Social Cognitive Networks and Social Cognitive Performance Across Individuals With Schizophrenia Spectrum Disorders and Healthy Controls

Supplementary Information

Supplemental Methods and Materials

Participants

Participants were recruited for SPINS from the Centre for Addiction and Mental Health (CAMH; Toronto, Canada), Zucker Hillside Hospital (ZHH; New York, USA), and the Maryland Psychiatric Research Center (MPRC; Maryland, USA). Data for this study included participants recruited from December 2014 to March 2018 (time of CAMH scanner upgrade). Of 180 participants with SSDs and 126 healthy individuals who completed all study visits and met eligibility requirements throughout, 164 participants with SSDs and 117 healthy individuals (cases:controls by site: CAMH 66:42; ZHH 42:34; MPRC 56:41) were included in data analyses after quality control. Participants with SSDs met DSM-5 diagnostic criteria for schizophrenia, schizoaffective disorder, schizophreniform disorder, delusional disorder, or psychotic disorder not otherwise specified, assessed using the Structured Clinical Interview for DSM (SCID-IV-TR), and had no change in antipsychotic medication or decrement in functioning/support level in the 30 days prior to enrollment. Controls did not have a current or past Axis I psychiatric disorder, excepting adjustment disorder, phobic disorder, and past major depressive disorder (over two years prior; presently unmedicated), or a first degree relative with a history of psychotic mental disorder. Additional exclusion criteria included a history of head trauma resulting in unconsciousness, a substance use disorder (confirmed by urine toxicology screening), intellectual disability, debilitating or unstable medical illness, or other neurological diseases. Participants also had normal or corrected-to-normal vision.

Clinical and Cognitive Assessment

Data collection occurred across three visits within a one-month period (Visit 1: Consent, screening, clinical scales; Visit 2: Magnetic resonance imaging (MRI); Visit 3: Non-social cognitive and social cognitive testing).

Administered social cognitive tasks ranged from basic emotion recognition to complex mental state inference, and were selected based on findings from the Social Cognition Psychometric Evaluation (SCOPE) study (1) and the Social Cognition and Functioning in Schizophrenia project (2). These included the Penn Emotion Recognition Test (ER40; 3), which assesses basic emotion recognition from static images, the Reading the Mind in the Eyes test (RMET; 4), involving mental state inference from the eye region of faces, and the Empathic Accuracy (EA) task (2, 5). Participants also completed The Awareness of Social Inference Test - Revised (TASIT; 6), which involves viewing social video clips and includes three subtests (TASIT 1: Identifying emotions; TASIT 2 and 3: Social inference, including detection of lies and sarcasm).

All participants also completed the Wechsler Test of Adult Reading (7) as a measure of premorbid IQ. Non-social cognition was evaluated using the MATRICS (Measurement and Treatment Research to Improve Cognition in Schizophrenia) Consensus Cognitive Battery (MCCB; 8), which includes tests of processing speed, reasoning and problem solving, attention/vigilance, working memory, and verbal and visual learning. Psychiatric symptoms were assessed in the SSD sample only using the Brief Psychiatric Rating Scale (BPRS; 9) and the Scale for the Assessment of Negative Symptoms (SANS; 10). Functioning was evaluated using the Birchwood Social Functioning Scale (BSFS; 11) across groups, and the Quality of Life Scale (QLS; 12) in the SSD group only.

MRI Data Acquisition

MRI scans were collected using harmonized scanning parameters on 3T scanners with multichannel head coils, including a General Electric Discovery (N=108; CAMH), a General Electric Signa (N=33; ZHH) and Siemens Prisma (N=43; ZHH), and a Siemens Tim Trio (N=55; MPRC) and Siemens Prisma (N=42; MPRC).

