

- thus the overall fluidic resistance is always approximately the *Rbypass* whether the cells are
- trapped in the confining channels or not. Hence a steady inlet pressure of the
- microchannels is maintained in the experiments.



**Figure S1.** (a) Design of the elasticity microcytometer (adapted from  $\frac{1}{2}$ ). Scale bars: 300 μm. (**b**) Diagram of the fluidic resistance of the device. (**c**) Concept figure of a cell driven by the hydraulic dragging force *Fdrag*. (**d**) Comsol simulation results for calculating the hydraulic dragging force *Fdrag*. The simulation results of cells with different sizes at 9 different locations are combined (adapted from ).

## **Simulation**

- To obtain the hydraulic forces exerted onto the encapsulated cells, we performed finite
- element analysis using commercial software (COMSOL Multiphysics 4.2, Burlington,
- MA, USA) of multiple models of the confining microchannel structure containing an
- encapsulated cell with different diameters (*Dcell*) at different encapsulated position (*L*), in
- order to obtain the hydraulic pressure profile exerted onto the encapsulated cell as a
- function of *Dcell* and *L* along the channel. The position and deformed shape of a cell were
- 1 preset in the geometry of the simulation and we set the same channel dimensions (*i.e.*
- height *Hchannel*, length *Lchannel* 2 , inlet width *Win* and outlet width *Wout*) identical to the
- 3 fabricated device in all the models, whereas in each model the deformed cell diameter
- 4 (*Ddeform*) was computed using **Eqn. 7**. We then obtained the resultant drag force *Fdrag* by
- 5 integrating the simulated pressure profile over the cell surface. By performing a series of
- 6 simulations of multiple models of with different location and deformation of an
- 7 encapsulated cell, we were able to obtain the relation among the drag force *Fdrag*, the
- 8 location *L* and cell diameter *Dcell.*
- 9

## 10 **Deviation analysis of the three models**

The whole cell strain could be calculated by  $\varepsilon = \frac{1}{\sqrt{2}} \int y dy$ *V y V* 11 The whole cell strain could be calculated by  $\varepsilon = \frac{1}{V}\int_{V} y dV$ , where *y* is the displacement of 12 the finite elements in a deformed cell along the direction perpendicular to the confining 13 microchannels. The whole cell strain could be expressed as:

$$
14 \t\varepsilon = (1 - \frac{W_{deform}}{D_{cell}})^2 (1 + \frac{W_{deform}}{2D_{cell}})
$$
\t(S1)

15

16 The strains of MCF-10A cells were:  $0.081 \pm SD$  0.059 at 100 Pa,  $0.172 \pm SD$  0.073 at

17 200 Pa,  $0.218 \pm SD$  0.086 at 300 Pa and  $0.270 \pm SD$  0.109 at 400Pa.

18





 **Figure S2.** Deviation analysis of the three models. *EH*, *E<sup>T</sup>* and *EHT* are the Young's moduli calculated by the Hertz model, the Tatara model and the hyperelastic Tatara model, respectively. (**a, b**) The deviations between and that originate from the geometric

correction is almost linear; (**c, d**) The deviations between and that originate from the

hyperelastic correction is strongly hyperelastic.

## **Statistics of the cellular and nuclear sizes**







6 Scattering plots of nuclear diameter versus cell diameter of MCF-10A ( $n = 30$ ), MCF-7

7 (n = 46), MDA-MB-231 (n = 43) and PC3 cells (n = 41). The linear fitting was conducted

by the least-squares method under the condition of intercept = 0. (**c**) Nucleus-cell length

ratio and (**d**) nucleus-cell volume ratio of the three types of cells. Error bars: S.E.M. \*

10 indicates  $p < 0.01$ .

- 
- 
- 

## **Reference**

- 1. S. Hu, G. Liu, W. Chen, X. Li, W. Lu, R. H. Lam and J. Fu, *small*, 2016, **12**, 2300-2311.
- 2. S. Hu and R. H. Lam, *Microfluidics and Nanofluidics*, 2017, **21**, 68.
-