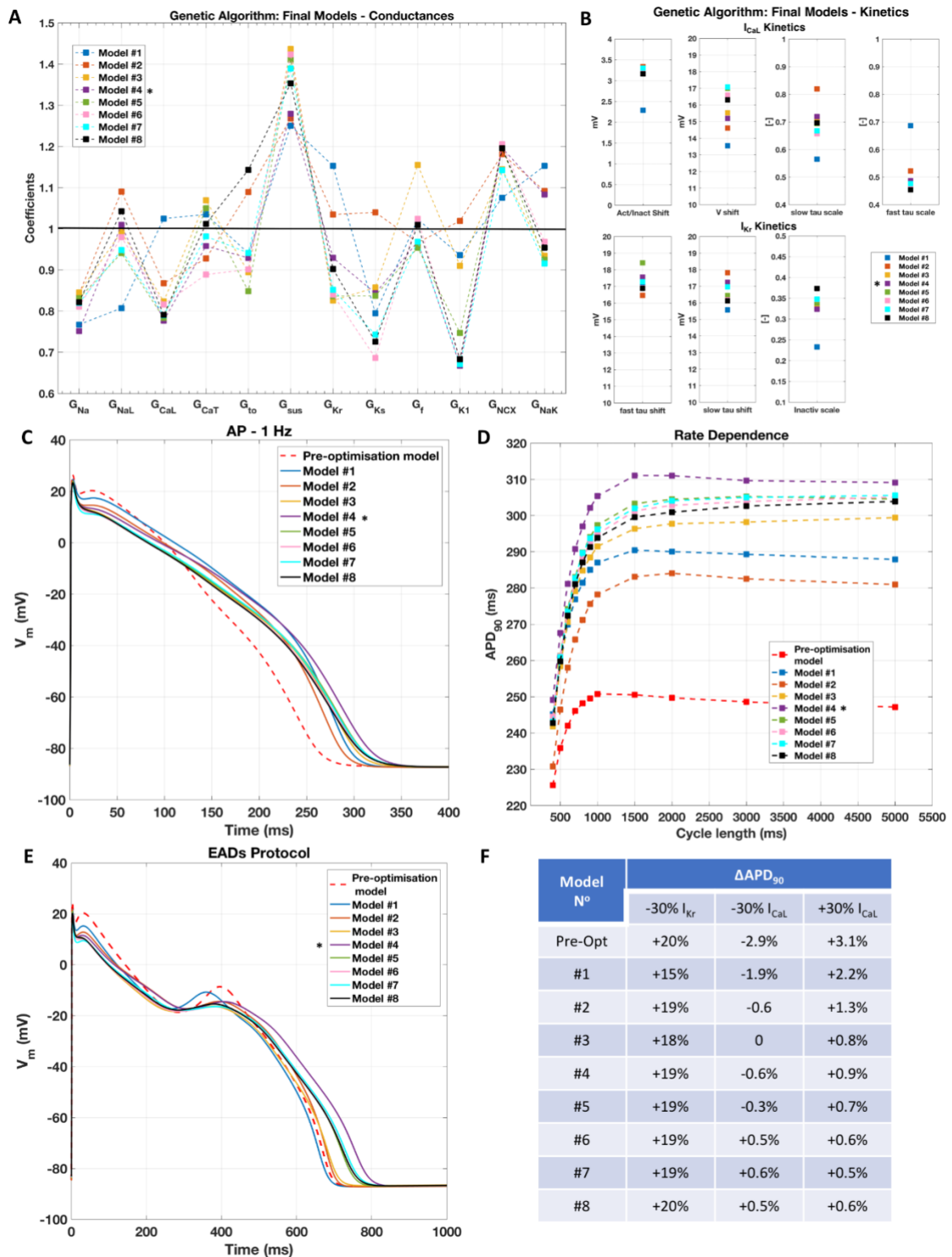
**Figure S1.** Overview of Dataset II. BCL: basic cycle length.  $dV/dt_{MAX}$ : maximum depolarisation rate;  $APD_x$ : AP Duration at X% of repolarisation; APA: action potential amplitude; TOP: take-off potential, voltage level before depolarisation; EOP: end of potential, voltage level at the end of repolarisation.



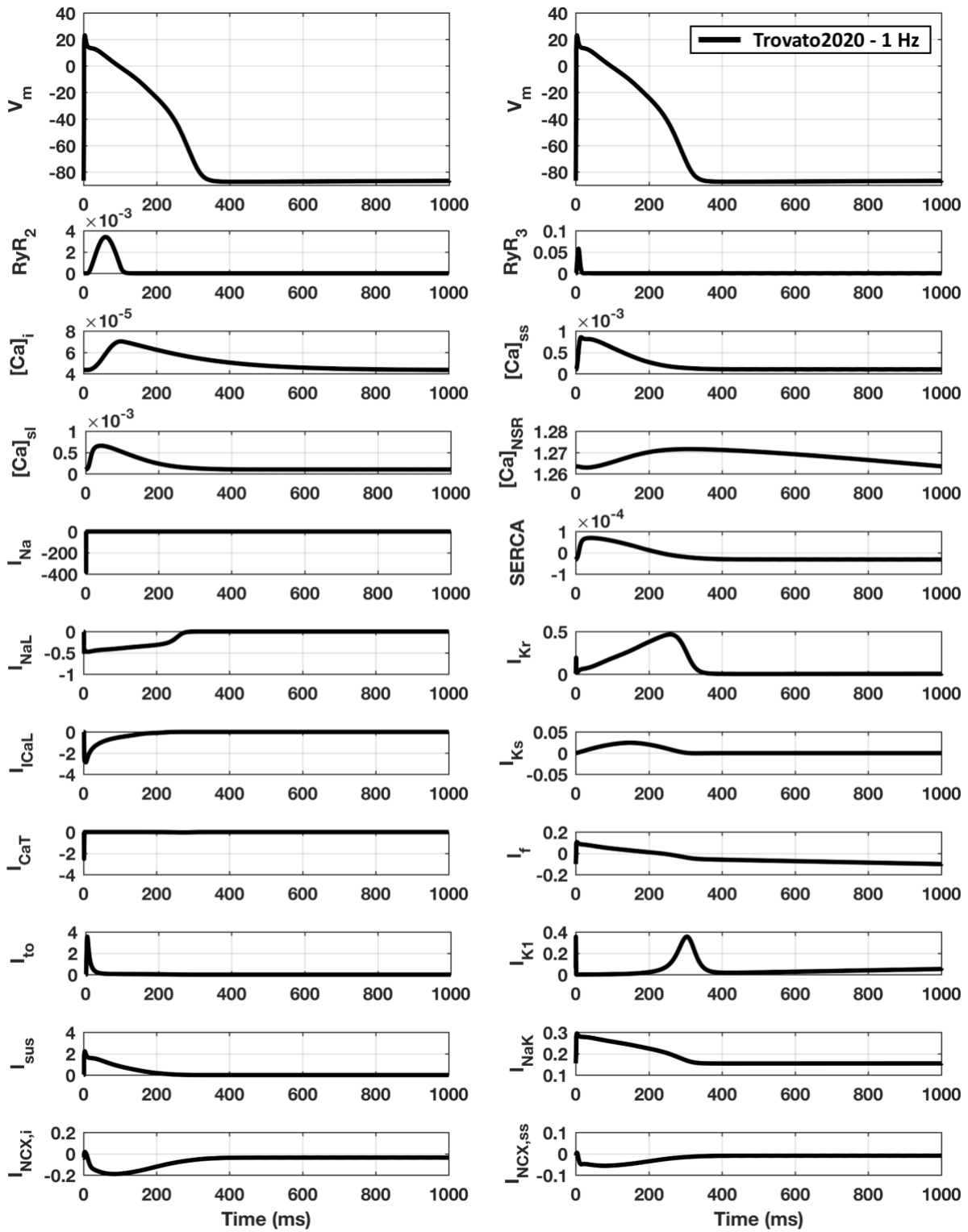
**Figure S2.** Sensitivity analysis performed on the initial model varying current conductances as reported in Table S1. Investigation of each current contribution in EADs inducibility and APD<sub>90</sub> response to  $I_{CaL}$  modulations. The legend indicates the percentage of modulation for each conductance. A) Simulated APs following Protocol 5 for EADs inducibility. B) Percentual changes in the APD<sub>90</sub> following Protocol 3 in response to  $I_{CaL}$  conductance changes ( $\pm 30\%$ ).



**Figure S3.** Sensitivity analysis performed on the initial model, varying  $I_{Kr}$  and  $I_{CaL}$  kinetics, as reported in the legend and in Table S1. Investigation of each current contribution in EADs inducibility and APD<sub>90</sub> response to  $I_{CaL}$  modulations. A) Simulated APs following Protocol 5 for EADs inducibility. B) Percentual changes in the APD<sub>90</sub> following Protocol 3 in response to  $I_{CaL}$  changes ( $\pm 30\%$ ). \*Nominal value for the initial model.

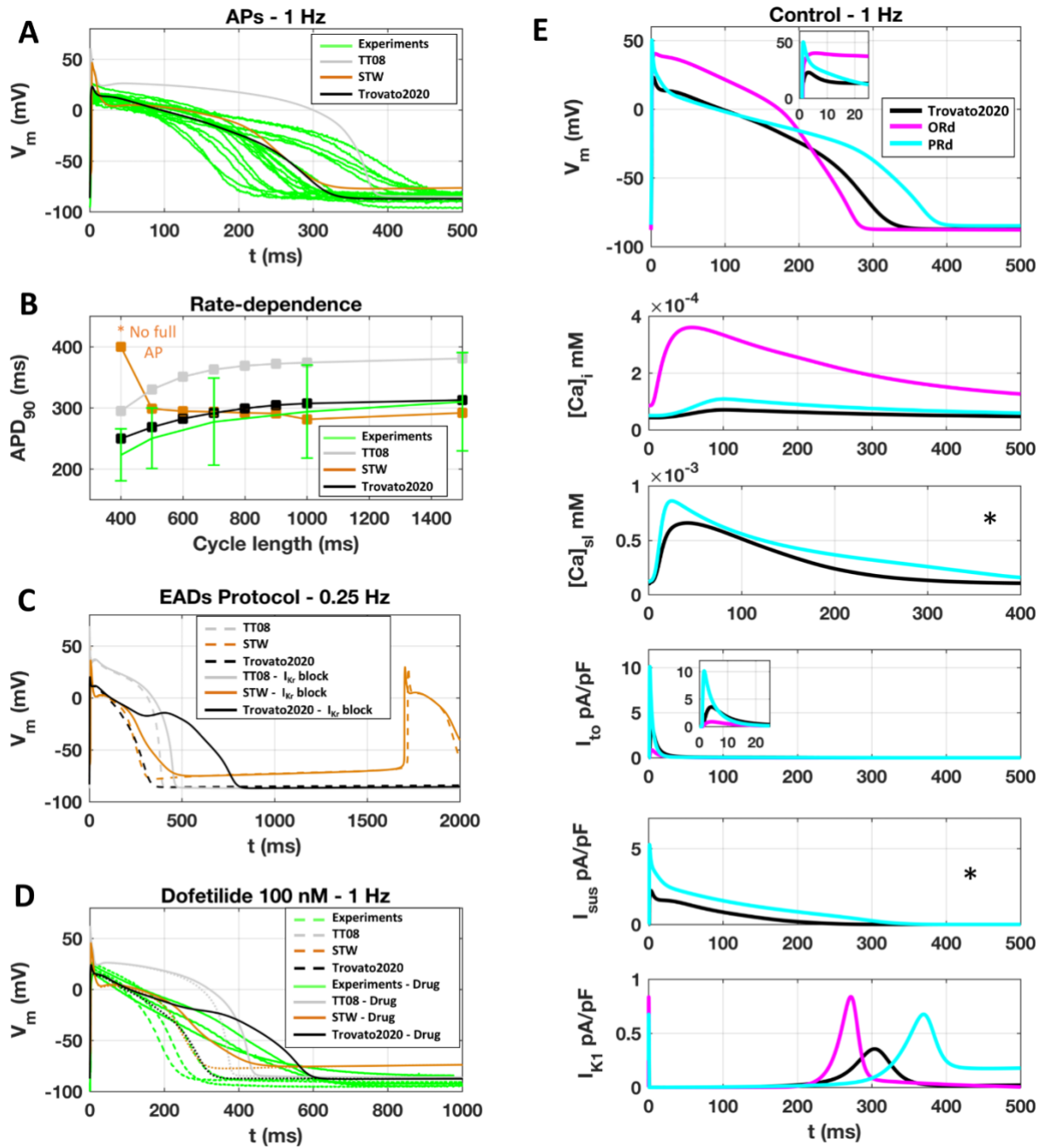


**Figure S4.** Models obtained through optimisation with the multi-objective genetic algorithm. Parameter set for the 8 final models for: A) current conductances B)  $I_{CaL}$  and  $I_{Kr}$  kinetics. Ranges are definite as in Table S1. C) Simulated APs at 1 Hz. D)  $APD_{90}$  rate dependence. E) Simulated APs to induce EADs. F)  $APD_{90}$  changes induced by  $I_{Kr}$  block or  $I_{CaL}$  modulation. \*Final Trovato2020 model.

