

## Supporting Information

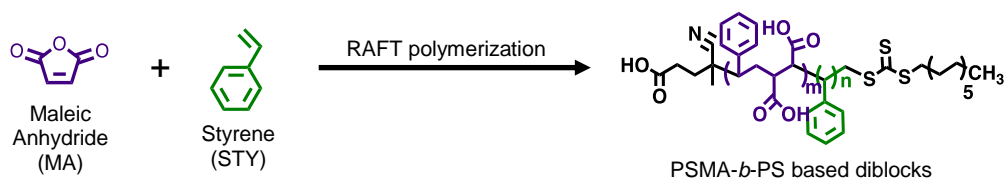
### **Nanoparticle-Mediated Delivery of Micheliolide Analogs to Eliminate Leukemic Stem Cells in the Bone Marrow**

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Giovani<sup>3</sup>, Benjamin J. Frisch<sup>1,2,4-6\*</sup>, Rudi Fasan<sup>3\*</sup>, and Danielle S.W. Benoit<sup>1,2,7,8\*</sup>*

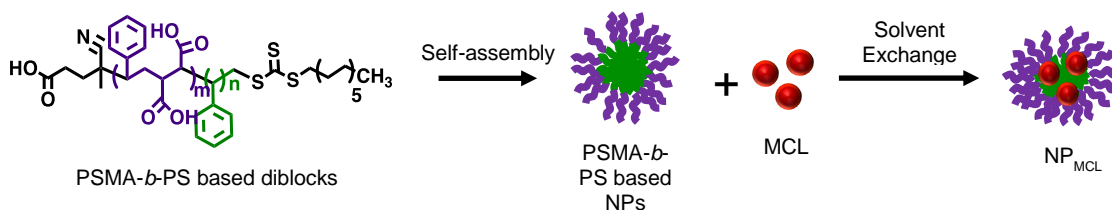
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**Schematic S1. RAFT polymerization schematic showing PSMA-*b*-PS nanoparticle self-assembly and subsequent loading with MCL analogs via solvent exchange**  
<sup>a</sup>Amphiphilic PSMA-*b*-PS diblock copolymers were synthesized via reversible addition-fragmentation chain transfer (RAFT) polymerizations using cyano-4-dodecylsulfanyltrithiocarbonyl sulfanyl pentanoic acid (DCT) chain transfer agent. C) Schematic showing the development of TBP-NP<sub>MCL-64</sub> using in efficacy studies. D) Representative transmission electron microscopy (TEM) image of NPs used for studies.

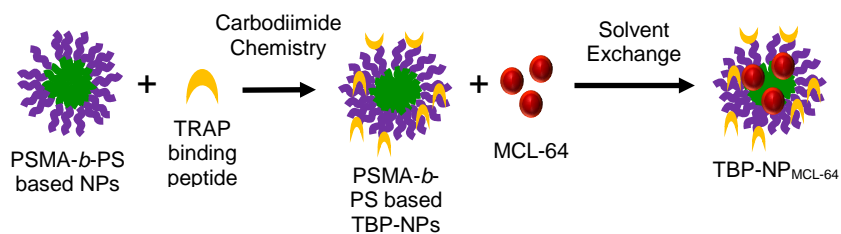
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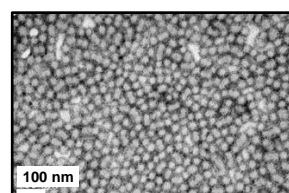
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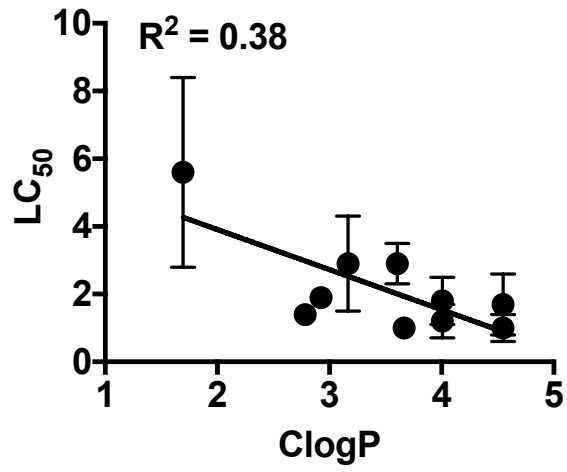


C)



D)

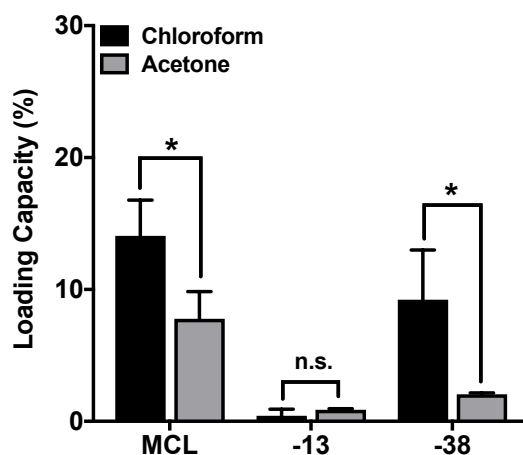




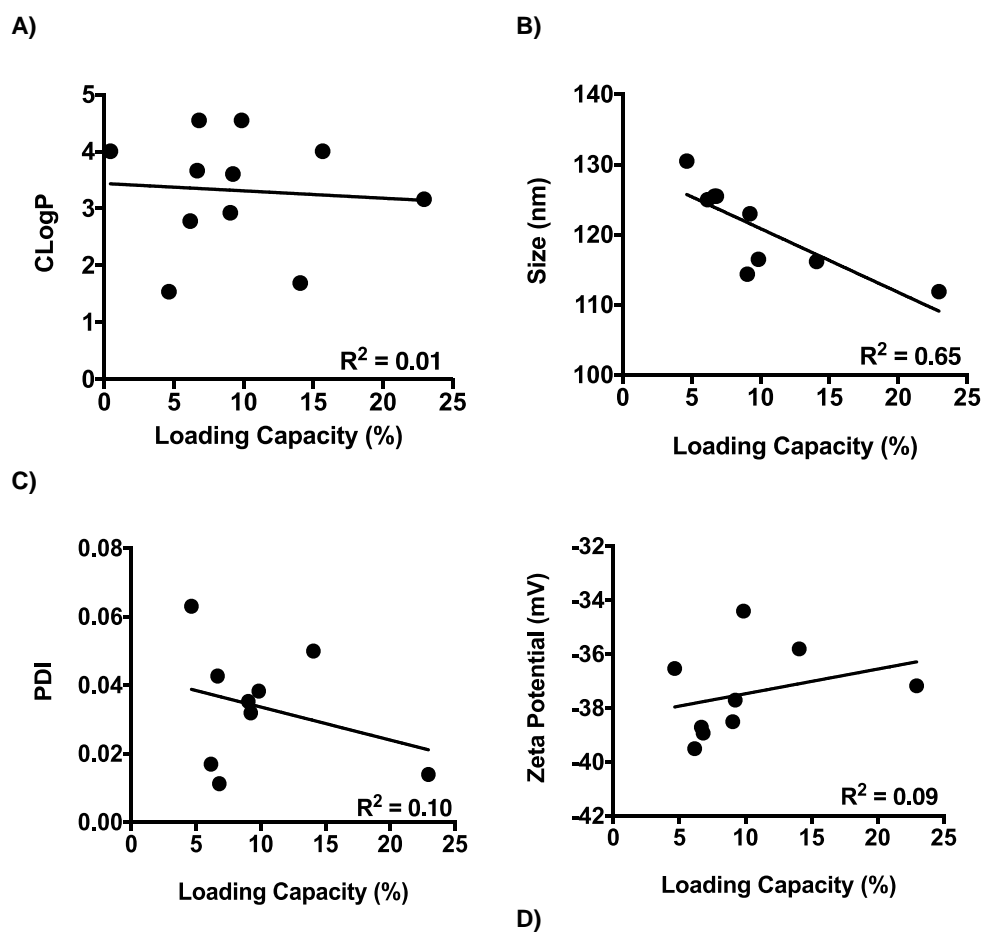
**Figure S1: Relationship between LC<sub>50</sub> and CLogP.** Line of best fit drawn using non-linear regression function on Prism V7.

### Solvent conditions alter loading capacity

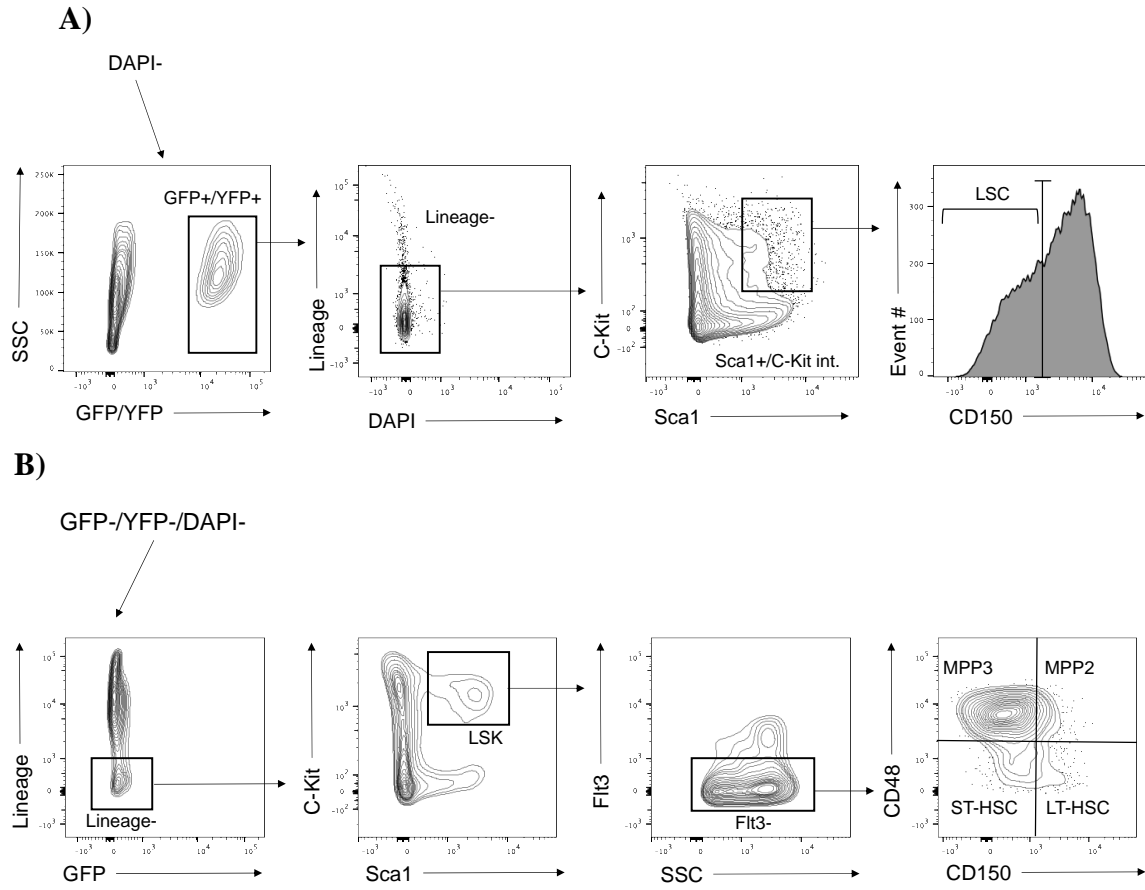
Since solvent choice has been previously shown to impact PSMA-*b*-PS loading [27], a subset of studies tested loading of MCL, MCL-13, and MCL-38 with acetone. The trends for the compounds were similar to loading with chloroform except that MCL and MCL-38 displayed reduced loading capacity of ~ 2-fold and ~ 5-fold while MCL-13 loading was unaffected. Since changing the solvent did not improve loading capacity of MCL, MCL-38 or MCL-13, acetone was omitted from loading experiments moving forward.



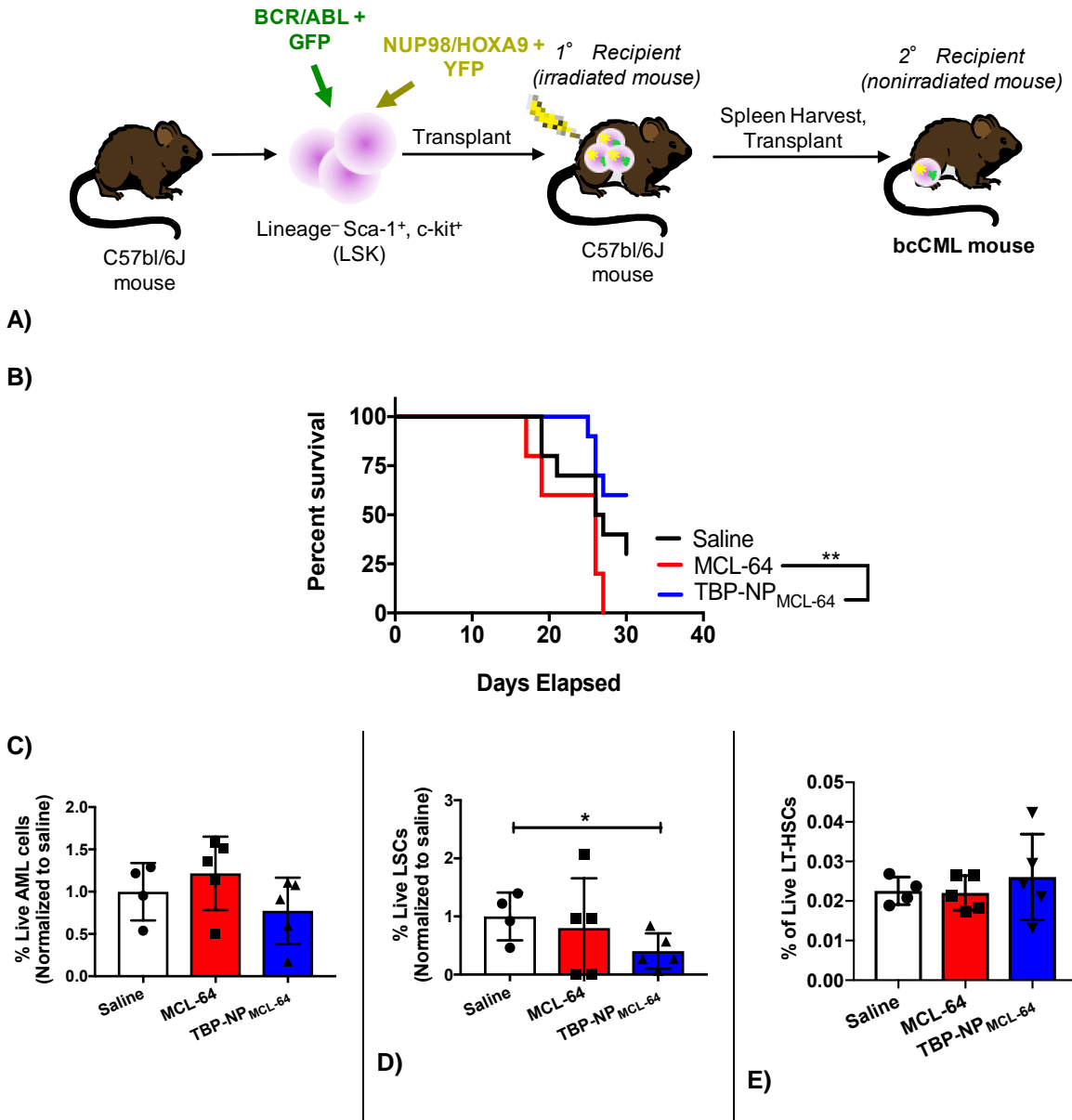
**Figure S2: Solvent dependent loading conditions. B)** Loading capacity for MCL and selected MCL analogs using acetone compared to chloroform.



