SUPPLEMENTAL MATERIAL

SUPPLEMENTAL METHODS

1) Positron Emission Tomography Protocol

Transmission CT scans were first performed for attenuation correction purposes. Intravenous bolus administration of $13N$ -ammonia (~20 mCi) was performed simultaneously with list mode imaging acquisition over 20 minutes. Thirty minutes after completion of the rest images, intravenous regadenoson (0.4 mg) was infused over 30 seconds. Thirty seconds after completion of the regadenoson administration, a second dose of $13N$ -ammonia was injected and images were recorded in the same manner. Heart rate, systemic blood pressure, and 12-lead electrocardiogram were recorded at baseline and every minute after regadenoson infusion.

2) Assessment For Scatter From Liver And Attentuation Correction Using An Anthropomorphic Phanton

We performed a phantom study to assess the biases in global and regional retention and myocardial perfusion reserve index (MPR index) estimates due to (1) scatter from liver activity and (2) lack of attenuation correction. The Data Spectrum Anthropomorphic Torso Phantom with cardiac insert was scanned on the D-SPECT camera under two conditions: Tc-99m activity in the cardiac insert only and Tc-99m activity in both the cardiac insert and the liver. Cardiac and liver activity concentrations were equal. Attenuation correction was performed by using a CT image acquired on a separate CT scanner. The CT image was registered to the SPECT image with an automatic rigid alignment algorithm and then converted into an attenuation coefficients map using a tri-linear transformation dependent on CT & SPECT photons energies. Then, the resulted attenuation coefficient map was filtered with a gaussian filter to match SPECT resolution, and to be used within the SPECT iterative reconstruction projection phase for correcting the pixels attenuation effect, as described previously²⁵⁻²⁷.

Reconstructed images were segmented using Corridor 4DM (INVIA Medical Imaging Solutions, Ann Arbor, Michigan). Comparison of cardiac-only and cardiac-and-liver images, after corrections for decay, yielded estimates of the contributions of liver activity to global myocardium and regional segments for equal activity concentrations. We assumed that effects of liver scatter on the LV blood pool were the same as for the global myocardium. The relative activity concentrations of myocardium and liver over time under rest conditions were obtained from published data for ⁹⁴Tc-MIBI PET dynamic images¹⁹; we assumed the same relationships for stress conditions. We also assumed that the contribution of liver activity to cardiac activity over time, determined for equal activity concentrations by the phantom experiment, was proportional to the published liver-to-heart ratio. This enabled us to calculate "scatter-free" time-activity curves for the LV blood pool, global myocardium, and the three segments. Similarly, comparison of attenuation-corrected and nonattenuation-corrected heart-and-liver images yielded estimates of the biases due to lack of attenuation correction and enabled us to calculate "attenuation-corrected" time-activity curves for the same regions. "Scatter-free" and "attenuation-corrected" TAC were calculated for 4 patients, for rest and stress conditions, using standard and spline-fitted reconstructions.

Mean K1 percentage differences between cardiac-only and cardiac-and-liver data in spline-fitted images were $5.85 \pm 0.17\%$ for global rest K1, 7.67 $\pm 0.45\%$ for global stress K1 and 1.93 $\pm 0.54\%$ for the stress/rest K1 ratio (myocardial perfusion reserve) (**Table S3**). Percentage differences of similar magnitude were observed for regional values during rest (5.74 \pm 0.18% in LAD, 6.16 \pm 0.15% in LCX, and $6.59 \pm 0.17\%$ in RCA territories), and stress (7.61 \pm 0.57% in LAD, 8.30 \pm 0.38% in LCX and 8.32 ± 0.71% in the RCA territories). The results were essentially the same for standard OSEM reconstruction; mean global K1 percentage differences between cardiac-only and cardiacand-liver data in spline-fitted images were 5.71 \pm 0.24% for global rest K1, 7.18 \pm 0.86% for global stress K1 and 1.57 ± 0.70% for the stress/rest K1 ratio (myocardial perfusion reserve). Similar results were obtained for regional rest K1 (5.62 \pm 0.25% in LAD, 6.03 \pm 0.27% in LCX, and 6.41 \pm 0.25% in RCA territories), and stress K1 (7.11 \pm 1.04% in LAD, 7.40 \pm 0.28% in LCX, and 8.24 \pm 1.50 in RCA territories).

We used the same sample of four patients to assess the impact of attenuation correction application on the global and regional retention values. The correction for attenuation led to relatively small changes in K1 and MPR index values independently of the reconstruction algorithm used (**Table S4**). Mean percentage difference between spline-fitted non-attenuation-corrected and attenuatedcorrected images were $3.62 \pm 0.10\%$ for global rest K1, 4.72 \pm 0.29% for global stress K1, and 1.15 ± 0.33% for global MPR index (stress/rest K1 ratio). Similar results were obtained for standard OSEM reconstruction, with 3.53 \pm 0.15% difference for global rest K1, 4.43 \pm 0.54% for global stress K1 and $0.93 \pm 0.42\%$ for global MPR index.

