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Supplemental Information

Rapid Precision Functional Mapping

of Individuals Using Multi-Echo fMRI

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Discarded by ME-ICA (OC-ME - ME-ICA)



Retained by ME-ICA



Discarded by MGTR (ME-ICA - MGTR)

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Retained by ME-ICA + MGTR (Fully Denoised)



2 Figure S1. Related to Figure 3. An event-related approach for establishing appropriate separation 3 of neurobiological (T_2^* -dependent; "BOLD-like") and non-neurobiological (S_0 -dependent; not "BOLD-like") fMRI signals. During each instructed deep breathing scan, sub-ME01 was prompted 4 5 every 70 seconds (via a visual cue) to take a deep breath. There are prominent T₂*- and S₀-6 dependent signals with predictable spatiotemporal characteristics (each described in turn below) 7 associated with deep breaths that are visually evident when these scans are viewed as "gray 8 plots" (Power, 2017) paired with head motion and respiration belt traces. Respiration (measured 9 using an abdominal belt sampling at 50 Hz; z = z-score) and head motion (frame-wise 10 displacement; filtered realignment parameters and calculated over two TRs instead of one; as 11 done in (Power, 2019)) are shown at the top of Fig. S1 as a blue and red traces, respectively. The 12 time-courses of all points in the brain before and after each denoising step are shown below these 13 traces as gray plots (Power, 2017), with white and black representing high and low signal values, 14 respectively. Four isolated deep breaths, each accompanied by a transient spike in head motion 15 and followed by pauses in ventilation, are visually apparent in an otherwise eupneic trace. For 16 each of these respiratory events, there is an increase in head motion, which manifests visually in 17 the gray plot as a vertical "salt-and-pepper" band time-locked to the deep breath. Because head 18 movement primarily influences S₀ and not T₂*, these signals are discarded by ME-ICA (second 19 gray plot; red box), as expected. Deep breaths also alter the concentration of carbon dioxide in 20 blood, however, which in turn influences cerebral blood flow (Hall and Guyton, 2011), and 21 therefore T_2^* and not S₀. Vertical black bands (represented most strongly in gray matter) lasting 22 tens of seconds after each deep breath, consistent with the expected cortex-wide decrease in 23 blood flow after a transient increase in ventilation, are retained by ME-ICA (third gray plot; blue 24 box). While this observation indicates the desired retention of T_2^* -dependent signals, it also 25 highlights a limitation that is inherent to ME-ICA. Specifically, that although cortex-wide 26 fluctuations in signal due to changes in respiration are not a signal of interest per se, they are 27 retained in the ME-ICA denoised time-series nonetheless because they are T2*-dependent (in 28 addition, ICA techniques cannot easily separate spatially diffuse signals from focal signals; see 29 (Power et al., 2019; Power et al., 2018)). Thus, additional denoising procedures (e.g., mean grey 30 matter time-series regression; MGTR) are required to remove them. ME-ICA paired with MGTR 31 vields an fMRI time-series free of the confounding influence of head motion (as well as other S₀-32 dependent artifacts) and respiration (fifth gray plot). These gray plots indicate appropriate 33 separation of S_0 - and T_2 *-dependent signals of interest using ME-ICA and MGTR. To better 34 understand the spatiotemporal profile of the signals that were discarded and retained by ME-ICA, 35 we extracted the average 40 second (-10 seconds to 30 seconds) epoch surrounding deep

breaths. These data are displayed on the subject's inflated cortical surface at the bottom of Fig. S1. The motion-related artifact at t=0 (this is the S₀-dependent "salt-and-pepper" band bounded by the red box in the OC-ME – ME-ICA gray plot; red box) is present in the OC-ME time-series but not the ME-ICA denoised time-series. The spatially diffuse decrease in signal begins approximately 14 seconds after the deep breath cue (this is the T_2^* -dependent vertical black band bounded by the blue box in the ME-ICA gray plot), and is retained in the ME-ICA time-series and only removed by MGTR.



51 Figure S2. Related to Figure 3. FC reliability values calculated using data from the first ten 52 minutes of scanning (the minimum scan duration across all four datasets) plotted relative to the 53 percentage of data retained after motion-censoring in Fig. S2A. Error bars indicate standard 54 deviation. A subset of MSC participants (purple circles) exhibiting high levels of head movement 55 (and less data retained after motion-censoring) exhibited the worst FC reliability. OC-ME + ME-56 ICA data (the red circles in Fig. S2A) yielded better FC reliability values than MyConnectome and 57 CAST single-echo data with an equivalent level of motion-censoring. An alternative set of time x 58 reliability curves (where the x-axis represents the amount data retained after motion-censoring 59 and not the scan duration prior to motion-censoring) is presented in Fig. S2B. This analysis 60 yielded a very similar set of curves as in Fig. 3B (with the exception of participants exhibiting