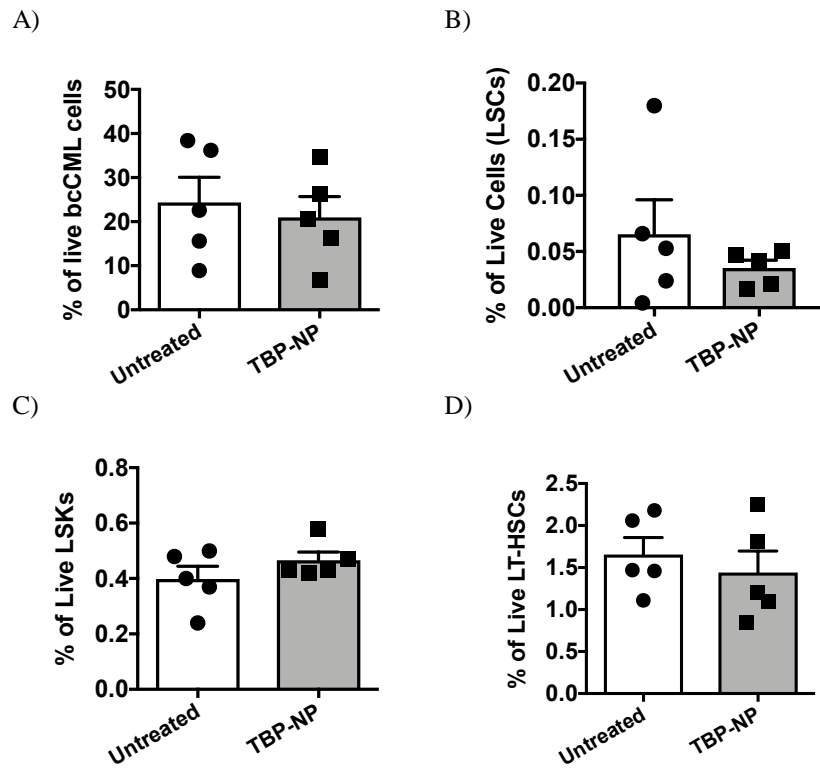
**Figure S3: Relationship between loading capacity and drug and NP physicochemical properties.** **A)** CLogP of compounds loaded, **B)** NP size after loading, **C)** polydispersity index of loaded NPs, **D)** Surface charge of loaded NPs. Line of best fit drawn using non-linear regression function.



**Figure S4:** Gating strategy used for identifying A) LSCs, B) LSKs, and LT-HSCs.

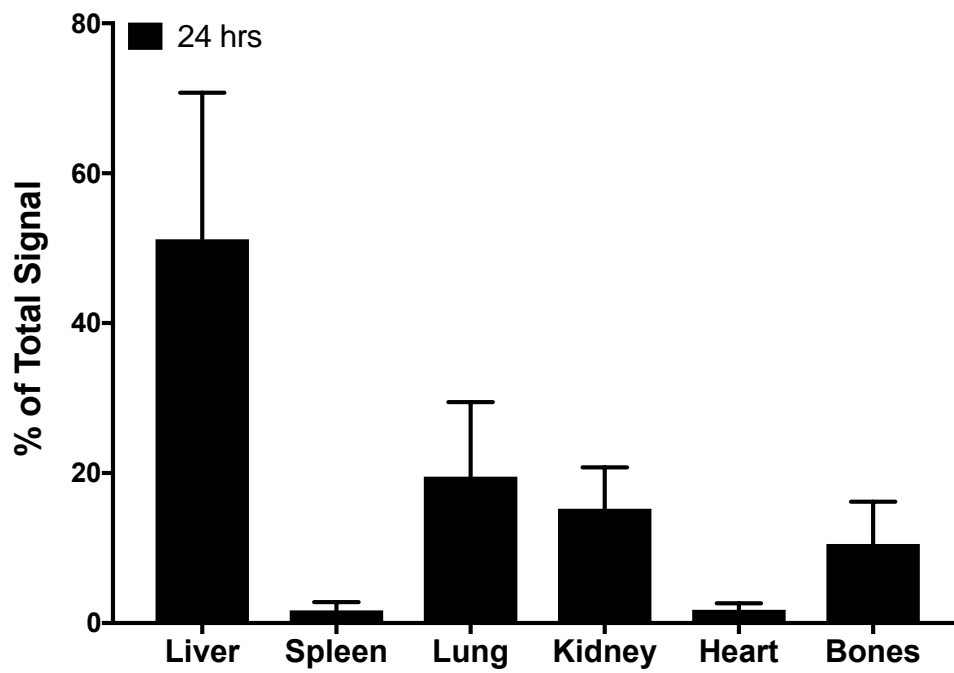


**Figure S5:** A) Schematic showing the initiation of the leukemia model used in these studies. B) bcCML mouse survival after treating with saline, free MCL-64 and NP loaded MCL-64 using 45 mg/kg free MCL and in TBP-NP. C) GFP+ bcCML cells in the marrow after treatment with 45 mg/kg MCL-64 as free drug and in NP. D) LSCs and E) LT-HSCs. Data represents mean  $\pm$  std (n = 4- 5). \* p < 0.05 represents statistical differences comparisons using unpaired *t*-tests.



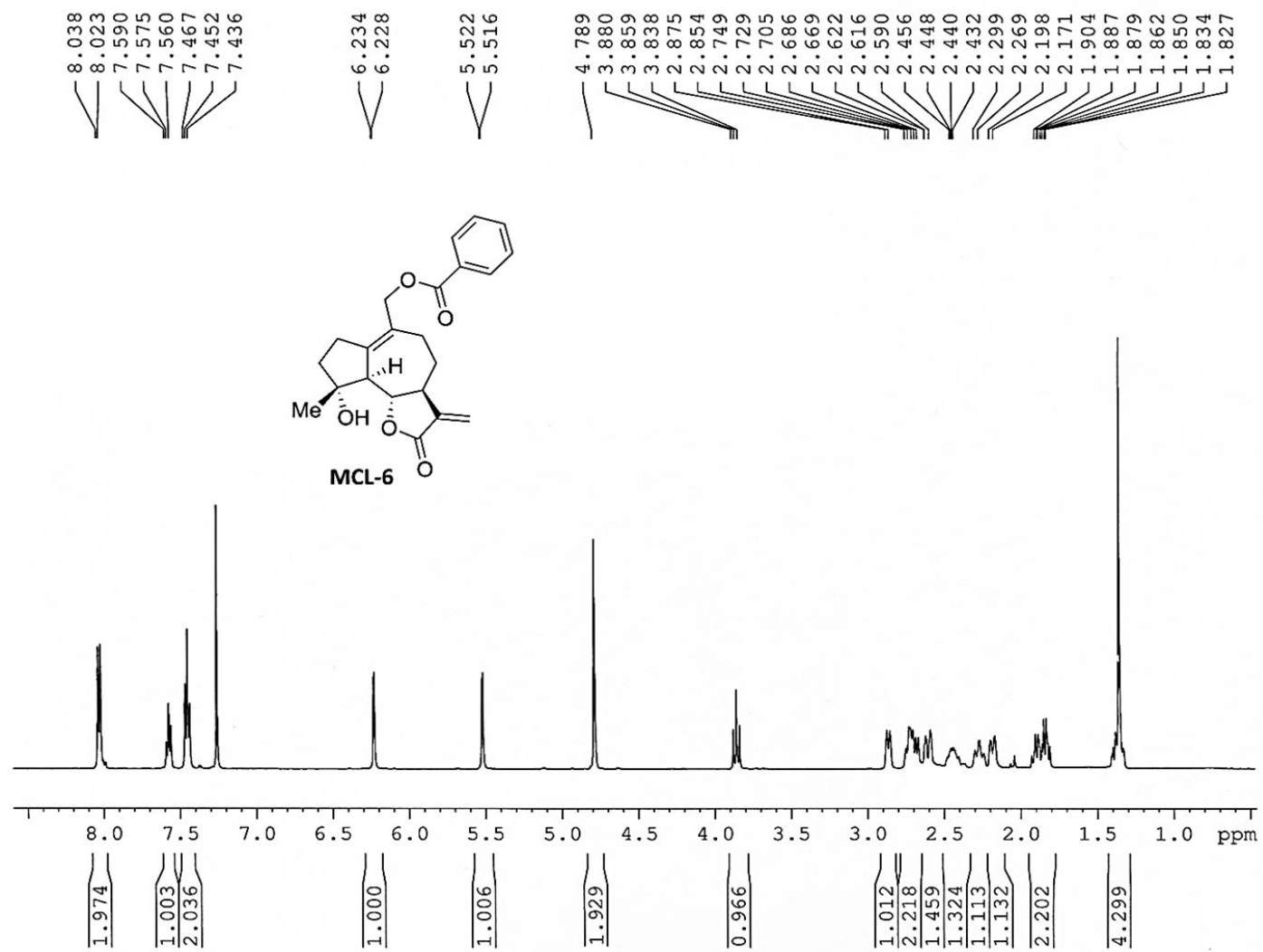
**Figure S6: bcCML in the marrow after treatment with empty TBP-NPs.** A) GFP+ bcCML cells, B) LSCs, C) LSKs, and D) LT-HSCs. Data represents mean  $\pm$  SEM ( $n = 5$ ). No statistical differences noted after statistical analysis via unpaired  $t$ -tests.

