

# DeepACSON Automated Segmentation of White Matter in 3D Electron Microscopy

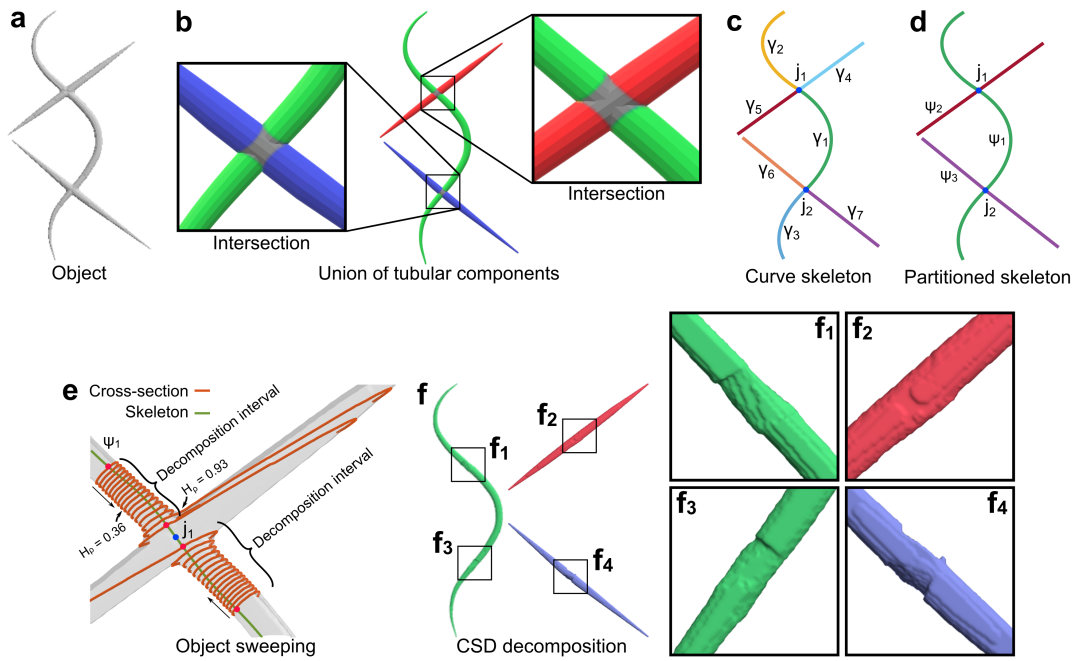
Ali Abdollahzadeh<sup>1</sup>, Ilya Belevich<sup>2</sup>, Eija Jokitalo<sup>2</sup>, Alejandra Sierra<sup>1\*+</sup>, and Jussi Tohka<sup>1+</sup>

<sup>1</sup>A. I. Virtanen Institute for Molecular Sciences, University of Eastern Finland, Kuopio, Finland

