

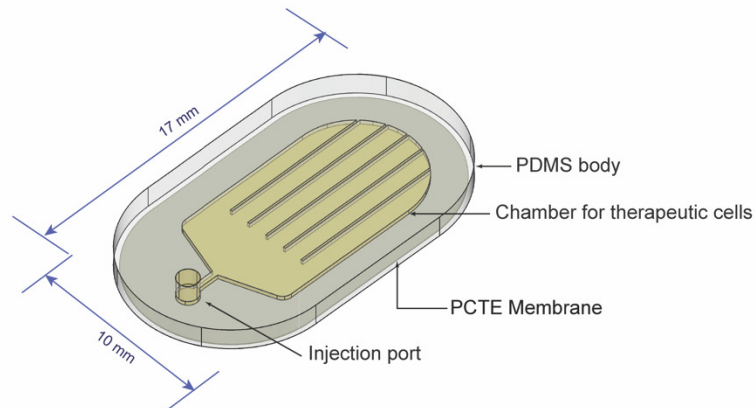
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Supplementary Table 1. Atomic composition of device surface measured using XPS (mean \pm s.e.m, n=3).

Material	C%	O%	Si%	N%	S%	P%
Native PDMS	44.4 \pm 1.76	28.3 \pm 1.8	27.2 \pm 0.13	-	-	-
CBMA	48.5 \pm 0.36	26.19 \pm 2.4	19.55 \pm 1.00	5.75 \pm 2.88	-	-
SBMA	56.73 \pm 2.01	27.78 \pm 0.57	9.24 \pm 2.01	3.26 \pm 0.63	3.14 \pm 0.35	-
MPC	53.02 \pm 2.67	30.57 \pm 1.68	8.86 \pm 2.53	3.57 \pm 0.56	-	3.82 \pm 0.52
THPT	60.6 \pm 0.31	19.8 \pm 0.73	9.6 \pm 1.25	9.9 \pm 1.12	-	-

a 3D model of the device



b Confocal microscopy imaging of the device

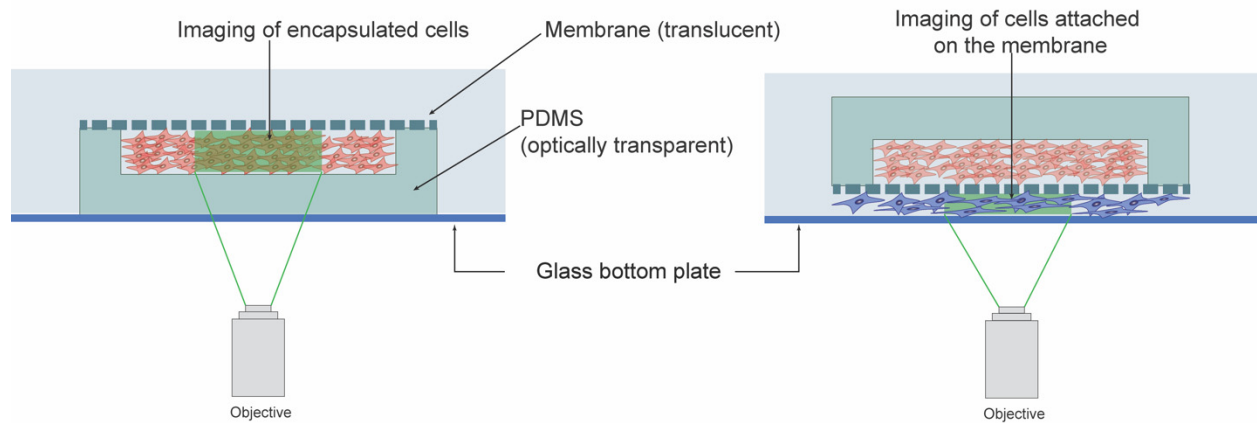


Figure S1: Design of the macrodevice. a) 3D CAD model of the device showing its various components. The PDMS is 1mm thick while the cell chamber is 150 microns in height. The drawing is to scale and shown in isometric view. b) Schematic showing the experimental setup for imaging the encapsulated cells and the cells attached to the device. The PDMS being transparent allows for direct imaging of the cells inside the device, while the cells attached to the membrane can be imaged by placing the device membrane-side-down on the imaging platform.

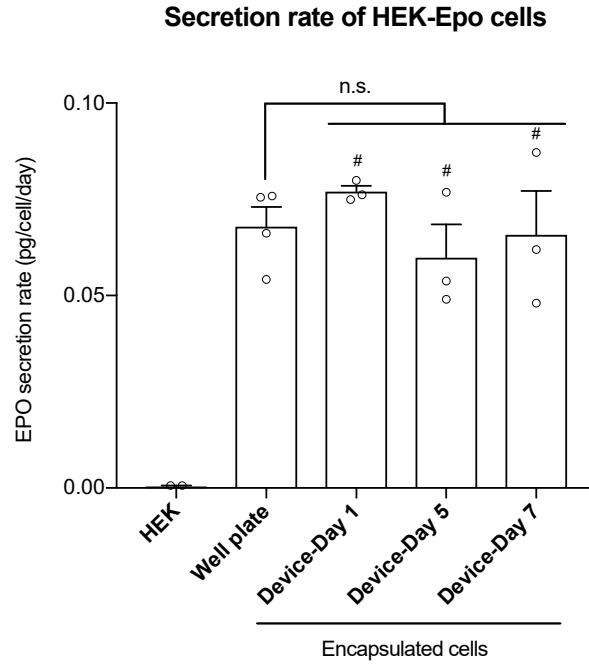
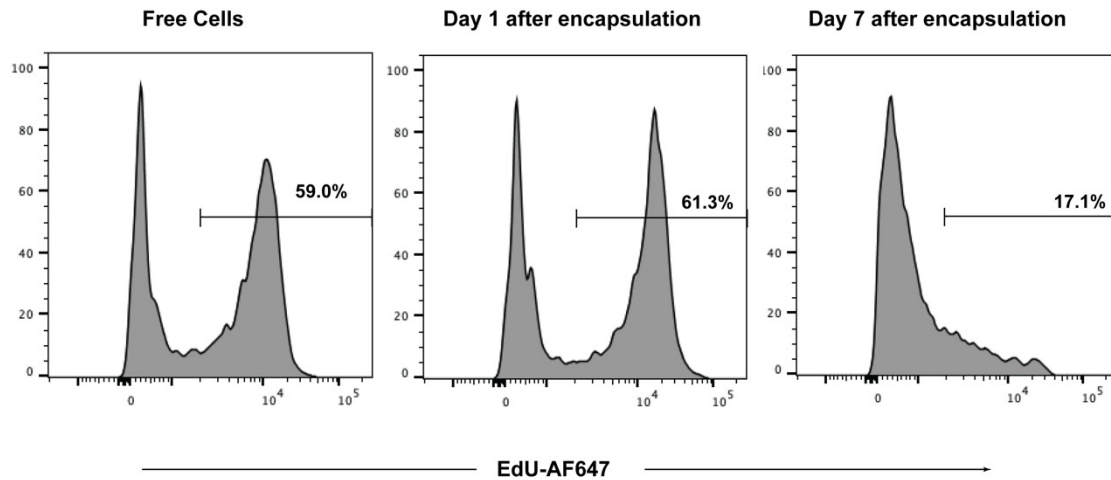