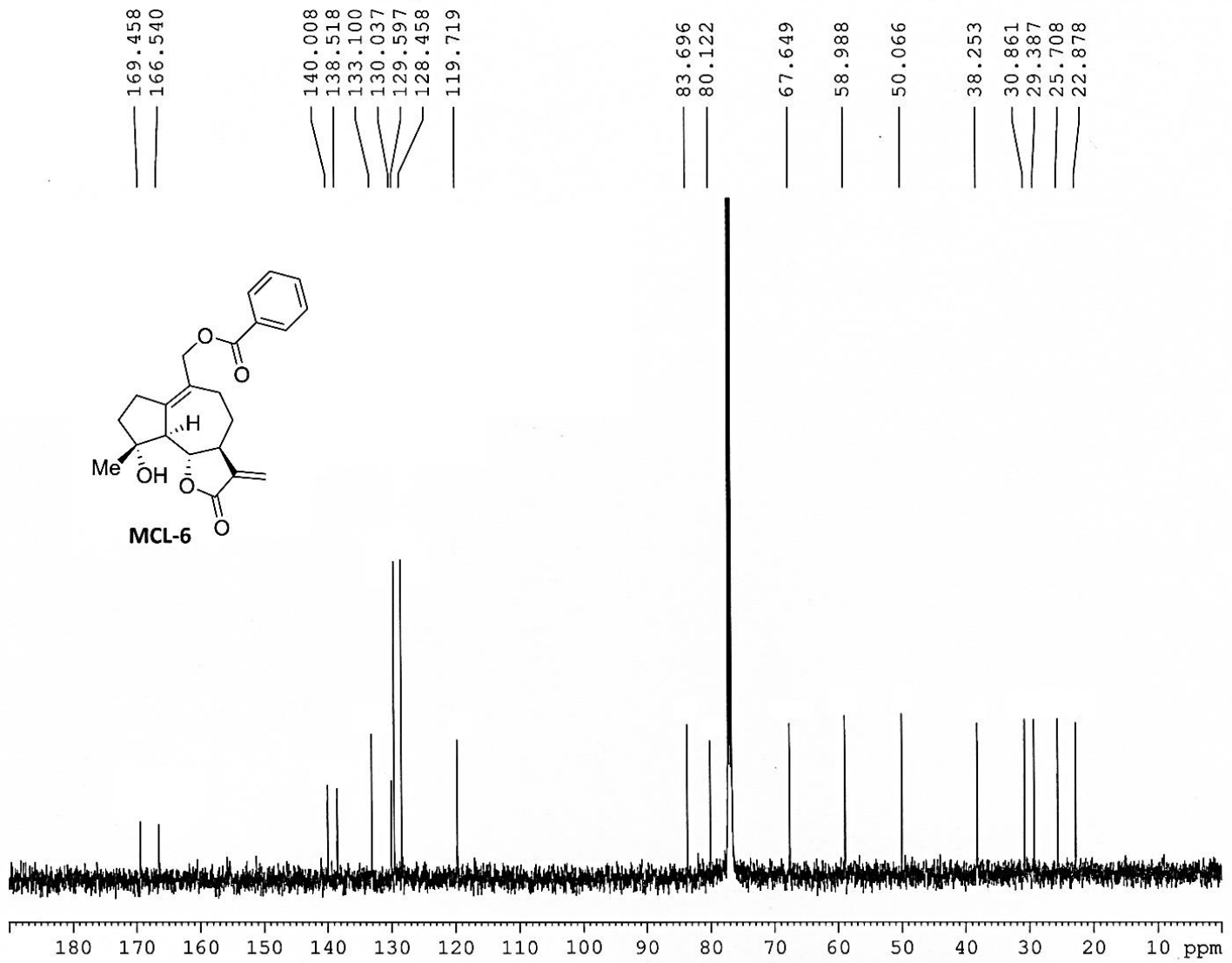


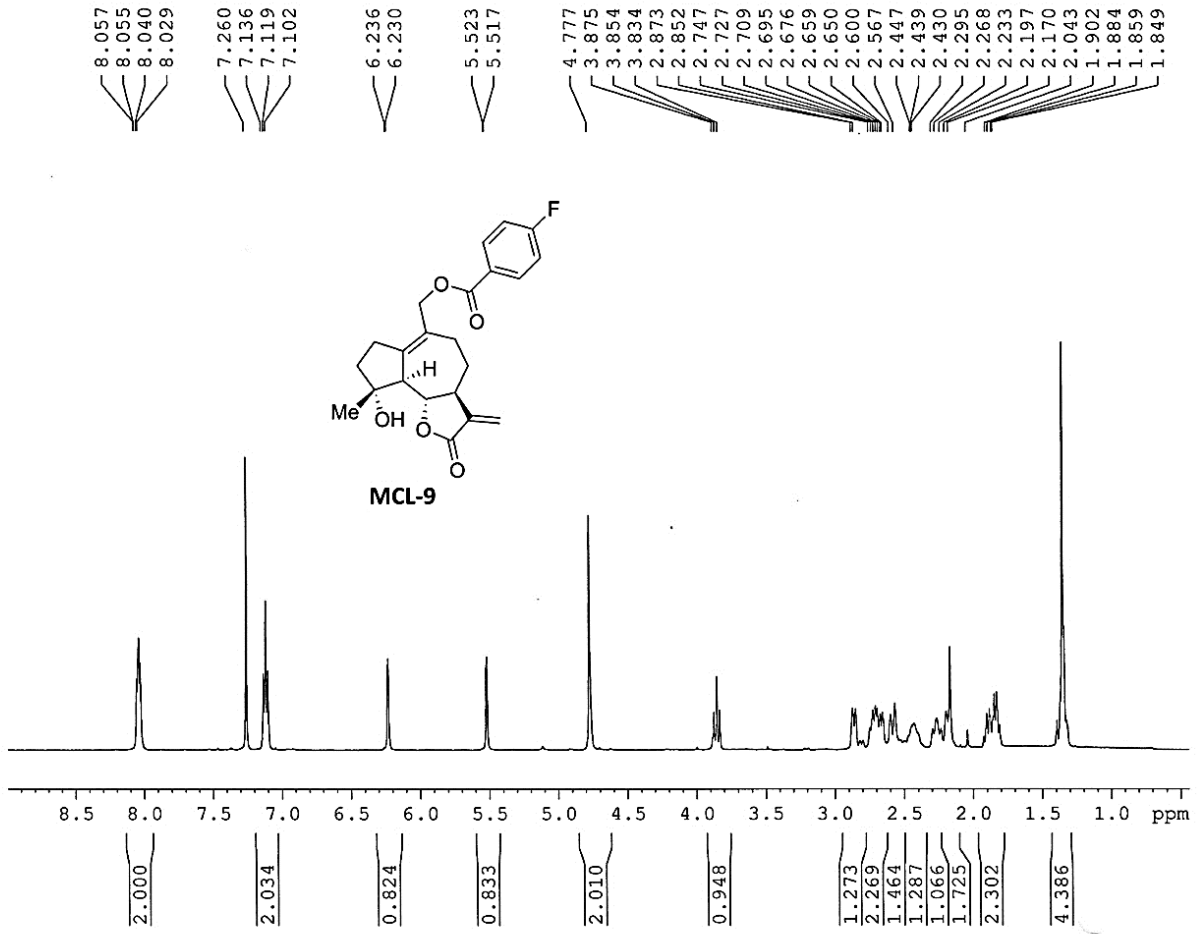


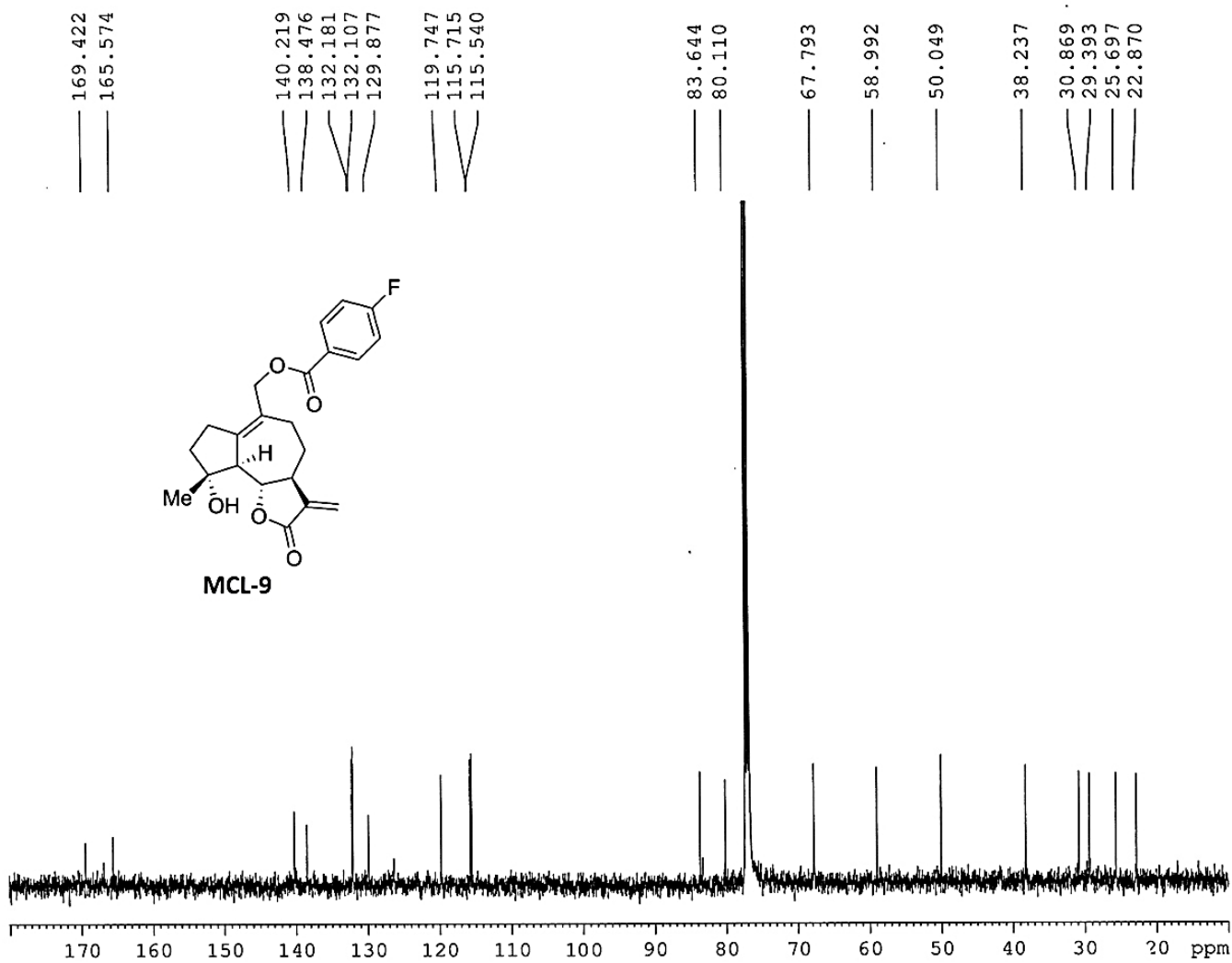
**Figure S7: TBP-NPs accumulate in bone of the bcCML model.** bcCML mice were injected at D7 with fluorescent TBP-NPs, and *in vivo* live imaging (IVIS) was performed 24 hours later after mice were sacrificed and tissues were collected. Data represents n = 5.

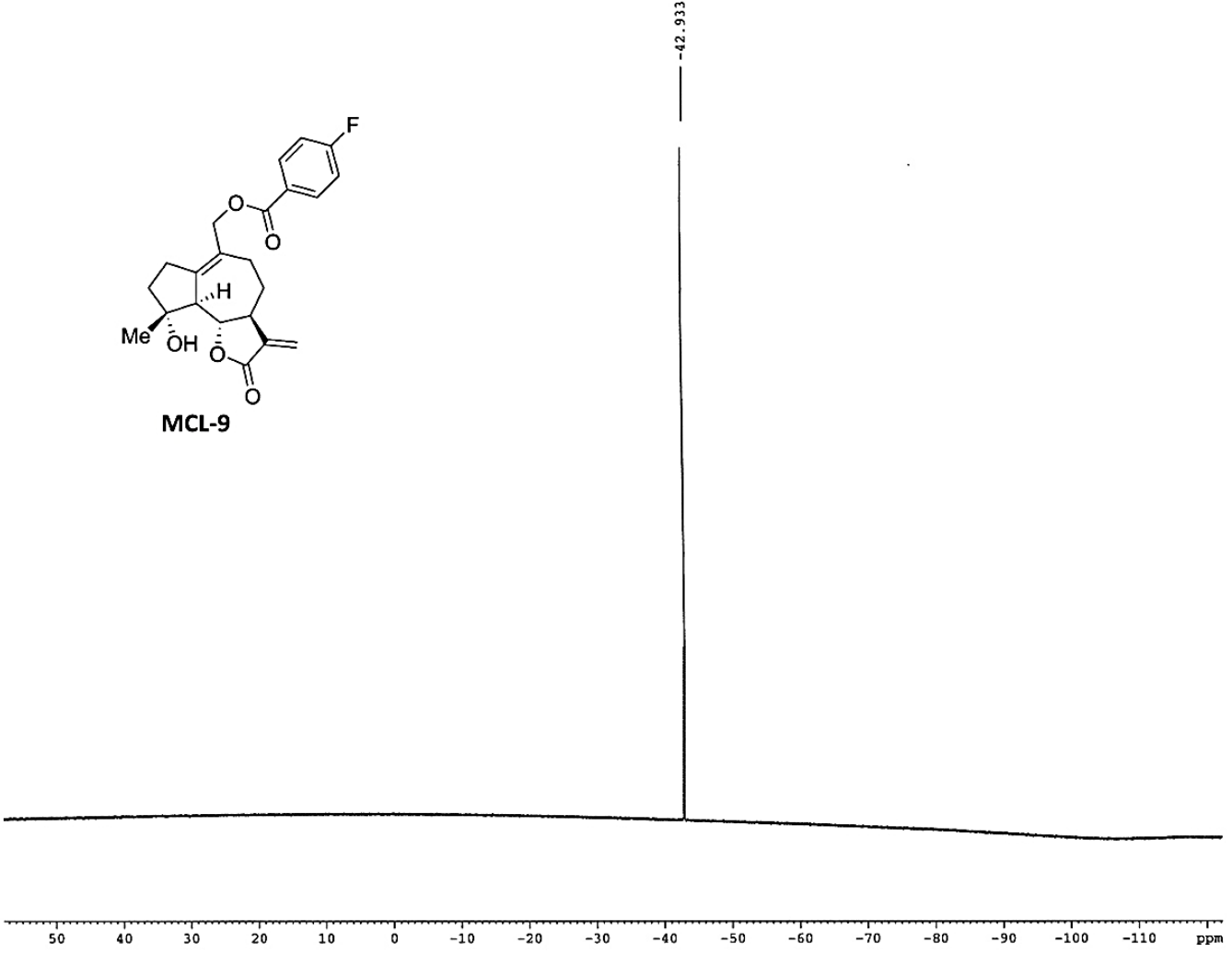
Figure S8: NMR spectra of MCL analogs synthesized.