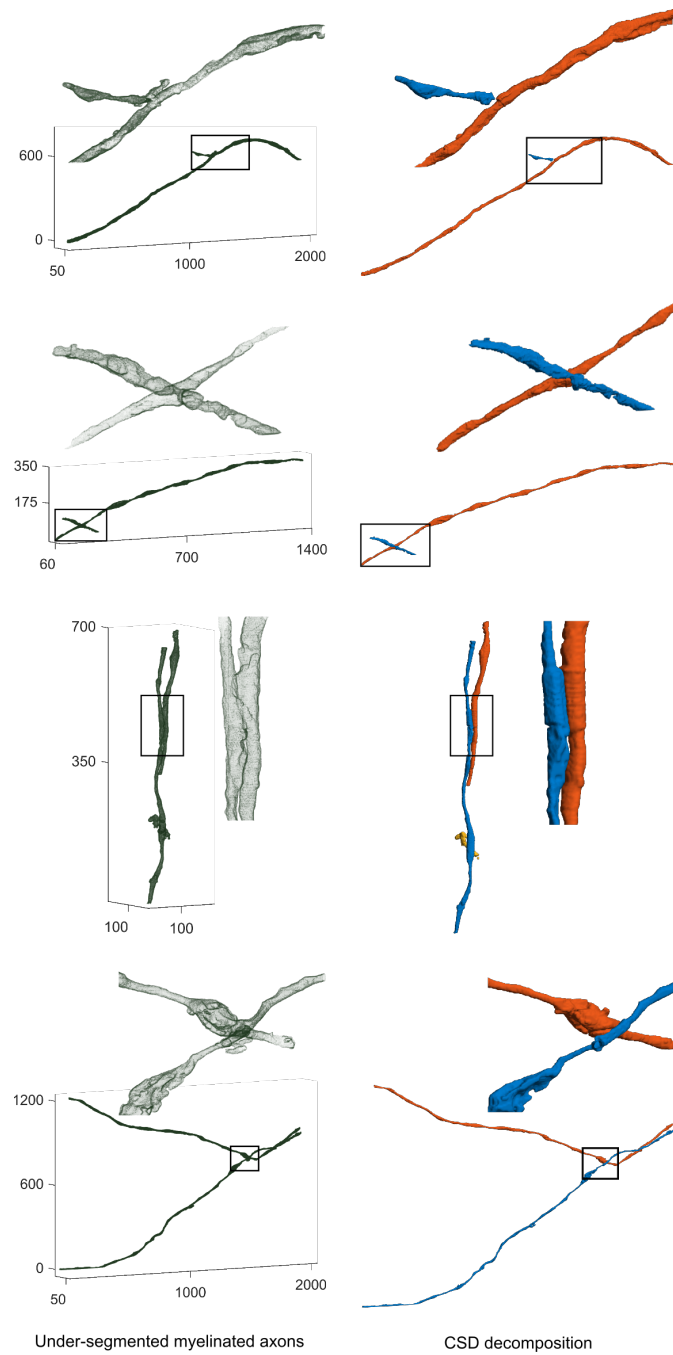
<sup>2</sup>Electron Microscopy Unit, Institute of Biotechnology, University of Helsinki, Helsinki, Finland