Empathic Accuracy (EA) Task

The EA task was completed during functional MRI. Prior to scanning, participants were trained using a practice version of the task in a mock scanner. During the task, participants watch 9 videos in a set order of individuals (5 females, 4 males) discussing emotional (4 positive, 5 negative) autobiographical events, such as taking a trip to Spain, seeing their favorite comedian, getting a part in a movie, not being paid on time, an uncle passing away, and having their truck broken into. This version of the EA task was designed to include adults varying in age, race, and ethnicity. The details of the video development are presented elsewhere (2, 13). Throughout the videos, participants provide continuous ratings of how positive or negative the individual in the video is feeling, on a 9-point scale (1 = extremely negative to 9 = extremely positive) using a button box. Thus, they provide a valence rating rather than having to explicitly infer higher-level, more complex mental states. EA was calculated for each participant by correlating their ratings with self-ratings provided by the individuals in the videos. These values were then Fisher r-to-z transformed. The task is presented in three runs $(\sim 10 \text{ mins/run})$ with three EA videos (120-150 s each) and two interleaved control videos (40 s each) per run. During the control condition, participants provide continuous ratings of the relative light or darkness of a greyscale circle as it changes shades, on a 9-point scale. This condition is included to ensure that participants are engaged in the task (controlling for avolition) and comprehend it.

fMRI Preprocessing

All scans were preprocessed using an in-house pipeline system, epitome [\[https://github.com/josephdviviano/epitome\]](https://github.com/josephdviviano/epitome), which uses FSL and AFNI. All scans had the first 4 TRs removed and were slice-time corrected. Time series outliers were removed using despiking and each run was scaled to have a global mean of 1000. Linear registrations were calculated between the EPI image and each subject's T1 image using FLIRT, and the T1 and MNI space, followed by a non-linear warp to MNI space using FNIRT.

For each participant, TRs with framewise displacement > .5 mm were censored (14), along with the preceding and trailing TR, and replaced with a linear interpolate to perform confound regression. A nuisance regression model was then applied to the data, including regressors for the

6 head motion correction parameters, a 2nd order detrend, mean white matter (WM) signal, mean cerebral spinal fluid (CSF) signal, the square, derivative, and square of the derivative for each of these regressors, and the top three principal components of the WM and CSF signals (aCompCor). This approach combines thorough regression of head motion parameters (15) and tissue-specific regressors (16). The data was then smoothed to a full width half maximum of 8 mm (17, 18) using 3dBlurToFWHM, and warped into MNI space using the previously calculated transform.

Following mean residual time series generation for selected regions of interest, censored TRs were then dropped, and participants were excluded if more than 30% of their time points were dropped across all three runs.

Data-Driven Social Cognitive Subnetwork Detection

Community detection is a data-driven method of defining densely connected subgroups of nodes, or modules, which have high intramodular connectivity and lower intermodular connectivity (19). Social cognitive subnetworks (or communities) were identified for each participant using the Louvain community detection algorithm for signed networks (positive and negative weights) from the Brain Connectivity Toolbox (20), which divides nodes into modules while maximizing withinmodule connections and minimizing between-module connections. This was done at network densities ranging from the top 20-70% of connections (5% intervals). To generate consensus partitions for each participant at each density, this algorithm was run 100 times per participant at each density, after which consensus clustering was performed using the Louvain algorithm (1000 iterations; 21) across the 100 partitions per participant at agreement thresholds of 30, 40, 50, and 60% (19), at each density. A group-level partition was then generated by performing the same consensus clustering procedure across the individual partitions at each density. Consensus clustering produces an agreement matrix based on the individual partitions (indicating the proportion of partitions where a pair of nodes were assigned to the same module). The agreement matrix is then thresholded by a given level of agreement and consensus partitions are created by running the algorithm iteratively on the agreement matrix, and repeating this until a single representation is achieved. The consistency of these consensus partitions was then examined across the 11 densities at each of the four agreement thresholds, and an overall parcellation was generated based on the most frequently assigned module across all consensus partitions.

Division of Sample Based on Social Cognitive Performance

The lower- and higher-level social cognition factor scores were estimated for each participant using multiple regression in the R package lavaan (22), based on our previous two-factor model of social cognition which demonstrated very good fit across individuals with SSDs and healthy controls (CFI = 1.00 , RMSEA = 0.00 ; 23). We also tested this two-factor model in the current sample using confirmatory factor analysis, confirming good fit for the data across participants (CFI = .990, RMSEA = .042). Model fit was assessed using ranges of acceptable fit values outlined by Hu and Bentler (24), including comparative fit index (CFI) \geq .95 and root mean square error of approximation (RMSEA) \leq .06 to suggest that the hypothesized model fits the observed data relatively well.