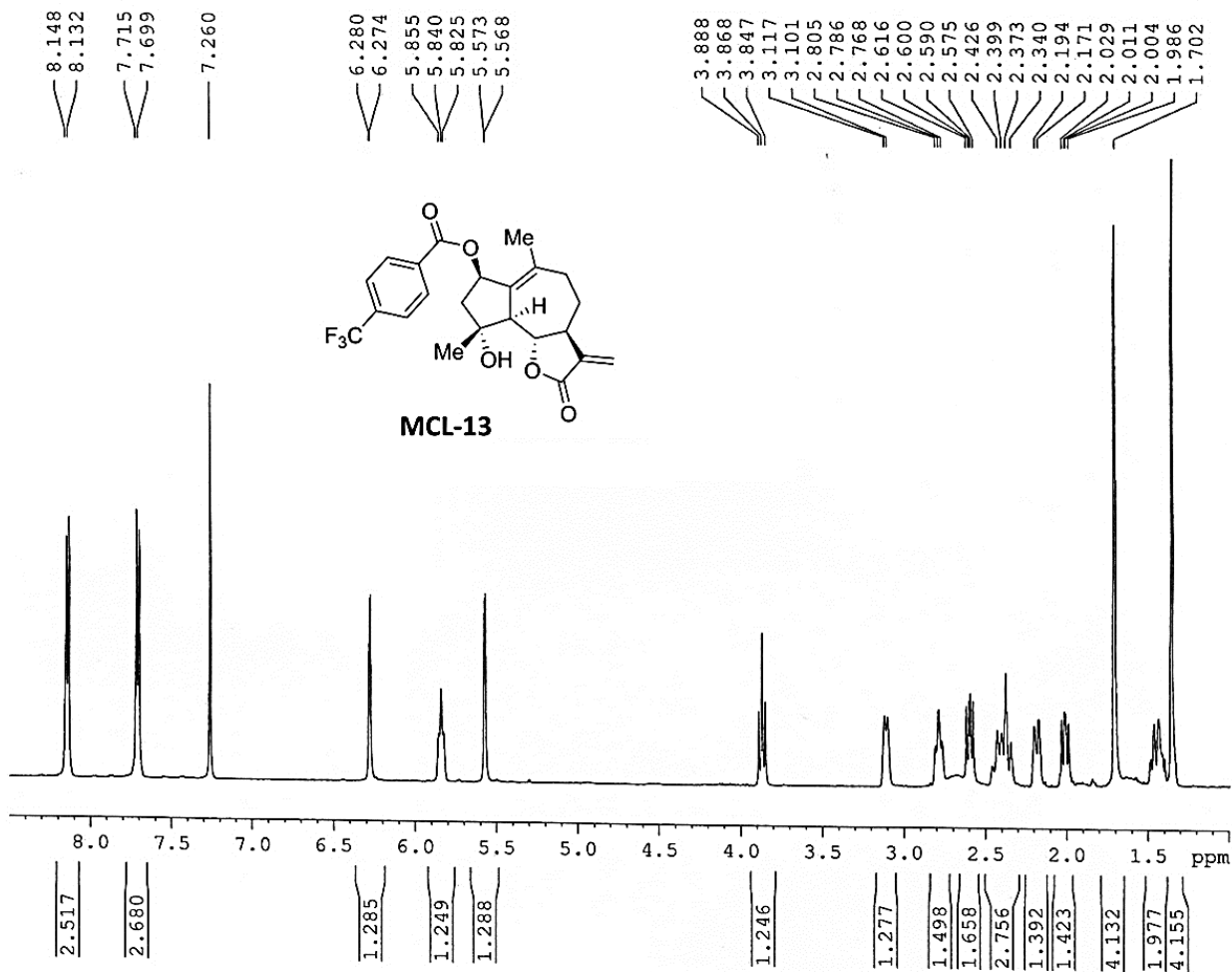


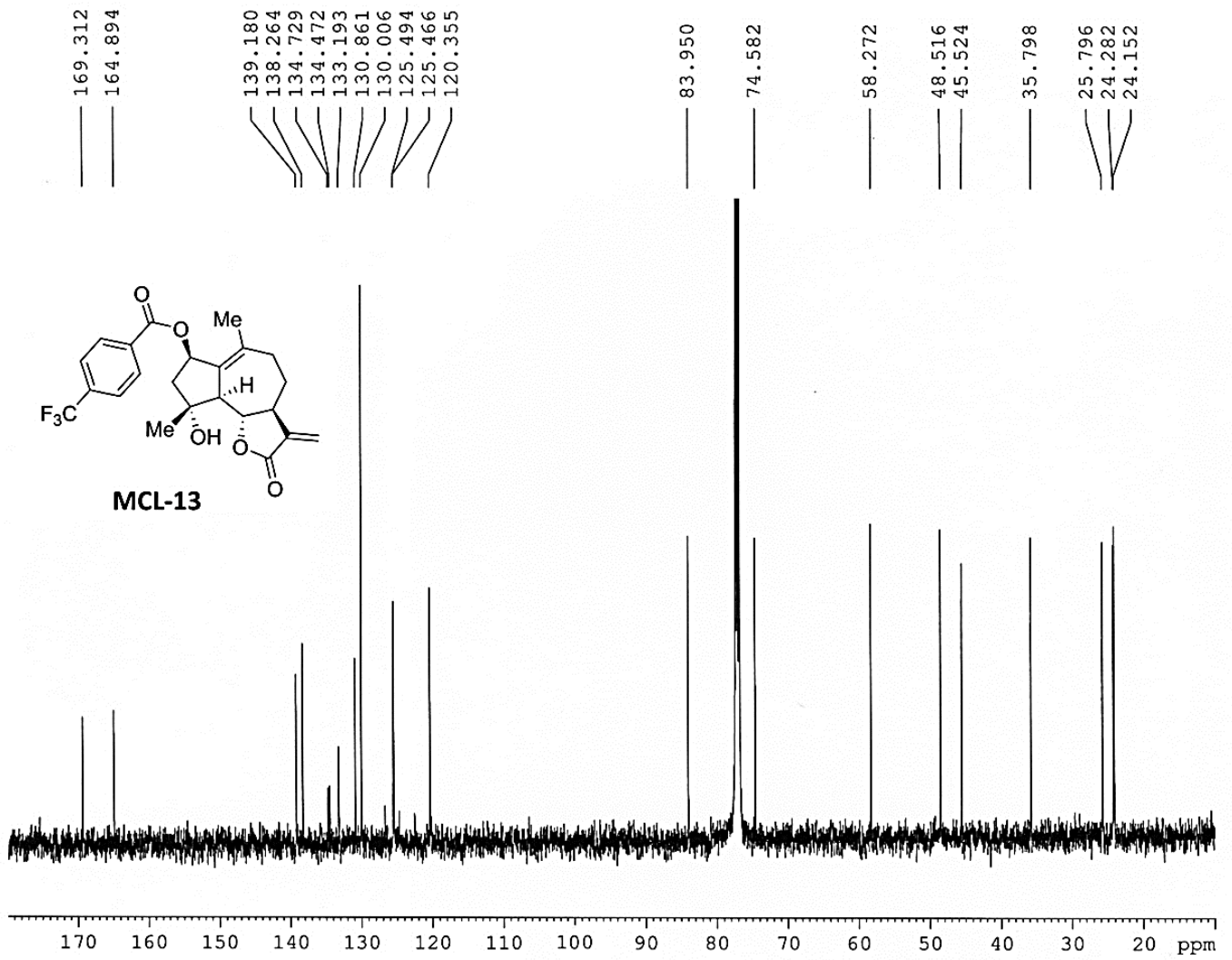




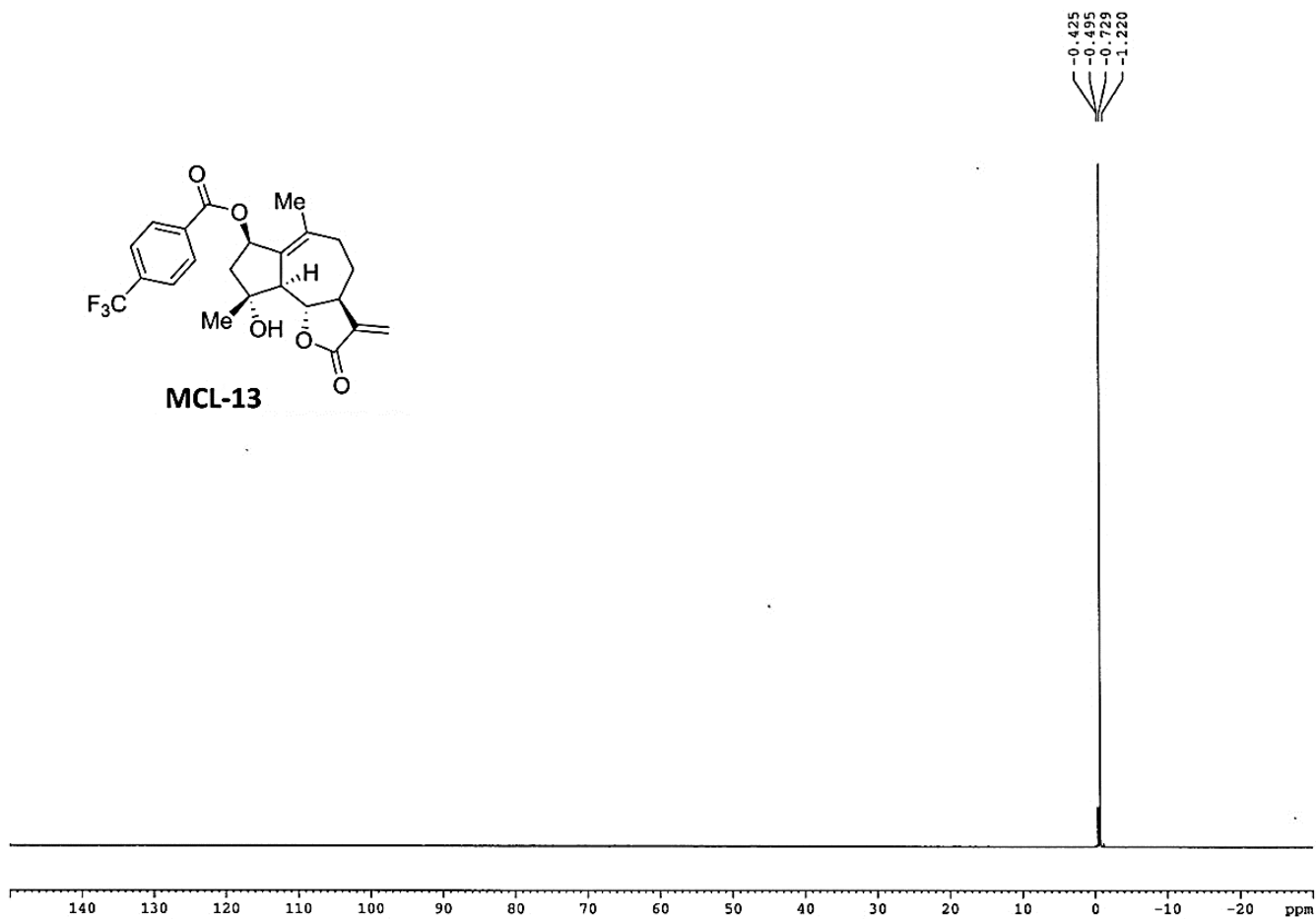
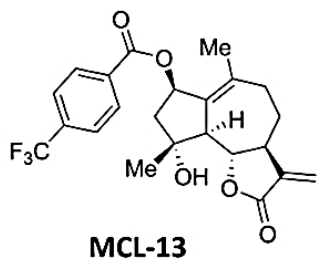


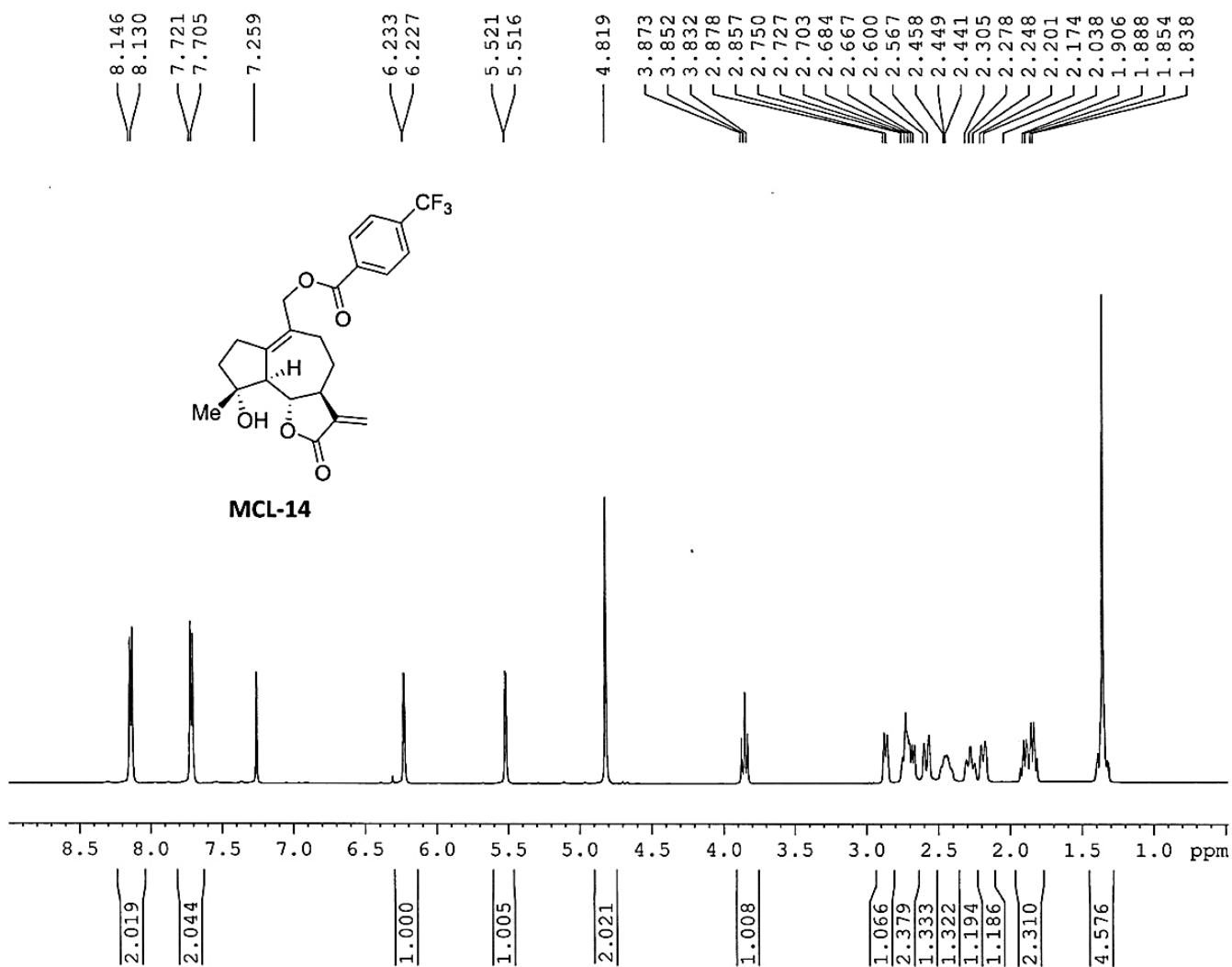
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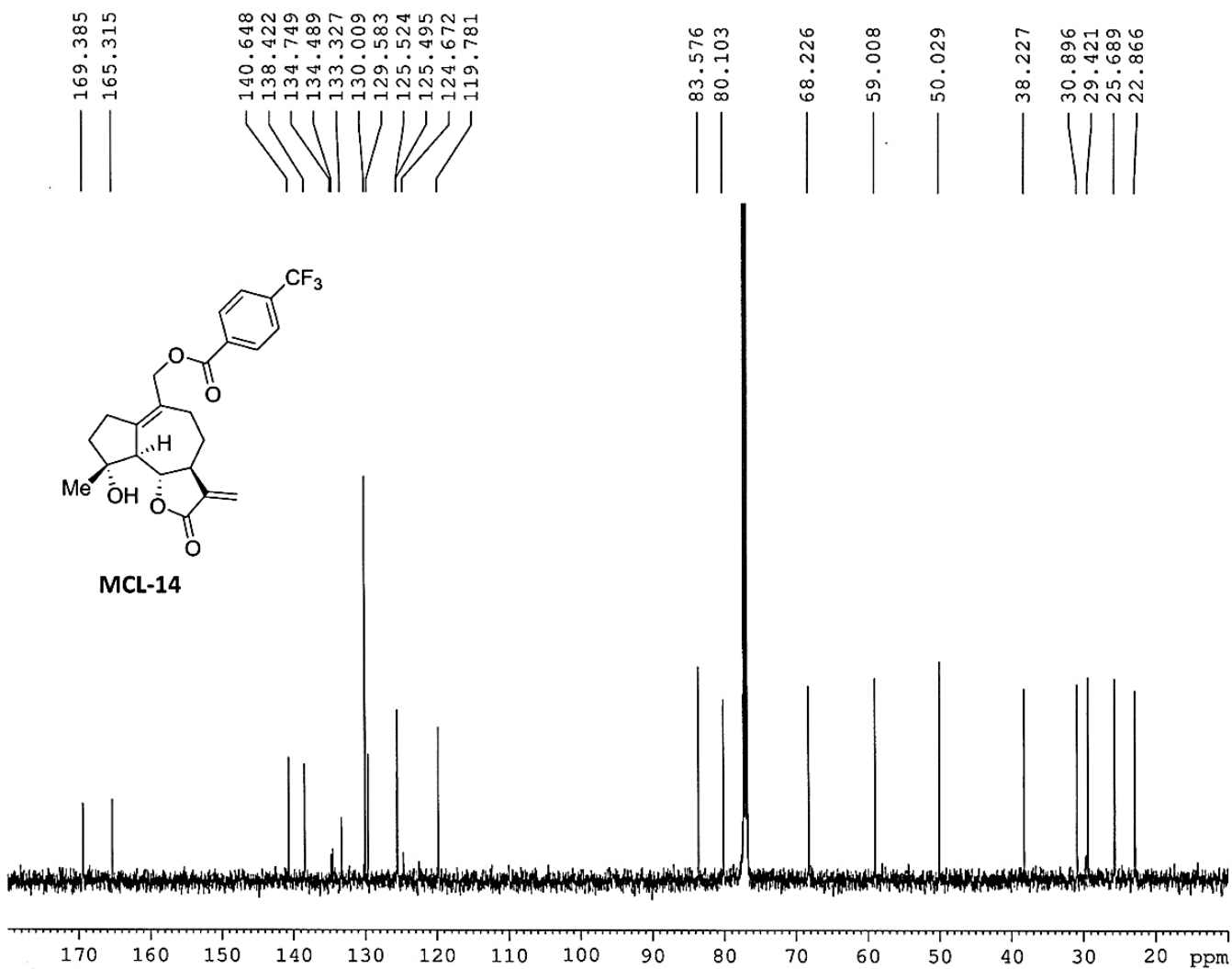