Larger clinical studies are needed to assess the need for scatter, attenuation, and motion correction in dynamic SPECT.

SUPPLEMENTAL FIGURES

Standard OSEM reconstruction

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Standard OSEM reconstruction

Standard OSEM reconstruction with spline fitting

SUPPLEMENTAL FIGURE LEGENDS

FIGURE S1: Schematic summary of study cohorts

FIGURE S2: Correlation of global rest and stress coronary vascular resistance (CVR) estimated with ^{99m}Tc-sestamibi SPECT and ¹³N-ammonia PET using standard ordered subset expectation maximization (OSEM) reconstruction without (panel A) and with spline fitting (panel B).

FIGURE S3: Sensitivity analyses of global rest and stress myocardial blood flow (MBF) and flow reserve (MFR) estimated with $13N$ -ammonia PET and $99m$ Tc -sestamibi SPECT using standard ordered subset expectation maximization (OSEM) reconstruction without spline fitting in 18 participants who had both reconstructions available. Correlation plots of 99m Tc -sestamibi and 13 Nammonia MBF (panel A) and MFR measurements (panel C). Bland–Altman plots of MBF (panel B) and MFR measurements (panel D).

FIGURE S4: Sensitivity analyses of global rest and stress myocardial blood flow (MBF) and flow reserve (MFR) estimated with $13N$ -ammonia PET and $99m$ Tc -sestamibi SPECT using standard ordered subset expectation maximization (OSEM) reconstruction with spline fitting in 18 participants who had both reconstructions available. Correlation plots of 99m Tc -sestamibi and 13 Nammonia MBF (panel A) and MFR measurements (panel C). Bland–Altman plots of MBF (panel B) and MFR measurements (panel D).

FIGURE S5: Regional rest and stress myocardial blood flow (MBF) measurements in the validation cohort using conventional ordered subset expectation maximization (OSEM) reconstruction without splines (N=30 participants/N=90 territories) (panels A and B) and OSEM with spline fitting (N=21 participants/N=63 territories) (panels C and D) reconstructions.

FIGURE S6: Reproducibility analyses of global rest and stress myocardial blood flow (MBF) and flow reserve (MFR) estimated with ^{99m}Tc-sestamibi SPECT within two weeks using standard ordered subset expectation maximization (OSEM) reconstruction without spline fitting. Correlation plots of rest and stress MBF (panel A) and MFR measurements (panel C). Bland–Altman plots of rest and stress MBF (panel B) and MFR measurements (panel D).

FIGURE S7: Regional rest and stress myocardial blood flow (MBF) measurements in the reproducibility cohort using conventional ordered subset expectation maximization (OSEM) without splines (N=12 participants/36 territories) (panels A and B) and OSEM with spline fitting (N=14 participants/42 territories) (panels C and D).

SUPPLEMENTAL TABLES

Table S1: Baseline characteristics and injected radiotracer doses in the validation groups according to available reconstructions (OSEM with and without spline fitting)

Values are presented as median and interquartile ranges (IQR) or n (%).

ACE=angiotensin-conversing enzyme; ARB=angiotensin-II receptor blocker; BMI = body mass index; CAD= coronary artery disease; CABG=coronary artery bypass grafting; PCI = percutaneous coronary intervention.

Table S2: Systemic hemodynamics and injected radiotracer doses in the study population

*P-values refer to the comparison between rest hemodynamics obtained during SPECT and PET scans (validation cohort) and between the two consecutive SPECT scans (reproducibility cohort).

† P-values refer to the comparison between peak stress hemodynamics obtained during SPECT and PET scans (validation cohort) and between the two consecutive SPECT scans (reproducibility cohort). Doses are expressed in milicurie (mCi)

BP: blood pressure; PET: positron emission tomography; SPECT: single photon emission computed tomography

Table S3: Mean percentage differences between global and regional cardiac-only and cardiacand-liver retention and myocardial perfusion reserve index (MPR index) for the assessment of scatter effect from liver

Table S4: Mean percentage differences between attenuation-corrected and non-corrected retention and myocardial perfusion reserve index (MPR index)

Table S5: Comparison between regional myocardial blood flow (MBF) and myocardial flow reserve (MFR) estimates obtained with¹³N-ammonia PET and ^{99m}Tc-sestamibi SPECT with and without spline fitting

Myocardial blood flow (MBF) is reported in mL/min/g. Myocardial flow reserve (MFR) is calculated as the ratio between stress MBF and that at rest.

*P-values refer to the comparison between ^{99m}Tc-sestamibi SPECT and ¹³N-ammonia groups and are based on the Wilcoxon signed-rank test.

PET: positron emission tomography; SPECT: single photon emission computed tomography; OSEM: ordered subset expectation maximization