Statistical Analysis

Figure S1: Representative example of total connectivity strength across network densities demonstrating consistent patterns by lower-level social cognitive performance group and connection-type

Supplemental Results

Table S1: Participant demographic and clinical characteristics by lower-level social cognitive performance group

SD = standard deviation, WTAR = Wechsler Test of Adult Reading, BSFS = Birchwood Social Functioning Scale

Table S2: Participant demographic and clinical characteristics by higher-level social cognitive performance group

SD = standard deviation, WTAR = Wechsler Test of Adult Reading, BSFS = Birchwood Social Functioning Scale

Network Connectivity

Within-Network Connectivity (Table 2)

The ANCOVAs comparing within-network connectivity values between groups all demonstrated a main effect of network (Table 2). Pairwise comparisons revealed that overall within-network connectivity was significantly greater in the mentalizing $(t(546) = 8.11, p < .0001)$ and motor resonance $(t(546) = 6.84, p < .0001)$ networks than the affect sharing network, but there was no difference between the mentalizing and motor resonance networks $(t(546) = 1.27, p > .1)$. There was also a main effect of connection-type, driven by greater within-network positive connectivity than negative connectivity $(t(273) = 80.25, p < .0001)$. Further, there was a significant network x connection-type interaction. This was characterized by greater positive within-network connectivity in the mentalizing $(t(1055) = 12.8, p < .0001)$ and motor resonance $(t(1055) = 10.9,$ $p < .0001$) networks than the affect sharing network, and marginally greater positive withinnetwork connectivity in the mentalizing than the motor resonance network ($t(1055) = 1.95$, $p =$.052). In contrast, greater negative within-network connectivity was seen in the affect sharing network than both the mentalizing $(t(1055) = 2.52, p = .036)$ and motor resonance $(t(1055) = 2.19,$ $p = .043$) networks, but there was no difference between the mentalizing and motor resonance networks (*t*(1055) = -.325, *p* > .1).

Between-Network Connectivity (Table 2)

Across group comparisons of between-network connectivity, there was a significant main effect of network (Table 2). This was driven by greater mentalizing-motor resonance connectivity, than both motor resonance-affect sharing $(t(546) = 2.90, p = .004)$ and mentalizing-affect sharing connectivity $(t(546) = 16.7, p < .0001)$ and greater motor resonance-affect sharing connectivity than mentalizing-affect sharing $(t(546) = 13.8, p < .0001)$. A main effect of connection-type was also observed, characterized by greater positive versus negative between-network connectivity $(t(273) = 7.77, p < .0001)$. Additionally, there was a significant network x connection-type interaction. Motor resonance-affect sharing positive connectivity was greater than both mentalizing-motor resonance $(t(843) = 4.19, p < .0001)$ and mentalizing-affect sharing $(t(843) =$ $34.7, p \leq 0.0001$) positive connectivity, and mentalizing-motor resonance positive connectivity was greater than mentalizing-affect sharing $(t(843) = 30.5, p < .0001)$. The opposite pattern was seen for negative between-network connectivity, with lower motor resonance-affect sharing than mentalizing-motor resonance $(t(843) = -6.96, p < .0001)$ and mentalizing-affect sharing $(t(843) =$ -21.45 , $p \leq .0001$) negative connectivity, and lower mentalizing-motor resonance than mentalizing-affect sharing negative connectivity $(t(843) = -14.49, p < .0001)$.

Figure S2: Within- and between-network connectivity strength by connection-type and lower-level social cognitive performance, higher-level social cognitive performance, and diagnostic groups

Prisma Subsample Connectivity

Regression analyses including positive and negative within- and between-network connectivity strengths in the Prisma subsample revealed that increased motor resonance-affect sharing negative connectivity was significantly associated with greater lower-level social cognition factor scores $(\beta=0.44, p=.045, R^2=0.250)$, as in the full sample, though this was not a significant predictor of higher-level social cognition factor scores in the subsample (β =0.30, p =.26, R ²=0.219).