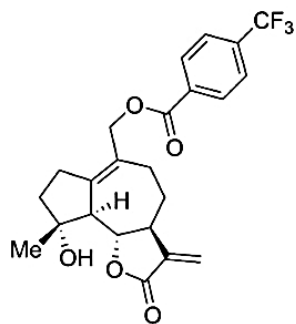




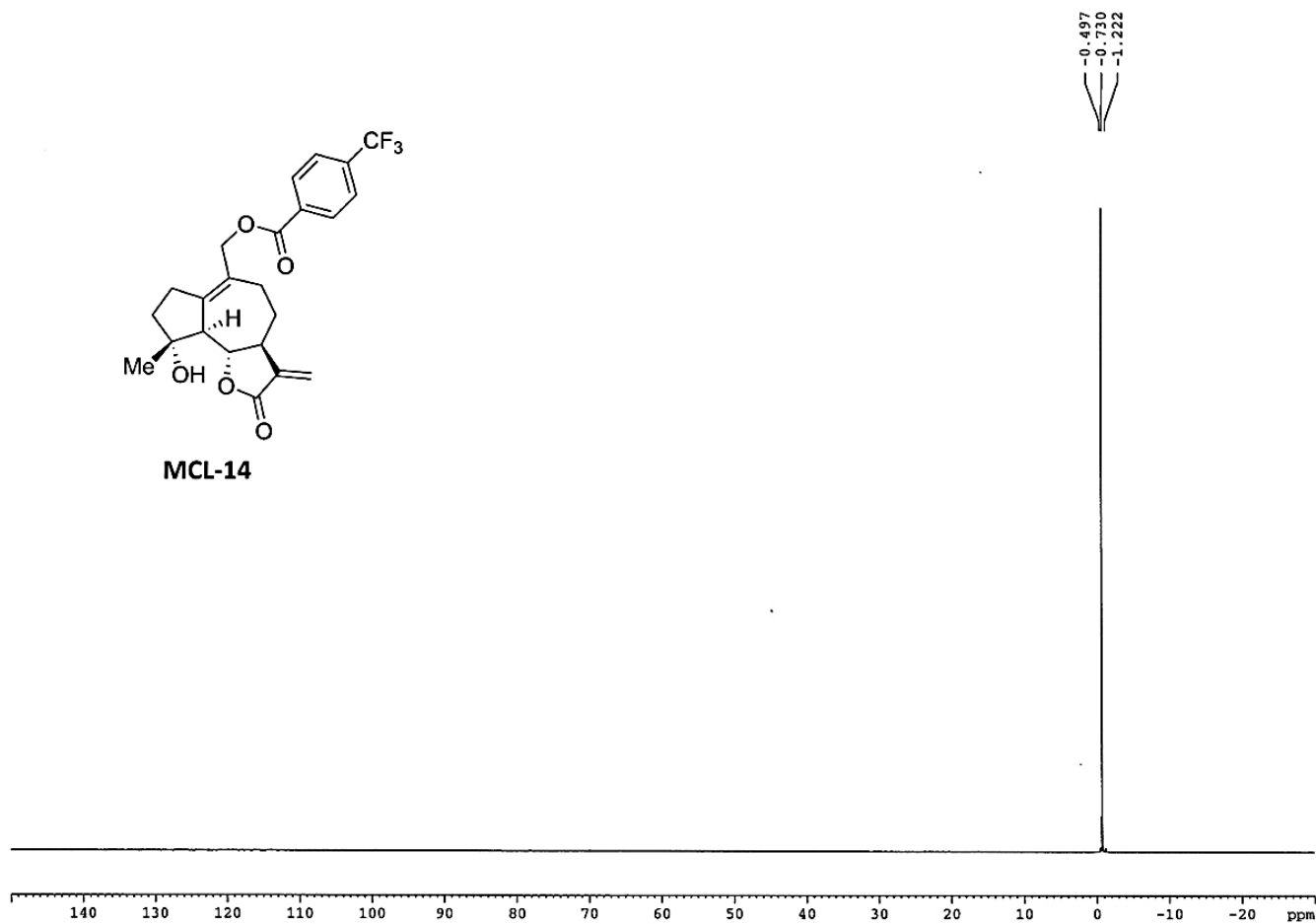


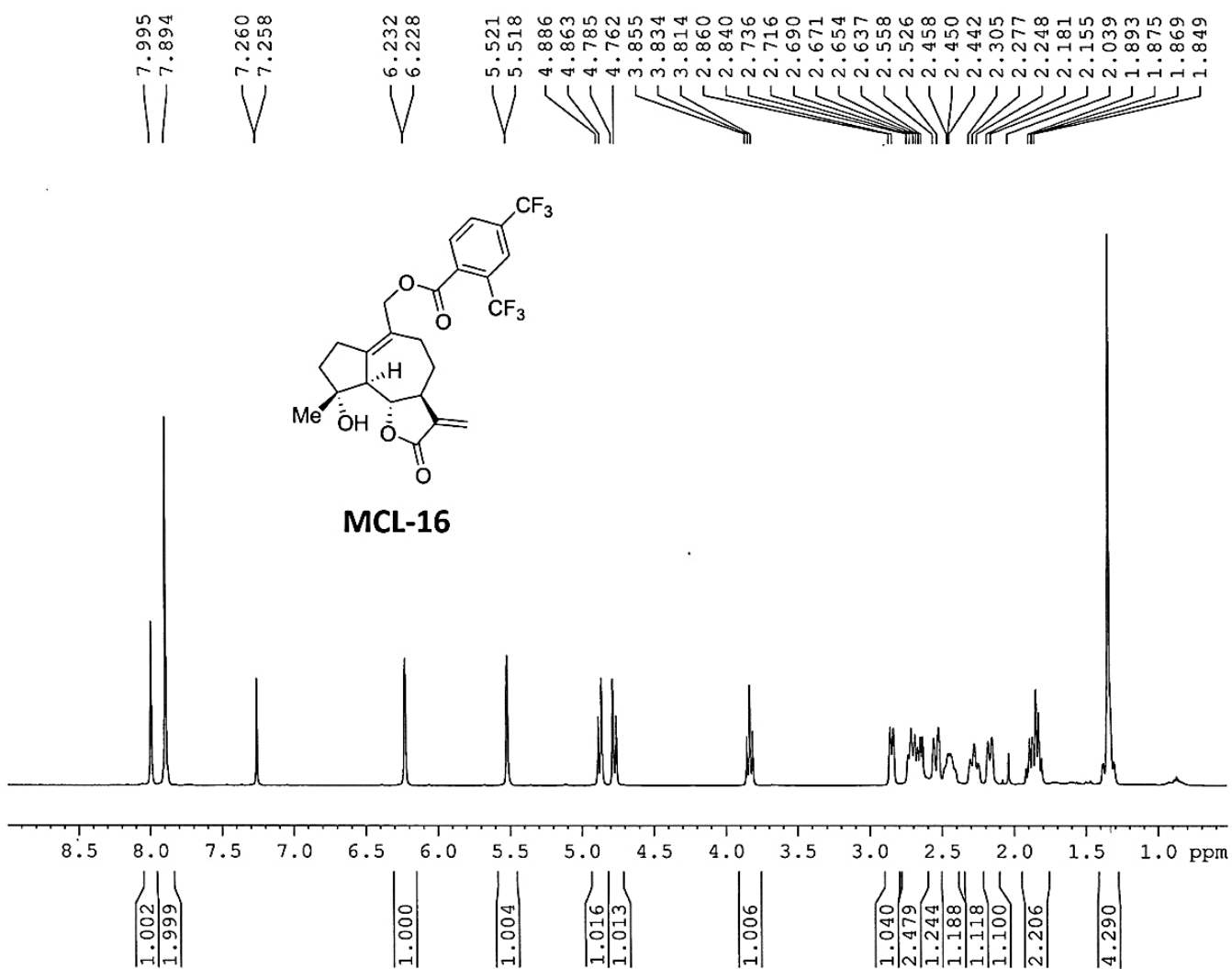


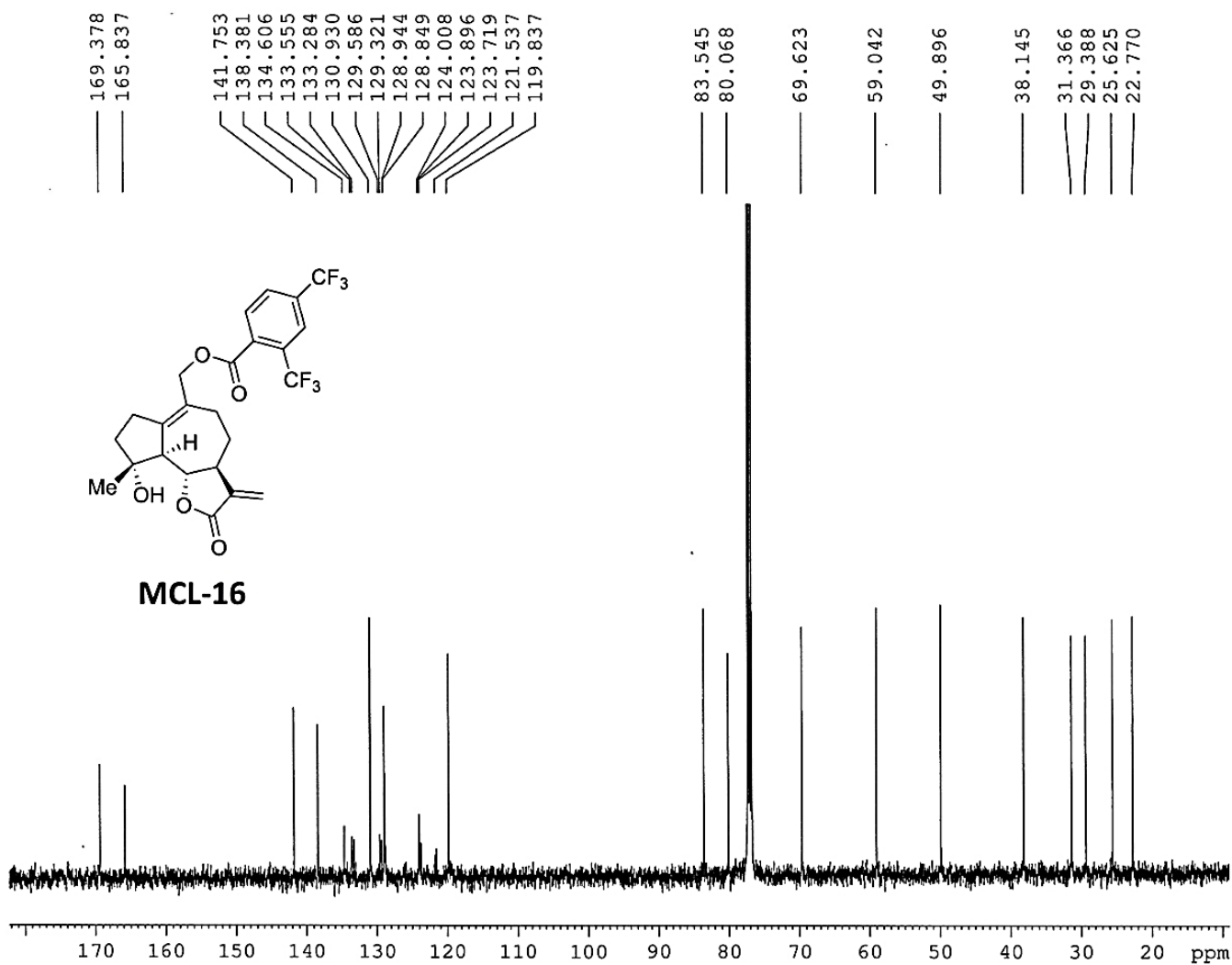


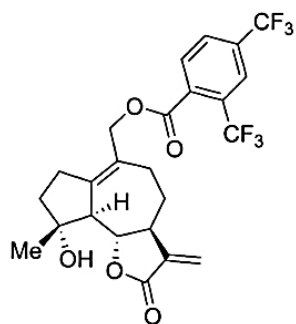


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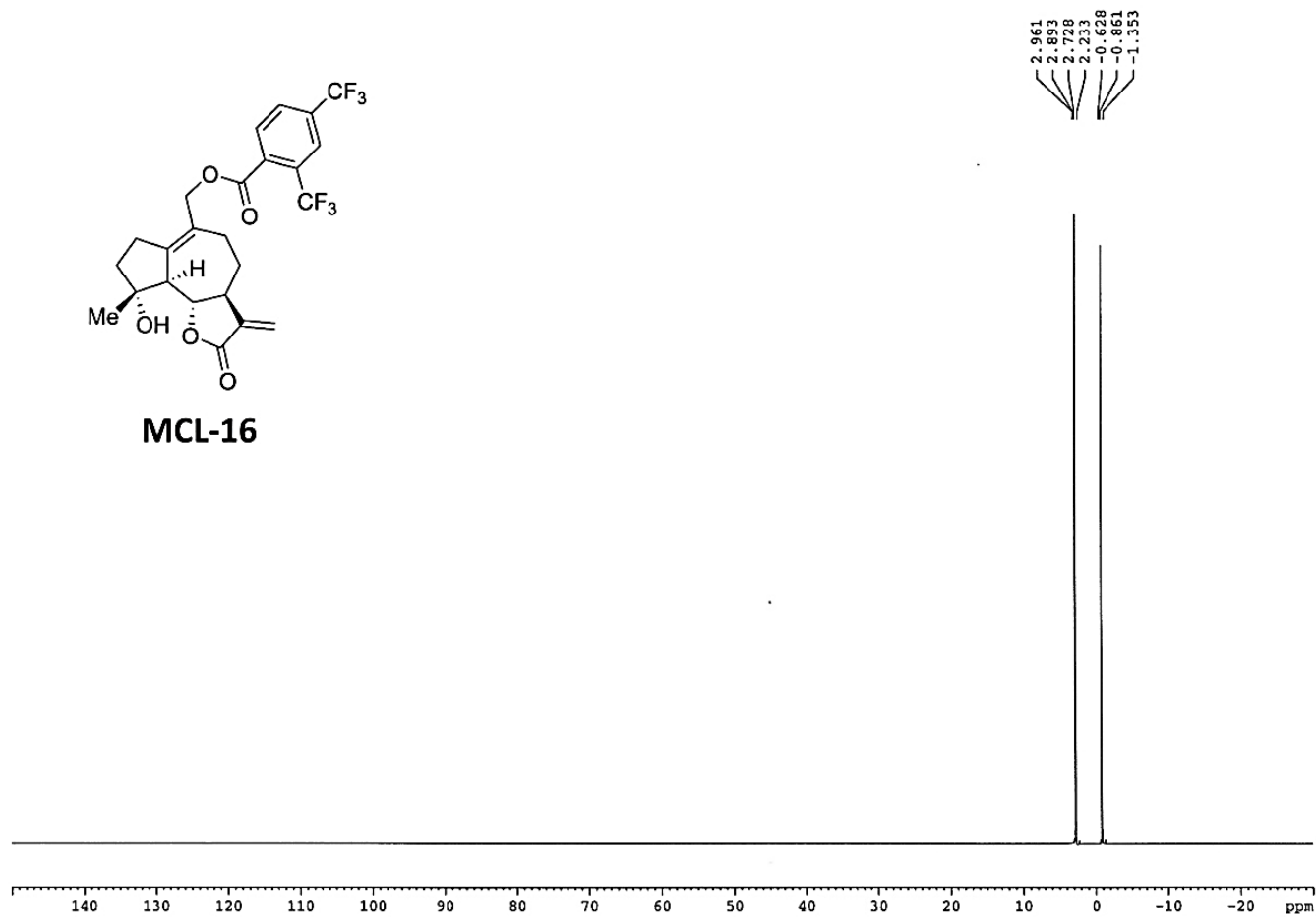