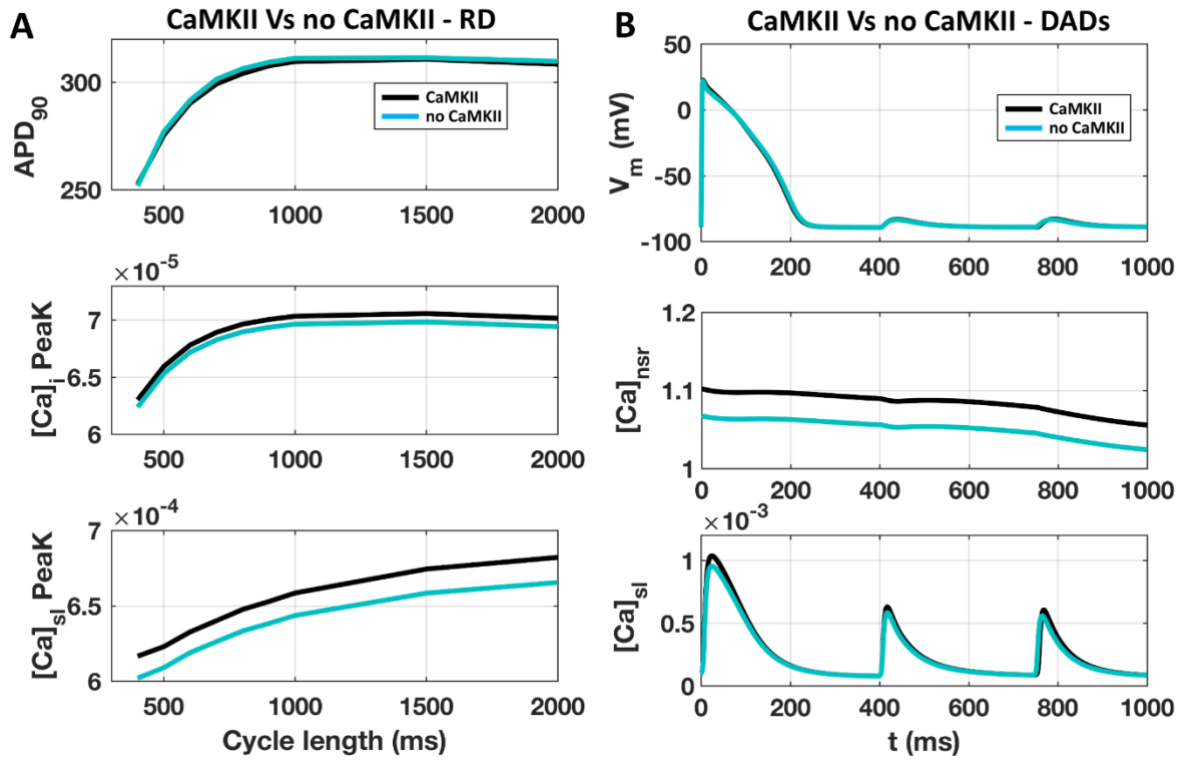


**Figure S5.** The new Trovato2020 model: simulated AP at 1 Hz in control condition, with the underlying ionic currents, pumps, exchangers, intracellular  $\text{Ca}^{2+}$  concentrations and fluxes.

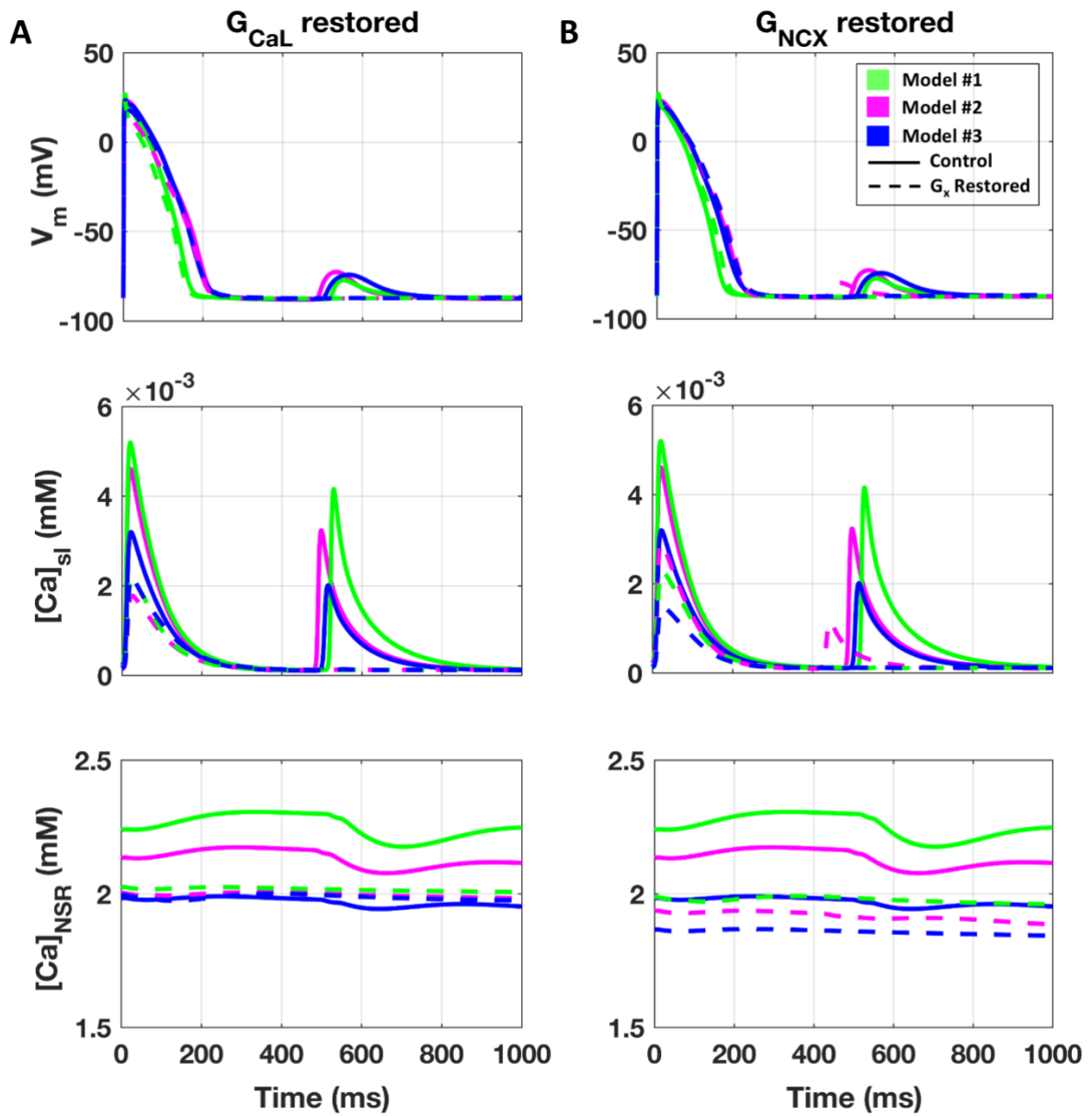




**Figure S6.** Comparison of different cardiomyocytes models. A) Human Purkinje: TT08 in grey (ten Tusscher and Panfilov 2008), STW in orange (Stewart et al. 2009), the new Trovato2020 model (black) and experiments (green). APs comparison at 1 Hz in control; B) APD90 rate-dependence; C) EADs protocol: 85%  $I_{Kr}$  block, pacing at BCL=4000 ms. Control (dash line), AP with  $I_{Kr}$  block (solid line); D) AP response to Dofetilide 100 nM: control (dash line), AP with Dofetilide (solid line). E) APs, intracellular and submembrane  $[Ca^{2+}]_i$ , and refitted  $K^+$  currents,  $I_{to}$ ,  $I_{K1}$ ,  $I_{sus}$  for Trovato2020 (black), ORd (O’Hara et al. 2011, pink) and PRd (Li and Rudy 2011, light blue) models. \*Not implemented into ORd.



**Figure S7.** Effects of CaMKII signalling on the Trovato2020 model: control (black) and no CaMKII signalling (light blue). A) APD<sub>90</sub> rate-dependence, [Ca<sup>2+</sup>]<sub>i</sub> and [Ca<sup>2+</sup>]<sub>sl</sub> peaks. B) DADs protocol, fast pacing with RyR hypersensitivity.



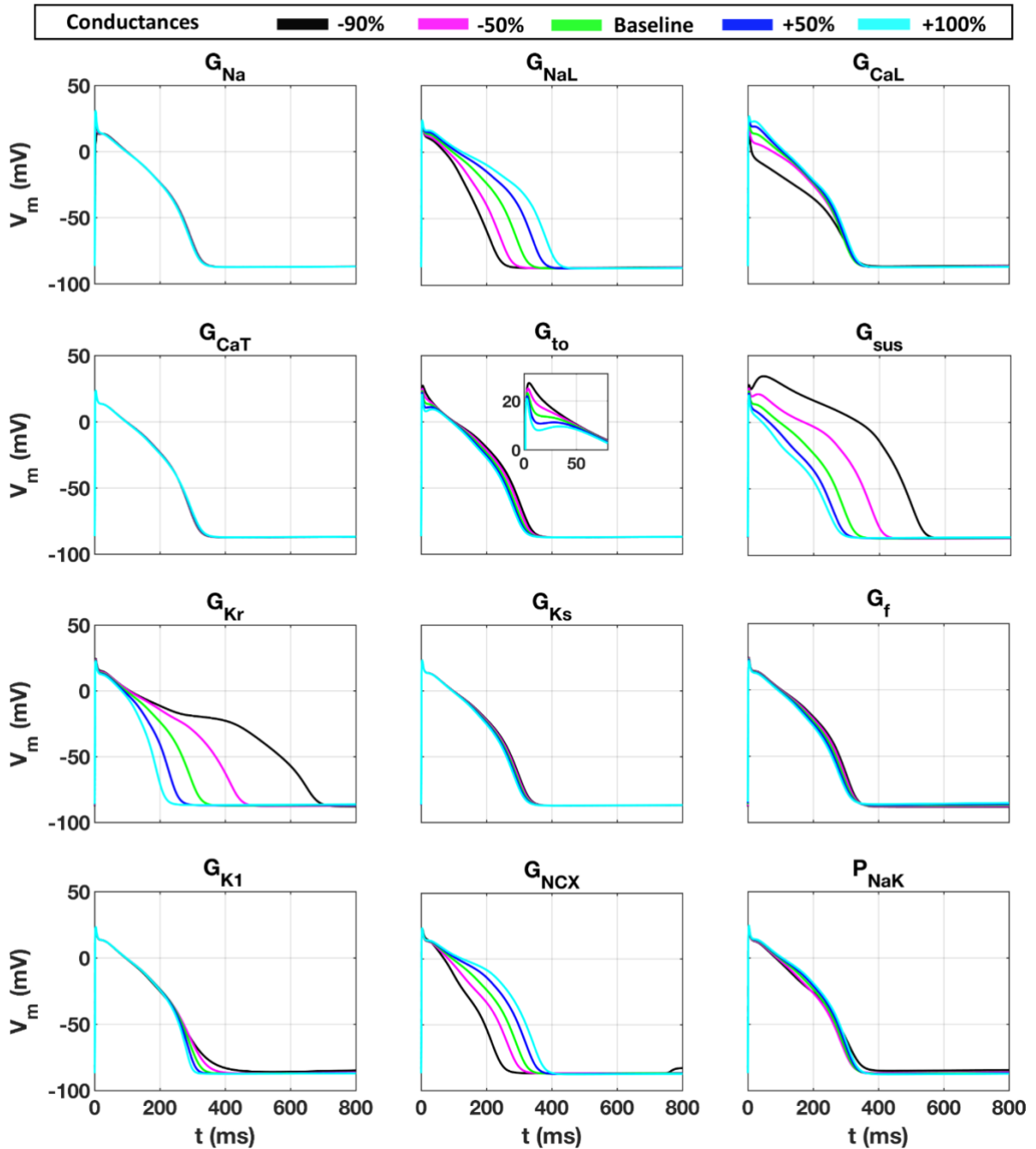
**Figure S8.** Simulated APs,  $[Ca^{2+}]_{SL}$  and  $[Ca^{2+}]_{NSR}$  for a selection of 3 models (green, pink and blue traces) from the population producing DADs, in control (solid line) and with selective conductance restored to the corresponding baseline value (dashed line): A)  $G_{CaL}$ ; B)  $G_{NCX}$ ;