61	especially high levels of head motion; e.g., sub-MSC08). Collectively, these two analyses indicate
62	that the enhanced reliability of FC measurements in the N=4 multi-echo dataset cannot be
63	explained by head movement levels.
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Figure S3. Related to Figure 3. Reliability of functional connectivity estimates in sub-ME03 and sub-ME04. The purpose of this analysis was to test whether the enhanced FC reliability observed in sub-ME01 and sub-ME02 could be replicated in other individuals. Each participant underwent 3 hours of scanning using a multi-echo fMRI sequence (12 x 14.5 minute scans) over a period of six months. Reliability maps were calculated using the three different denoising strategies, leveraging both (OC-ME + ME-ICA), one (OC-ME + ICA-AROMA), or no (TE₂ + ICA-AROMA) advantages of a multi-echo fMRI sequence. Time x reliability curves (Fig. S3B) show the average reliability value obtained in cortex, subcortical structures (accumbens, amygdala, caudate, hippocampus, pallidum, putamen, and thalamus), and cerebellum given different scan durations. Curves from the three independent single-echo datasets were again provided as comparators). This analysis yielded results consistent with those observed in sub-ME01 and sub-ME02 - the OC-ME and ME-ICA procedures enhanced the reliability of FC. When using the full scan duration, 32% and 72% of cortex exhibited reliable (> 0.7) FC in sub-ME03 and sub-ME04, respectively. One sample t-tests revealed that 10 minutes of OC-ME + ME-ICA data yielded FC estimates that were more reliable than those derived from 3x as much single-echo Midnight Scan Club and Cast-induced Plasticity data in cortex [t(12) = 3.49, p=0.004, Cohen's d = 0.97] and cerebellum [t(12)] = 3.67, p=0.003, Cohen's d = 1.03]. In subcortex, 10 minutes of OC-ME + ME-ICA data yielded rsFC estimates more reliable than those derived from an equivalent amount of single-echo data [t(12) = 6.20, p<0.001, Cohen's d = 0.81]. These findings are consistent with those from our analysis of sub-ME01 and sub-ME02 (Fig. 3).



- 128 **Figure S4.** Related to Figure 3. Head movement for all four study participants summarized
- 129 using concatenated frame-wise displacement (FD) traces. Multiple formulations of FD are
- 130 shown to convey the effect of the stopband filter ("Filtered FD 1-TR" vs. "Not Filtered FD-1TR")
- 131 and over 2-TRs ("Filtered FD 2-TRs" versus "Filtered FD 1-TR"). Note that sub-SE01 is
- 132 participant sub-ME01, but scanned using a separate fast-TR single-echo sequence.



- 135 **Figures S5.** Related to Figure 4. FC of seed region in left caudate in participant ME01 when using
- 136 different amounts of multi-echo (OC-ME + ME-ICA) and single-echo data (TE₂ + ICA-AROMA,
- 137 Fast-TR SE + ICA-AROMA) from 3 example scans. S = scan.



- 140 **Figures S6.** Related to Figure 4. FC of seed region in left dorsal somatomotor cortex in participant
- 141 ME01 when using different amounts of multi-echo (OC-ME + ME-ICA) and single-echo data (TE₂
- 142 + ICA-AROMA, Fast-TR SE + ICA-AROMA) from 3 example scans. S = scan.



- 145 **Figures S7.** Related to Figure 4. FC of seed region in ventral somatomotor cortex in participant
- 146 ME01 when using different amounts of multi-echo (OC-ME + ME-ICA) and single-echo data (TE₂
- 147 + ICA-AROMA, Fast-TR SE + ICA-AROMA) from 3 example scans. S = scan.



150	Figures S8. Related to Figure 4. FC of seed region in lateral prefrontal cortex in participant ME01
151	when using different amounts of multi-echo (OC-ME + ME-ICA) and single-echo data (TE ₂ + ICA-
152	AROMA, Fast-TR SE + ICA-AROMA) from 3 example scans. $S = scan$.
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- **Table 1.** Related to Star Methods. Summary of the sequence parameters associated with each
- 184 of the datasets used in this investigation.

Dataset	Scanner	Spatial	Repetition	Echo Time	Multi-	Number of
	Model	Resolution	Time (TR)	(TE)	band	volumes
					Factor	
Midnight Scan	Siemens	4 x 4 x 4	2200 ms	TE ₁ : 27 ms	None	818
Club	TRIO 3T	mm				
Cast-induced	Siemens	2.6 x 2.6 x	1100 ms	TE₁: 33 ms	4	1636
Plasticity	Prisma 3T	2.6 mm				
MyConnectome	Siemens	2.4 x 2.4 x	1160 ms	TE₁: 30 ms	4	518
	Skyra 3T	2.4 mm				
Multi-Echo	Siemens	2.4 x 2.4 x	1355 ms	TE ₁ : 13.40 ms	6	640
	Magnetom	2.4 mm		TE ₂ : 31.11 ms		
	Prisma 3T			TE ₃ : 48.82 ms		
				TE ₄ : 66.53 ms		
				TE ₅ : 84.24 ms		
"Fast-TR"	Siemens	2.4 x 2.4 x	800 ms	TE ₁ : 30 ms	6	1084
Singe-Echo	Magnetom	2.4 mm				
-	Prisma 3T					