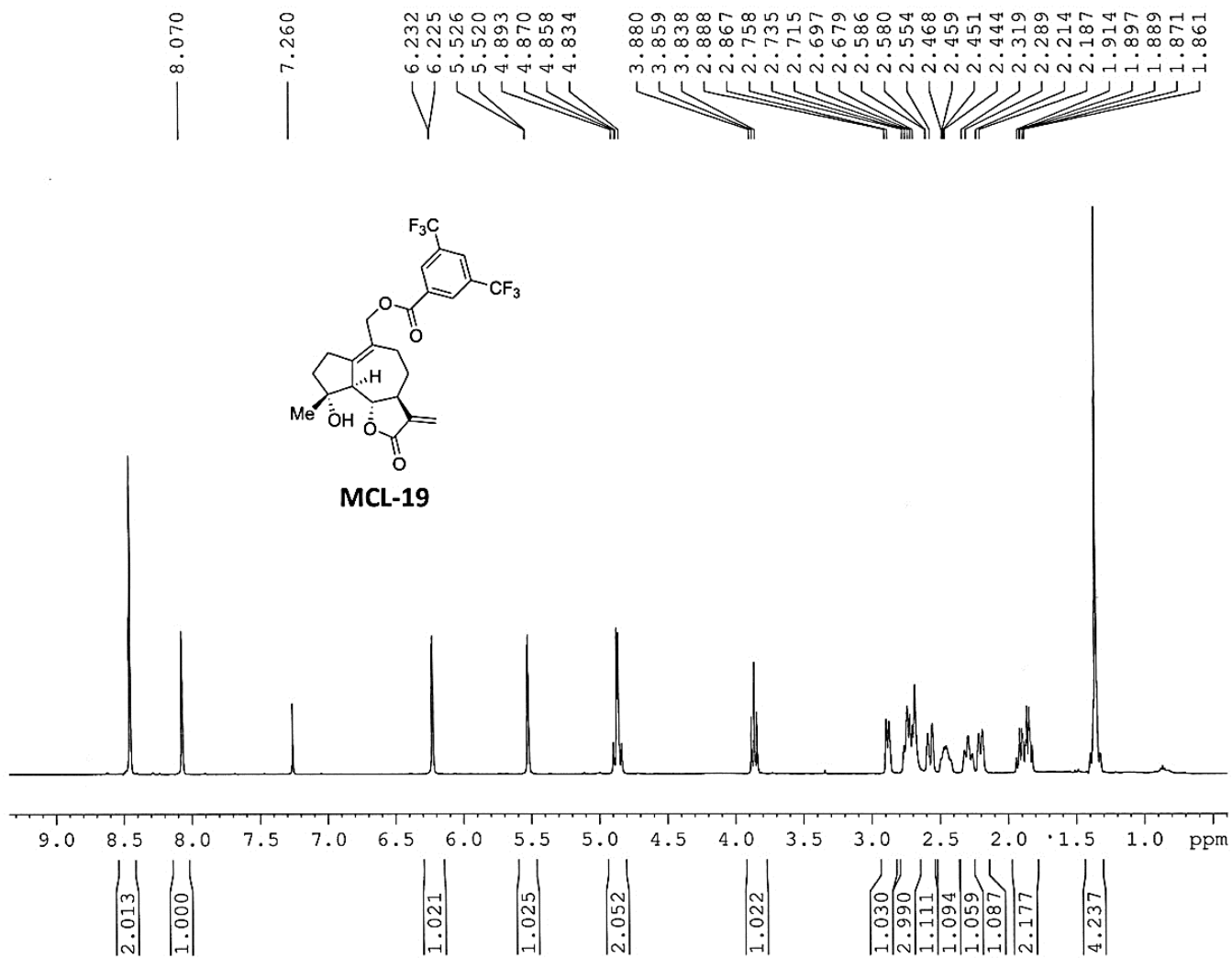




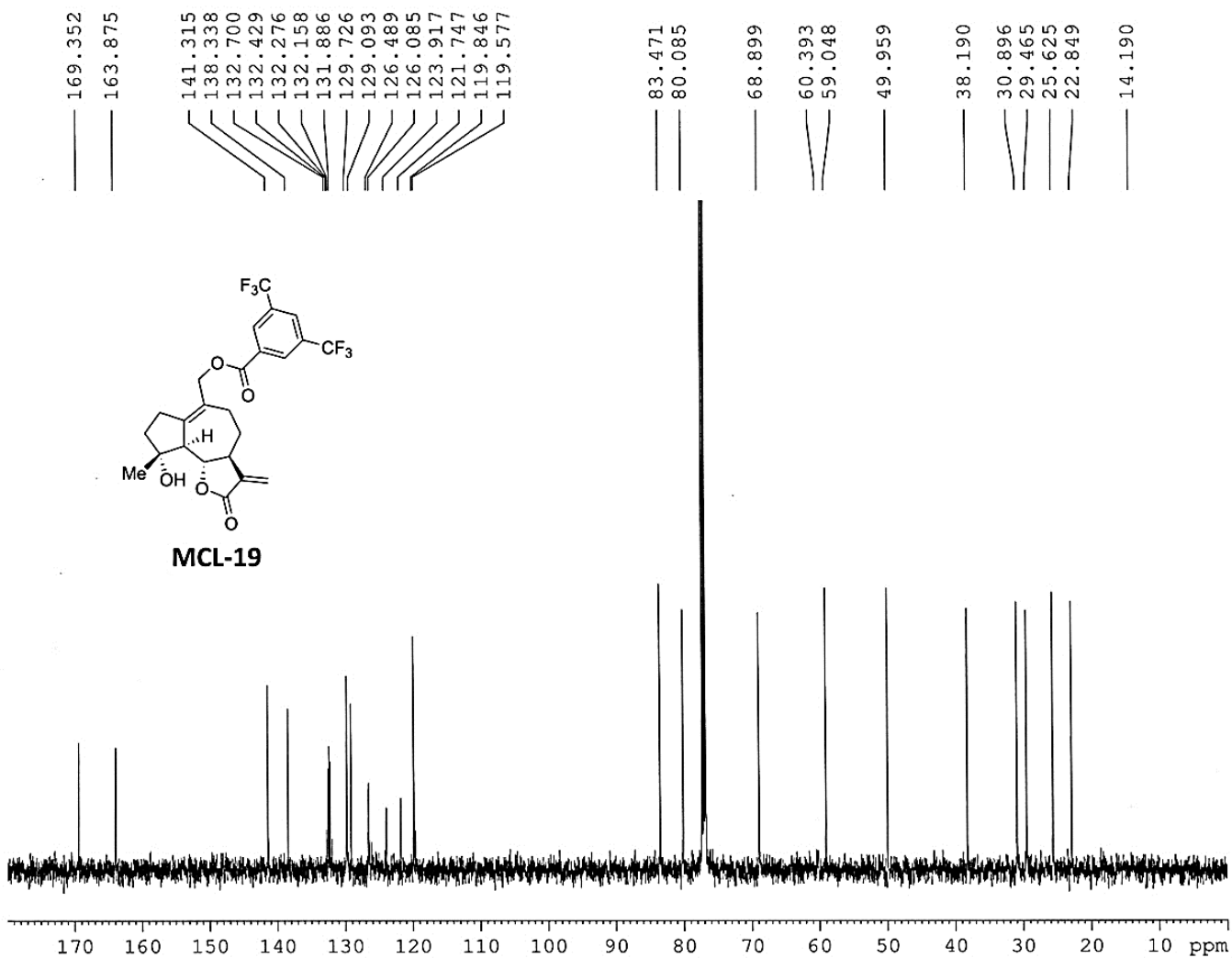


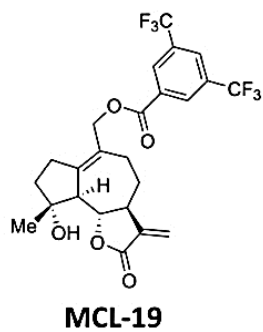
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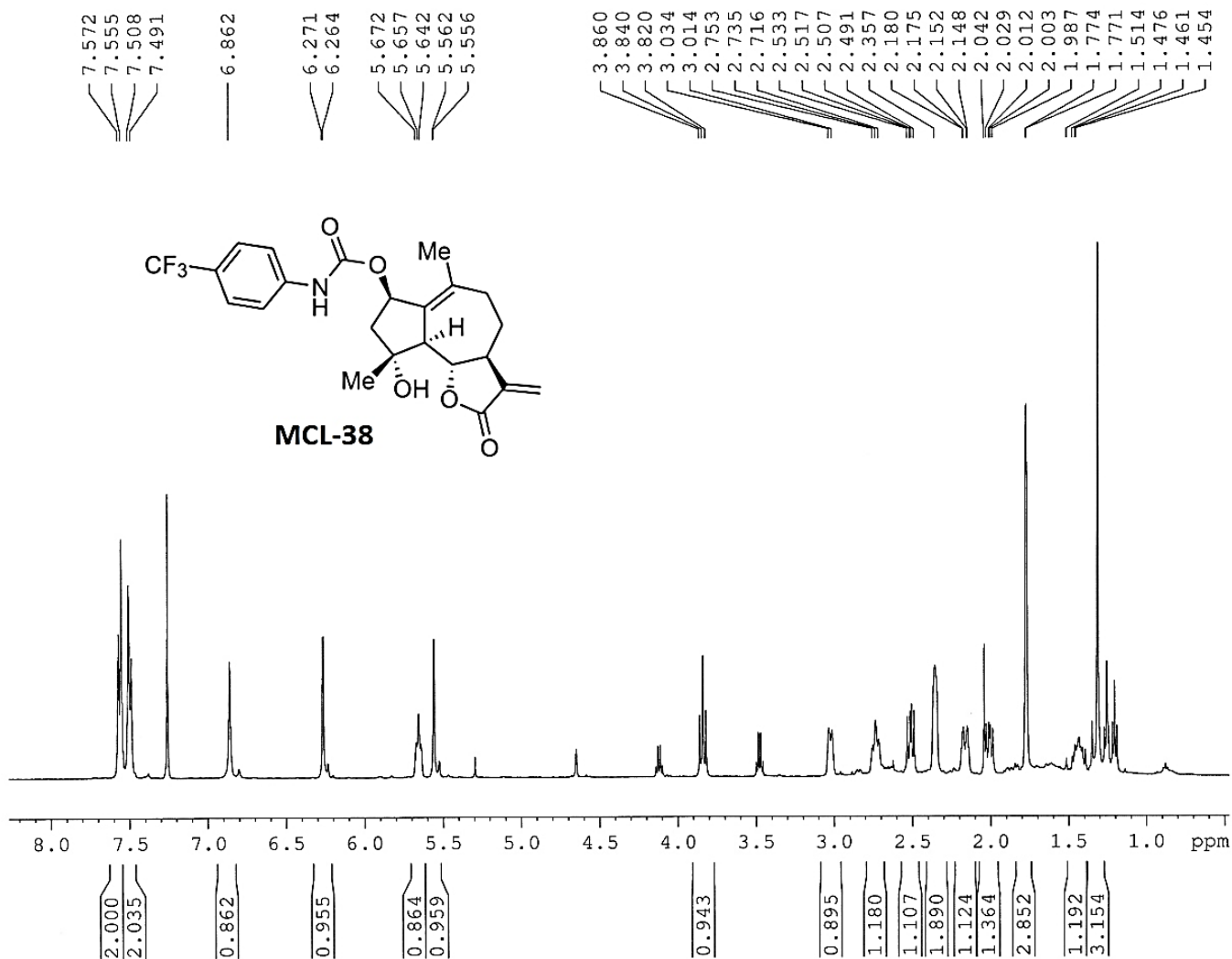


