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Blood Pressure Variability and Closed-loop Baroreflex Assessment in Adolescent Chronic Fatigue Syndrome during Supine Rest and Orthostatic Stress

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Abstract

Hemodynamic abnormalities have been documented in the chronic fatigue syndrome (CFS), indicating functional disturbances of the autonomic nervous system responsible for cardiovascular regulation. The aim of this study was to explore blood pressure variability and closed-loop baroreflex function at rest and during mild orthostatic stress in adolescents with CFS.

We included a consecutive sample of 14 adolescents 12 to 18 years old with CFS diagnosed according to a thorough and standardized set of investigations, and 56 healthy control subjects of equal sex and age distribution. Heart rate and blood pressure were recorded continuously and non-invasively during supine rest and during lower body negative pressure (LBNP) of -20 mm Hg to simulate mild orthostatic stress. Indices of blood pressure variability and baroreflex function (α -gain) were computed from monovariate and bivariate spectra in the low-frequency (LF) band (0.04–0.15 Hz) and the high-frequency (HF) band (0.15–0.50 Hz), using an autoregressive algorithm.

Variability of systolic blood pressure in the HF range was lower among CFS patients as compared to controls both at rest and during LBNP. During LBNP compared to controls, α -gain HF decreased more, and α -gain LF and the ratio of α -gain LF/ α -gain HF increased more in CFS patients, all suggesting greater shift from parasympathetic to sympathetic baroreflex control.

CFS in adolescents is characterized by reduced systolic blood pressure variability, and a sympathetic predominance of baroreflex heart rate control during orthostatic stress. These findings may have implications for the pathophysiology of CFS in adolescents.

Keywords

Blood pressure variability; baroreflex sensitivity; chronic fatigue syndrome; autonomic nervous system; cardiovascular regulation

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Conflicts of interests

There are no conflicts of interests

Introduction

The chronic fatigue syndrome (CFS) is a disabling disease, mainly affecting adolescents and young adults (Natelson 2001); recently, the prevalence among 8–17 years olds was reported as high as 1.3 % (Farmer et al. 2004). Certain infections (such as mononucleosis) and dramatic life events are considered important precipitating factors (Natelson 2001). The condition usually last for years, but spontaneous improvement is common, particularly among adolescents.

The CFS pathophysiology is unknown, but recent evidence suggests that abnormalities of cardiovascular regulation may play an important role. Various forms of orthostatic intolerance have been demonstrated both in adult (Bou-Holaigah et al. 1995) and pediatric (Galland et al. 2008; Rowe et al. 1995; Rowe and Calkins 1998; Wyller et al. 2007a; Wyller et al. 2008b) patients, as well as abnormalities in cerebral (Tanaka et al. 2002), muscle (McCully et al. 2004) and skin (Spence et al. 2000; Wyller et al. 2007b) hemodynamics. Taken together, these observations indicate that CFS is characterized by functional disturbances of the autonomic nervous system affecting cardiovascular regulation.

One direction of investigation has applied variability analyses of heart rate and blood pressure during orthostatic challenge to explore in more detail the mechanisms of autonomic cardiovascular control in CFS. However, CFS studies based on such methodology have yielded conflicting results (Boneva et al. 2007; Duprez et al. 1998; Stewart 2000; Yataco et al. 1997; Yoshiuchi et al. 2004). Two reasons may account for this. Firstly, most studies use an ordinary head-up tilt-test for the orthostatic challenge. However, in an experimental setting, the test may not be ideal due to the varying effects of the muscle venous pump among different participants in some experimental protocols, and the high rate of false positives in adolescents (De Jong-De Vos van Steenwijk et al. 1995). Secondly, the mathematical algorithm used for variability analyses may not be optimal. For instance, when estimating baroreflex-sensitivity, most techniques fail to account for the feed-forward effect (i.e. the mechanical influence) of heart rate on blood pressure (Barbieri et al. 1996).

The technique of lower body negative pressure (LBNP) is generally considered to mimic orthostasis effectively. Compared to most upright tilt protocols, it provides a more accurate tool for studies of cardiovascular adjustments during orthostatic stress because the subjects do not move and the effect of the muscle venous pump is eliminated (Stevens and Lamb 1965). Previously, we have reported evidence of altered heart rate variability in CFS patients during LBNP, indicating a predominance of sympathetic heart rate control during mild orthostatic stress (Wyller et al. 2008a). However, the autonomic neurons controlling heart rate are continuously influenced by different sources, including baroreceptor afferents, respiration and central command (Saul 1990). Thus, the aim of the present study was to assess blood pressure variability and one of the factors that influence both RR and blood pressure variability, the arterial baroreflex, both at rest and during LBNP. We hypothesized that indices of blood pressure variability and baroreflex function would differ between CFS patients and controls, indicating a predominance of sympathetic cardiovascular control in the former.

Methods

Subjects

CFS patients 12–18 years old were consecutively recruited from the outpatient clinic at the Dept. of Pediatrics, Rikshospitalet University Hospital, Oslo, Norway, serving as a national referral center for children and adolescents with unexplained chronic fatigue. Based upon our previous experiences, we assumed that a total number of approximately 15 CFS patient

would be sufficient (Wyller et al. 2008a; Wyller et al. 2008b) Other disease states that might explain their present symptoms, such as autoimmune, endocrine, neurologic or psychiatric disorders, were ruled out by a thorough and standardized set of investigations. Different case definitions of CFS exist. This study used a slight modification of the definition from the Centers for Disease Control and Prevention (CDC). The main criterion of at least six months of chronic or relapsing fatigue, severely affecting daily activities (Fukuda et al. 1994) was required in this study. However, the CDC-definition also requires patients having at least 4 of 8 specific accompanying symptoms. Since the validity of this last demand has been questioned (Cho et al. 2006), particularly in the pediatric population (Franklin 1998), accompanying symptoms were not required in this study.

