

Subdiffuse scattering and absorption model for single fiber reflectance spectroscopy: supplement

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Supplemental materials

Here we will demonstrate that the diffuse contribution to the SFR signal can be rewritten as a function of $\mu_s'd$ and μ_a/μ_s' . The diffuse reflectance per unit area as a function of radial coordinate ρ is given by Farrell *et al* as [1]:

$$R(\rho) = \frac{a'}{4\pi} \left(z_0 \left[\mu_{eff} + \frac{1}{r_1} \right] \frac{e^{-\mu_{eff}r_1}}{r_1^2} + (z_0 + 2z_b) \left[\mu_{eff} + \frac{1}{r_2} \right] \frac{e^{-\mu_{eff}r_2}}{r_2^2} \right) \quad (S1)$$

where $a' = \mu_s' / (\mu_s' + \mu_a)$ and μ_{eff} is the effective attenuation coefficient, $\mu_{eff} = \sqrt{\mu_a/D} = \sqrt{3\mu_a\mu_s'}$. The position of the point source in the medium is set at one reduced mean free path given by $z_0 = 1/\mu_s'$. The location of the 'virtual boundary', where the fluence rate has to be zero, is given by $z_b = 2AD$ where A is a parameter that depends on the refractive index mismatch between the fiber and the tissue [2]. We can express equation S1 in terms of dimensionless variables $x = \mu_s'd$, $y = \mu_a/\mu_s'$ and $\beta = \rho/d$. We also use the constant $c_A = 1 + 4A/3$ to compact the expression. Using these substitutions, the distances r_1 and r_2 are:

$$r_1^2 = z_0^2 + \rho^2 = \left(\frac{d}{x}\right)^2 + d^2 \cdot \beta^2 = \frac{d^2}{x^2} (1 + x^2\beta^2) \quad (S2)$$

$$r_2^2 = (z_0 + 2z_b)^2 + \rho^2 = \left(\frac{d}{x} + \frac{4A \cdot d}{3x}\right)^2 + d^2 \cdot \beta^2 = \frac{d^2}{x^2} \left(\left(1 + \frac{4A}{3}\right)^2 + x^2\beta^2 \right) \quad (S3)$$

and

$$\begin{aligned} \frac{d^2}{x^2} \cdot R(y, x\beta) = & \frac{(1+y)^{-1}}{4\pi} \left[\left(\frac{\sqrt{3y}}{1+(x\beta)^2} + \frac{1}{(1+(x\beta)^2)^{\frac{3}{2}}} \right) e^{-\sqrt{3y(1+(x\beta)^2)}} \right. \\ & \left. + c_A \left(\frac{\sqrt{3y}}{c_A^2+(x\beta)^2} + \frac{1}{(c_A^2+(x\beta)^2)^{\frac{3}{2}}} \right) e^{-\sqrt{3y(c_A^2+(x\beta)^2)}} \right] \end{aligned} \quad (S4)$$

Likewise, the probability distribution for distances on the fiber surface:

$$p(\rho) = \frac{16\rho}{\pi d^2} \cos^{-1}\left(\frac{\rho}{d}\right) - \frac{16}{\pi d} \left(\frac{\rho}{d}\right)^2 \sqrt{1 - \left(\frac{\rho}{d}\right)^2} \quad (S5)$$

can be rewritten as:

$$d \cdot p(\beta) = \left(\frac{16}{\pi} \beta \cos^{-1}(\beta) - \frac{16}{\pi} \beta^2 \sqrt{1 - \beta^2} \right) \quad (S6)$$

Such that the integrated reflectance

$$R_{dif} = \frac{\pi}{4} \cdot d^2 \cdot \int_0^d R(\rho) \cdot p(\rho, d) d\rho \quad (S7)$$

Is rewritten as:

$$R_{dif}(x, y) = \frac{\pi}{4} \cdot x^2 \cdot \int_0^1 R(y, \beta x) \cdot p(\beta) d\beta \quad (S8)$$

For the integration in this form with integration variable β ; the factors x and y are simply constants that are carried over. Consequently, in the resulting expression the absorption coefficient will appear in the ratio μ_a/μ_s' , and the fiber diameter will appear in the product $\mu_s'd$.

References

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2. F. Martelli, S. Del Bianco, A. Ismaelli, and G. Zaccanti, *Light Propagation through Biological Tissue and Other Diffusive Media: Theory, Solutions, and Software* (SPIE, 2009).