## *4 - Sensitivity Analysis*

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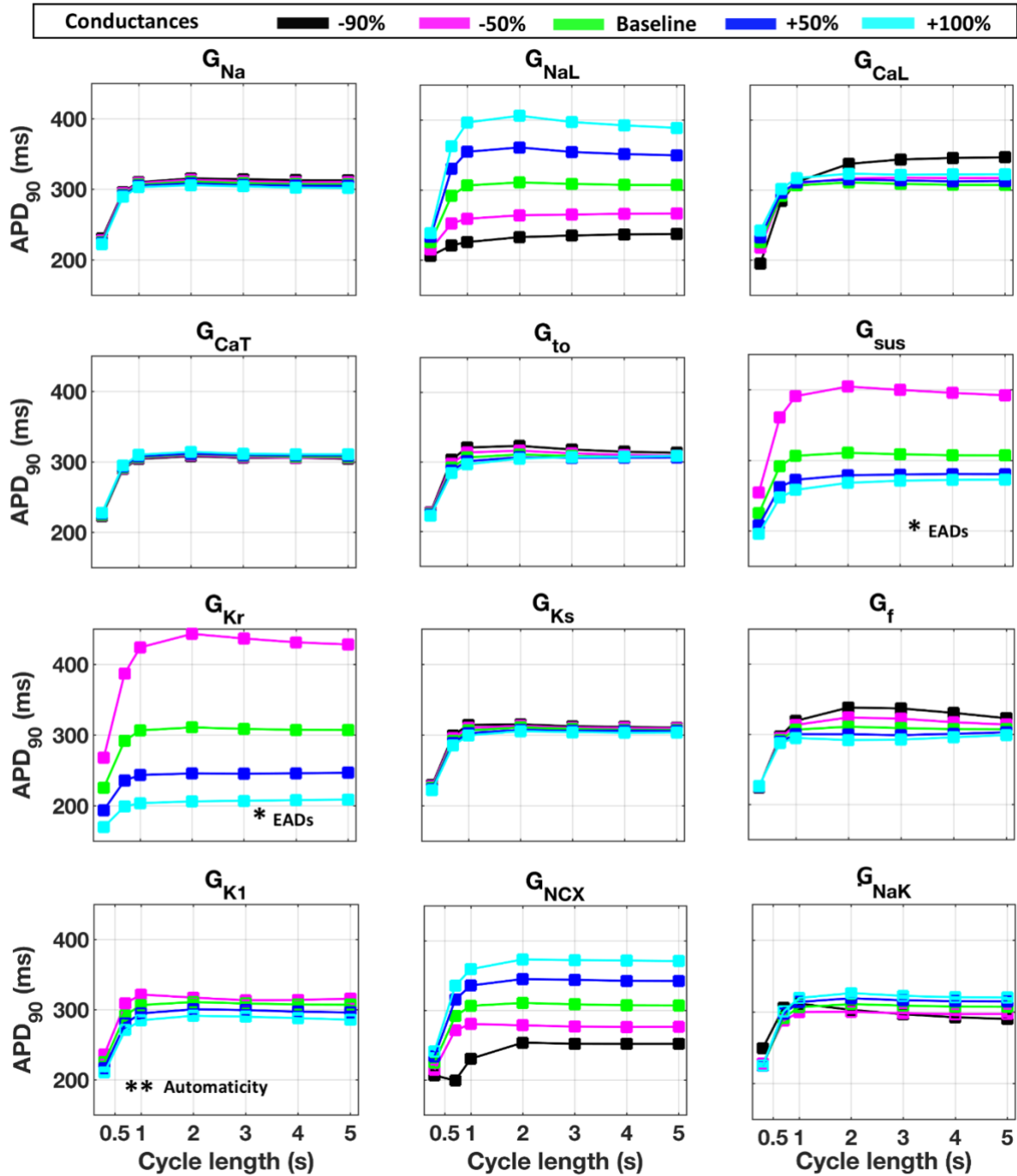
**Optimised model  
Trovato2020**

## Control – 1 Hz



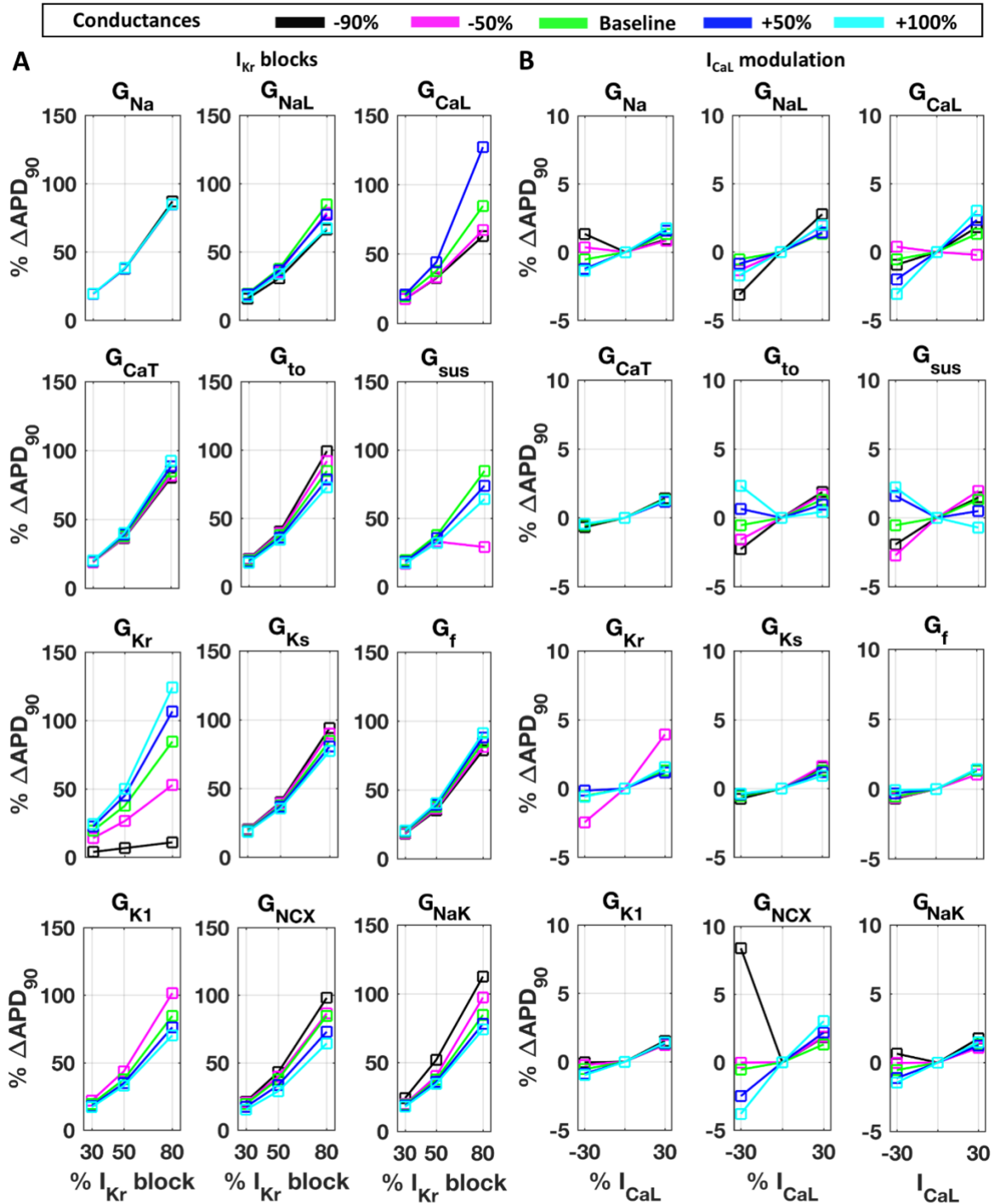
**Figure SA1.** Single current conductances modulation: simulated APs of the optimised new Trovato2020 model, following Protocol 1 for each changed conductance in the range [0.1 - 2]% of their nominal value (Table S1).

# APD<sub>90</sub> – Rate dependence



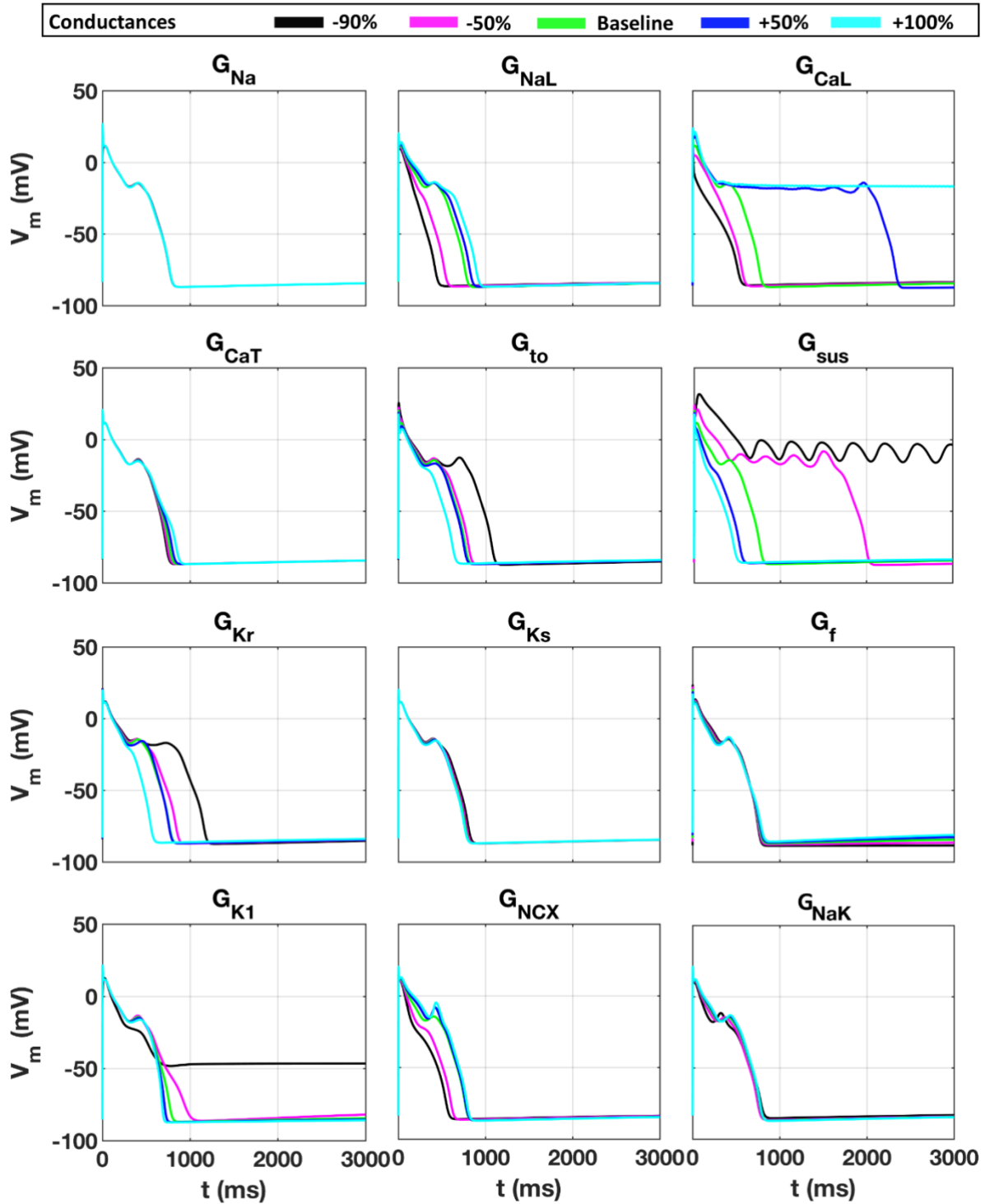
**Figure SA2.** Simulation of the APD<sub>90</sub> rate-dependence behaviour in response to single current conductances modulation in the range [0.1 - 2]% of their nominal value (Table S1) using the optimised new Trovato2020 model. \*EAD were induced in case of slow pacing rate with  $I_{sus}$  and  $I_{Kr}$  downregulation (-90%). \*\*Automaticity was observed at slow pacing rate with  $I_{K1}$  downregulation (-90%).