\*alejandra.sierralopez@uef.fi

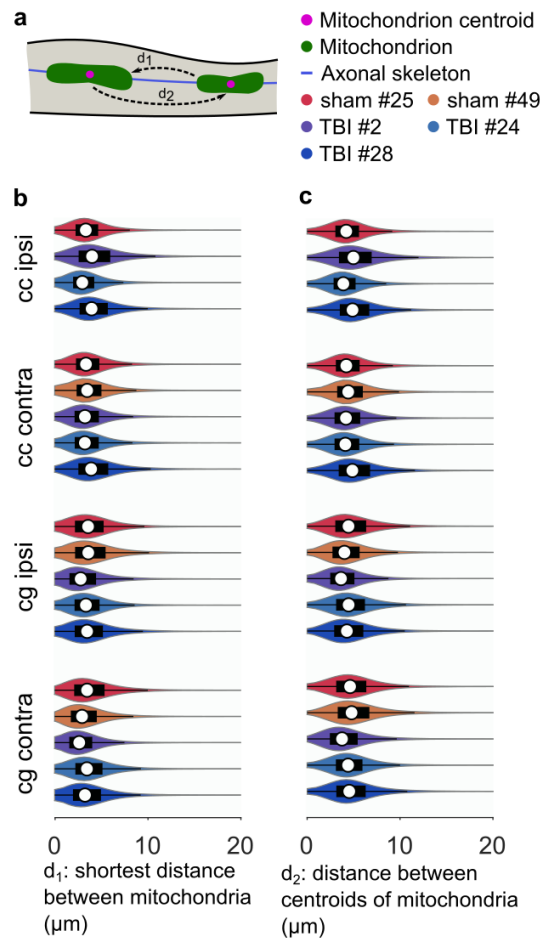
+These authors contributed equally



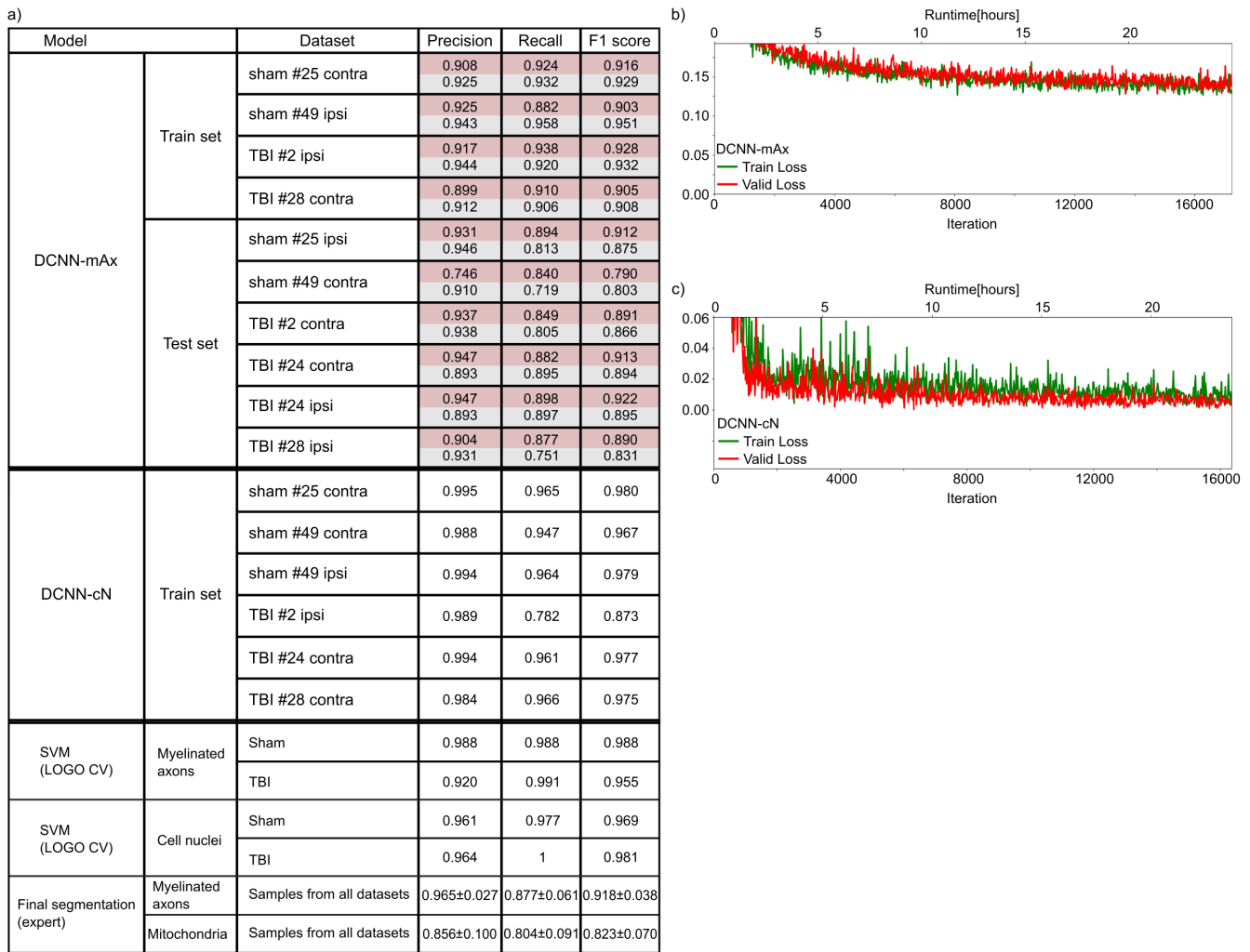
**Supplementary Figure S1.** Cylindrical shape decomposition algorithm<sup>1</sup>. **(a)** An object is a union of several semantic-components. **(b)** These semantic-components of the object in **(a)** are color-coded. Intersections of the semantic-components are colored grey. **(c)** The curve skeleton of the synthetic object in **(a)** is the union of all skeleton branches. Skeleton branches are color-coded and denoted as  $\gamma$ . We defined a skeleton junction-point  $j$  as such a point that skeleton branches connect. Junction-points are shown as blue-filled-circles. **(d)** We found  $m$  maximal length sub-skeletons denoted as  $\psi$  via minimizing an orientation cost-function. The sub-skeletons are color-coded. **(e)** On a sub-skeleton  $\psi$  and in the proximity of a junction-point  $j \in \psi$ , we defined two decomposition intervals. The boundaries of decomposition intervals are shown with red-filled-circles. In each interval, the cross-section of the object was swept along  $\psi$  and towards the joint  $j$  to find a critical point. At a critical point, the normalized Hausdorff distance  $H_p$  between a cross-sectional contour and the mean of visited cross-sectional contours exceeds  $\theta_H$ . Sweeping directions are shown with arrows. **(f)** We cut the object at critical points to obtain object-parts. The object-parts along the same sub-skeleton were assigned the same label to construct a semantic-component. The semantic-components were further reconstructed between their comprising object-parts using generalized cylinders, magnified in **(f<sub>1</sub>-f<sub>4</sub>)**. The synthetic object in **(a)** comprised of seven object-parts, and our algorithm decomposed it into three semantic-components.