The same ANCOVA analyses in the Prisma subsample also revealed very similar effects to those found in the full sample (Table S3). Significant main effects and interactions coincided with findings in the full sample for between-network connectivity, including a significant connectiontype x lower-level social cognitive performance group interaction and a network x connectiontype x higher-level social cognitive performance group interaction. For within-network connectivity, though lower- and higher-level social cognitive performance group effects and interactions were not statistically significant, the network x connection-type x higher-level social cognitive performance group interaction effect size was larger than that in the full sample. There also remained to be no significant main effects of, or interactions with, diagnostic group for withinor between-network connectivity.

Table S3: Prisma subsample within- and between-network connectivity results by lower-level social cognitive performance, higher-level social cognitive performance, and diagnostic groups

Nodal Connectivity (Table S4)

Regions exhibiting greater positive within-network connectivity in poor versus good lower-level social cognitive performers (Figure 2) included the left dorsal anterior cingulate cortex (ACC) and posterior temporoparietal junction (TPJ; mentalizing network). Greater positive between-network connectivity was demonstrated in poor performers in bilateral inferior parietal lobule (IPL) nodes (affect sharing network), whereas greater negative between-network connectivity was seen in good performers in the right IPL/intraparietal sulcus (affect sharing network) and bilateral supplementary motor area (SMA) and inferior frontal gyrus (IFG; motor resonance network).

Fewer nodes showed higher-level social cognitive performance group-based differences (Figure 3), though greater positive within-network connectivity in poor versus good performers was also seen in left posterior TPJ (mentalizing network), and between-network negative connectivity was greater in right IPL/intraparietal sulcus (affect sharing network) in better performers.

No nodes demonstrated significant diagnostic group differences in positive or negative withinnetwork connectivity strength. However, cases showed greater between-network positive connectivity in bilateral IPL nodes (affect sharing network) than controls, whereas the right IPL (affect sharing network) exhibited greater between-network negative connectivity in controls (see Table S4 for details).

Table S4: Nodal connectivity results by lower-level social cognitive performance, higher-level social cognitive performance, and diagnostic groups

Negative Between-Network Connectivity Strength

Diagnostic Group Comparisons

Positive Within-Network Connectivity Strength

No regions with significant differences

Negative Within-Network Connectivity Strength

No regions with significant differences

 $R =$ right, $L =$ left, Good = good social cognitive performance group, Poor = poor social cognitive performance group, BA = Brodmann area, dACC = dorsal anterior cingulate cortex, pTPJ = posterior temporoparietal junction, SMG = supramarginal gyrus, IPL = inferior parietal lobule, IPS = intraparietal sulcus, SMA = supplementary motor area, IFG = inferior frontal gyrus, mPFC = medial prefrontal cortex

Supplemental References

1. Pinkham AE, Penn DL, Green MF, Buck B, Healey K, Harvey PD. The social cognition psychometric evaluation study: Results of the expert survey and RAND panel. Schizophr Bull. 2014;40:813-823.

2. Kern RS, Penn DL, Lee J, Horan WP, Reise SP, Ochsner KN, Marder SR, Green MF. Adapting social neuroscience measures for schizophrenia clinical trials, Part 2: Trolling the depths of psychometric properties. Schizophr Bull. 2013;39:1201-1210.

3. Kohler CG, Bilker W, Hagendoorn M, Gur RE, Gur RC. Emotion recognition deficit in schizophrenia: Association with symptomatology and cognition. Biological psychiatry. 2000;48:127-136.

4. Baron-Cohen S, Wheelwright S, Hill J, Raste Y, Plumb I. The "Reading the Mind in the Eyes" Test revised version: A study with normal adults, and adults with Asperger syndrome or highfunctioning autism. J Child Psychol Psychiatry. 2001;42:241-251.

5. Olbert CM, Penn DL, Kern RS, Lee J, Horan WP, Reise SP, Ochsner KN, Marder SR, Green MF. Adapting social neuroscience measures for schizophrenia clinical trials, Part 3: fathoming external validity. Schizophr Bull. 2013;39:1211-1218.