# $I_{Kr}$ blocks and $I_{CaL}$ modulation



**Figure SA3.** Simulated AP responses to selective channel blockers at different concentrations and conductances modulation in the range [0.1 - 2]% of their nominal value (Table S1) using the optimised Trovato2020 model: A)  $I_{Kr}$  block at 30%, 50% and 80%; B)  $\pm 30\%$   $I_{CaL}$  modulation.

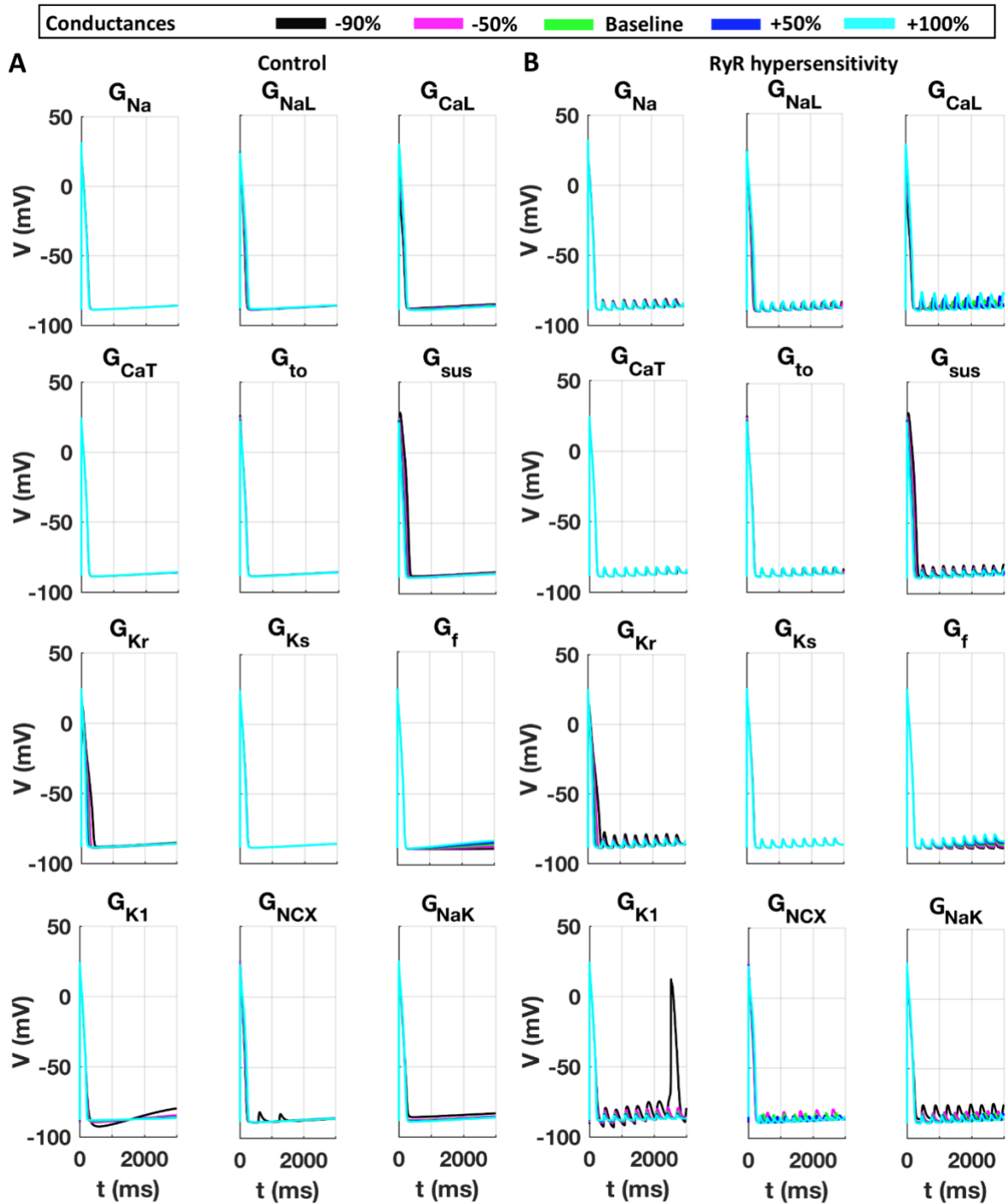
# EADs Protocol



**Figure SA4.** Simulated APs at slow pacing and with 85%  $I_{Kr}$  block and selective conductances modulation in the range [0.1 - 2]% of their nominal value (Table S1) using the optimised new Trovato2020 model. EADs are enhanced by increased  $I_{CaL}$ ,  $I_{NaL}$ , or  $I_{NCX}$  and reduced  $I_{to}$ ,  $I_{sus}$ , or  $I_{Kr}$ , while modulation of the other currents ( $I_{Na}$ ,  $I_{CaT}$ ,  $I_{Ks}$ ,  $I_f$ ,  $I_{K1}$  and  $I_{NaK}$ ) do not seem to play a significant role.



# DADs - 3.3 Hz



**Figure SA5.** Simulated APs at fast pacing in control (A) and with RyR hypersensitivity (B) and selective conductances modulation in the range [0.1 - 2]% of their nominal value (Table S1) using the optimised new Trovato2020 model. In control, DADs were observed only with high  $I_{NCX}$  downregulation and in every case when including RyR hypersensitivity.

## 5 - Model Parameters and Equations

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### Stimulus

$$\text{Amplitude } I_{\text{stim}} = -40 \frac{\mu A}{\mu F} \quad \text{Duration} = 1 \text{ms.}$$

### Extracellular Concentrations

$$[\text{Na}^+]_o = 140 \text{ mM}; \quad [\text{Ca}^{2+}]_o = 1.8 \text{ mM}; \quad [\text{K}^+]_o = 5.4 \text{ mM}$$

### Cell Geometry

$$L = 0.0164 \text{ cm}$$

$$r = 0.00175 \text{ cm}$$

$$A_{\text{geo}} = 2\pi \cdot r^2 + 2\pi \cdot r \cdot L = 2 \cdot 10^{-4} \text{ cm}^2$$

$$A_{\text{cap}} = 2 \cdot A_{\text{geo}} = 4 \cdot 10^{-4} \mu\text{L}$$

$$v_{\text{cell}} = \pi \cdot r^2 \cdot L = 16 \cdot 10^{-5} \mu\text{L}$$

$$v_{\text{myo}} = 0.6 \cdot v_{\text{cell}} = 9.5 \cdot 10^{-5} \mu\text{L}$$

$$v_{\text{nsr}} = 0.04 \cdot v_{\text{cell}} = 6.3 \cdot 10^{-6} \mu\text{L}$$

$$v_{\text{ss}} = 0.02 \cdot v_{\text{cell}} = 3.1 \cdot 10^{-6} \mu\text{L}$$

$$v_{\text{jsr}} = 0.002 \cdot v_{\text{cell}} = 3.1 \cdot 10^{-7} \mu\text{L}$$

$$v_{\text{sl}} = 0.15 \cdot v_{\text{cell}} = 2.4 \cdot 10^{-5} \mu\text{L}$$

$$v_{\text{csr}} = 0.008 \cdot v_{\text{cell}} = 1.3 \cdot 10^{-6} \mu\text{L}$$

### Steady State conditions at 1Hz (after 1000 beats)

1 V = 86.55;	j = 0.8;	ffp = 1;
2 $[\text{Na}^+]_i = 8.23$ ;	hsp = 0.6 ;	fcafp = 1;
3 $[\text{Na}^+]_{\text{SL}} = 8.23$ ;	jp = 0.8;	b = 0;
4 $[\text{Na}^+]_{\text{SS}} = 8.23$ ;	mL = 0;	g = 1;
5 $[\text{K}^+]_i = 144$ ;	hL = 0.5;	xrf = 0;
6 $[\text{K}^+]_{\text{SL}} = 144$ ;	hLp = 0.2;	xrs = 0.6;
7 $[\text{K}^+]_{\text{SS}} = 144$ ;	a = 0;	xs1 = 0.2;
8 $[\text{Ca}^{2+}]_i = 4.36 \cdot 10^{-5}$ ;	i = 0.6;	xs2 = 0;
9 $[\text{Ca}^{2+}]_{\text{SL}} = 1.0 \cdot 10^{-4}$ ;	i2 = 1;	xk1 = 1;
10 $[\text{Ca}^{2+}]_{\text{SS}} = 1 \cdot 10^{-4}$ ;	d = 0;	y = 0.2;
11 $[\text{Ca}^{2+}]_{\text{JSR}} = 1.25$ ;	ff = 1;	CaMkt = 0;
12 $[\text{Ca}^{2+}]_{\text{NSR}} = 1.27$ ;	fs = 1;	u = 0.5;
13 $[\text{Ca}^{2+}]_{\text{CSR}} = 1.27$ ;	fcaf = 1;	Jrel1 = 0;
14 m = 0;	fcas = 1;	Jrel2 = 0;
15 hf = 0.8;	jca = 1;	
16 hs = 0.8 ;	nca = 0;	

Maximum Current Conductances (mS/ $\mu$ F)

<b>G<sub>Na</sub></b>	39.46
<b>G<sub>NaL</sub></b>	0.0189
<b>G<sub>CaL</sub></b>	7.7677e-05
<b>G<sub>CaT</sub></b>	0.0754
<b>G<sub>to</sub></b>	0.192
<b>G<sub>sus</sub></b>	0.0301
<b>G<sub>Kr</sub></b>	0.0342
<b>G<sub>Ks</sub></b>	0.0029
<b>G<sub>fNa</sub></b>	0.0116
<b>G<sub>fK</sub></b>	0.0232
<b>G<sub>K1</sub></b>	0.0455
<b>G<sub>NaK</sub></b>	32.4872
<b>G<sub>NCX</sub></b>	9.5709e-04

Calcium Buffer Constants

<b>BSR<sub>MAX</sub></b>	0.019975
<b>K<sub>mBSR</sub></b>	0.00087
<b>BSL<sub>MAX</sub></b>	0.4777
<b>K<sub>mBSL</sub></b>	0.0087
<b>CSQN<sub>MAX,CSR</sub></b>	2.88
<b>CSQN<sub>MAX,JSR</sub></b>	1.2
<b>K<sub>mCSQN</sub></b>	0.8
<b>CMDN<sub>MAX,i</sub></b>	0.1125
<b>CMDN<sub>MAX,sl</sub></b>	1.25e-2
<b>K<sub>mCMDN</sub></b>	0.00238
<b>TRPN<sub>MAX,i</sub></b>	3.15e-2
<b>TRPN<sub>MAX,SL</sub></b>	3.5e-3
<b>K<sub>mTRPN</sub></b>	0.0005

## Voltage

$$C_m \frac{dV}{dt} = -(I_{ion} + I_{stim})$$

$$I_{ion} = I_{Na} + I_{NaL} + I_{to} + I_{sus} + I_{CaL} + I_{CaT} + I_{CaNa} + I_{CaK} + I_{Kr} + I_{Ks} + I_f + I_{K1} + I_{NaCa} + I_{NaK} \\ + I_{Nab} + I_{Cab} + I_{pCa} + I_{stim}$$