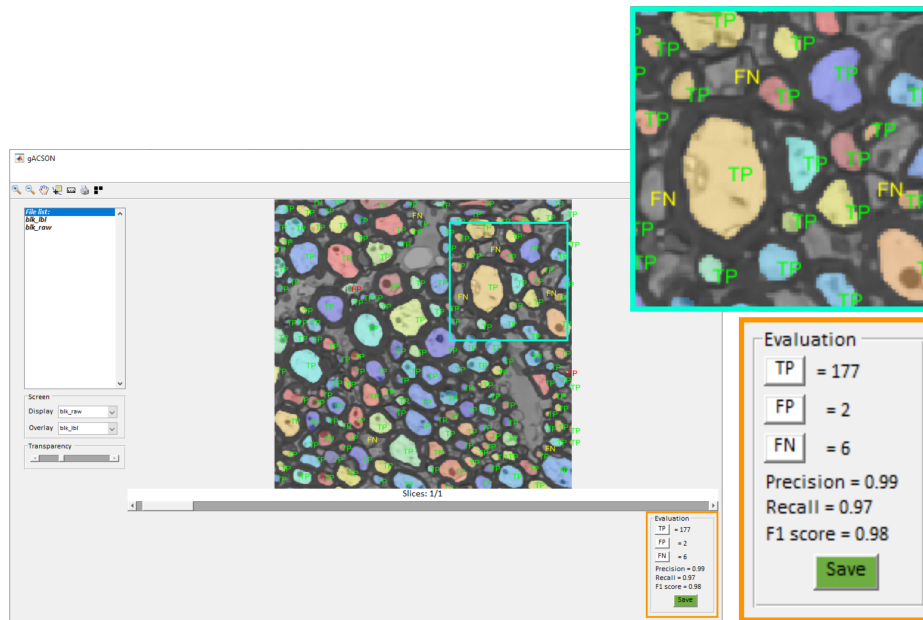
**Supplementary Figure S2.** Decomposition of Under-segmented myelinated axons into their semantic axonal components using the CSDalgorithm<sup>1</sup>.



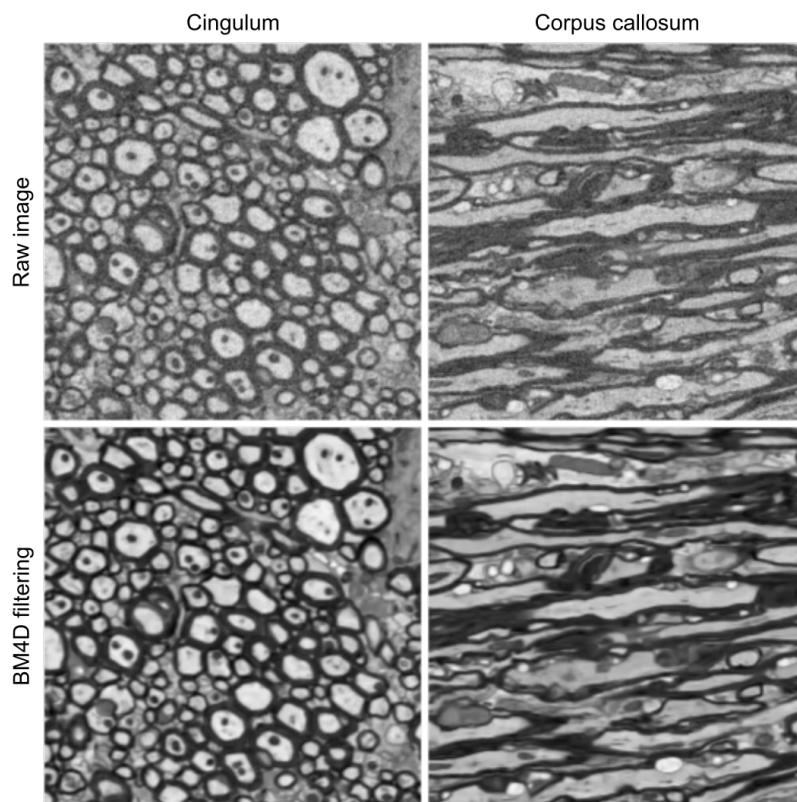
**Supplementary Figure S3.** Quantification of the inter-mitochondrial distance. **(a)** We defined the inter-mitochondrial distance in two, alternate ways: 1) we projected the entirety of mitochondria on the axonal skeleton and measured the shortest geodesic distance between two consecutive mitochondria ( $d_1$ ); 2) we projected the centroids of mitochondria on the axonal skeleton and measured the geodesic distance between the consecutive projected centroids ( $d_2$ ). **(b, c)** We compared the inter-mitochondrial distance, **(b):**  $d_1$  definition, **(c):**  $d_2$  definition), between sham-operated and TBI rats. We did not find significant differences between the groups in any of the brain areas. On each bean plot, the central mark indicates the median, and the left and right edges of the box indicate the 25<sup>th</sup> and 75<sup>th</sup> percentiles, respectively. The whiskers extend to the most extreme data points not considered outliers. The colors correspond with the animal ID.