Figure S2: Secretion rate of EPO from native HEK cells and transformed cells (HEKEpo cells). Cells were cultured either free or within macrodevices in vitro, and the total amount of EPO in the culture supernatant over 24 hours was measured using ELISA assay. The total number of cells was measured using CellTiter Glo assay and used for normalizing EPO secretion values. Error bar: mean \pm s.e.m (n = 3 biological replicates). One-way ANOVA with Bonferroni multiple comparison correction. #, $P > 0.999$ indicated significance value for comparison with 'Well plate' group.

a



b

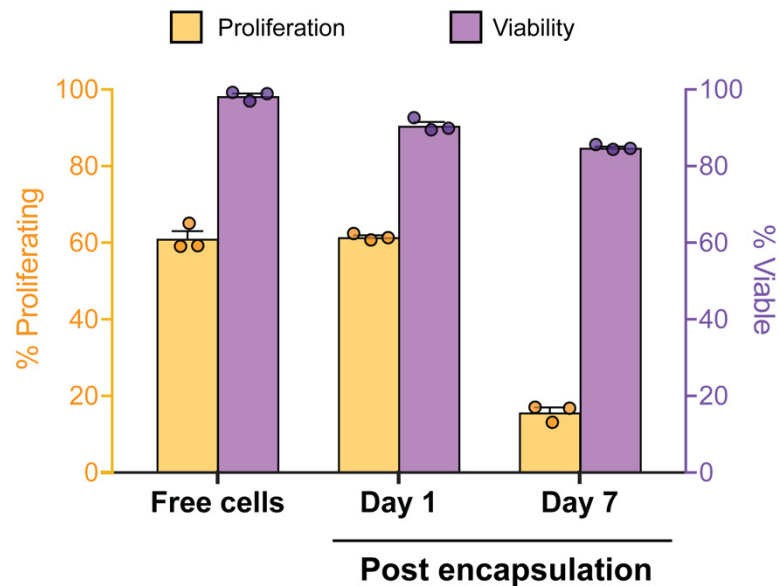


Figure S3: Proliferation and viability of the HEK293T cells inside the device. HEK293T cells were encapsulated inside macrodevices and cultured in vitro. Proliferation of cells was measured by assaying for the amount of EdU incorporated over 2 hr (a), while viability was assayed using Sytox blue staining of the cells. a) Flow cytometry images of cells showing EdU incorporation within proliferating cells inside the macrodevice. Normal cells cultured in well plates (not encapsulated) is shown for comparison. b) Combined data of proliferation and viability of free and encapsulated cells. Error bars: mean \pm s.e.m (n=3).

