

## Supplementary methods

### Subjects and data collection

#### *Discovery dataset*

30 patients with treatment-resistant depression received MRI scans prior to a routine course of clinical TMS at the Berenson-Allen Center for Noninvasive Brain Stimulation in Boston, MA. Patients were referred for clinical treatment due to treatment-resistant major depression. 3000 pulses of high-frequency TMS were delivered at 120% of resting motor threshold (RMT) in 4-second trains with a 26-second inter-train interval using a NeuroStar clinical stimulator (Neuronetics Inc, Malvern, PA) or a MagStim Super Rapid stimulator (Magstim Company Ltd, UK)<sup>1</sup>. Treatment was targeted to a scalp location 5.5 cm anterior to the site that induced a contraction in the right abductor pollicis brevis muscle. The stimulation site was recorded using stereotactic neuronavigation.

Self-report Beck Depression Inventory (BDI) and clinician-report 24-item Hamilton Rating Scale for Depression (HAM-D) were collected before and after the treatment course. This protocol was approved by the Committee on Clinical Investigations at Beth Israel Deaconess Medical Center. The first 25 of these 30 patients were used in a prior publication<sup>1</sup>.

#### *Replication dataset*

168 subjects with treatment-resistant depression received MRI scans as part of the OPT-TMS trial, a multi-site randomized clinical trial of TMS for major depression<sup>2,3</sup>. Data were collected at the Medical University of South Carolina, Columbia University, the University of Washington, and Emory University. 81 subjects received active treatment, while 87 received sham. 3000 pulses of high-frequency 10 Hz TMS were delivered at 120% of RMT in 4-second trains with a 26-second inter-train interval using a Neuronetics Model 2100 Therapy System (Neuronetics Inc, Malvern, PA). For 67% of subjects, treatment was delivered at a scalp location 5 cm anterior to the site that induced a contraction in the contralateral abductor pollicis brevis muscle. The stimulation site was recorded by placing a Vitamin E capsule over the stimulation site during the MRI scan. When this stimulation site overlapped with premotor cortex (33% of subjects), the stimulation site was moved an additional 1 cm anteriorly.

Self-report Inventory of Depressive Symptoms (IDS) and clinician-report 28-item Hamilton Rating Scale for Depression (HAM-D) were collected before and after the treatment course. Montgomery-Asberg Depression Rating Scale (MADRS) was also collected as a secondary clinician-report measure. Patients who demonstrated at least 30% improvement after 3 weeks (active or sham groups) received additional blinded treatment for up to 3 weeks or until remission was reached. Nonremitters were then transferred to an open-label extension phase for up to 6 weeks or until remission was reached<sup>2</sup>. For simplicity and to allow direct comparison to sham, the 3-week time point was used as our primary outcome measure. However, we also repeated our analysis using the timepoint immediately after the blinded phase, which could be anywhere between 3 and 6 weeks depending on the patient. The protocol was approved by the institutional review board at each participating institution.

### Seed-based connectivity analysis

#### *Generation of stimulation site connectivity maps*

For each subject in all three datasets, a region of interest (ROI) representing the stimulation volume was defined using concentric spheres of progressively decreasing intensity with a maximum radius of 12 mm

as described previously<sup>4</sup>. Resting-state functional connectivity between this ROI and all other brain voxels was computed using fMRI data from a large cohort of normal subjects (n=1000)<sup>5</sup> as described previously<sup>1</sup>. The resulting connectivity maps were used for all subsequent analyses. Except where otherwise specified, all subsequent analyses were conducted using MATLAB R2018b.

#### *Calculation of symptom-response maps across all subjects*

These stimulation site connectivity maps were compared with improvement in each of the 21 symptoms on the Beck Depression Inventory (BDI). At each voxel, correlation was computed between stimulation site connectivity and clinical improvement. Clinical improvement was defined as absolute change in each symptom between the pre-treatment and post-treatment assessment. This analysis was repeated for each symptom at each voxel in the brain. At each voxel, this yielded a correlation coefficient between that voxel's stimulation site connectivity and improvement in each symptom. Across all voxels, this yielded 21 maps depicting the degree to which each brain voxel predicted improvement in each of the 21 symptoms. We refer to these voxel-wise maps as "symptom-response maps" (Figure 1C, main text).

These maps were not individually tested for significance due to the risk for multiple comparisons artifact, as there were a total of over 1,000,000 analyses (21 symptoms x 65,536 voxels in each symptom map). The maps were also not thresholded in order to avoid bias introduced by arbitrary threshold selection. Instead, all subsequent analyses were conducted based on spatial correlation between pairs of maps, as this approach reduces all of the comparisons into a single analysis.