6. McDonald S, Flanagan S, Rollins J: The Awareness of Social Inference Test - Revised (TASIT-R). Sydney, Pearson Assessment; 2011.

7. Wechsler D: Wechsler Test of Adult Reading (WTAR). San Antonio, TX, The Psychological Corporation; 2001.

8. Nuechterlein KH, Green MF, Kern RS, Baade LE, Barch DM, Cohen JD, Essock S, Fenton WS, Frese FJ, 3rd, Gold JM, Goldberg T, Heaton RK, Keefe RS, Kraemer H, Mesholam-Gately R, Seidman LJ, Stover E, Weinberger DR, Young AS, Zalcman S, Marder SR. The MATRICS Consensus Cognitive Battery, part 1: Test selection, reliability, and validity. American Journal of Psychiatry. 2008;165:203-213.

9. Overall JE, Gorham DR. The Brief Psychiatric Rating Scale. Psychological reports. 1962:799– 812.

10. Andreasen NC. Negative symptoms in schizophrenia: Definition and reliability. Archives of general psychiatry. 1982;39:784-788.

11. Birchwood M, Smith J, Cochrane R, Wetton S, Copestake S. The Social Functioning Scale. The development and validation of a new scale of social adjustment for use in family intervention programmes with schizophrenic patients. Br J Psychiatry. 1990;157:853-859.

12. Heinrichs DW, Hanlon TE, Carpenter WT, Jr. The Quality of Life Scale: An instrument for rating the schizophrenic deficit syndrome. Schizophr Bull. 1984;10:388-398.

13. Olbert CM, Penn DL, Kern RS, Lee J, Horan WP, Reise SP, Ochsner KN, Marder SR, Green MF. Adapting social neuroscience measures for schizophrenia clinical trials, part 3: Fathoming external validity. Schizophr Bull. 2013;39:1211-1218.

14. Cole MW, Bassett DS, Power JD, Braver TS, Petersen SE. Intrinsic and task-evoked network architectures of the human brain. Neuron. 2014;83:238-251.

15. Satterthwaite TD, Elliott MA, Gerraty RT, Ruparel K, Loughead J, Calkins ME, Eickhoff SB, Hakonarson H, Gur RC, Gur RE, Wolf DH. An improved framework for confound regression and filtering for control of motion artifact in the preprocessing of resting-state functional connectivity data. NeuroImage. 2013;64:240-256.

16. Muschelli J, Nebel MB, Caffo BS, Barber AD, Pekar JJ, Mostofsky SH. Reduction of motionrelated artifacts in resting state fMRI using aCompCor. NeuroImage. 2014;96:22-35.

17. Mikl M, Marecek R, Hlustik P, Pavlicova M, Drastich A, Chlebus P, Brazdil M, Krupa P. Effects of spatial smoothing on fMRI group inferences. Magnetic resonance imaging. 2008;26:490-503.

18. Pajula J, Tohka J. Effects of spatial smoothing on inter-subject correlation based analysis of FMRI. Magnetic resonance imaging. 2014;32:1114-1124.

19. Fornito A, Zalesky A, Bullmore ET: Fundamentals of Brain Network Analysis. Amsterdam ; Boston, Elsevier/Academic Press; 2016.

20. Rubinov M, Sporns O. Complex network measures of brain connectivity: Uses and interpretations. NeuroImage. 2010;52:1059-1069.

21. Lancichinetti A, Fortunato S. Consensus clustering in complex networks. Sci Rep. 2012;2:336.

22. Rosseel Y. lavaan: An R Package for Structural Equation Modeling. Journal of Statistical Software. 2012;48:1-36.

23. Oliver LD, Haltigan JD, Gold JM, Foussias G, DeRosse P, Buchanan RW, Malhotra AK, Voineskos AN, Group S. Lower- and higher-level social cognitive factors across individuals with schizophrenia spectrum disorders and healthy controls: Relationship with neurocognition and functional outcome. Schizophr Bull. 2018.

24. Hu L, Bentler PM. Cutoff criteria for fit indexes in covariance structure analysis: Conventional criteria versus new alternatives. Structural Equation Modeling. 1999;6:1-55.