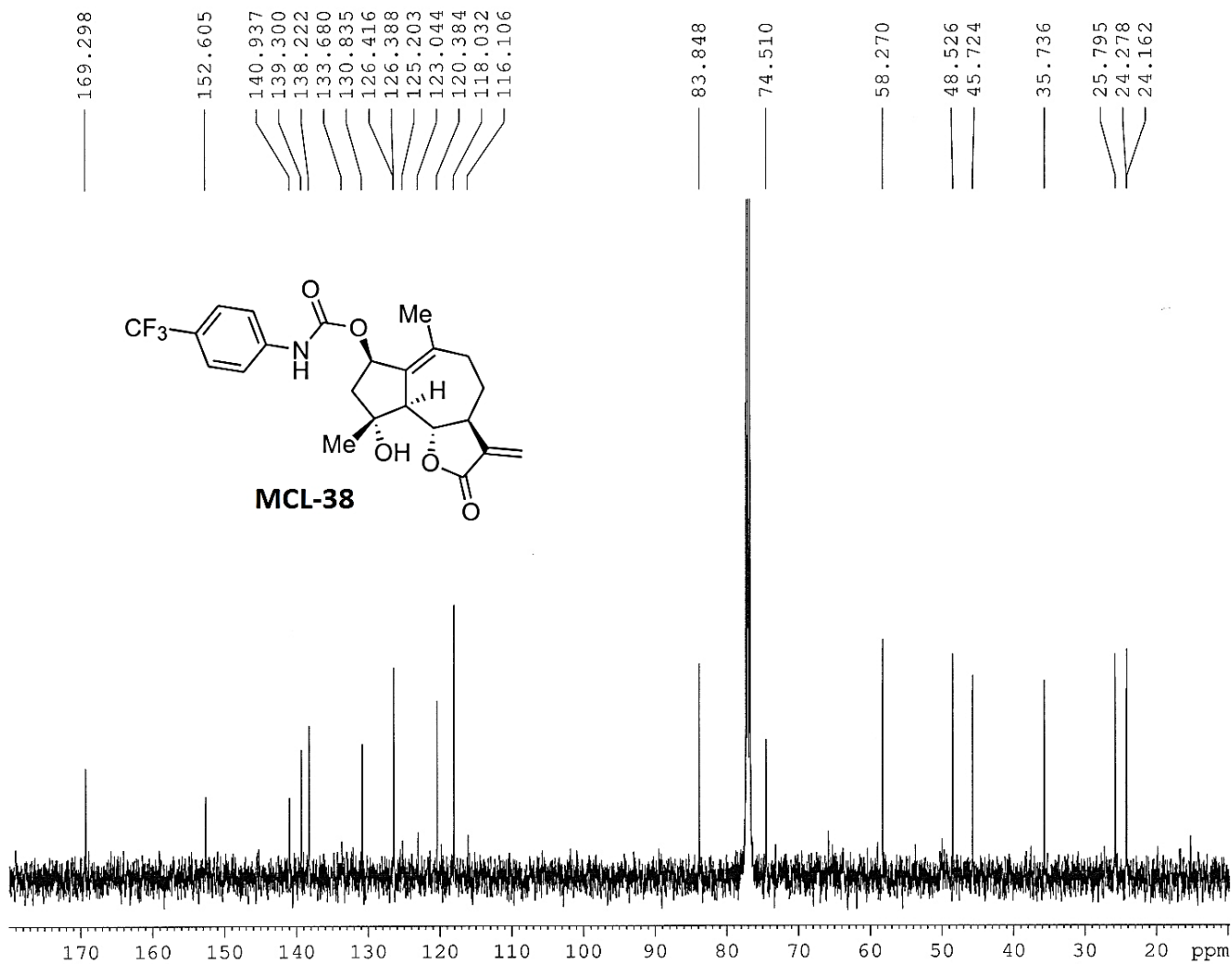


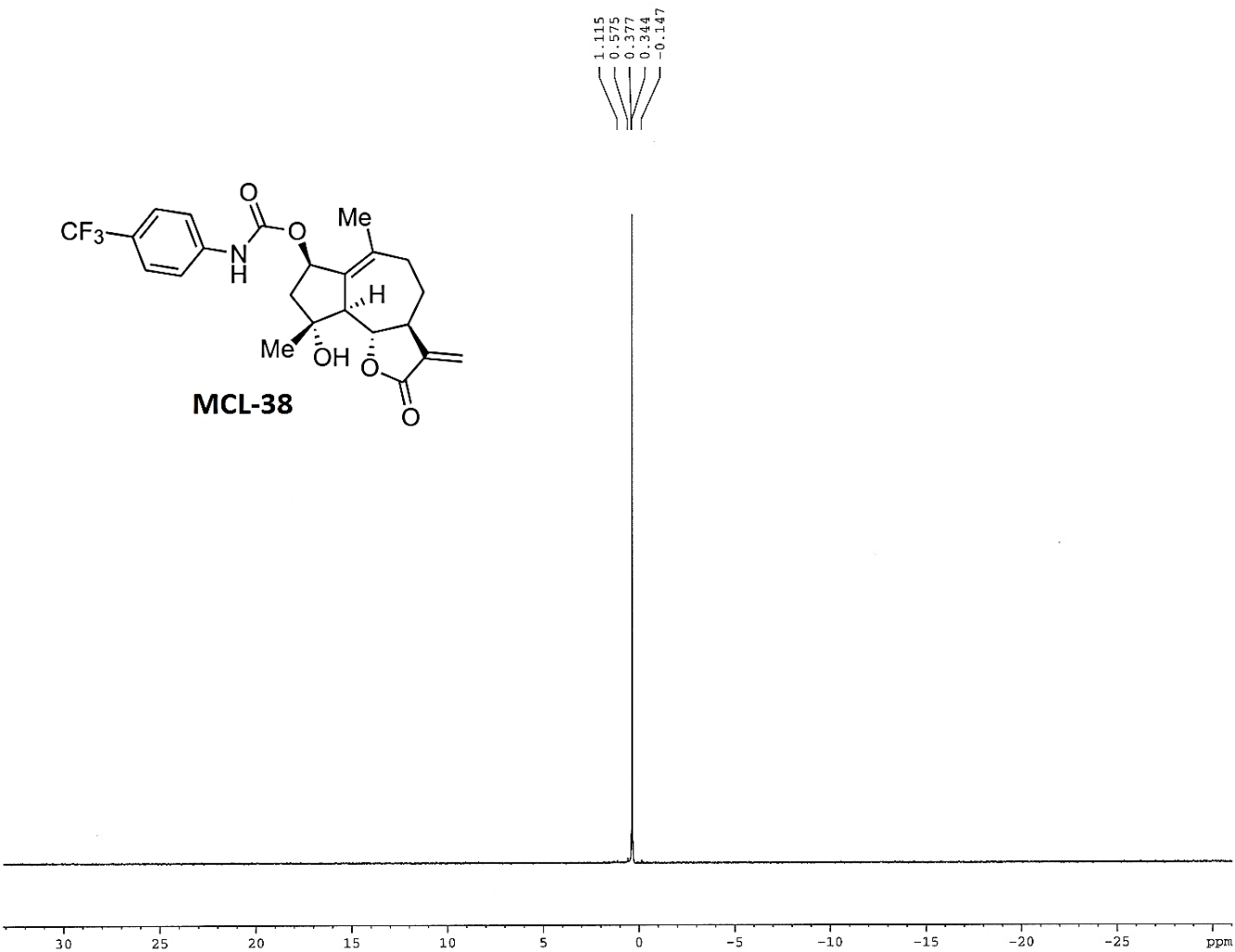




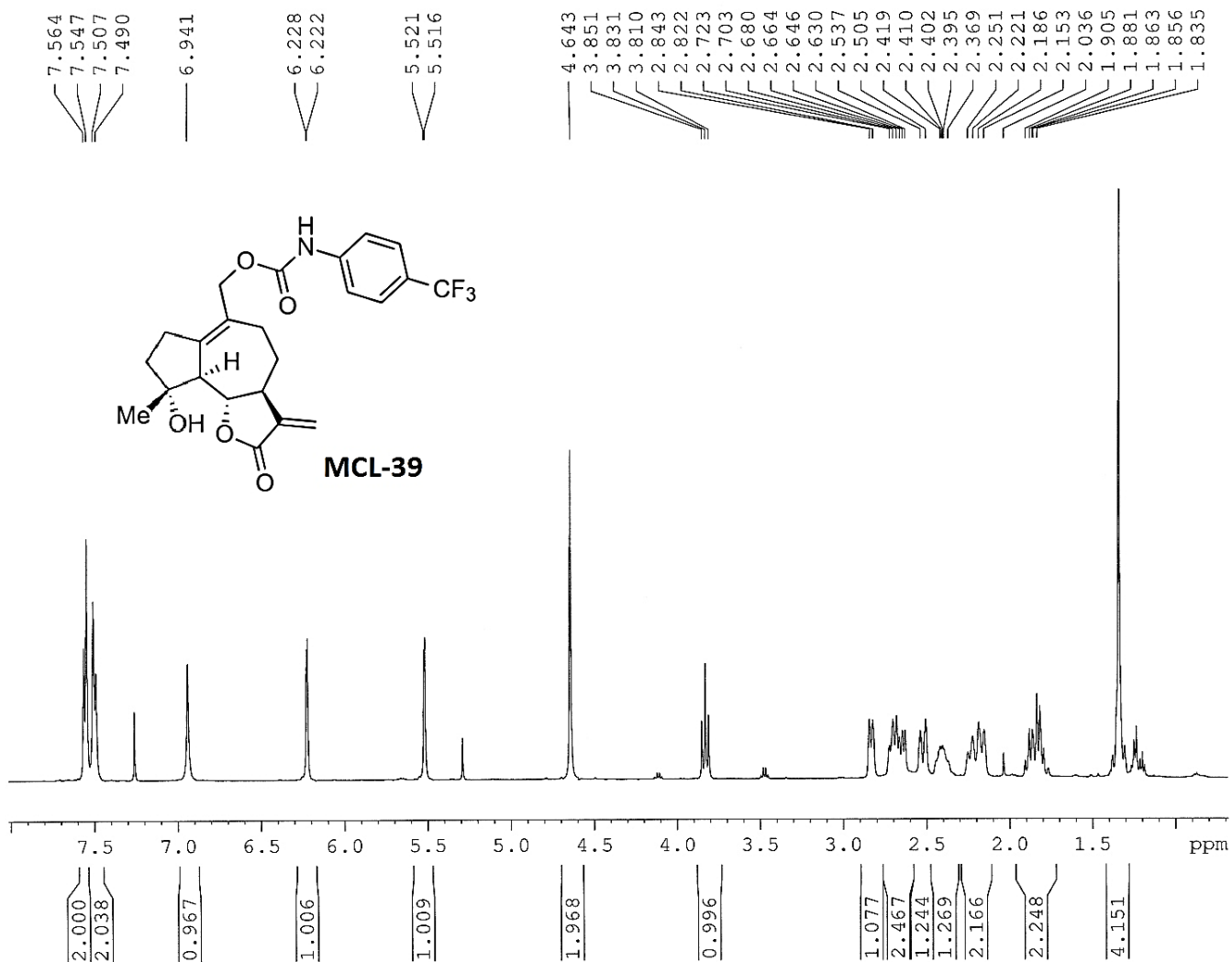


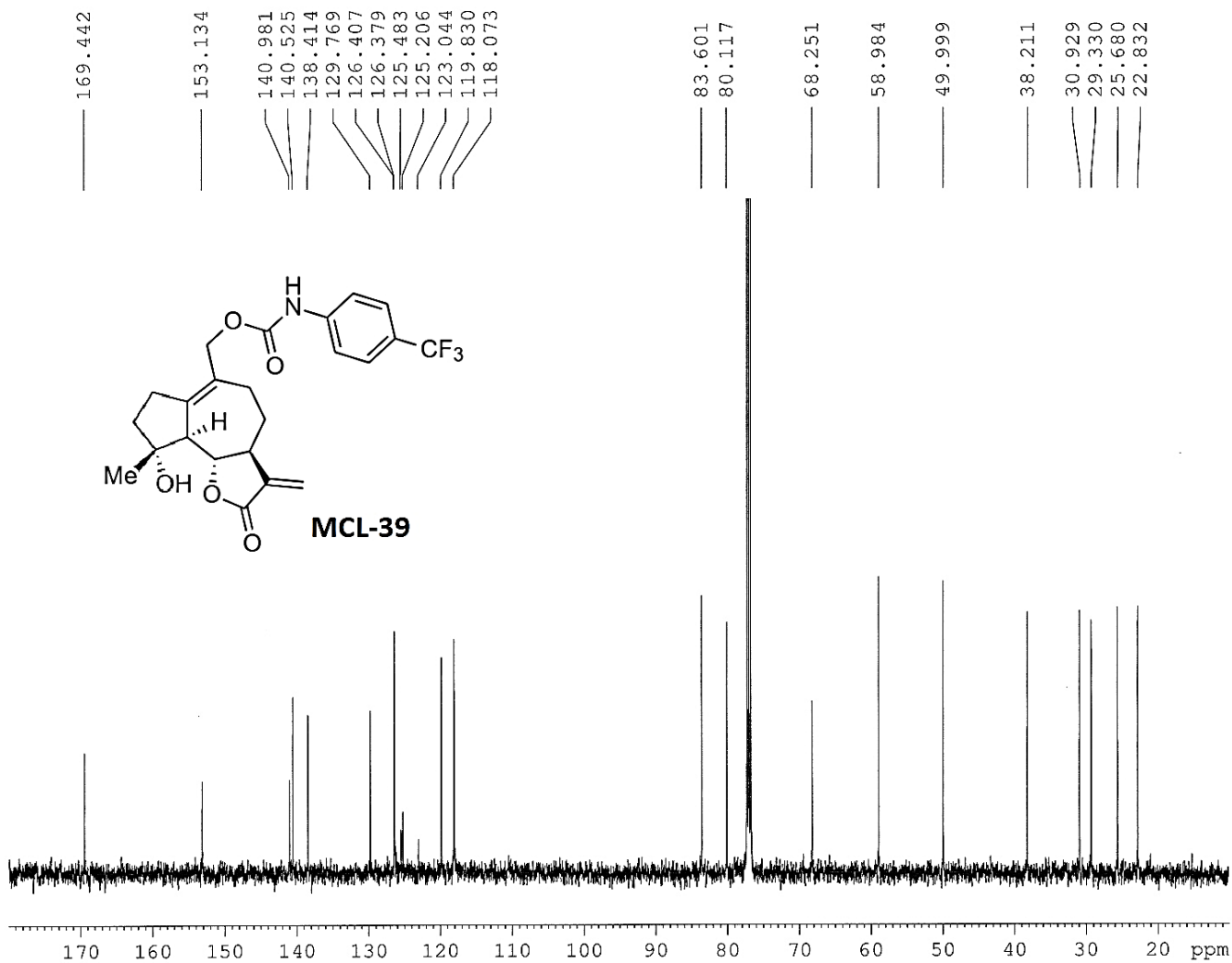


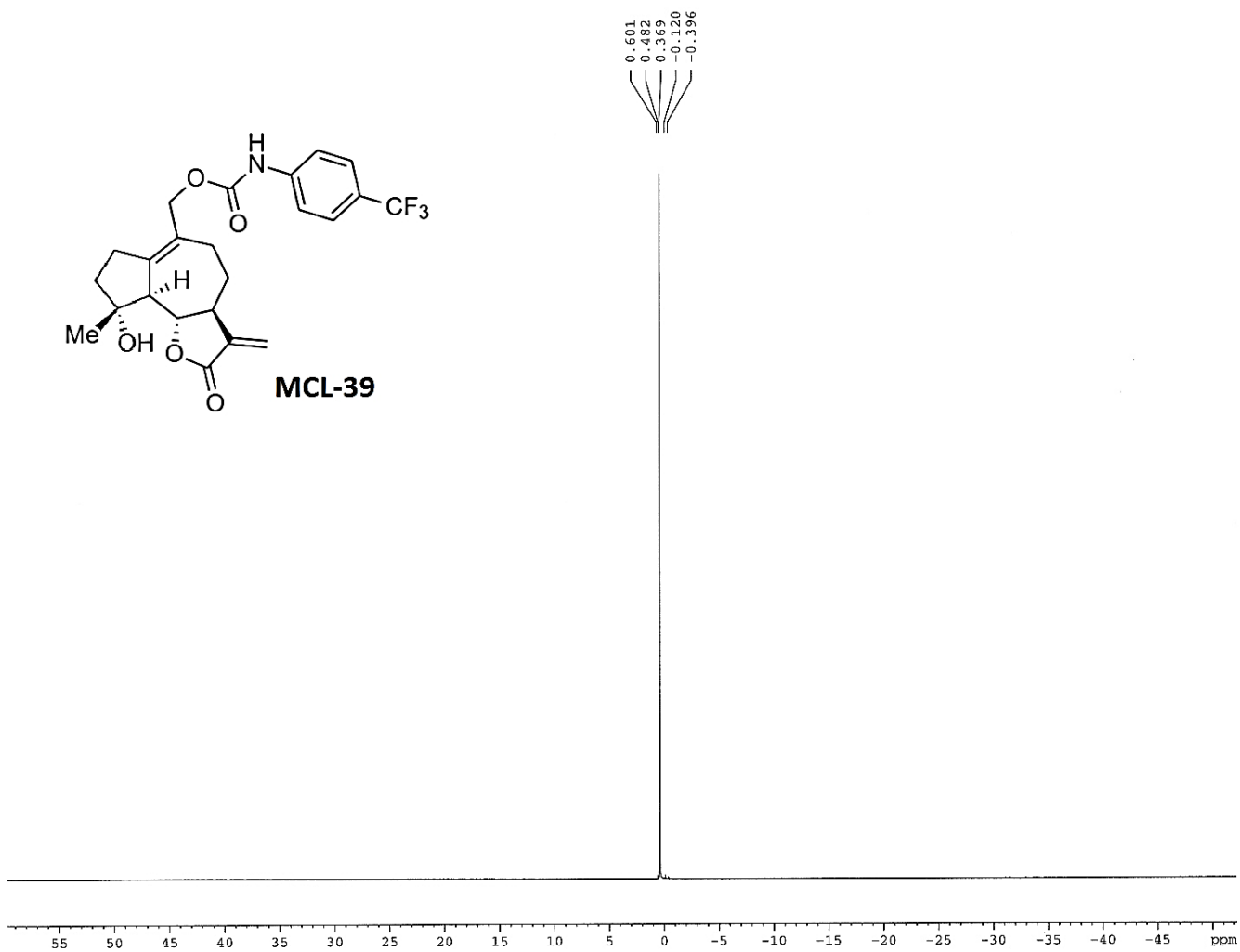




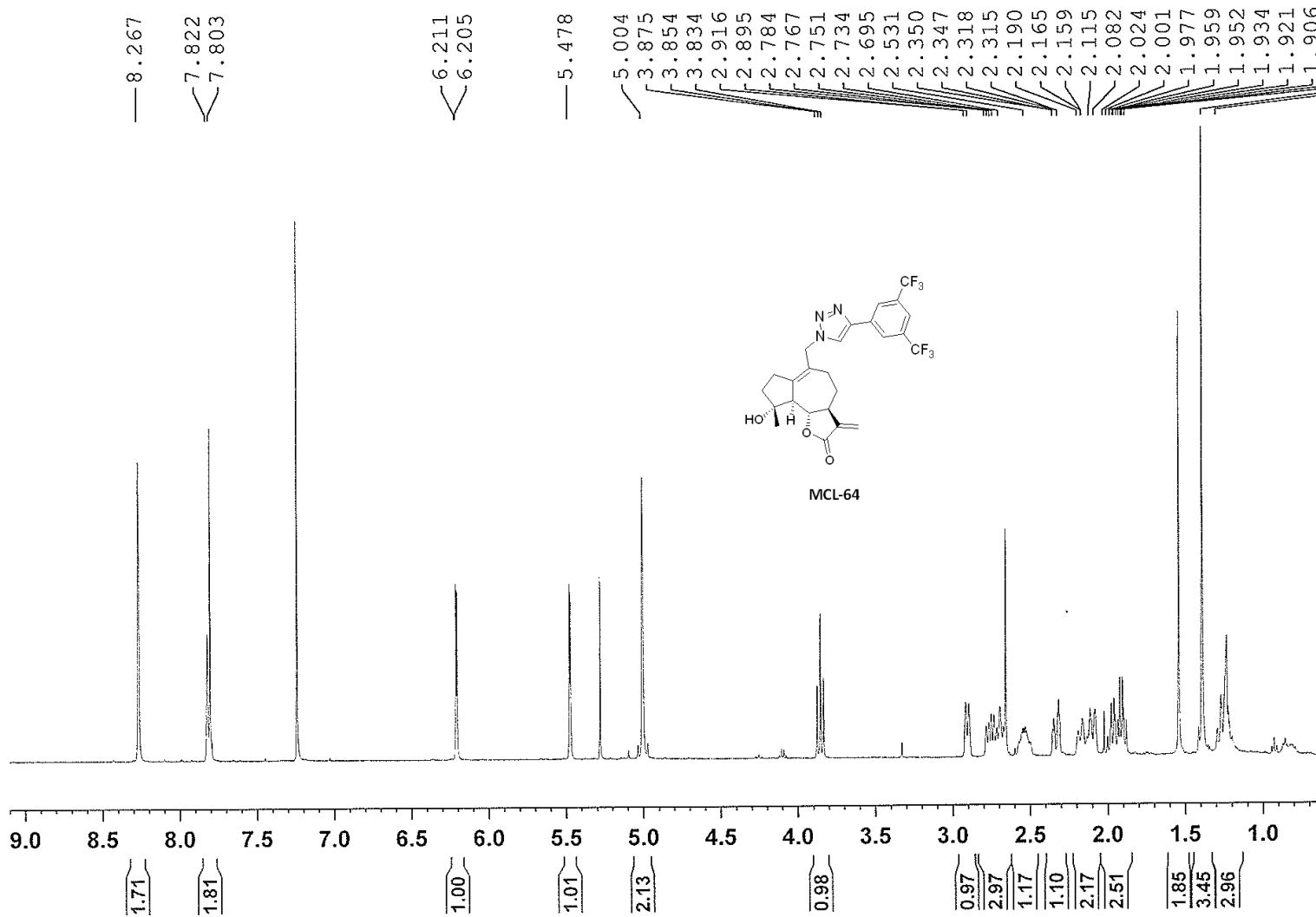