## Clustering

#### *Clustering of circuit maps*

Connections correlated with improvement in each depression symptom (symptom-response maps) were generated as above. The similarity between these 21 maps was determined by computing spatial correlations between each pair of maps. This yielded a 21 x 21 correlation matrix that quantifies the similarity between each pair of maps. To identify clusters in this matrix, the individual symptoms were treated as nodes and the cross-correlations were treated as distance metrics. The values were clustered using Ward's minimum variance method for hierarchical clustering. The optimal cluster solution was determined using the gap criterion, which identifies the minimum number of clusters required to approach an asymptote in error measurement<sup>6</sup>. This approach was chosen because it provides a single metric for the strength of the clustering solution (percent variance explained, measured by the gap statistic), facilitating control analyses and comparison to randomly permuted data. This also eliminates the risk of multiple comparisons artifact, as the maps are all reduced to a single metric of clustering strength. The cluster solutions were depicted using a force-directed graph visualization algorithm in Gephi 0.9.2.

#### *Control analyses*

Control analyses were conducted to confirm that the clustering results were not driven by the following four factors:

1. *Characteristics of the stimulation site alone*: The clustering analysis was repeated using baseline symptom severity rather than symptom improvement. Baseline symptom severity should be unrelated to stimulation site, thereby isolating the effects of stimulation site alone. Similarity

between each pair of symptom-response maps was calculated (absolute value of the spatial cross-correlation) and statistically compared to the real data using an unpaired t-test (Fig. S1b).

2. *Covariance in symptom response alone*: The clustering analysis was repeated based on correlation between symptom change alone, without considering the stimulation sites or their connectivity. The strength of clustering was compared to our primary result using the gap statistic (Fig. S1c).
3. *Random chance*: The clustering analysis was repeated after randomly assigning each patient's stimulation site to a different patient's clinical response. A two-cluster solution was forced in this analysis. Similarity between each pair of symptom-response maps was calculated as above, and the mean was compared to real data using a permutation test with 10,000 iterations. The strength of clustering was compared to real data using the gap statistic (Fig. S1d). The analysis was also repeated without forcing a two-cluster solution in order to determine the frequency with which a two-cluster solution would arise spontaneously.
4. *Artificial binarization of a continuous distribution*: To test whether our clustering could have artificially binarized a normal distribution, we tested for normality using a Kolmogorov-Smirnov test.
5. *Influence of confounders*: To determine whether our results may have been driven by relevant clinical confounders, we repeated the circuit mapping procedure after including age, sex, and number of extant psychotropic medications as covariates. The resulting maps were compared with the original cluster maps to determine the influence of these confounders.

#### *Replication of clustering model*

The full clustering analysis was repeated for both symptom inventories in both datasets. This resulted in a pair of cluster-response maps for each dataset and symptom inventory, including the discovery BDI, discovery HAMD, replication HAMD, and replication IDS. In the replication dataset, maps were computed independently for active and sham data.

To test whether our clustering model replicated across symptom scales, we compared the self-report maps from our discovery dataset to the clinician-report maps for our discovery dataset, and the self-report maps from our replication dataset to the clinician-report maps from our replication dataset. Similarity between maps was assessed using spatial correlation, producing four  $r$  values (2 cluster response maps  $\times$  2 datasets). These four  $r$  values were converted to a normal distribution using Fisher's  $r$  to  $z$  transform, then averaged to produce a single number reflecting the reproducibility of our maps across symptom scales. Significance was assessed via permutation testing (repeating the above analysis 10,000 times with random shuffling of stimulation sites and symptom responses in both datasets). In the randomly permuted data, the cluster containing the "sadness" item was labeled as "dysphoric," and the other cluster was labeled as "anxiosomatic."

To test whether our clustering model replicated across datasets, we compared the discovery cluster-response maps to the replication cluster-response maps. For simplicity, we first averaged the self-report and clinician-report maps within each dataset to generate two dysphoric cluster response maps and two anxiosomatic maps (one for each dataset). Similarity between maps was assessed using spatial correlation, producing two  $r$  values (one for the dysphoric cluster and one for the anxiosomatic cluster). These two  $r$  values were converted to a normal distribution using Fisher's  $r$ -to- $z$  transform, then averaged to produce a single number reflecting the reproducibility of our maps across datasets. Significance was assessed via

permutation testing as above, permuting only the replication dataset while leaving the discovery dataset unchanged.

To test whether the replication was specific to active versus sham stimulation, we repeated the above analysis using the sham arm of the replication dataset. As above, a single spatial correlation value was computed to represent the reproducibility of our maps across datasets. We hypothesized that this value would be higher for the active arm of the replication dataset compared the sham arm of the replication dataset and computed the difference between these two values. To determine whether this difference was larger than expected by chance, we re-computed this difference 10,000 times after randomly permuting the active and sham data from the replication dataset while leaving the discovery dataset unchanged.