**Supplementary Figure S4.** DeepACSON evaluation scores. (a) We evaluated DeepACSON neural networks on test sets using Precision, Recall, and F1 score metrics. The same metrics over the training set are provided as a reference. No large differences between the training and test metrics exist, demonstrating in part that the network did not overfit. In the DCNN-mAx section, red rows show evaluations of myelin semantic segmentation, and gray rows show evaluations of the semantic segmentation of intra-axonal spaces. The DCNN-cN training set included only ten cell nuclei, and we used all the volumes for training. The performance of SVMs was evaluated using leave-one-group-out (LOGO) cross-validation (CV). An expert evaluated the final segmentation of myelinated axons and mitochondria as an added qualitative measure over the entire pipeline. The maximum value of all scores is one. (b) The training and validation losses of DCNN-mAx. (c) The training and validation losses of DCNN-cN. We trained the networks on an NVIDIA Tesla P100-16 GB GPU for one day.



**Supplementary Figure S5.** DeepACSON evaluation. We developed a GUI-based software tool, gACSON<sup>2</sup>, in Matlab to load and visualize thesegmentation for proofreading. gACSON is designed for the visualization of the large-scale image-datasets/segmentation. Using gACSON, an expert evaluated the DeepACSON segmentation of myelinated axons and mitochondria at the object-level. We randomly sampled each low-resolution dataset and its corresponding segmentation by non-overlapping images of size  $300 \times 300$  voxels. The sampled images were quantified for the number of true-positives (TP), false-positives (FP), and false-negatives (FN) to calculate the precision, recall, and F1 score. The expert had no access to the dataset ID nor the sampling location.