Imaging cell escape from macrodevice

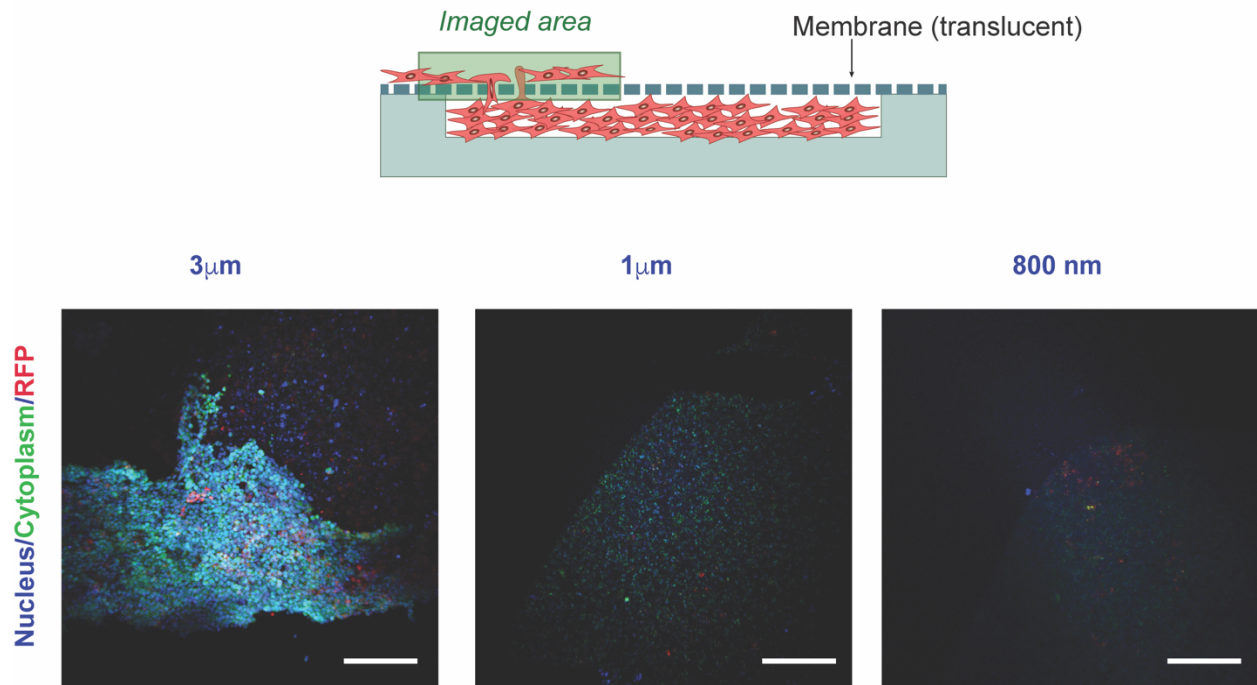


Figure S4: Escape of encapsulated cells from macrodevices. Macrodevices made with membranes of varying pore size (0.8 μm, 1 μm, and 3 μm) were loaded with 2×10^6 HEK293T cells per device and cultured in vitro for one week. The cells were then stained with Calcein AM (cytosol/viability) and Hoechst 33342 (nucleus). Confocal microscopy was used to image the membrane surface as (shown in the schematic above) to identify cells escaping from the membrane pores. Representative z-stacked images shown in the bottom pane reveal encapsulated cells escaping from the 3 μm membranes (seen as the bright patch of cells growing on the membrane surface) while no cell escape was seen with 1 μm or lower membranes. Experiments were repeated twice with similar results. Scale bar: 100 μm.

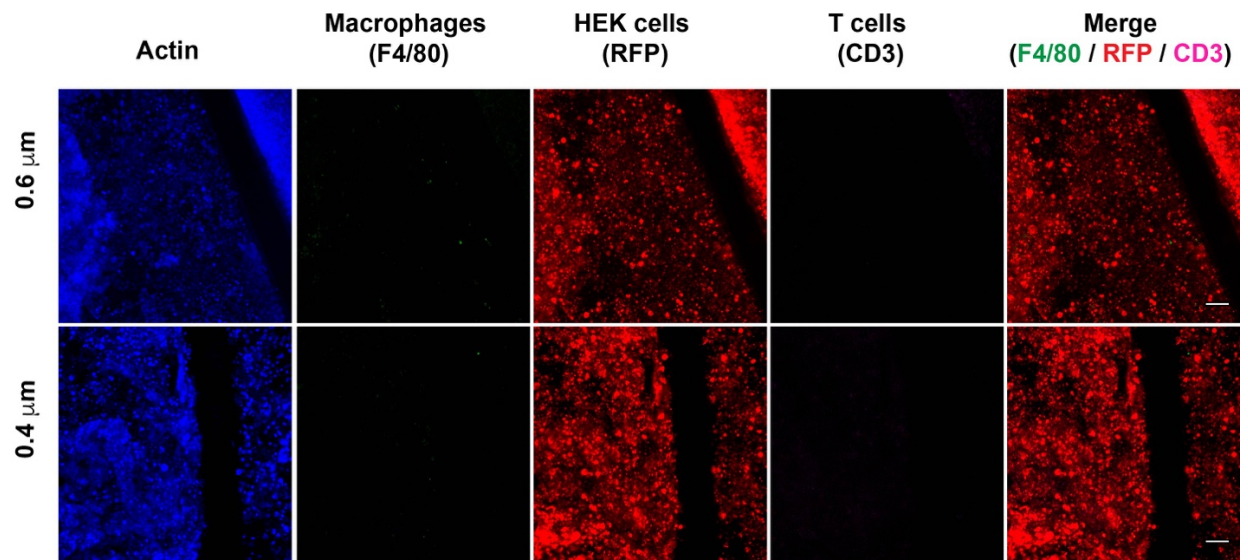


Figure S5: Representative z-stack images of devices in **Figure 2** with membrane pore sizes of 0.6 μm and 0.4 μm . Experiments were repeated twice with similar results. Scale bar 100 μm .

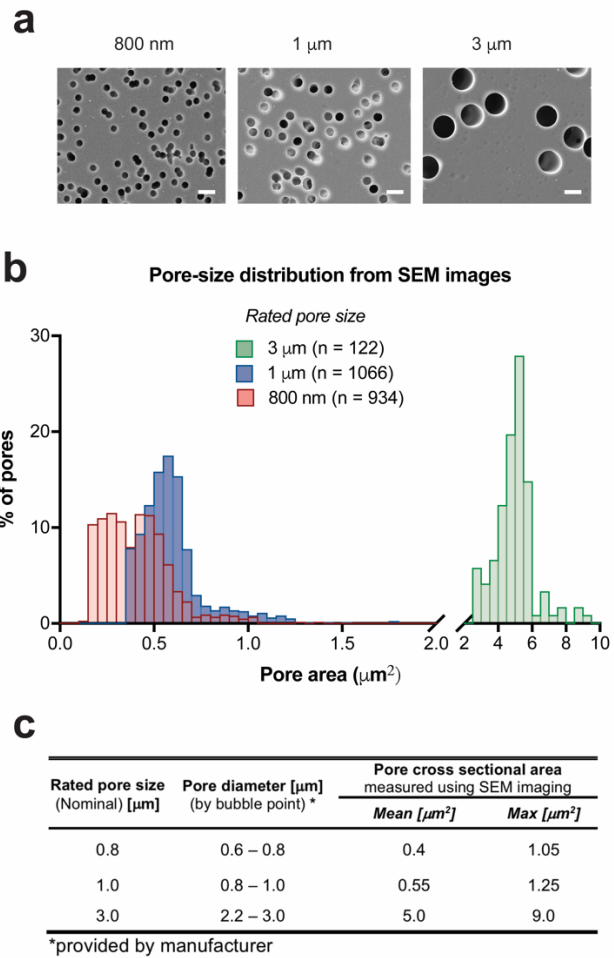


Figure S6: Estimation of pore-size distribution on 0.8 μm , 1 μm , and 3 μm membranes. a) SEM images of the membranes used for analysis. Scale bar 2 μm b) Distribution of pore cross-sectional area from SEM imaging. Measurements represents aggregate of three separate samples for each pore size, each sample imaged at five random locations. The total number of pores analyzed is indicated in the legend. c) A summary chart for the membrane measurements. Experiments were repeated twice with similar results