### Fast-Sodium Current ( $I_{Na}$ )

from (Dutta et al. 2017; Passini et al. 2016)

$$m_{\infty} = \frac{1}{1 + e^{-\left(\frac{V+48.6264}{9.871}\right)}}$$

$$\tau_m = \frac{1}{6.755 \cdot e^{\left(\frac{V+11.64}{34.77}\right)} + 8.552 \cdot e^{-\left(\frac{V+77.42}{5.955}\right)}}$$

$$h_{\infty} = \frac{1}{1 + e^{\left(\frac{V+78.5}{6.22}\right)}}$$

$$\tau_{h,fast} = \frac{1}{3.686 \cdot 10^{-6} \cdot e^{-\left(\frac{V+3.8875}{7.8579}\right)} + 16 \cdot e^{\left(\frac{V-0.4963}{9.1843}\right)}}$$

$$\tau_{h,slow} = \frac{1}{0.009764 \cdot e^{-\left(\frac{V+17.95}{28.05}\right)} + 0.3343 \cdot e^{\left(\frac{V+5.730}{56.66}\right)}}$$

$$A_{h,fast} = 0.99, \quad A_{h,slow} = 1 - A_{h,fast}$$

$$h = A_{h,fast} \cdot h_{fast} + A_{h,slow} \cdot h_{slow}$$

$$j_{\infty} = h_{\infty}$$

$$\tau_j = 4.8590 + \frac{1}{0.8628 \cdot e^{-\left(\frac{V+166.7}{7.6}\right)} + 1.1096 \cdot e^{\left(\frac{V+6.2719}{9.0358}\right)}}$$

$$h_{CaMK,\infty} = \frac{1}{1 + e^{\left(\frac{V+84.7}{6.22}\right)}}$$

$$\tau_{h,CaMK,slow} = 3 \cdot \tau_{h,slow}$$

$$A_{h,CaMK,fast} = A_{h,fast}$$

$$A_{h,CaMK,slow} = A_{h,slow}$$

$$h_{CaMK,\infty} = h_{fast}$$

$$h_{CaMK} = A_{h,CaMK,fast} \cdot h_{CaMK,fast} + A_{h,CaMK,slow} \cdot h_{CaMK,slow}$$

$$j_{CaMK,\infty} = j_{\infty}$$

$$\tau_{j,CaMK} = 1.46 \cdot \tau_j$$

$$K_{m,CaMK} = 0.15,$$

$$\phi_{INa,CaMK} = \frac{1}{1 + \frac{K_{m,CaMK}}{K_{m,CaMK,active}}}$$

$$I_{Na,fast} = G_{Na} \cdot (V - E_{Na}) \cdot m^3 \cdot ((1 - \phi_{INa,CaMK}) \cdot h \cdot j + \phi_{INa,CaMK} \cdot h_{CaMK} \cdot j_{CaMK})$$

### Late-Sodium Current ( $I_{NaL}$ )

from (O'Hara et al. 2011)

$$m_{L,\infty} = \frac{1}{1 + e^{-\left(\frac{V+42.85}{5.264}\right)}}$$

$$\tau_{m,L} = \tau_m$$

$$h_{L,\infty} = \frac{1}{1 + e^{-\left(\frac{V+87.61}{7.488}\right)}}$$

$$\tau_{h,L} = 200 \text{ ms}$$

$$h_{L,CaMK,\infty} = \frac{1}{1 + e^{-\left(\frac{V+93.81}{7.488}\right)}}$$

$$\tau_{h,LCaMK} = 3 \cdot \tau_{h,L}$$

$$K_{m,CaMK} = 0.15,$$

$$\phi_{INaL,CaMK} = \frac{1}{1 + \frac{K_{m,CaMK}}{K_{m,CaMK,active}}}$$

$$I_{Na,late} = G_{NaL} \cdot (V - E_{Na}) \cdot m_L \cdot ((1 - \phi_{INaL,CaMK}) \cdot h_L + \phi_{INaL,CaMK} \cdot h_{L,CaMK})$$

### L-type Calcium Current ( $I_{CaL}$ )

from (O'Hara et al. 2011), modified as described in 1.1

$$d = \frac{1}{1 + e^{-\left(\frac{V+7.24}{4.23}\right)}}$$

$$\tau_d = 0.6 + \frac{1}{e^{-0.05 \cdot (V+6)} + e^{-0.09 \cdot (V+14)}}$$

$$f_{\infty} = \frac{1}{1 + e^{-\left(\frac{V+22.88}{3.696}\right)}}$$

$$\tau_{f,fast} = 7 + \frac{1}{0.0045 \cdot e^{-\left(\frac{V+35.19}{10}\right)} + 0.0045 \cdot e^{-\left(\frac{V+35.19}{10}\right)}}$$

$$\tau_{f,slow} = 1000 + \frac{1}{0.000035 \cdot e^{-\left(\frac{V+20.19}{4}\right)} + 0.000035 \cdot e^{-\left(\frac{V+20.19}{4}\right)}}$$

$$A_{f,fast} = 0.6,$$

$$A_{f,slow} = 1 - A_{f,fast}$$

$$f = A_{f,fast} \cdot f_{fast} + A_{f,slow} \cdot f_{slow}$$

$$f_{Ca,\infty} = f_{\infty}$$

$$\tau_{f, \text{Ca}, \text{fast}} = 7 + \frac{1}{0.04 \cdot e^{-\left(\frac{V-11.19}{7}\right)} + 0.04 \cdot e^{\left(\frac{V-11.19}{7}\right)}}$$

$$\tau_{f, \text{Ca}, \text{slow}} = 100 + \frac{1}{0.00012 \cdot e^{-\left(\frac{V+20}{3}\right)} + 0.00012 \cdot e^{\left(\frac{V+20}{7}\right)}}$$

$$A_{f, \text{Ca}, \text{fast}} = 0.3 + \frac{0.6}{1 + e^{\left(\frac{V-10}{10}\right)}}, \quad A_{f, \text{Ca}, \text{slow}} = 1 - A_{f, \text{Ca}, \text{fast}}$$

$$f_{\text{Ca}} = A_{f, \text{Ca}, \text{fast}} \cdot f_{\text{Ca}, \text{fast}} + A_{f, \text{Ca}, \text{slow}} \cdot f_{\text{Ca}, \text{slow}}$$

$$j_{\text{Ca}, \infty} = f_{\text{Ca}, \infty}$$

$$\tau_{j, \text{Ca}} = 75$$

$$f_{\text{CaMK}, \infty} = f_{\infty}$$

$$\tau_{f, \text{CaMK}, \text{fast}} = 2.5 \cdot \tau_{f, \text{fast}}$$

$$A_{f, \text{CaMK}, \text{fast}} = A_{f, \text{fast}}, \quad A_{f, \text{CaMK}, \text{slow}} = A_{f, \text{slow}}$$

$$f_{\text{CaMK}, \text{slow}} = f_{\text{slow}}$$

$$f_{\text{CaMK}} = A_{f, \text{CaMK}, \text{fast}} \cdot f_{\text{CaMK}, \text{fast}} + A_{f, \text{CaMK}, \text{slow}} \cdot f_{\text{CaMK}, \text{slow}}$$

$$f_{\text{Ca}, \text{CaMK}, \infty} = f_{\infty}$$

$$\tau_{f, \text{Ca}, \text{CaMK}, \text{fast}} = 2.5 \cdot \tau_{f, \text{Ca}, \text{fast}}$$

$$A_{f, \text{Ca}, \text{CaMK}, \text{fast}} = A_{f, \text{Ca}, \text{fast}}, \quad A_{f, \text{Ca}, \text{CaMK}, \text{slow}} = A_{f, \text{Ca}, \text{slow}}$$

$$f_{\text{Ca}, \text{CaMK}, \text{slow}} = f_{\text{Ca}, \text{slow}}$$

$$f_{\text{Ca}, \text{CaMK}} = A_{f, \text{Ca}, \text{CaMK}, \text{fast}} \cdot f_{\text{Ca}, \text{CaMK}, \text{fast}} + A_{f, \text{Ca}, \text{CaMK}, \text{slow}} \cdot f_{\text{Ca}, \text{CaMK}, \text{slow}}$$

$$K_{m, n} = 0.002, \quad K_{+2, n} = 1000, \quad K_{-2, n} = j_{\text{Ca}}$$

$$\alpha_n = \frac{1}{\frac{K_{+2, n}}{K_{-2, n}} + \left(1 + e^{\left(\frac{K_{m, n}}{[\text{Ca}^{2+}]_{\text{sl}}}\right)}\right)^4}$$

$$\gamma_{\text{Ca}i} = 1, \quad \gamma_{\text{Ca}o} = 0.341, \quad z_{\text{Ca}} = 2$$

$$\Psi_{\text{Ca}} = z_{\text{Ca}}^2 \cdot \frac{VF^2}{RT} \cdot \frac{\gamma_{\text{Ca}i} \cdot [\text{Ca}^{2+}]_{\text{SS}} \cdot e^{\frac{z_{\text{Ca}}VF}{RT}} - \gamma_{\text{Ca}o} \cdot [\text{Ca}^{2+}]_o}{e^{\frac{z_{\text{Ca}}VF}{RT}} - 1.0}$$

$$\overline{I_{\text{Ca}L}} = G_{\text{Ca}L} \cdot \Psi_{\text{Ca}}$$

$$P_{\text{Ca}Na} = 0.00125 \cdot P_{\text{Ca}}, \quad \gamma_{\text{Na}i} = 0.75, \quad \gamma_{\text{Na}o} = 0.75, \quad z_{\text{Na}} = 1$$

$$\Psi_{\text{Ca}Na} = z_{\text{Na}}^2 \cdot \frac{VF^2}{RT} \cdot \frac{\gamma_{\text{Na}i} \cdot [\text{Na}^+]_{\text{SS}} \cdot e^{\frac{z_{\text{Na}}VF}{RT}} - \gamma_{\text{Na}o} \cdot [\text{Na}^+]_o}{e^{\frac{z_{\text{Na}}VF}{RT}} - 1.0}$$

$$\overline{I_{\text{Ca}Na}} = P_{\text{Ca}Na} \cdot \Psi_{\text{Ca}Na}$$

$$P_{CaK} = 3.574 \cdot 10^{-4} \cdot P_{Ca} , \quad \gamma_{Ki} = 0.75, \quad \gamma_{Ko} = 0.75, \quad z_K = 1$$

$$\Psi_{CaK} = z_K^2 \cdot \frac{VF^2}{RT} \cdot \frac{\gamma_{Ki} \cdot [K^+]_{SS} \cdot e^{\frac{z_K VF}{RT}} - \gamma_{Ko} \cdot [K^+]_o}{e^{\frac{z_K VF}{RT}} - 1.0}$$

$$\overline{I_{CaK}} = P_{CaK} \cdot \Psi_{CaK}$$

$$P_{Ca,CaMK} = 1.1 \cdot G_{CaL}$$

$$\overline{I_{CaL,CaMK}} = P_{Ca,CaMK} \cdot \Psi_{Ca}$$

$$P_{CaNa,CaMK} = 0.00125 \cdot P_{Ca,CaMK}$$

$$\overline{I_{CaNa,CaMK}} = P_{CaNa,CaMK} \cdot \Psi_{CaNa}$$

$$P_{CaK,CaMK} = 3.574 \cdot 10^{-4} \cdot P_{Ca,CaMK}$$

$$\overline{I_{CaK,CaMK}} = P_{CaK,CaMK} \cdot \Psi_{CaK}$$

$$K_{m,CaMK} = 0.15 , \quad \phi_{ICaL,CaMK} = \frac{1}{1 + \frac{K_{m,CaMK}}{CaMK_{active}}}$$

$$I_{CaL} = \overline{I_{CaL}} \cdot d \cdot (1 - \phi_{ICaL,CaMK}) \cdot (f \cdot (1 - n) + f_{Ca} \cdot n \cdot j_{Ca}) + \overline{I_{CaL,CaMK}} \cdot d \cdot \phi_{ICaL,CaMK} \cdot (f_{CaMK} \cdot (1 - n) + f_{Ca,CaMK} \cdot n \cdot j_{Ca})$$

$$I_{CaNa} = \overline{I_{CaNa}} \cdot d \cdot (1 - \phi_{ICaL,CaMK}) \cdot (f \cdot (1 - n) + f_{Ca} \cdot n \cdot j_{Ca}) + \overline{I_{CaNa,CaMK}} \cdot d \cdot \phi_{ICaL,CaMK} \cdot (f_{CaMK} \cdot (1 - n) + f_{Ca,CaMK} \cdot n \cdot j_{Ca})$$

$$I_{CaK} = \overline{I_{CaK}} \cdot d \cdot (1 - \phi_{ICaL,CaMK}) \cdot (f \cdot (1 - n) + f_{Ca} \cdot n \cdot j_{Ca}) + \overline{I_{CaK,CaMK}} \cdot d \cdot \phi_{ICaL,CaMK} \cdot (f_{CaMK} \cdot (1 - n) + f_{Ca,CaMK} \cdot n \cdot j_{Ca})$$