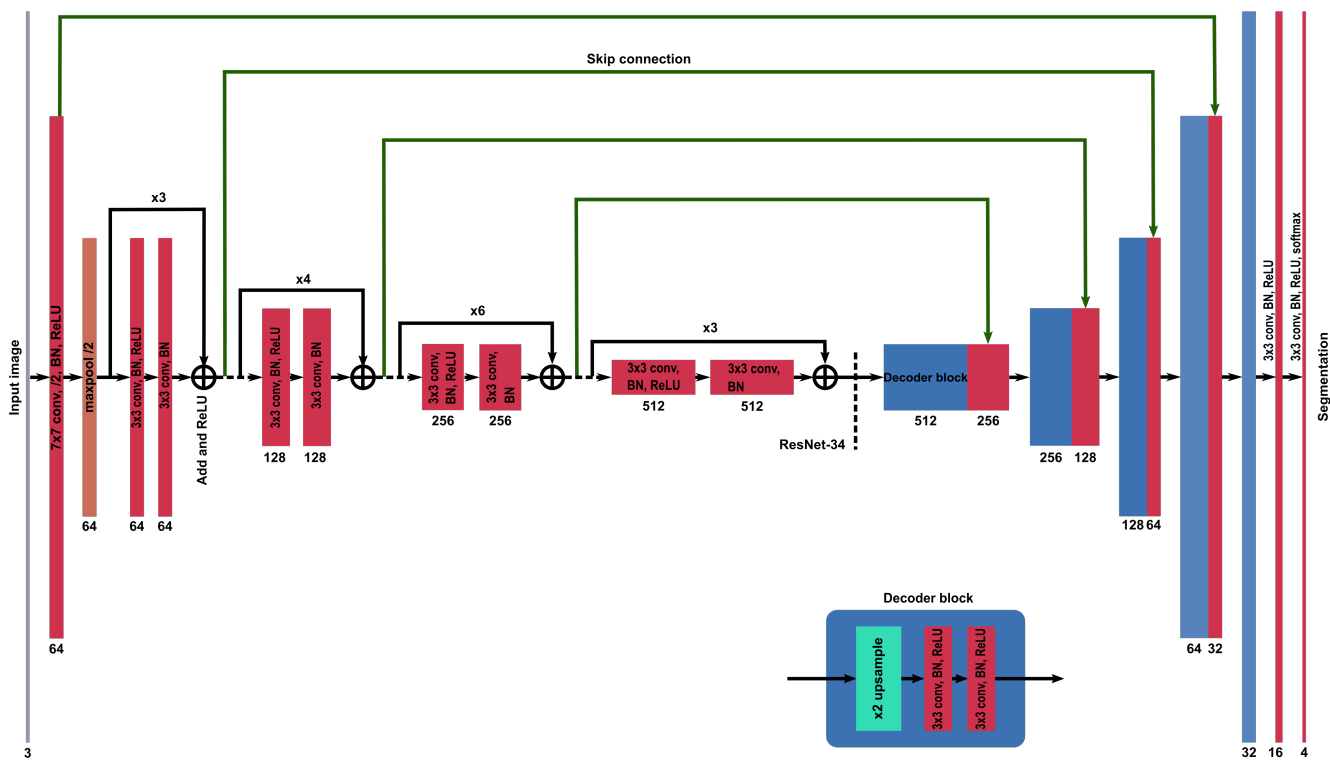


**Supplementary Figure S6.** BM4D<sup>3</sup> filtering of the low-resolution SBEM datasets. BM4D recognized the noise as Gaussian-distributed with the standard deviation in the range [17, 22] in our low-resolution SBEM datasets. Shown images were acquired from the cingulum and corpus callosum of low-resolution sham #25 dataset.

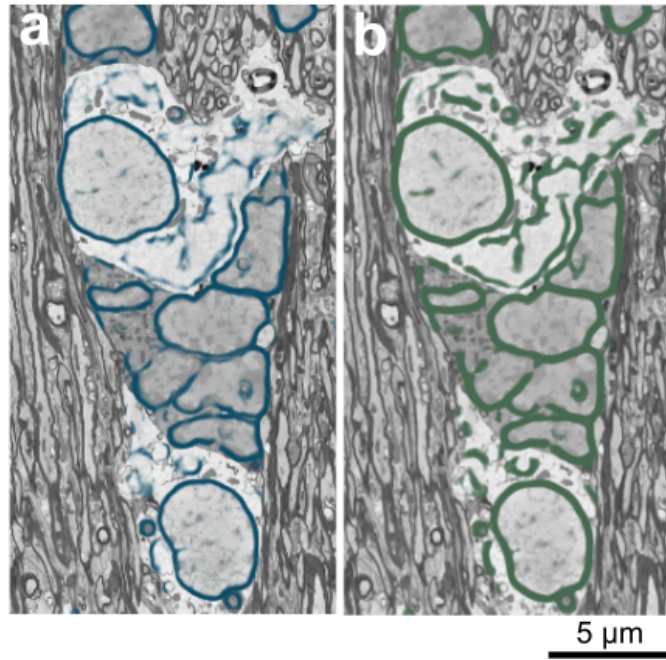


**Supplementary Figure S7.** The architecture of DCNNs used in DeepACSON. We used the same architecture for DCNN-m Ax and DCNN-cN. The size of the convolutional kernels is denoted as  $Conv(x,y,z)$ . The number of channels/feature maps created from a layer of convolutional kernels is denoted by @ $n$ . The size of the max pooling operation is denoted as  $Max\ pool(x,y,z)$ .





**Supplementary Figure S8.** A U-Net<sup>4</sup> architecture with residual modules. We used a ResNet-34<sup>5</sup>, pre-trained on the ImageNet dataset<sup>6</sup>, as the encoder of the U-Net. In the encoding path of the U-Net, the height and width of the feature maps were halved, and the depth of the feature maps was doubled. In the decoding path of the U-Net, the height and width of the feature maps were doubled, and the depth of the feature maps was halved. The basic residual blocks of ResNet-34 were constructed on  $3 \times 3$  convolutional layers, using rectified linear unit (ReLU) as the activation function, and batch normalization (BN)<sup>7</sup>. The basic decoding blocks applied nearest-neighbor interpolation for up-sampling the feature maps to recover the spatial resolution of input images. Feature maps generated in the encoding path were concatenated to the corresponding feature maps in the decoding path by the skip connections. The model was trained by minimizing cross-entropy loss.