#### *Generation of conglomerate cluster maps across multiple datasets*

Symptom-response maps were generated for all 97 symptoms in all four scales across both datasets. This yielded a total of 97 symptom response maps, which were clustered using the same methods described above. This conglomerate cluster solution was depicted using a force-directed graph visualization. The size of nodes was proportional to the normalized PageRank score, which quantifies the importance of a network node based on its connectedness<sup>7</sup>. This score was used to assess the contribution of each symptom to the clustering solution. For each scale in each dataset, the two most-contributory symptoms were identified for each cluster.

For the conglomerated clusters in each dataset, the symptom-response maps in that cluster were averaged to create an overall conglomerate pair of cluster maps.

## Prediction of clinical utility

#### *Identification of potential treatment targets*

By definition, TMS to brain voxels whose connectivity is similar to our dysphoric cluster response map should improve dysphoric symptoms while TMS to brain voxels whose connectivity is similar to our anxiosomatic map should improve anxiosomatic symptoms. We therefore identified potential TMS treatment targets by identifying brain voxels that best matched these connectivity patterns. For each voxel in the brain, the connectivity profile of that voxel was compared with each cluster-response map using spatial correlations. Each voxel was labeled with this spatial r-value, which represents the similarity between that voxel's connectivity and our dysphoric and anxiosomatic circuits. This yielded a map of targets expected to modulate each symptom cluster. Because these maps showed minimal overlap, the difference between the two maps was computed to produce an overall "targeting atlas." The voxel values on this targeting atlas should predict relative improvement in dysphoric versus anxiosomatic symptoms.

Using the same procedure described above, a separate targeting atlas was also computed for each dataset alone, yielding a distinct "discovery" and "replication" targeting atlas. The discovery targeting atlas was used to predict clinical improvement in the replication active and sham datasets, while the replication targeting atlas was used to predict clinical improvement in the discovery dataset.

### *Validation across studies*

A systematic literature review was conducted to identify therapeutic TMS studies that measured distinct mood and anxiety rating scales, which were considered as proxies for dysphoric and anxiousomatic clusters. This followed an approach similar to what was used in prior work involving retrospective analysis of multiple studies for identification of optimal TMS targets<sup>8</sup>. Studies were included if they satisfied the following criteria:

1. At least one mood scale and one anxiety scale were reported.
2. At least 3 weeks of daily therapeutic repetitive TMS were administered to the prefrontal cortex.
3. Treatment intensity was at least 5 Hz, as lower frequencies likely have inhibitory effects which were not included in our predictive model.
4. Stimulation site was clearly reported with adequate detail (or citation) to determine the location of the stimulation site with respect to our targeting atlas.
5. All subjects included in the study carried a primary DSM-IV or DSM-5 psychiatric diagnosis; for instance, studies of stroke rehabilitation or chronic pain were not included.

For each of these studies (listed in Table S3), the stimulation site was identified and converted to MNI coordinates. MNI coordinates for the EEG F3 target were estimated based on the report in Fox *et al.*, 2012<sup>8</sup>. The Beam F3 target was estimated based on Fried *et al.*, 2014<sup>9</sup>. The left-sided “5 cm” target was determined empirically as the mean location of all stimulation sites in the replication dataset, while the right-sided 5cm target was identified at the corresponding contralateral site. The left-sided “5.5 cm” target was determined empirically based on the mean of all stimulation sites in the discovery dataset. The “6 cm” target was estimated by extrapolating based on the distance between the “5 cm” and “5.5 cm” targets. The location of the task fMRI-based target was calculated empirically based on the mean of all neuronavigated stimulation sites in the dataset. The published dmPFC target coordinates included a superficial coordinate (0,60,60) and a deep brain coordinate (0,30,30)<sup>10-12</sup>, neither of which was on the surface of the brain; as a result, the stimulated volume was estimated as the mean of these two coordinates, which was on the cortical surface. The anti-sgACC target coordinate<sup>13</sup> was reported directly in the original paper.

For studies that reported multiple mood scales, the analysis was based on the mood scale that was most similar to the anxiety scale. For instance, if the study’s main anxiety metric was the Beck Anxiety Inventory, the mood analysis was based on the Beck Depression Inventory. If the study’s main anxiety metric was the Hamilton Anxiety Rating Scale, the mood analysis was based on the Hamilton Depression Rating Scale. If there was no mood scale to directly correspond with the anxiety scale, then the study’s pre-defined primary mood scale was used for the analysis. There were no studies reporting multiple scales that directly measure anxiety.

For each study, the mean stimulation site was plotted on the overall TMS targeting atlas. The voxel value of the stimulation site was compared with the ratio of percentage improvement in anxiety symptoms to percentage improvement in mood symptoms. A Pearson correlation was used to quantify this relationship. The success rate of the target map was also calculated based on the percentage of studies in which the TMS targeting atlas map successfully predicted which symptom type would preferentially improve. A single-proportion z-test was used to determine whether this percentage was significantly different from 50%.

## References (supplementary methods)

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