Registration of pre-surgical MRI and histopathology images from radical prostatectomy via RAPSODI

Rusu et. al.

ADDITIONAL INFORMATION

Prior Work

Although numerous automated approaches for the registration of radiology and histopathology images have been developed, manual approaches are still employed, even in recent publications [1-5]. Some manual or semi-automatic approaches utilize landmark-based registration approaches, either alone [1, 2, 5] or in combination with automated registration steps [2, 6]. These approaches are laborintensive and require the human operator to possess expertise in both MRI and histopathology, and necessitate identification of corresponding landmarks on both modalities. Other approaches [3, 7]employ cognitive alignment in which a radiologist with the help of a pathologist directly outlines the cancer region on MRI considering the histopathology images as reference. Such methods are tedious to apply and may be prone to underestimating the dimensions of the lesion [8], while MRI invisible lesions are hard if not impossible to outline and thereby they are often omitted from followup analysis. A few approaches use interactive image transformations [9], in which a user indicates scaling, rotations, and translations to be applied to the images. Such approaches are also tedious to utilize and require extensive knowledge in both radiology and pathology of the prostate.

The automated registration of histopathology images with pre-surgical prostate MRI has been performed in proof-of-concept studies, which usually only include a small number of subjects, often < 20 (TABLE S1). Most approaches assume a slice-to-slice correspondence between the histopathology images and T2 weighted (T2w) MRI slices. Some partial correspondence commonly results from the gross sectioning of the prostate in histologic preparation, which is done perpendicular to the urethra in the apical part of the prostate. In some studies, more advanced methods have been introduced to enforce such correspondences. For example, three dimensional (3D) printed patientspecific molds [7] have been used [6, 10, 11] to help preserve the correspondences during tissue sectioning. Some studies additionally included blockface picture [12], ex vivo MRI [6, 11–13] or external fiducials [13] to help improve the accuracy of the registration. These approaches required modifications of the clinical protocols, usually resulting in only a small number of subjects recruited for such research studies.

Once correspondences between the histopathology images and T2w MRI are identified, their registration can still be challenging, partially due to the artifacts induced by the tissue preparation. Textural features [14, 15] have been proposed, yet they may be cumbersome to use due to the high-dimensional scoring function optimization and the choice of textural features. Other approaches rely solely on image intensity to drive the deformable alignment [16, 17], but require accurate affine alignment prior to the deformable registration.

Previous work in the lung [18, 19], breast [20] or prostate [16, 17], has relied on approaches that reconstruct the sequential histopathology slices and created a 3D volume representing the histopathology specimen prior to sectioning, which facilitates the spatial registration with the 3D volumetric MRI and alleviates the need for slice correspondences. However, these methods are prone to overfitting the histopathology reconstruction due to a large number of degrees of freedom and may suffer from partial volume effects due to thick MRI slices and the histopathology slice spacing.

SUPPLEMENTARY TABLES

TABLE S1: Summary of previous approaches (not exhaustive). We excluded publications with <2 subjects [21], only synthetic data [22], or manually intensive approaches [9]. All summarized methods require as input the in vivo pre-surgical T2 weighted MRI, digitized serial histopathology images, and the segmentation of the prostate on MRI and histopathology images; Additional input requirements are listed here; Abbreviations: TPS - Thin Plate Spline; NA - Not available

	Subject				Landmark
Publication	#	Approach	Additional Input	Dice Coef.	Error (mm)
Park 2008		3D reconstruction $+$ affine	block face picture, ex		
[12]	2	and TPS registration	vivo MRI	NA	3-3.74
Chappelow		Feature Based Mutual In-			
2011[14]	25	formation $+$ BSpline	-	NA	NA
Ward 2012		2D Affine + TPS	Strand-shaped fiducials,		
[13]	13	Registration	Ex vivo MRI	NA	1.1
Kalavagunta			Internal landmarks, 3D		
2014 [10]	35	Local affine registration	Printed Molds	0.99	$1.54{\pm}0.64$
Reynolds		2D TPS registration + de-	Control Points, ex vivo		
2015 [6]	6	formable registration	MRI, sectioning box	0.93	3.3
		Multi-Scale Represen-			
		tation + deformable			
Li 2017 [15]	19	registration	-	$0.96 {\pm} 0.01$	$2.96 {\pm} 0.76$
		3D histopathology recon-			
Losnegard		struction, 3D affine and de-			
2018 [16]	12	formable registration	-	0.94	5.4
		2D Rigid, TPS Reg-			
Wu 2019		istration (automatic	ex vivo MRI, 3D printed		
[11]	17	landmarks)	molds	0.87 ± 0.04	2.0 ± 0.5
		3D histopathology			
Rusu 2019		reconstruction, 2D			
[17]	15	Affine+Deformable	3D printed Molds	0.94 ± 0.02	1.11 ± 0.34

TABLE S2: Quantitative results for the three cohorts and aggregated for all subjects in our study.