### T-type Calcium Current ( $I_{CaT}$ )

From (Pan and Rudy 2011)

$$b_{\infty} = \frac{1}{1 + e^{-\left(\frac{V+30}{7}\right)}}$$

$$\tau_b = \frac{1}{1.068 \cdot e^{-\left(\frac{V-16.3}{30}\right)} + 1.068 \cdot e^{\left(\frac{V-16.3}{30}\right)}}$$

$$g_{\infty} = \frac{1}{1 + e^{\left(\frac{V+61}{5}\right)}}$$

$$\tau_b = \frac{1}{0.015 \cdot e^{-\left(\frac{V-71.7}{83.3}\right)} + 0.015 \cdot e^{\left(\frac{V+71.7}{15.4}\right)}}$$

$$I_{CaT} = G_{CaT} \cdot b \cdot g \cdot (V - E_{Ca})$$

### Transient Outward Current ( $I_{to}$ )

Data from (Han et al. 2002)

$$a_{\infty} = \frac{1}{1 + e^{\left(\frac{20-V}{13}\right)}}$$

$$\tau_a = \frac{1.0515}{\left( \frac{1}{1.2 \cdot (1 + \exp(-\frac{V-18.41}{29.38}))} + \frac{3.5}{1 + \exp(\frac{V+100}{29.38})} \right)}$$

$$i_{1,\infty} = \frac{1}{1 + e^{\left(\frac{V+27}{13}\right)}}$$

$$i_{2,\infty} = i_{1,\infty}$$

$$\tau_{i,S} = 43 + \frac{1}{0.001416 \cdot \exp\left(-\frac{V+96.52}{59.05}\right) + 1.7 \cdot 10^{-8} \cdot \exp\left(\frac{V+114.1}{8.079}\right)}$$

$$\tau_{i,F} = 6.16 + \frac{1}{0.39 \cdot \exp\left(-\frac{V+100}{100}\right) + 0.08 \cdot \exp\left(\frac{V-8}{8.59}\right)}$$

$$I_{to} = g_{to} \cdot a \cdot i_S \cdot i_F \cdot g \cdot (V - E_K)$$

### Sustained Potassium Current ( $I_{sus}$ )

Data from (Han et al. 2002)

$$a_{sus} = \frac{1}{1 + e^{-\left(\frac{V-12}{16}\right)}}$$

$$i_{sus} = g_{sus} \cdot a_{sus} \cdot (V - E_K)$$

### Rapid Delayed Rectifier Potassium Current ( $I_{Kr}$ )

from (O'Hara et al. 2011), modified as described in 1.1

$$x_{r\infty} = \frac{1}{1 + e^{-\left(\frac{V+8.337}{6.789}\right)}}$$

$$\tau_{xr,fast} = 12.98 + \frac{1}{0.3652 \cdot e^{\left(\frac{V-14.06}{3.869}\right)} + 4.123 \cdot 10^{-5} \cdot e^{-\left(\frac{V-30.18}{20.38}\right)}}$$

$$\tau_{xr,slow} = 1.865 + \frac{1}{0.06629 \cdot e^{\left(\frac{V-19.7}{7.355}\right)} + 1.128 \cdot 10^{-5} \cdot e^{-\left(\frac{V-12.54}{25.94}\right)}}$$

$$A_{xr,fast} = \frac{1}{1 + e^{\left(\frac{V+54.81}{38.21}\right)}}, \quad A_{xr,slow} = 1 - A_{xr,fast}$$

$$x_r = A_{xr,fast} \cdot x_{r,fast} + A_{xr,slow} \cdot x_{r,slow}$$

$$R_{Kr} = \frac{1}{\left(1 + e^{\left(\frac{V+55}{24}\right)}\right) \cdot \left(1 + e^{\left(\frac{V-10}{9.6}\right)}\right)}$$

$$i_{Kr} = g_{Kr} \cdot \sqrt{\frac{[K^+]_o}{5.4}} \cdot x_r \cdot R_{Kr} \cdot (V - E_K)$$



### Slow Delayed Rectifier Potassium Current ( $I_{Ks}$ )

from (O'Hara et al. 2011)

$$x_{s1,\infty} = \frac{1}{1 + e^{-\left(\frac{V+11.6}{8.932}\right)}}$$
$$\tau_{x,s1} = 817.3 + \frac{1}{0.001292 \cdot e^{-\left(\frac{V+210}{230}\right)} + 2.326 \cdot 10^{-4} \cdot e^{\left(\frac{V+48.28}{17.8}\right)}}$$
$$x_{s2,\infty} = x_{s1,\infty}$$
$$\tau_{x,s2} = \frac{1}{0.01 \cdot e^{\left(\frac{V-50}{20}\right)} + 0.0193 \cdot e^{-\left(\frac{V+66.54}{31}\right)}}$$
$$i_{Ks} = g_{Ks} \cdot \left( 1 + \frac{0.6}{1 + \left(\frac{3.8 \cdot 10^{-5}}{[Ca^{2+}]_{sl}}\right)^{1.4}} \right) \cdot x_{s1} \cdot x_{s2} \cdot (V - E_{Ks})$$

### Hyperpolarization-activated Current ( $I_f$ )

from (Pan and Rudy 2011)

$$y_{\infty} = \frac{1}{1 + e^{\left(\frac{V+87}{9.5}\right)}}$$
$$\tau_y = \frac{2000}{\exp\left(-\frac{V+132}{10}\right) + \exp\left(\frac{V+57}{60}\right)}$$
$$i_{f,K} = g_{f,K} \cdot y \cdot (V - E_K)$$
$$i_{f,Na} = g_{f,Na} \cdot y \cdot (V - E_{Na})$$
$$i_f = i_{f,K} + i_{f,Na}$$

### Inward Rectifier Potassium Current ( $I_{K1}$ )

Data from (Han et al. 2002)

$$x_{K1,\infty} = \frac{1}{1 + e^{-\left(\frac{V+2.5538 \cdot [K^+]_o + 144.59}{1.5692 \cdot [K^+]_o + 3.8115}\right)}}$$
$$\tau_{x,K1} = \frac{122.2}{e^{-\left(\frac{V+127.2}{20.36}\right)} + e^{\left(\frac{V+236.8}{69.33}\right)}}$$
$$R_{K1} = \frac{1}{1 + e^{\left(\frac{V+116-5.5 \cdot [K^+]_o}{11}\right)}}$$
$$i_{K1} = g_{K1} \cdot \sqrt{\frac{[K^+]_o}{5.4}} \cdot x_{K1} \cdot R_{K1} \cdot (V - E_K)$$

### Sodium-Calcium Exchange Current ( $I_{NaCa}$ )

from (O'Hara et al. 2011)

For,  $Y \in \{i, ss\}$ :

$$K_{Na1} = 15 \text{ mM}, \quad K_{Na2} = 5 \text{ mM}, \quad K_{Na3} = 88.12 \text{ mM}, \quad K_{asymm} = 12.5$$

$$\omega_{Na} = 6 \cdot 10^4 \text{ Hz}, \quad \omega_{Ca} = 6 \cdot 10^4 \text{ Hz}, \quad \omega_{NaCa} = 5 \cdot 10^3 \text{ Hz}$$

$$k_{Ca,on} = 1.5 \cdot 10^6 \frac{\text{mM}}{\text{ms}}, \quad k_{Ca,off} = 5 \cdot 10^3 \text{ Hz}$$

$$q_{Na} = 0.5224, \quad q_{Ca} = 0.1670$$

$$h_{Ca} = \exp\left(\frac{q_{Ca}VF}{RT}\right), \quad h_{Na} = \exp\left(\frac{q_{Na}VF}{RT}\right),$$

$$h_1 = 1 + \frac{[Na^+]_Y}{k_{Na3}}(1 + h_{Na})$$

$$h_2 = \frac{[Na^+]_Y \cdot h_{Na}}{k_{Na3} \cdot h_1}$$

$$h_3 = \frac{1}{h_1}$$

$$h_4 = 1 + \frac{[Na^+]_Y}{k_{Na1}} \left(1 + \frac{[Na^+]_Y}{k_{Na2}}\right)$$

$$h_5 = \frac{[Na^+]_Y^2}{k_4 \cdot k_{Na1} \cdot k_{Na2}}$$

$$h_6 = \frac{1}{h_4}$$

$$h_7 = 1 + \frac{[Na^+]_o}{k_{Na3}} \left(1 + \frac{1}{h_{Na}}\right)$$

$$h_8 = \frac{[Na^+]_o}{k_{Na3} \cdot h_{Na} \cdot h_7}$$

$$h_9 = \frac{1}{h_7}$$

$$h_{10} = k_{asymm} + 1 + \frac{[Na^+]_o}{k_{Na1}} \left(1 + \frac{[Na^+]_o}{k_{Na2}}\right)$$

$$h_{11} = \frac{[Na^+]_o^2}{h_{10} \cdot k_{Na1} \cdot k_{Na2}}$$

$$h_{12} = \frac{1}{h_{10}}$$

$$k_1 = h_{12} \cdot [Ca^{2+}]_o \cdot k_{Ca,on}$$

$$k_2 = k_{Ca,off}$$

$$k_3' = h_9 \cdot \omega_{Ca}$$

$$k_3'' = h_8 \cdot \omega_{NaCa}$$

$$k_3 = k_3' + k_3''$$

$$k_4' = \frac{h_3 \cdot \omega_{Ca}}{h_{Ca}}$$

$$k_4'' = h_2 \cdot \omega_{NaCa}$$

$$k_4 = k_4' + k_4''$$

$$k_5 = k_{Ca,off}$$

$$k_6 = h_6 \cdot [\text{Ca}^{2+}]_Y \cdot k_{\text{Ca,on}}$$

$$k_7 = h_5 \cdot h_2 \cdot \omega_{\text{Na}}$$

$$k_8 = h_8 \cdot h_{11} \cdot \omega_{\text{Na}}$$

$$x_1 = k_2 \cdot k_4 \cdot (k_7 + k_6) + k_5 \cdot k_7 \cdot (k_2 + k_3)$$

$$x_2 = k_1 \cdot k_7 \cdot (k_4 + k_5) + k_4 \cdot k_6 \cdot (k_1 + k_8)$$

$$x_3 = k_1 \cdot k_3 \cdot (k_7 + k_6) + k_8 \cdot k_6 \cdot (k_2 + k_3)$$

$$x_4 = k_2 \cdot k_8 \cdot (k_4 + k_5) + k_3 \cdot k_5 \cdot (k_1 + k_8)$$

$$E_1 = \frac{x_1}{x_1 + x_2 + x_3 + x_4}$$

$$E_2 = \frac{x_2}{x_1 + x_2 + x_3 + x_4}$$

$$E_3 = \frac{x_3}{x_1 + x_2 + x_3 + x_4}$$

$$E_4 = \frac{x_4}{x_1 + x_2 + x_3 + x_4}$$

$$K_{\text{mCaAct}} = 150 \cdot 10^{-6} \text{ mM}$$

$$\text{allo}_Y = \frac{1}{1 + \left( \frac{K_{\text{mCaAct}}}{[\text{Ca}^{2+}]_Y} \right)^2}$$

$$J_{\text{NaCa,Na,Y}} = 3 \cdot (E_4 \cdot k_7 - E_1 \cdot k_8) + E_3 \cdot k_4'' - E_2 \cdot k_3''$$

$$J_{\text{NaCa,Ca,Y}} = E_2 \cdot k_2 - E_1 \cdot k_1$$

$$z_{\text{Na}} = 1 ; z_{\text{Ca}} = 2 ;$$

$$I_{\text{NaCa,i}} = G_{\text{NaCa}} \cdot 0.8 \cdot \text{allo}_i \cdot (z_{\text{Na}} \cdot J_{\text{NaCa,Na,i}} + z_{\text{Ca}} \cdot J_{\text{NaCa,Ca,i}})$$

$$I_{\text{NaCa,ss}} = G_{\text{NaCa}} \cdot 0.2 \cdot \text{allo}_{\text{ss}} \cdot (z_{\text{Na}} \cdot J_{\text{NaCa,Na,ss}} + z_{\text{Ca}} \cdot J_{\text{NaCa,Ca,ss}})$$

$$I_{\text{NaCa}} = I_{\text{NaCa,i}} + I_{\text{NaCa,ss}}$$

### Sodium-Potassium ATPase Current ( $I_{\text{NaK}}$ )

from (O'Hara et al. 2011)

$$k_1^+ = 949.5 \text{ Hz} ; k_1^- = 182.4 \text{ mM}^{-1} ; k_2^+ = 687.2 \text{ Hz} ; k_2^- = 39.4 \text{ Hz}$$

$$k_3^+ = 1899 \text{ Hz} ; k_3^- = 79300 \text{ Hz} \cdot \text{mM}^{-2} ; k_4^+ = 639.0 \text{ Hz} ; k_4^- = 40 \text{ Hz}$$