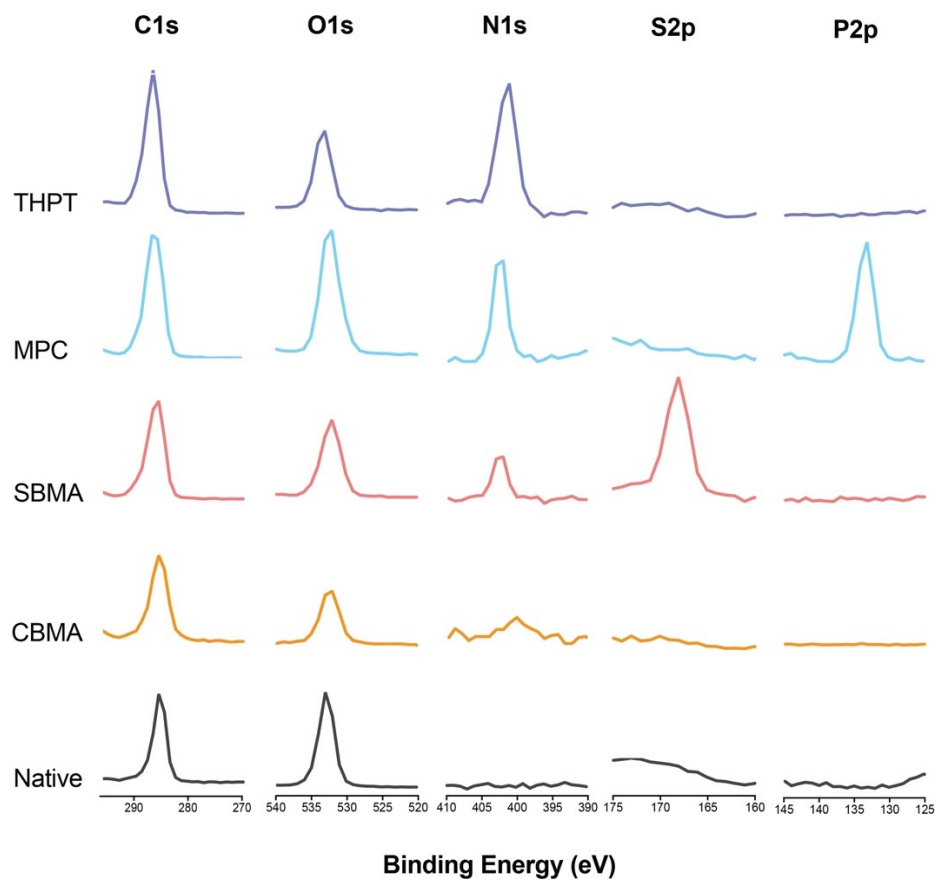


Figure S7: XPS spectrum of key elements (Carbon C, Oxygen O, Nitrogen N, Sulfur S, Phosphorus P) obtained from analysis of device surface after ATRP modification.

Contact angle measurements

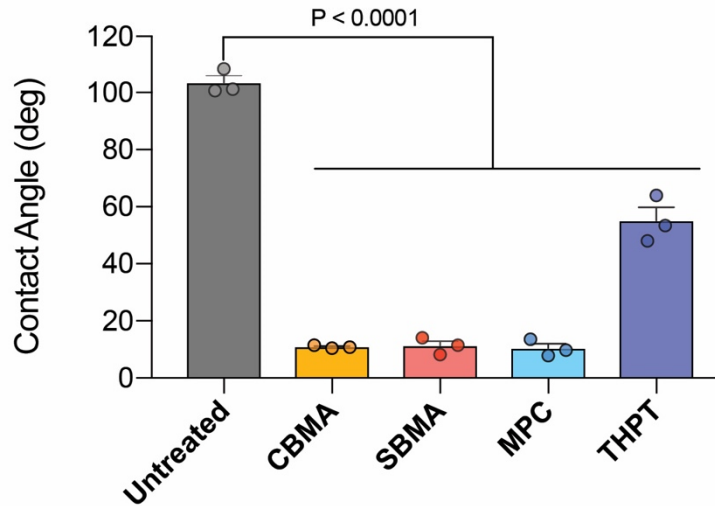
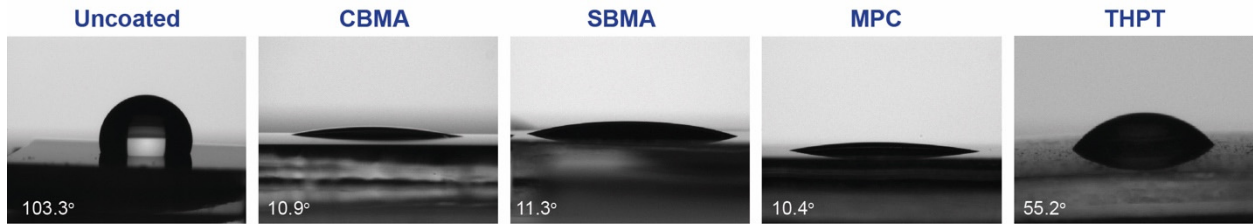


Figure S8: Effect of surface coating on hydrophilicity of the device. Contact angle was measured using the sessile drop technique on a DSA100 (Kruss). The top panel shows representative images of the sessile drop on the device surface. The bottom graph shows the summary of the measurements indicating significant reduction in contact angle, especially for the zwitterionic coatings. Error bar: mean \pm s.e.m (n = 3 samples). P-value was analyzed using one-way ANOVA with Bonferroni multiple comparison correction.