**Supplementary Figure S9.** Frangi filtering<sup>8</sup> the probability map of the membrane of cell nuclei. **(a)** The probability map of the membrane of cell nuclei returned by DCNN-cN. **(b)** Application of Frangi filtering on **(a)**.

**Supplementary Table S1.** Characteristics of the low-resolution (LR) and high-resolution (HR) SBEM datasets. We collected the low-resolution images from the ipsi- and contralateral corpus callosum and cingulum for each rat. The low-resolution images from the ipsilateral hemisphere of the sham #49 rat included only the cingulum. The high-resolution images were collected from the ipsi- and contralateral corpus callosum. The size of datasets is given in voxels ( $x,y,z$ ).

Condition	Rat ID	LR-size (voxel)	LR (nm <sup>3</sup> )	HR-size (voxel)	HR (nm <sup>3</sup> )
Sham	#25 contra	2044 × 4096 × 1306	50 × 50 × 50	1042 × 1048 × 285	13.8 × 13.8 × 50
	#25 ipsi	4096 × 2048 × 1384	50 × 50 × 50	1049 × 1076 × 285	15.4 × 15.4 × 50
	#49 contra	4096 × 2048 × 1882	50 × 50 × 50	1081 × 1053 × 285	18.3 × 18.3 × 50
	#49 ipsi	2048 × 2048 × 1210	50 × 50 × 50	1037 × 1058 × 285	13.0 × 13.0 × 50
TBI	#2 contra	4096 × 2048 × 1086	50 × 50 × 50	1048 × 1124 × 285	15.0 × 15.0 × 50
	#2 ipsi	2154 × 4134 × 620	50 × 50 × 50	1343 × 1316 × 285	15.0 × 15.0 × 50
	#24 contra	4091 × 2028 × 1348	50 × 50 × 50	1289 × 1280 × 285	15.0 × 15.0 × 50
	#24 ipsi	2946 × 2162 × 1250	50 × 50 × 50	1290 × 1295 × 285	15.0 × 15.0 × 50
	#28 contra	4096 × 2048 × 1278	50 × 50 × 50	1076 × 1051 × 285	16.5 × 16.5 × 50
	#28 ipsi	4075 × 2000 × 1300	50 × 50 × 50	1035 × 1056 × 285	16.5 × 16.5 × 50

**Supplementary Table S2.** Volumetry of ultrastructures. The volume of myelin and myelinated axons was expressed as a percentage of the corresponding SBEM dataset. The volume fraction that was occupied by a cell body/process varied between the datasets. Therefore, a direct comparison of the volumes is not reasonable.

Treatment	Tissue	Rat ID	Myelin (%)	mAxons (%)	Cell nuclei	mAxons	Mitochondria
Sham	Cc	#25 contra	48.74	22.24	218	42318	168512
		#25 ipsi	49.07	23.17	214	43209	175508
		#49 contra	43.53	23.39	161	30723	116123
		#49 ipsi	-	-	-	-	-
TBI	Cc	#2 contra	46.42	19.56	133	25865	91997
		#2 ipsi	44.13	19.95	124	29883	58089
		#24 contra	51.38	19.40	221	49866	172241
		#24 ipsi	52.20	22.94	102	23256	96032
		#28 contra	42.32	19.31	226	34804	104102
		#28 ipsi	40.16	18.61	213	35553	114204
Sham	Cg	#25 contra	52.61	29.14	90	16076	58583
		#25 ipsi	49.72	28.58	97	15868	62838
		#49 contra	50.18	28.19	70	10537	55825
		#49 ipsi	48.42	26.49	126	16932	71742
TBI	Cg	#2 contra	49.14	22.76	120	23039	97777
		#2 ipsi	42.98	12.19	100	14094	21722
		#24 contra	49.32	21.98	76	16495	58180
		#24 ipsi	41.26	14.72	108	20374	63798
		#28 contra	42.68	22.89	131	17510	77116
		#28 ipsi	39.79	16.58	167	18297	48830

**Supplementary Table S3.** Computation time. M1: Intel Core i7 6700 CPU 3.4 GHz with 64 GB RAM. M2: 2 × Intel Xeon E5 2630 CPU 2.4 GHz machine with 512 GB RAM. M3: NVIDIA Tesla P100-16 GB GPU. Because the size of datasets and the number of instances segmented in each dataset are different, we measured the computation time based on the sham #25 dataset in the last column.