$$K_{\text{Nai}}^0 = 9.073 \text{ mM} ; K_{\text{NaO}}^0 = 27.78 \text{ mM}$$

$$\Delta = -01550$$

$$K_{\text{Nai}} = K_{\text{Nai}}^0 \cdot \exp\left(\frac{\Delta \cdot V \cdot F}{3 \cdot R \cdot T}\right) ; K_{\text{NaO}} = K_{\text{NaO}}^0 \cdot \exp\left(\frac{(1-\Delta) \cdot V \cdot F}{3 \cdot R \cdot T}\right)$$

$$K_{\text{Ki}} = 0.5 \text{ mM} ; K_{\text{Ko}} = 0.3582 \text{ mM}$$

$$[\text{MgADP}] = 0.05 ; [\text{MgATP}] = 9.8$$

$$[\text{KMgATP}] = 1.698 \cdot 10^{-7} \text{ mM}$$

$$[\text{H}^+] = 10^{-7} \text{ mM}$$

$$[\Sigma\text{P}] = 4.2 \text{ mM}$$

$$K_{\text{H,P}} = 1.698 \cdot 10^{-7} \text{ mM}, K_{\text{Na,P}} = 224 \text{ mM}, K_{\text{K,P}} = 292 \text{ mM}$$

$$[\text{P}] = \frac{[\Sigma\text{P}]}{\left(1 + \frac{[\text{H}^+]}{K_{\text{H,P}}} + \frac{[\text{Na}^+]_i}{K_{\text{Na,P}}} + \frac{[\text{K}^+]_i}{K_{\text{K,P}}}\right)}$$

$$\alpha_1 = \frac{k_1^+ \cdot \left(\frac{[\text{Na}^+]_i}{K_{\text{Nai}}}\right)^3}{\left(1 + \frac{[\text{Na}^+]_i}{K_{\text{Nai}}}\right)^3 + \left(1 + \frac{[\text{K}^+]_i}{K_{\text{Ki}}}\right)^2 - 1}$$

$$\beta_2 = k_1^- \cdot [\text{MgADP}]$$

$$\alpha_2 = k_2^+$$

$$\beta_2 = \frac{k_2^- \cdot \left(\frac{[\text{Na}^+]_o}{K_{\text{Nao}}}\right)^3}{\left(1 + \frac{[\text{Na}^+]_o}{K_{\text{Nao}}}\right)^3 + \left(1 + \frac{[\text{K}^+]_o}{K_{\text{Ko}}}\right)^2 - 1}$$

$$\alpha_3 = \frac{k_3^+ \cdot \left(\frac{[\text{K}^+]_o}{K_{\text{Ko}}}\right)^2}{\left(1 + \frac{[\text{Na}^+]_o}{K_{\text{Nao}}}\right)^3 + \left(1 + \frac{[\text{K}^+]_o}{K_{\text{Ko}}}\right)^2 - 1}$$

$$\beta_3 = \frac{k_3^- \cdot [\text{P}] \cdot [\text{H}^+]}{1 + \frac{[\text{MgATP}]}{K_{\text{MgATP}}}}$$

$$\alpha_4 = \frac{k_4^+ \cdot [\text{P}] \cdot [\text{H}^+]}{1 + \frac{[\text{MgATP}]}{K_{\text{MgATP}}}}$$

$$\beta_4 = \frac{k_4^- \cdot \left(\frac{[\text{K}^+]_i}{K_{\text{Ki}}}\right)^3}{\left(1 + \frac{[\text{Na}^+]_i}{K_{\text{Nai}}}\right)^3 + \left(1 + \frac{[\text{K}^+]_i}{K_{\text{Ki}}}\right)^2 - 1}$$

$$x_1 = \alpha_1 \cdot \alpha_2 \cdot \alpha_4 + \beta_2 \cdot \beta_3 \cdot \beta_4 + \alpha_2 \cdot \beta_3 \cdot \beta_4 + \beta_3 \cdot \alpha_1 \cdot \alpha_2$$

$$x_2 = \alpha_1 \cdot \alpha_2 \cdot \alpha_3 + \beta_1 \cdot \beta_2 \cdot \beta_4 + \alpha_3 \cdot \beta_1 \cdot \beta_4 + \beta_4 \cdot \alpha_2 \cdot \alpha_3$$

$$x_3 = \alpha_2 \cdot \alpha_3 \cdot \alpha_4 + \beta_1 \cdot \beta_2 \cdot \beta_3 + \alpha_4 \cdot \beta_2 \cdot \beta_1 + \beta_1 \cdot \alpha_3 \cdot \alpha_4$$

$$x_4 = \alpha_1 \cdot \alpha_3 \cdot \alpha_4 + \beta_2 \cdot \beta_3 \cdot \beta_4 + \alpha_1 \cdot \beta_2 \cdot \beta_3 + \beta_2 \cdot \alpha_1 \cdot \alpha_4$$

$$E_1 = \frac{x_1}{x_1 + x_2 + x_3 + x_4}$$

$$E_2 = \frac{x_2}{x_1 + x_2 + x_3 + x_4}$$

$$E_3 = \frac{x_3}{x_1 + x_2 + x_3 + x_4}$$

$$E_4 = \frac{x_4}{x_1 + x_2 + x_3 + x_4}$$

$$z_{\text{Na}} = 1; z_{\text{K}} = 1;$$

$$J_{\text{NaK,Na}} = 3 (E_1 \cdot \alpha_3 - E_2 \cdot \beta_3)$$

$$J_{\text{NaK,K}} = 2 (E_4 \cdot \beta_1 - E_3 \cdot \alpha_1)$$

$$I_{\text{NaK}} = G_{\text{NaK}} \cdot (z_{\text{Na}} \cdot J_{\text{NaK,Na}} + z_{\text{K}} \cdot J_{\text{NaK,K}})$$

**Background currents:  $I_{\text{Nab}}$ ,  $I_{\text{Cab}}$ ,  $I_{\text{pCa}}$**

from (O'Hara et al. 2011)

$$P_{\text{Nab}} = 3.75 \cdot 10^{-10} \text{ cm/s}; z_{\text{Na}} = 1;$$

$$I_{Na} = P_{Na} \cdot z_{Na}^2 \cdot \frac{VF^2}{RT} \cdot \frac{[Na^+]_i \cdot \exp\left(\frac{VFz_{Na}}{RT}\right) - [Na^+]_o}{\exp\left(\frac{VFz_{Na}}{RT}\right) - 1}$$

$$P_{Ca} = 2.5 \cdot 10^{-8} \text{ cm/s}; \quad \gamma_{Ca_i} = 1; \quad \gamma_{Ca_o} = 0.341; \quad z_{Ca} = 2;$$

$$I_{Ca} = P_{Ca} \cdot z_{Ca}^2 \cdot \frac{VF^2}{RT} \cdot \frac{\gamma_{Ca_i} \cdot [Ca^{2+}]_i \cdot \exp\left(\frac{VFz_{Ca}}{RT}\right) - \gamma_{Ca_o} \cdot [Ca^{2+}]_o}{\exp\left(\frac{VFz_{Ca}}{RT}\right) - 1}$$

$$G_{pCa} = 0.0005 \text{ mS/uF};$$

$$I_{pCa} = G_{pCa} \cdot \frac{[Ca^{2+}]_{sl}}{0.0005 + [Ca^{2+}]_{sl}}$$

### **Calcium/Calmodulin-Dependent Protein Kinase (CaMK)**

from (O'Hara et al. 2011)

$$\alpha_{CaMK} = 0.05 \text{ ms}^{-1}; \quad \beta_{CaMK} = 0.00068 \text{ ms}^{-1};$$

$$CaMK_0 = 0.05; \quad K_{mCaM} = 0.0015 \text{ mM}$$

$$CaMK_{bound} = CaMK_0 \cdot \frac{1 - CaMK_{trap}}{1 + \frac{K_{mCaM}}{[Ca^{2+}]_{ss}}}$$

$$CaMK_{active} = CaMK_{bound} + CaMK_{trap}$$

$$\frac{dCaMK_{trap}}{dt} = \alpha_{CaMK} \cdot CaMK_{bound} \cdot (CaMK_{bound} + CaMK_{trap}) - \beta_{CaMK} \cdot CaMK_{trap}$$

### **Sarcoplasmic Reticulum Ca<sup>2+</sup> Fluxes**

from in (Pan and Rudy 2011)

- **RyR3**

$$Rel_{RyR3} = - \left( I_{CaL} \cdot \frac{A_{cap}}{V_{SS} \cdot 2 \cdot F} - (J_{RyR3} + J_{IP3R}) \cdot \frac{V_{JSR}}{V_{SS}} + J_{diff1} \right) \cdot \frac{1}{2 \cdot \left( 1 + \frac{1}{1 + \left( \frac{0.28}{[CaMK_{active}]}\right)^8} \right)}$$

$$\tau_{RyR3} = \frac{1}{1 + \frac{0.0123}{[Ca^{2+}]_{JSR}}}$$

If ( $Rel_{RyR3} > 0$ )

$$RyR3_{\infty} = \frac{15 \cdot Rel_{RyR3} \cdot \left( 1 + \frac{1}{1 + \left( \frac{0.28}{[CaMK_{active}]}\right)^8} \right)}{1 + \left( \frac{1}{[Ca^{2+}]_{JSR}} \right)^8}$$

else

$$RyR3_{\infty} = 0$$

$$\frac{dJ_{RyR3}}{dt} = \frac{RyR3_{\infty} - J_{RyR3}}{\tau_{RyR3}}$$

- **RyR2**

$$\text{Rel}_{\text{RyR2}} = -J_{\text{SERCA}} \cdot \frac{V_{\text{NSR}}}{V_{\text{Myo}}} + J_{\text{diff2}} \cdot \frac{V_{\text{SL}}}{V_{\text{Myo}}} + J_{\text{RyR2}} \cdot \frac{V_{\text{CSR}}}{V_{\text{Myo}}}$$

$$\tau_{\text{RyR2}} = \frac{6 \cdot \left(1 + \frac{1}{1 + \left(\frac{0.28}{[\text{CaMK}_{\text{active}}]}\right)^8}\right)}{1 + \frac{0.0123}{[\text{Ca}^{2+}]_{\text{CSR}}}}$$

If ( $\text{Rel}_{\text{RyR2}} > 0$ )

$$\text{RyR2}_{\infty} = \frac{91 \cdot \text{Rel}_{\text{RyR2}} \cdot \left(1 + \frac{1}{1 + \left(\frac{0.28}{[\text{CaMK}_{\text{active}}]}\right)^8}\right)}{1 + \left(\frac{1}{[\text{Ca}^{2+}]_{\text{CSR}}}\right)^8}$$

else

$$\text{RyR2}_{\infty} = 0$$

$$\frac{dJ_{\text{RyR2}}}{dt} = \frac{\text{RyR2}_{\infty} - J_{\text{RyR2}}}{\tau_{\text{RyR2}}}$$

- **IP<sub>3</sub>R Ca<sup>2+</sup> release:**

$$k_0 = 96000 \text{ mM}^{-1}\text{s}^{-1}; k_{0a} = 9.6 \text{ s}^{-1}; k_1 = 150000 \text{ mM}^{-1}\text{s}^{-1}; k_{1a} = 16.5 \text{ s}^{-1}$$

$$k_2 = 1800 \text{ mM}^{-1}\text{s}^{-1}; k_{2a} = 0.21 \text{ s}^{-1}; \tau_{\text{IP3R}} = 3.7 \text{ s}^{-1}$$

$$[\text{IP}_3] = 0.001 \text{ mM/L};$$

$$\frac{du_{\text{IP3R}}}{dt} = [\text{Ca}^{2+}]_{\text{SS}} \cdot k_2 \cdot (1 - u_{\text{IP3R}}) - k_{2a} \cdot u_{\text{IP3R}}$$

$$J_{\text{IP3R}} = 10.92 \cdot \frac{\tau_{\text{IP3R}} \cdot [\text{IP}_3] \cdot [\text{Ca}^{2+}]_{\text{SS}} \cdot (1 - u_{\text{IP3R}})}{\left(1 + \frac{[\text{IP}_3] \cdot k_0}{k_{0a}}\right) \cdot \left(1 + [\text{Ca}^{2+}]_{\text{SS}} \frac{k_1}{k_{1a}}\right)} \left([\text{Ca}^{2+}]_{\text{JSR}} - [\text{Ca}^{2+}]_{\text{SS}}\right)$$