Scanning Electron Microscopy of surfaces after ATRP coating

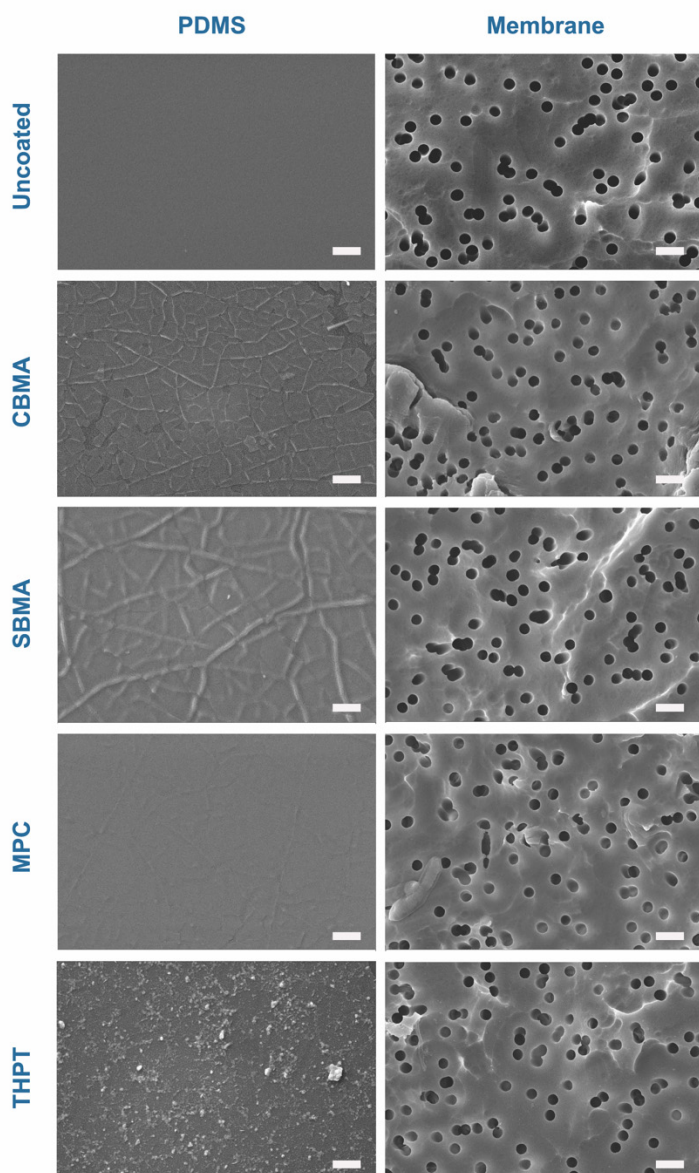


Figure S9: Surface analysis of the device using scanning electron microscopy (SEM). SEM images showing the surface of the macrodevices before and after the surface coating. The polymer coating on the surface can be clearly seen. The wrinkles on the zwitterionic coated devices (CBMA, SBMA, and MPC) is an artifact due to dehydration during the sample preparation process. Experiments were repeated thrice with similar results. Scale bar: 1 μ m.

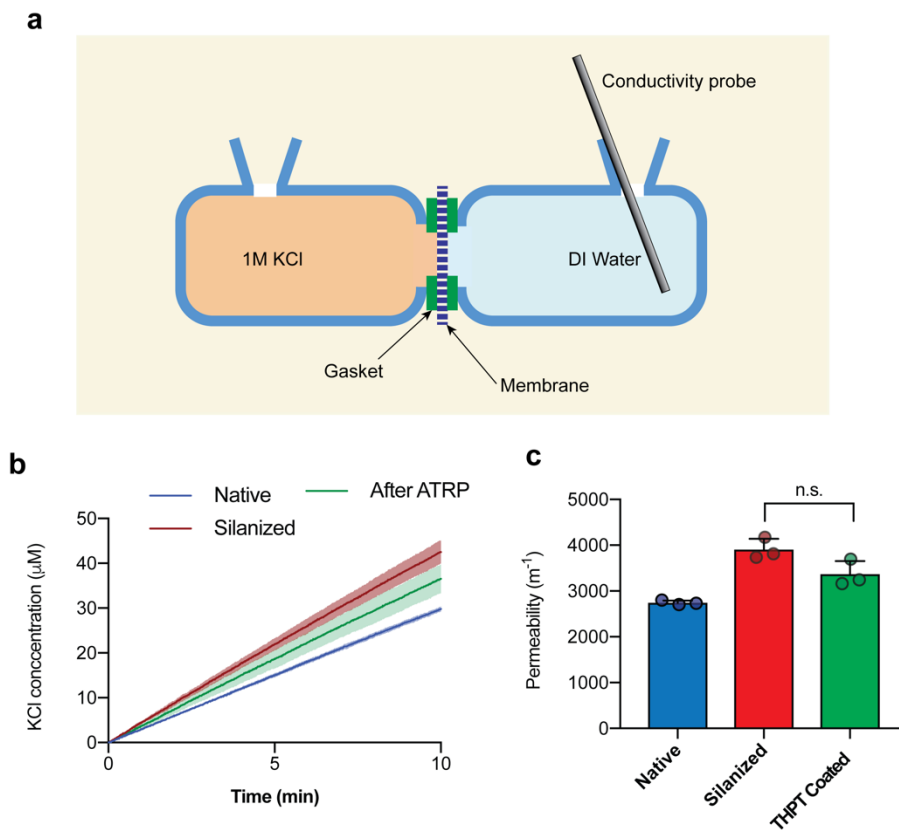


Figure S10: Measuring permeability of membranes. a) A horizontal Franz-diffusion cell setup for measuring membrane permeability. b) KCl concentration curves over time on the right side of the cell measured using the conductivity probe. c) Comparison of absolute membrane permeability of native (obtained from vendor), silanized (after APTES treatment as present on uncoated devices) and after THPT-coating. Error bar: mean \pm s.e.m (n=3). Comparison done by two-tailed unpaired t-test; ns, P = 0.0647.