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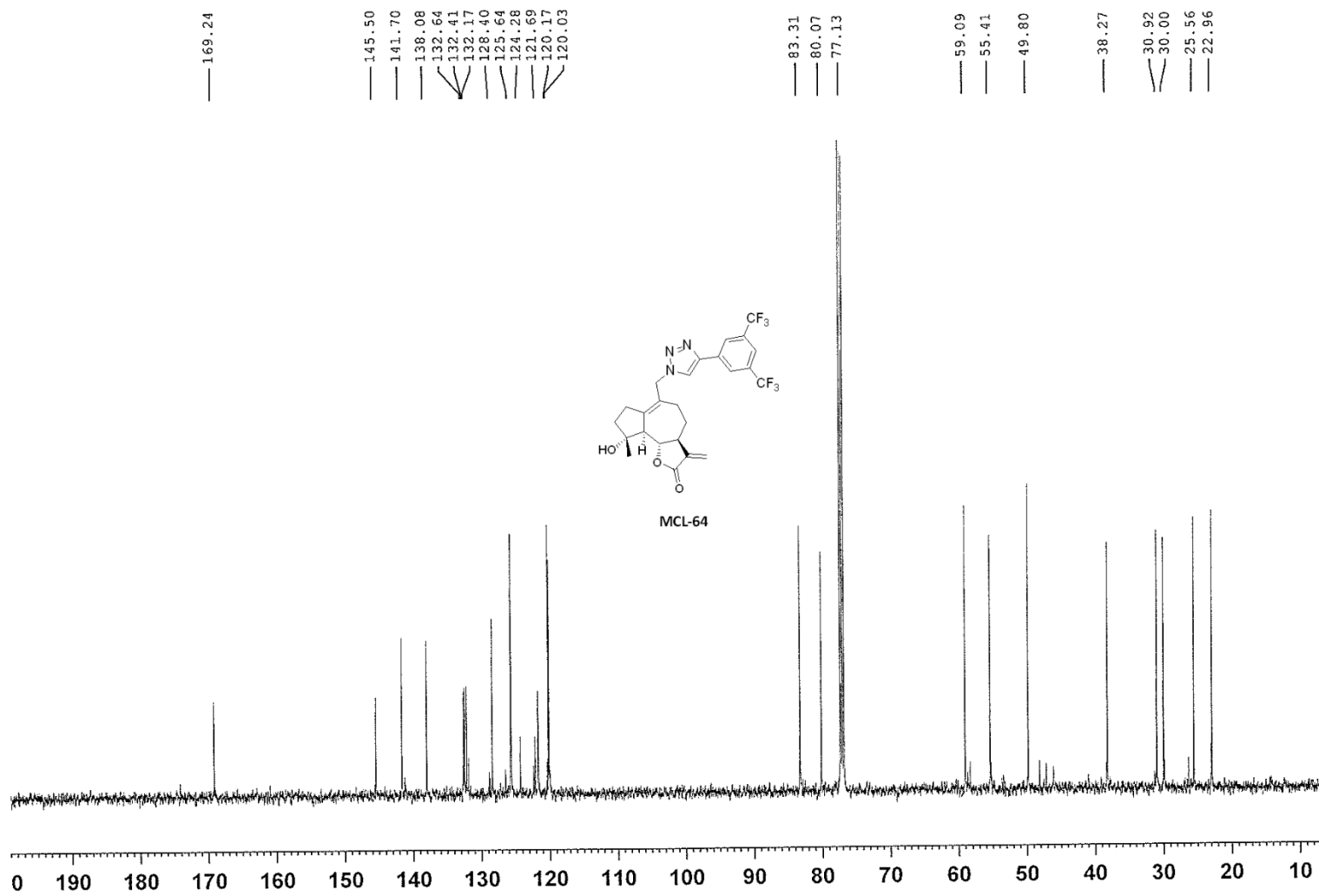


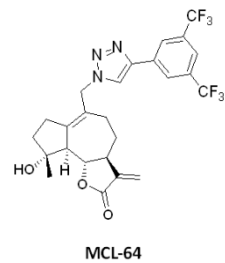
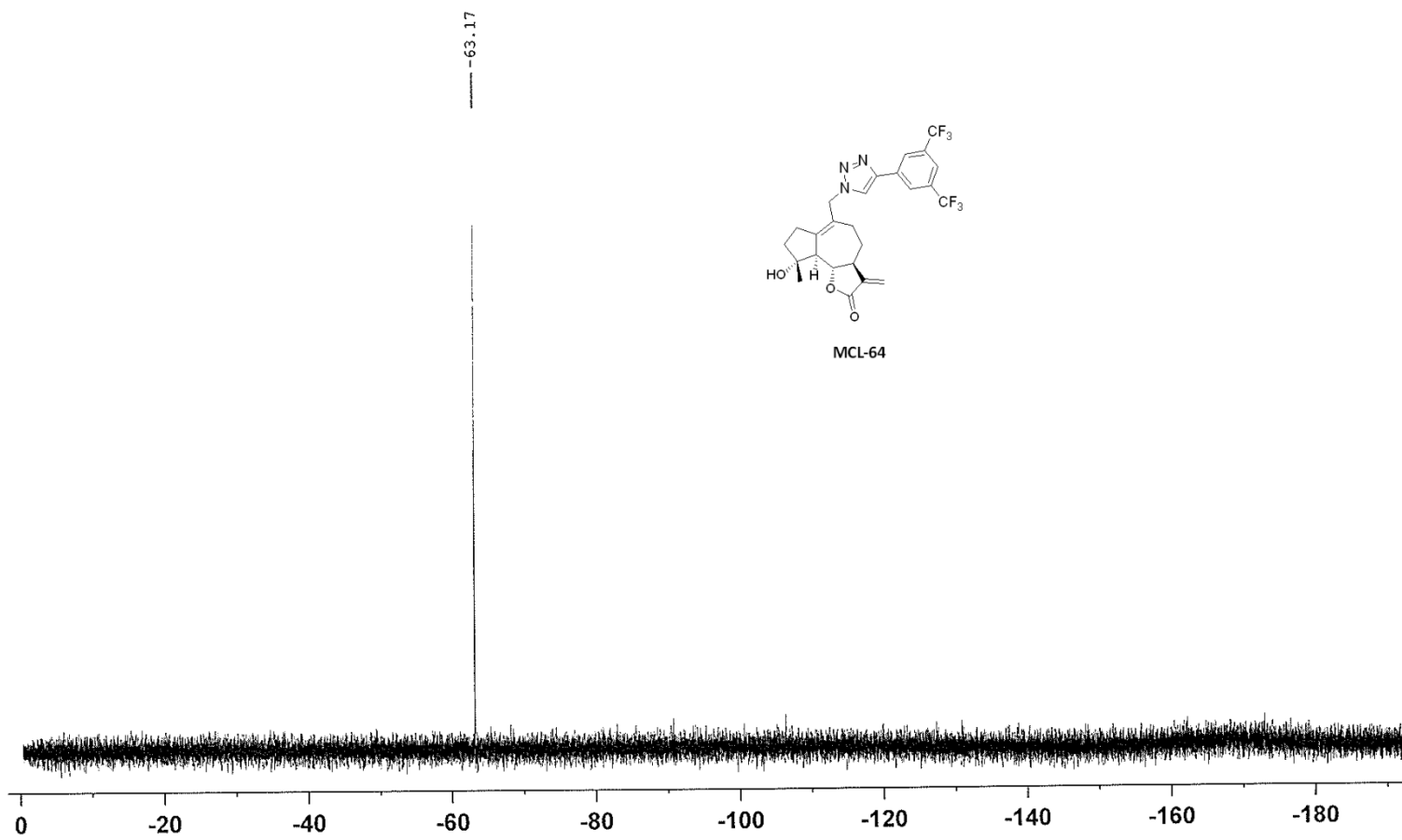












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