- **Ca<sup>2+</sup> uptake via SERCA:**

$$\Delta K_{0m, \text{PLB}} = 0.00017 \frac{\text{mM}}{\text{L}}; \quad \Delta J_{0, \text{SERCA, CAMK}} = 0.75; \quad K_{m, \text{CAMK}} = 0.15;$$

$$J_{0, \text{SERCA, 1}} = 0.0002 \frac{\text{mM}}{\text{L}}/\text{ms}; \quad J_{0, \text{SERCA, 2}} = 0.0026 \frac{\text{mM}}{\text{L}}/\text{ms}; \quad K_{m, \text{SERCA}} = 0.00028 \frac{\text{mM}}{\text{L}};$$

$$\overline{\text{NSR}} = 15 \frac{\text{mM}}{\text{L}}$$

$$\Delta K_{m, \text{PLB}} = \Delta K_{0m, \text{PLB}} \cdot \frac{\text{CAMK}_{\text{active}}}{K_{m, \text{CAMK}} + \text{CAMK}_{\text{active}}}$$

$$\Delta J_{\text{SERCA, CAMK}} = \Delta J_{0, \text{SERCA, CAMK}} \cdot \frac{\text{CAMK}_{\text{active}}}{K_{m, \text{CAMK}} + \text{CAMK}_{\text{active}}}$$

$$J_{\text{SERCA, 1}} = J_{0, \text{SERCA, 1}} \cdot \frac{(1 + \Delta J_{\text{SERCA, CAMK}})}{1 + \frac{K_{m, \text{SERCA}} - \Delta K_{m, \text{PLB}}}{[\text{Ca}^{2+}]_{\text{SL}}}} - 0.0042 \cdot \frac{[\text{Ca}^{2+}]_{\text{NSR}}}{\overline{\text{NSR}}}$$

$$J_{SERCA,2} = J_{0,SERCA,2} \cdot \frac{(1 + \Delta J_{SERCA,CAMK})}{1 + \frac{K_{m,SERCA} - \Delta K_{m,PLB}}{[Ca^{2+}]_i}} - 0.00105 \cdot \frac{[Ca^{2+}]_{NSR}}{NSR}$$

### Diffusion Fluxes

$$\tau_{tr} = 120 \text{ ms}$$

$$J_{tr,1} = \frac{([Ca^{2+}]_{NSR} - [Ca^{2+}]_{JSR})}{\tau_{tr}}; \quad J_{tr,2} = \frac{([Ca^{2+}]_{NSR} - [Ca^{2+}]_{CSR})}{\tau_{tr}}$$

$$\tau_{diff1} = 0.2 \text{ ms}; \quad \tau_{diff2} = 12 \text{ ms}$$

$$J_{diff1,Ca} = \frac{([Ca^{2+}]_{SS} - [Ca^{2+}]_{SL})}{\tau_{diff1}}; \quad J_{diff2,Ca} = \frac{([Ca^{2+}]_{SL} - [Ca^{2+}]_i)}{\tau_{diff2}}$$

$$J_{diff1,Na} = \frac{([Na^+]_{SS} - [Na^+]_{SL})}{\tau_{diff1}}; \quad J_{diff2,Na} = \frac{([Na^+]_{SL} - [Na^+]_i)}{\tau_{diff2}}$$

$$J_{diff1,K} = \frac{([K^+]_{SS} - [K^+]_{SL})}{\tau_{diff1}}; \quad J_{diff2,K} = \frac{([K^+]_{SL} - [K^+]_i)}{\tau_{diff2}}$$

### Ionic Concentrations

- $[Ca^{2+}]_{SS}$

$$\beta_{PCS} = \frac{1}{1 + \overline{BSR} \cdot \frac{K_{m,BSR}}{([Ca^{2+}]_{SS} + K_{m,BSR})} + \overline{BSL} \cdot \frac{K_{m,BSL}}{([Ca^{2+}]_{SS} + K_{m,BSL})}}$$

$$\frac{d[Ca^{2+}]_{SS}}{dt} = \beta_{PCS} \cdot (-I_{CaL} - 2 \cdot I_{NaCa,SS}) \cdot \frac{A_{Cap}}{\overline{V}_{PCS} \cdot 2 \cdot F} + (J_{RyR2} + J_{IP3R}) \cdot \frac{V_{JSR}}{\overline{V}_{PCS}} - J_{diff1})$$

- $[Ca^{2+}]_{SL}$

$$\frac{d[Ca^{2+}]_{SL}}{dt} = -(I_{CaT} + I_{pCa} + I_{Cab} - 2 \cdot I_{NaCa,SL}) \cdot \frac{A_{Cap}}{\overline{V}_{SL} \cdot 2 \cdot F} + J_{diff1} \cdot \frac{V_{SS}}{\overline{V}_{SL}} - J_{SERCA,1} \cdot \frac{V_{NSR}}{\overline{V}_{SL}} - J_{diff2}$$

$$TRPN_{SL} = \overline{TRPN}_{SL} \cdot \frac{[Ca^{2+}]_{SL}}{[Ca^{2+}]_{SL} + K_{m,TRPN}}$$

$$CMDN_{SL} = \overline{CMDN}_{SL} \cdot \frac{[Ca^{2+}]_{SL}}{[Ca^{2+}]_{SL} + K_{m,CMDN}}$$

$$[Ca^{2+}]_{SL,tot} = [Ca^{2+}]_{SL} + TRPN_{SL} + CMDN_{SL} + d[Ca^{2+}]_{SL}$$

$$b_{SL} = \overline{TRPN}_{SL} + \overline{CMDN}_{SL} - [Ca^{2+}]_{SL,tot} + K_{m,TRPN} + K_{m,CMDN}$$

$$c_{SL} = K_{m,TRPN} \cdot K_{m,CMDN} - [Ca^{2+}]_{SL,tot} \cdot (K_{m,TRPN} + K_{m,CMDN}) + \overline{TRPN}_{SL} \cdot K_{m,CMDN} + \overline{CMDN}_{SL} \cdot K_{m,TRPN}$$

$$d_{SL} = -K_{m,TRPN} \cdot c_{SL} K_{m,TRPN} \cdot [Ca^{2+}]_{SL,tot}$$

$$[Ca^{2+}]_{SL} = \frac{2}{3} \cdot \sqrt{b_{SL}^2 - 3 \cdot c_{SL}} \cdot \cos \left( \frac{1}{3} \cos^{-1} \left( \frac{9b_{SL}c_{SL} - 2b_{SL}^3 - 27d_{SL}}{2(b_{SL}^2 - 3c_{SL})^{1.5}} \right) \right) - \frac{b_{SL}}{3}$$

• **[Ca<sup>2+</sup>]<sub>i</sub>**

$$\frac{d[Ca^{2+}]_i}{dt} = J_{diff2} \cdot \frac{V_{SL}}{V_{Myo}} - J_{SERCA,2} \cdot \frac{V_{NSR}}{V_{Myo}} + J_{RyR2} \cdot \frac{V_{CSR}}{V_{Myo}}$$

$$TRPN_{Myo} = \overline{TRPN}_{Myo} \cdot \frac{[Ca^{2+}]_i}{[Ca^{2+}]_i + K_{m,TRPN}}$$

$$CMDN_{Myo} = \overline{CMDN}_{Myo} \cdot \frac{[Ca^{2+}]_i}{[Ca^{2+}]_i + K_{m,CMDN}}$$

$$[Ca^{2+}]_{i,tot} = [Ca^{2+}]_i + TRPN_{Myo} + CMDN_{Myo} + d[Ca^{2+}]_i$$

$$b_{Myo} = \overline{TRPN}_{Myo} + \overline{CMDN}_{Myo} - [Ca^{2+}]_{i,tot} + K_{m,TRPN} + K_{m,CMDN}$$

$$c_{Myo} = K_{m,TRPN} \cdot K_{m,CMDN} - [Ca^{2+}]_{i,tot} \cdot (K_{m,TRPN} + K_{m,CMDN}) + \overline{TRPN}_{Myo} \cdot K_{m,CMDN} + \overline{CMDN}_{Myo} \cdot K_{m,TRPN}$$

$$d_{Myo} = -K_{m,TRPN} \cdot c_{Myo} K_{m,TRPN} \cdot [Ca^{2+}]_{i,tot}$$

$$[Ca^{2+}]_i = \frac{2}{3} \sqrt{b_{Myo}^2 - 3 \cdot c_{Myo}} \cos \left( \frac{1}{3} \cos^{-1} \left( \frac{9b_{Myo}c_{Myo} - 2b_{Myo}^3 - 27d_{Myo}}{2(b_{Myo}^2 - 3c_{Myo})^{1.5}} \right) \right) - \frac{b_{Myo}}{3}$$

• **[Ca<sup>2+</sup>]<sub>JSR</sub>**

$$\frac{d[Ca^{2+}]_{JSR}}{dt} = J_{tr1} - J_{RyR3} - J_{IP3R}$$

$$CSQN_{JSR} = \overline{CSQN}_{JSR} \cdot \frac{[Ca^{2+}]_{JSR}}{[Ca^{2+}]_{JSR} + K_{m,CSQN}}$$

$$b_{JSR} = \overline{CSQN}_{JSR} + CSQN_{JSR} - [Ca^{2+}]_{JSR} + d[Ca^{2+}]_{JSR} + K_{m,CSQN}$$

$$c_{JSR} = K_{m,CSQN} \cdot (CSQN_{JSR} + [Ca^{2+}]_{JSR} + d[Ca^{2+}]_{JSR})$$

$$[Ca^{2+}]_{JSR} = \frac{\sqrt{b_{JSR}^2 - 4 \cdot c_{JSR}} - b_{JSR}}{2}$$

• **[Ca<sup>2+</sup>]<sub>CSR</sub>**

$$\frac{d[Ca^{2+}]_{CSR}}{dt} = J_{tr2} - J_{RyR2}$$

$$CSQN_{CSR} = \overline{CSQN}_{CSR} \cdot \frac{[Ca^{2+}]_{CSR}}{[Ca^{2+}]_{CSR} + K_{m,CSQN}}$$

$$b_{CSR} = \overline{CSQN}_{CSR} + CSQN_{CSR} - [Ca^{2+}]_{CSR} + d[Ca^{2+}]_{CSR} + K_{m,CSQN}$$



$$c_{CSR} = K_{m,CSQN} \cdot (CSQN_{CSR} + [Ca^{2+}]_{CSR} + d[Ca^{2+}]_{CSR})$$

$$[Ca^{2+}]_{CSR} = \frac{\sqrt{b_{CSR}^2 - 4 \cdot c_{CSR}} - b_{CSR}}{2}$$

- **[Ca<sup>2+</sup>]<sub>NSR</sub>**

$$\frac{d[Ca^{2+}]_{NSR}}{dt} = J_{SERCA,1} + J_{SERCA,2} - J_{tr1} \cdot \frac{V_{JSR}}{V_{NSR}} - J_{tr2} \cdot \frac{V_{CSR}}{V_{NSR}}$$

- **[Na<sup>+</sup>]<sub>SS</sub>**

$$\frac{d[Na^+]_{SS}}{dt} = -(I_{CaNa} + 3 \cdot I_{NaCa,SS}) \cdot \frac{A_{Cap}}{V_{SS} \cdot z_{Na} \cdot F} - J_{diff1,Na}$$

- **[Na<sup>+</sup>]<sub>SL</sub>**

$$\frac{d[Na^+]_{SL}}{dt} = -(3 \cdot I_{NaK} + I_{Na} + I_{NaL} + I_{NaCa,i} + I_{fNa} + I_{Nab}) \cdot \frac{A_{Cap}}{V_{SL} z_{Na} F} + J_{diff1,Na} \frac{V_{SS}}{V_{SL}} - J_{diff2,Na}$$

- **[Na<sup>+</sup>]<sub>i</sub>**

$$\frac{d[Na^+]_i}{dt} = J_{diff2,Na} \cdot \frac{V_{SL}}{V_{Myo}}$$

- **[K<sup>+</sup>]<sub>SS</sub>**

$$\frac{d[K^+]_{SS}}{dt} = -I_{CaK} \cdot \frac{A_{Cap}}{V_{SS} \cdot z_K \cdot F} - J_{diff1,K}$$

- **[K<sup>+</sup>]<sub>SL</sub>**

$$\frac{d[K^+]_{SL}}{dt} = -(I_{to} + I_{sus} + I_{Kr} + I_{Ks} + I_{f,K} + I_{K1} + I_{stim} - 2 \cdot I_{NaK}) \cdot \frac{A_{Cap}}{V_{SL} \cdot z_K \cdot F} + J_{diff1,K} \frac{V_{SS}}{V_{SL}} - J_{diff2,K}$$

- **[K<sup>+</sup>]<sub>i</sub>**

$$\frac{d[K^+]_i}{dt} = -J_{diff2,K} \frac{V_{SL}}{V_{Myo}}$$

## 6 - References

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