	Dice	Haussdorff Dis	stance	Urethra	Devia-	Landmarks Deviation	
Cohort	Prostate	(mm)		tion (mm)		(mm)	Dice Cancer
C1	$0.98 {\pm} 0.01$	$1.84{\pm}0.54$		$2.74{\pm}0.85$		2.80 ± 0.59	-
C2	$0.96 {\pm} 0.01$	$2.57{\pm}1.05$		3.13 ± 1.25		-	$0.55 {\pm} 0.14$
C3	$0.97 {\pm} 0.01$	2.35 ± 0.85		$3.52{\pm}2.04$		-	-
All	0.97 ± 0.01	$1.99{\pm}0.71$		3.09 ± 1.45		2.80 ± 0.59	$0.55 {\pm} 0.14$

SUPPLEMENTARY FIGURES

TABLE S3: Data Summary: Abbreviations: T2-weighted MRI (T2w), Hematoxylin & Eosin
(H&E), Relaxation Time (TR), Echo Time (TE) ; MRI Matrix Size: $K \times L \times M$, Histology
Matrix Size: W×H, * estimated, pseudo-whole mount: stitched adjacent quadrants; # : number;
Pr: Prostate, Lm: Landmarks, Ure: Urethra, Ca: Cancer

		Cohort C1	Cohort C2	Cohort C3
Cohort	Data Source	Internal	Public [23]	Public [24]
	Subject Number	116	16	25
	Number of slice	759	65	83
MRI	Manufacturer	GE	Siemens	Philips
	Coil type	Surface	Endorectal	Endorectal
	Sequence	T2w	T2w	T2w
	TR (s)	3.9-6.3	3.7-7.0	8.9
	TE (ms)	122-130	107	120
	Matrix Size: K,L	256-512	320	512
	Matrix Size: M	20-44	21-31	26
	Pixel Spacing (mm)	0.27-0.94	0.41-0.43	0.27
	Distance Between Slices (mm)	3.0-5.2	4	3
	Annotations	Pr, Ure, Lm	Pr, Ca, Ure	Pr, Ure
Histopathology	Stain	H&E	H&E	H&E
	Туре	whole-mount	pseudo-whole mount	whole-mount; Low-res
	Matrix Size: W,L	1572-7556	2368-6324	360-2401
	Pixel Spacing (mm)	0.008,0.016	0.007^{*}	0.021*
	Use 3D printed Molds	Yes	No	Yes
	Distance Between Slices (mm)	Same as MRI	Same as MRI	Same as MRI
	Annotations	Pr, Lm, Ure, Ca	Pr, Ure, Ca	Pr, Ure, Ca



FIG. S1: RAPSODI results for the registration of histopathology and T2w MRI slices in the digital phantom where an imperfect correspondence between the histopathology and T2w MRI slices exist (they are 2 mm apart from each other in the Sagittal and coronal planes, e.g., Figures 2d,2f): (a-b) Dice Coefficient; (c-d) Hausdorff Distance; (e-f) Urethra Deviation. (a,c,e) Experiment where only the rotation angle was varied between 0-40°; (b,d,f) The histopathology images were shrunk by 0-30% of the original size.



FIG. S2: Overlay of registered histopathology and T2w images (same as slice as shown in FIG. 4 Raw 2). Histopathology shown with a progressive transparency from (a) right-left, and (b) left-right with cancer outlines (green – Gleason Group 3, yellow-Gleason group 1 [25]).



FIG. S3: Qualitative results showing the registration for all the histopathology slices from apex to base in subject aaa0059 from Cohort C2. (Column 1) Input histopathology slices with cancer outlines (red); (Column 2) Histopathology slices registered to MRI; (Column 3) Overlay of the registered histopathology and corresponding T2w MRI with histopathology images shown transparent. (Column 4) Corresponding T2w MRI with cancer outlines obtained via RAPSODI (red) or provided by dataset authors (blue); (Column 5) Closeup into the cancer region with outlines shown at the same resolution as the T2w MRI. Asterisk (*) in row 4 indicates predominant features seen on both histopathology images and MRI that could be used as landmark to assess the registration.



FIG. S4: Slicer Interface

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