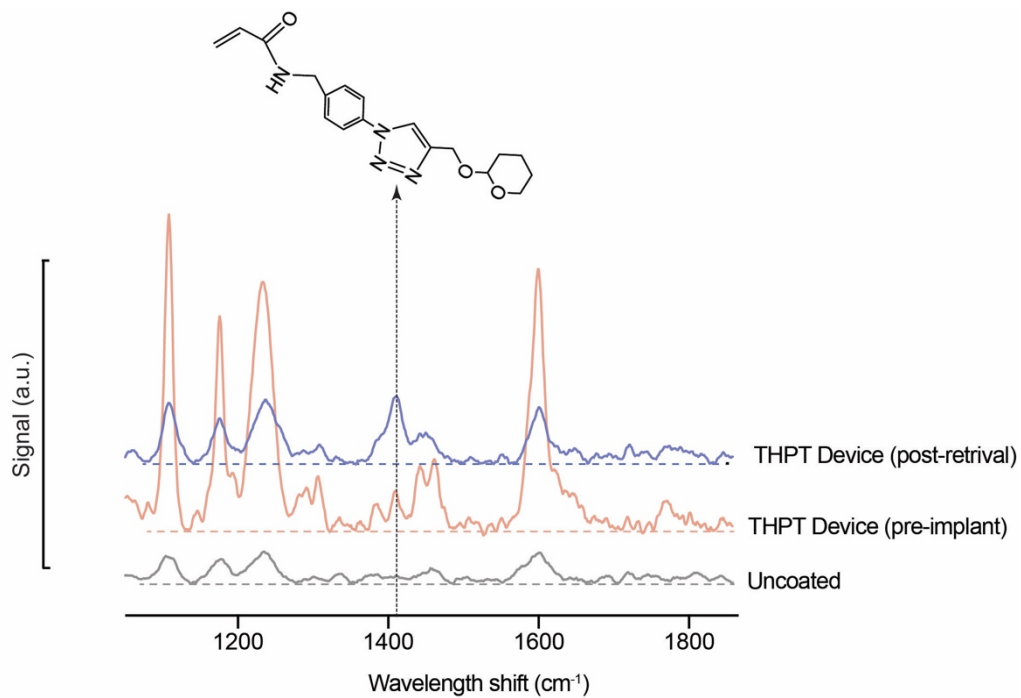


Figure S11: Confocal raman mapping of THPT-coated device membranes, retrieved 28 days after transplantation in i.p. of BALB/c mice. The peak 1410 cm⁻¹ corresponding to the triazole ring can be seen on both the pre-transplant and explanted devices confirming that the THPT coating did not leach *in vivo*. Experiments were repeated twice with similar results.

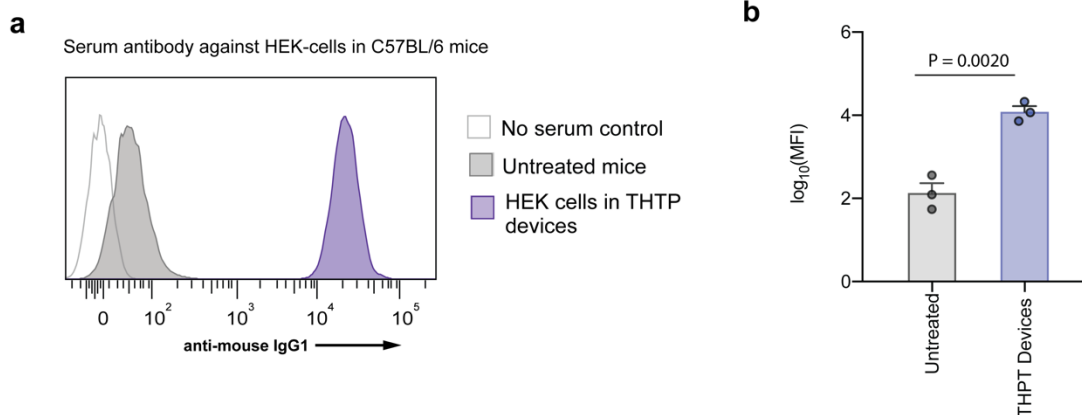


Figure S12: Detection of graft specific antibody in serum of C57BL/6 mice harboring THPT-devices with HEKepo cells. HEK cells incubated with animal serum (day 35) and counterstained with anti-mouse IgG-AF647 was analyzed using flow-cytometry **(a)** which showed the presence of cell specific antibodies in all the animals receiving the devices. **(b)** Quantification of mean fluorescence intensity (MFI) showed significant levels of anti-graft IgG with the devices over untreated animals. Error bars mean \pm s.e.m. $n = 3$ per group. Statistical analysis: two-tailed unpaired t-test.

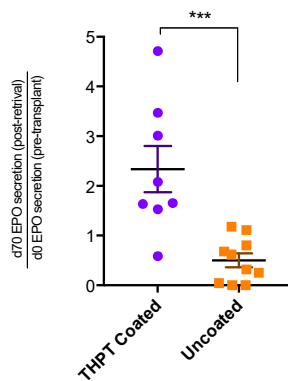


Figure S13: Fold change in EPO secretion rate of THPT-coated and uncoated devices prior to transplantation and after retrieval on day 70 post-transplantation. Experiment is detailed in *Figure 5e*, and EPO secretion was measured in vitro. Error bars: mean \pm s.e.m; $n = 8$ (THPT coated devices) and 10 (uncoated devices). Statistical test: two-tailed unpaired t-test. ***, $P = 0.0008$.

