SUPPLEMENTARY INFORMATION

Supplementary Table 1

Abbreviation	Definition
CGM	Continuous glucose monitoring
FND	Fluorescent nano-diamond
FRET	Fluorescence resonance energy transfer
FDA	The Food and Drug Administration
ISF	Interstitial fluid
PBS	Phosphate-buffered saline
рН	Potential of hydrogen
FITC	Fluorescein isothiocyanate
Con A	Concanavalin A
3 D	Three-dimensional
IPGTT	Intraperitoneal glucose tolerance test
IL	Interleukin
HCI	Hydrogen chloride
MRI	Magnetic resonance imaging
СТ	Computed Tomography
UV/VIS	Ultraviolet/Visible
FTIR	Fourier transform infrared
ARC	Animal resource center
IACUC	The Institutional Animal Care and Use Committee
IM	Intramuscular
H&E	Hematoxylin and Eosin
HPE	High-power field
SD	Standard deviation

List of Abbreviation

Figure S1: Schematic illustration of the skin-mountable device for fluorescent detection of glucose.

Figure S2: Fabrication of fluorescent nano-diamond hydrogel for glucose sensing.

(A) Surface functionalization of the nano-diamond with octadecylamine and triethoxyvinylsilane. (B-E) Fluorescent nano-diamond was characterized by transmission electron microscopy image (B), dynamic light scattering (C), emission spectra at 355, 370, 380, 400, and 410 nm excitation (D), and excitation spectra at 400 and 450 nm emission (E).

Figure S3: The preparation of fluorescent nano-diamond based hydrogel. (A) The chemical equation of silanization of the bore of the microneedle. (B) The glucose responsive hydrogel was synthesized as a polyacrylamide gel with fluorescent nano-diamond and phenylboronic acid functionalization. (C) Photograph of the fluorescent nano-diamond based boronic hydrogel prepared on the glass bottom of a tissue culture dish.

Figure S4: Characterization of the fluorescent nano-diamond based boronic hydrogel. (A) Experimental setup to detect fluorescence emission from the nanodiamond based boronic hydrogels in glucose solution. (B) Nano-diamond based hydrogel exhibited excellent photostability with 15 x 4 minutes, 5 W/cm², 460 nm exposure. n = 4. Data are presented as mean \pm SD. All error bars represent SD. (C) Value of the relative fluorescent intensity over 4000 cyclic illumination cycles for the control and the nano-diamond based hydrogel. 1 illumination cycle represents 1 second of illumination using a LED with a wavelength of 400 nm and a power of 6 W/cm². (D) No significant cytotoxicity of the nano-diamond hydrogel was found on day 1 and day 3 with the WST-1 cellular viability assay. n = 4. Data are presented as mean \pm SD. All error bars near \pm SD. **Figure S5: Characterization of the microneedle for glucose sensing. (A)** Microscopic image of the microneedle bottom. **(B-C)** Fluorescence images of the microneedle bottom without (B) or with (C) nano-diamond based hydrogel under 400 nm excitation light. **(D)** Representative microscopic image of the cross-section of the microneedle showing the translucent hydrogel inside the microneedle's bore.

Figure S6: Fabrication of the detection device for glucose monitoring. (A) Schematic illustration of the 3D structure of the microneedle device. (B) 3D structure of the multifunctional chip. An optical sensor and a light resource are configured on a single chip. (C) Side view of the device compared to the Airpod case.

Figure S7: Microneedle device with the nano-diamond hydrogel can detect glucose *in vitro* and *in vivo*. (A) Changes of glucose concentration *in vitro* can be repeatedly measured by the device after 3 months of storage in ambient light. n = 3. Data are presented as mean ± SD. All error bars represent SD. (B-C) Similar as data in Fig. 4A and B, blood glucose level can be detected by a separate device with glucose-challenged (C) or insulin-challenged (D) mice. (D-E) Similar as data in Fig. 4C and D, after storage of, blood glucose level can be monitored with a different microneedle device after 3 months storage at ambient light, for glucose-challenged (D) or insulin-challenged (E) animals.

Figure S8: Fluorescence intensity detected by the nano-diamond based device can continuously trace glucose level even under strong magnetic field. The photos of the sensor (A), internal metal electronics (B), and magnetic attraction (C) of the Abbott FreeStyle Libre 2 continuous glucose monitoring system. The experimental setup without (D) and with (E) the magnet approached. (F) Notification popped up and the sensor did not function when the magnet approached. (G) Fluorescent nano-diamond based sensor detected glucose level even under strong magnetic field, but not the Abbott FreeStyle Libre 2.

Figure S9: Fluorescence intensity detected by the nano-diamond based device can continuously trace glucose level under in low oxygen environments. (A) In PBS buffers, fluorescent nano-diamond boronic hydrogel based device and Abbott FreeStyle Libre 2 were able to reflect the glucose level. n = 4. Data are presented as mean \pm SD. All error bars represent SD. (B) Placing the Libre 2 sensor from regular buffer into deoxygenated buffer with the same glucose concentration resulted in a decrease in the number of resulting glucose concentrations and the detection function quickly became unusable. (C) Nano-diamond based device was able to detect the glucose level in deoxygenated PBS buffers. n = 4. Data are presented as mean \pm SD. All error bars represent SD.

Figure S10: The fluorescence intensity detected by our device correlates with glucose concentrations in vitro over the physiological temperature values. (A) Sensor dysfunction after rapid change in ambient temperature. (B) Nano-diamond based device can monitor the glucose level change in water bath at 30 °C, 37 °C, and 42 °C. n = 4. Data are presented as mean \pm SD. All error bars represent SD.

Figure S11: Sections of the skin after microneedle insertion or full-thickness skin wounds (3 mm) were stained with Trichrome, F4/80 or CD3 antibodies. Red dashed lines denote lesion area.

Figure S12: Another representative result of glucose monitoring with porcine skin model.

























500 µm