Process	Machine	Time	Time/dataset (h)
BM4D filtering	M1 - MATLAB R2017b	0.056 MB/s	54.23
Training DCNN-mAx	M3 - Python 2.7	24 h	-
Training DCNN-cN	M3 - Python 2.7	24 h	-
DCNN-mAx inference	M3 - Python 2.7	0.297 MB/s	10.23
DCNN-cN inference	M3 - Python 2.7	0.299 MB/s	10.16
CSD	M2 - Python 2.7	~ 113.8 s/myelinated axon	44.66
Myelinated Axon feature extraction	M2 - MATLAB R2017b	~ 15 s/myelinated axon	5.89
2D Frangi filtering	M1 - MATLAB R2017b	0.267 MB/s	11.38
Cell nucleus feature extraction	M1 - MATLAB R2017b	~ 30 s/nucleus	5.76
SVM Bayesian optimization	M1 - MATLAB R2017b	173 s	-
SVM inference	M1 - MATLAB R2017b	~ 4.4 $\mu$ s/component	$5.14 \times 10^{-5}$

## Supplementary References

1. Abdollahzadeh, A., Sierra, A. & Tohka, J. Cylindrical shape decomposition for 3D segmentation of tubular objects. *CoRR abs/1911.00571* (2019). URL <http://arxiv.org/abs/1911.00571>.
2. Behanova, A., Abdollahzadeh, A., Sierra, A. & Tohka, J. gACSON software to visualize, process, and analyze three-dimensional electron microscopy images (2020). URL <https://github.com/AndreaBehan/g-ACSON>. DOI 10.5281/zenodo.3693563.
3. Maggioni, M., Katkovnik, V., Egiazarian, K. & Foi, A. Nonlocal Transform-Domain Filter for Volumetric Data Denoising and Reconstruction. *IEEE Transactions on Image Process.* **22**, 119–133 (2013). URL <http://ieeexplore.ieee.org/document/6253256/>. DOI 10.1109/TIP.2012.2210725.
4. Ronneberger, O., Fischer, P. & Brox, T. U-Net: Convolutional Networks for Biomedical Image Segmentation. In Navab, N., Hornegger, J., Wells, W. & Frangi, A. (eds.) *MICCAI 2015*, 234–241 (Springer International Publishing, Cham, 2015). URL [http://link.springer.com/10.1007/978-3-319-24574-4\\_28](http://link.springer.com/10.1007/978-3-319-24574-4_28). DOI 10.1007/978-3-319-24574-4\_28.
5. He, K., Zhang, X., Ren, S. & Sun, J. Deep Residual Learning for Image Recognition. In *2016 IEEE Conference on Computer Vision and Pattern Recognition (CVPR)*, vol. 2016-Decem, 770–778 (IEEE, 2016). URL <http://ieeexplore.ieee.org/document/7780459/>. DOI 10.1109/CVPR.2016.90.
6. Jia Deng *et al.* ImageNet: A large-scale hierarchical image database. In *2009 IEEE Conference on Computer Vision and Pattern Recognition*, 248–255 (IEEE, 2009). URL <http://ieeexplore.ieee.org/lpdocs/epic03/wrapper.htm?arnumber=5206848>. DOI 10.1109/CVPRW.2009.5206848.
7. Ioffe, S. & Szegedy, C. Batch normalization: Accelerating deep network training by reducing internal covariate shift. *32nd Int. Conf. on Mach. Learn. ICML 2015* **1**, 448–456 (2015).
8. Frangi, A. F., Niessen, W. J., Vincken, K. L. & Viergever, M. A. Multiscale vessel enhancement filtering. In Wells, W., Colchester, A. & Delp, S. (eds.) *Medical Image Computing and Computer-Assisted Intervention — MICCAI'98. MICCAI 1998. Lecture Notes in Computer Science*, 130–137 (Springer, Berlin, Heidelberg, 1998). URL <http://link.springer.com/10.1007/BFb0056195>. DOI 10.1007/BFb0056195.