In-vitro charecterization of HEKepo-tetR cells

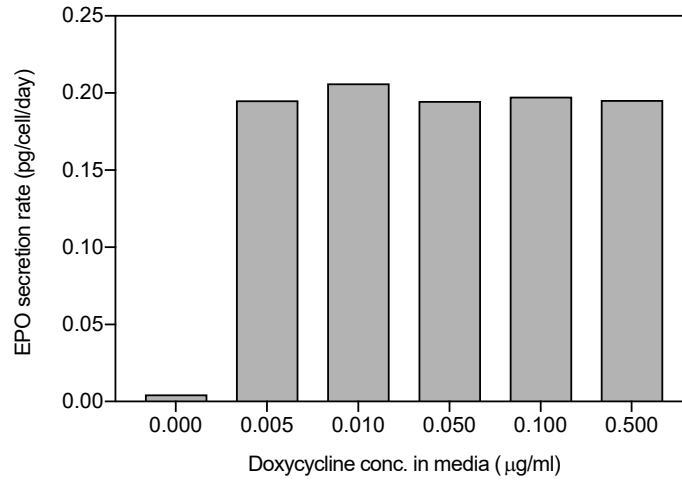


Figure S14: Secretion rate of EPO at different doxycycline concentration in media (treated for 48 hrs) from dox-inducible HEKepo cells used in **Figure 5f**. Error bars: mean \pm s.e.m (n = 3 biological replicate).

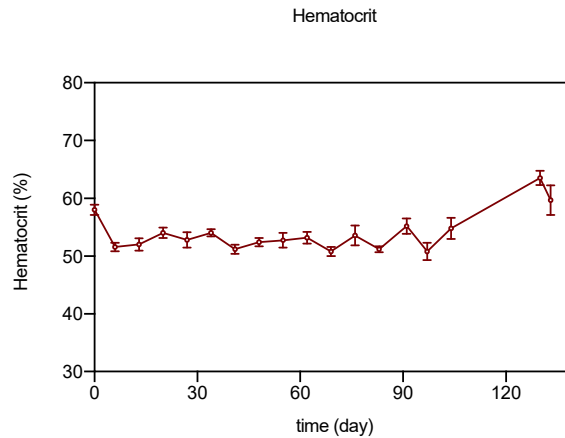


Figure S15: Hematocrit of animals receiving THPT-coated devices encapsulating doxycycline inducible HEKepo cells, showing excellent control of hematocrit levels. Error bars: mean \pm s.e.m. n = 5 animals.

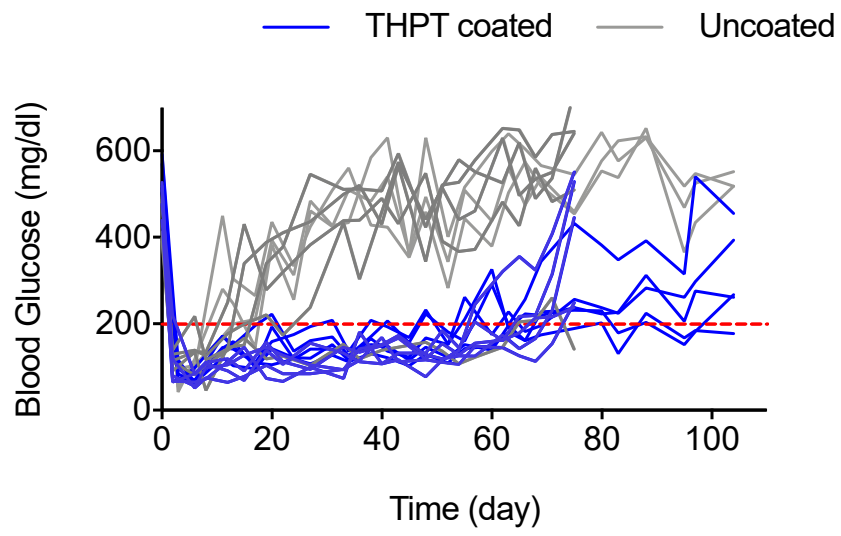


Figure S16: Individual BG plots of Figure 6.

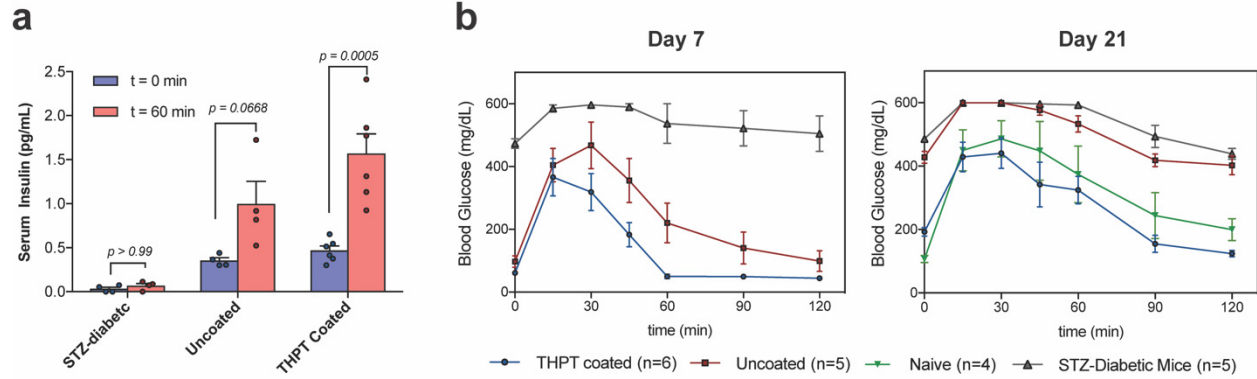


Figure S17: Additional Intravenous Glucose Tolerance Test (IVGTT) with transplanted rat islets inside macrodevices into STZ-diabetic C57BL/6 mice: a) Serum insulin levels during IVGTT on day 7 post transplantation shows significant rise in serum insulin levels in response to glucose in the treated mice groups. Error bar: mean \pm s.e.m. Group size n = 6 animals (THPT), 4 animals (Uncoated and STZ-diabetic). Two-way ANOVA with Bonferroni multiple comparison correction. P-values are indicated on the graph. b) The blood glucose kinetic after glucose injection is shown for 7 and 21 days after transplantation. Error bar: mean \pm s.e.m.

Islets retrivals

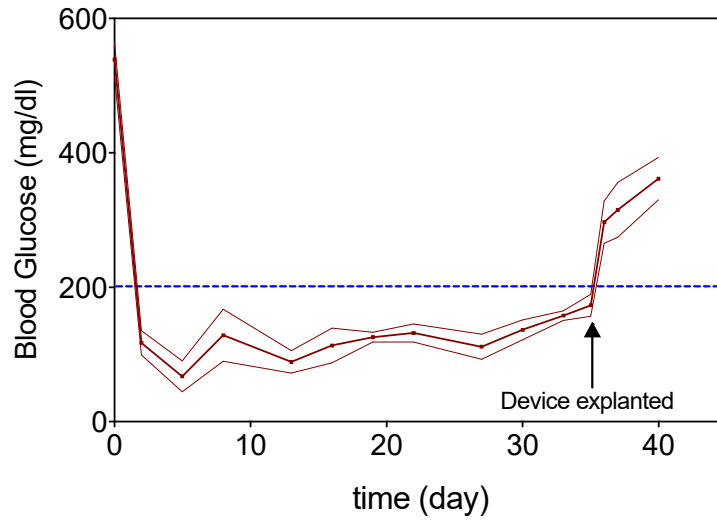


Figure S18: BG correction of STZ-diabetic C57BL/6 mice implanted with THPT-coated devices encapsulating 200 IEs rat islets, showing animals maintained euglycemia until devices were explanted (day 35, indicated by an arrow), after which the animals promptly became diabetic. Data points represents group mean (n=5) while the shaded region is s.e.m.

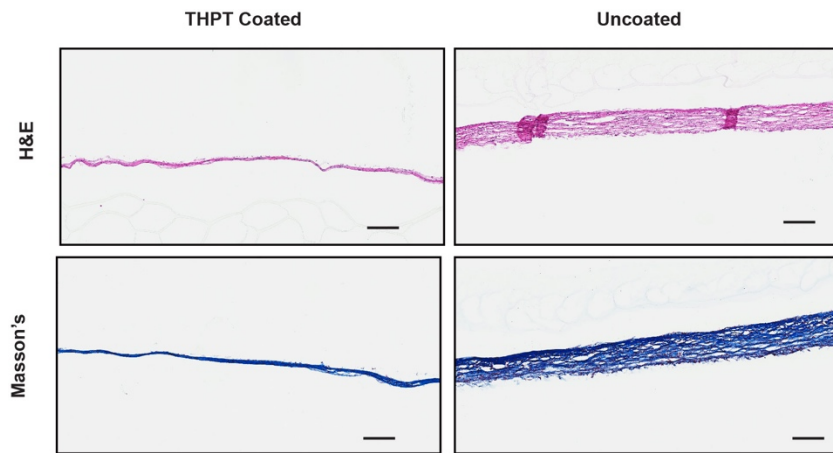


Figure S19: Representative histology images of the devices carrying rat islets retrieved from STZ-diabetic C57BL/6 mice after 110d, showing the THPT-coated devices remained biocompatible with only a thin fibrotic capsule. Histological sections shows fibrosis on the device membrane with H&E stain and masson's trichrome. Experiments were repeated twice with similar results. Scale bar: 100 μ m.

Estimating membrane pore-size distribution

Our studies with membranes having different pore-sizes demonstrated that controlling pore-size can change the intensity and type of immune cell infiltration inside the device. Specifically, we found that while membranes with 3 μm pores allowed infiltration by T-cells and macrophages, pores with a rated diameter of 1 μm allowed selective infiltration of macrophages, and 800 nm pores completely prevented cell infiltration. The results are significant since cell migration through pores below 7 μm^2 area ($\sim 3\mu\text{m}$ diameter) has not been observed before. However, we wanted to accurately determine the pore-size distribution on membranes to ascertain the cut-off range for cell infiltration.

The polycarbonate track-etched (PCTE) membranes used in this study contain straight pores of narrow diameter range. The pores are made by exposing thin sheets of PC to charged ions, creating defects or 'tracks' within the material, which are then chemically etched to obtain straight cylindrical pores. It is difficult to accurately characterize the pore structure and distribution of membranes, and the available methodologies have their own limitations. Bubble point measurement gives an accurate estimate of pore-diameters and is used by manufacturers to rate the PCTE membranes. The rated pore-size is the largest pore diameter present on the membrane. But this method underestimates the pore cross-section area since it does not accurately account for overlapping/merged pores present on membranes.

Scanning Electron Microscopy (SEM) imaging provides another method for estimating pore cross-section area (and size distribution) which might be more relevant for cell migration. Therefore, we used this method to further characterize the membranes used in this study. Membranes were coated with 2nm of gold using a sputter coater and imaged on a Zeiss Crossbeam 540 microscope at 5 kV beam. Three separate membranes for each pore size were imaged at five random locations. The images were analyzed using ImageJ software, where they were filtered using an intensity threshold to identify the pores, then the pore area was calculated using the inbuilt Analyze Particle function.

The results of our analysis are shown in **Figure S6**. We found that while majority of pores were within the rated size (based on the diameter) about 10-15% of pores with larger sizes were present on all membranes. Pores up to 1 μm^2 in area were found on the 800 nm membranes indicating that this might be the size-cutoff for preventing cell infiltration. Although a majority of pores on the 1 μm membranes overlapped in size with those on the 800 nm membranes, about 4% of pores were of larger area. Hence it seems likely that these pores in the size range of 1 – 1.25 μm^2 area were responsible for the selective infiltration of macrophages as seen with the 1 μm membranes.