Healthy controls 12–18 years old volunteered from local schools. In line with our previous experimental studies (Wyller et al. 2008a; Wyller et al. 2008b), we sought a 1:4 relation between patients and controls in order to increase the statistical power. Through communication with the responsible teachers, a recruiting process was established that assured an equal distribution of age and sex among the two groups. Subjects having a chronic disease (such as allergy) or using any medications on a regular basis (including contraceptive pills) were excluded.

One week prior to the experiments, all participants were instructed not to drink beverages containing alcohol or caffeine, not to take any drugs, and not to use tobacco products. They were instructed to fast overnight the day prior to the experiments.

Written, informed consent was obtained from all participants and their parents. The study was approved by the Regional committee for ethics in medical research. The RR variability data from these same subjects were reported previously (Wyller et al. 2008a).

Lower body negative pressure (LBNP) with handgrip

Experiments started at 11 a.m. The participants had been offered a light, standardized meal (1–2 pieces of bread, 1 glass of juice) two hours before, but were otherwise not allowed to eat or drink. They lay supine with their lower body in a plastic chamber, in which air could be evacuated very rapidly, thus reaching a pre-defined negative pressure within milliseconds (Hisdal et al. 2003). In order to prevent air leak, rubber devices were used to make a tight seal around the subjects' waist. They were lightly dressed, the ambient temperature was kept between 23 and 26 °C, and approximately 30 minutes were used for acclimatization prior to experiments. They were familiarized with the test situations in two pilot experiments.

Five minutes were used for baseline registration of cardiovascular variables. Then, LBNP of –20 mm Hg was applied. After 6 minutes of LBNP, the subjects were asked to perform left-sided handgrip for one minute with 30 % of maximal voluntary contraction force. This procedure was repeated once after a one minute resting interval. One minute after termination of the second handgrip, LBNP was turned off. The cardiovascular adjustments during combined LBNP and handgrip have been reported elsewhere (Wyller et al. 2008b)

The procedure was performed twice with a 5 minute rest period between applications of LBNP. However, in two subjects (one patient, one control), only one complete run of LBNP and handgrip was performed, due to dizziness or other unpleasant experience. Two additional recordings were excluded from the analyses due to low technical quality.

Instantaneous heart rate (HR) was obtained from the R-R interval (RRI) of the ECG. Photoplethysmography on the right middle finger was used to obtain a non-invasive, continuous recording of arterial blood pressure (2300 Finapres, Ohmeda, Madison, WI, US). This method correlates satisfactorily with invasive pressure measurements (Parati et al.

1989), and has also been validated in adolescents and children (Seifer and Kenny 2001). In addition, non-invasive techniques were used for continuous recording of aortic blood flow (bidirectional ultrasound Doppler velocimeter located at the suprasternal notch), brachial artery blood flow (bidirectional ultrasound Doppler velocimeter located at the elbow) and acral skin blood flow (laser-Doppler probe located at the right index finger). These measurements are not reported in this paper. All recorded signals, including the pressure in the LBNP chamber, were on-line transferred to a recording computer running a program for real-time data acquisition (developed by Morten Eriksen, Dept. of Physiology, University of Oslo, Norway).

RRI and BP monovariate spectral analysis

Beat-to-beat series of RRI and maximum (Systolic: SBP) and minimum (Diastolic: DBP) interbeat arterial blood pressure (ABP) values were converted to 3 Hz time series. For each experimental run, segments of 120 s length were selected, respectively, prior to LBNP and during LBNP prior to the handgrip periods, and subjected to spectral analyses using an autoregressive algorithm (Barbieri et al. 2001). Spectral components were decomposed, and power densities were computed in the low-frequency band (0.04–0.15 Hz) and the high-frequency band (0.15–0.5 Hz). For subjects with two experimental recordings, the arithmetical mean for each variable was computed from corresponding experimental epochs.

Spectral closed-loop analysis

The 3 Hz time series were also analyzed by a bivariate AR Yule-Walker algorithm (Barbieri et al. 2001), where the bivariate autoregressive model of order p is described by the following vector equation:

$$Y[n] = \sum_{k=1}^p A[k]Y[n-k] + W[n]$$

When applied to the interactions between SBP (or DBP) and RRI, the matrices are defined as:

$$\mathbf{A}[k] = \begin{bmatrix} a_{11}[k] & a_{12}[k] \\ a_{21}[k] & a_{22}[k] \end{bmatrix} \quad \mathbf{Y}[n] = \begin{bmatrix} RRI[n] \\ ABP[n] \end{bmatrix} \quad \mathbf{W}[n] = \begin{bmatrix} w_{RRI}[n] \\ w_{ABP}[n] \end{bmatrix}$$

The p matrices of coefficients $A(k)$ were calculated by solving the extended Yule-Walker equations. The order p of the model was fixed at 16 throughout the analysis. This was done in order to guarantee a homogeneous high order across all segments. Of note, this order was generally higher than the minimum order required by the Akaike criterion.

The bivariate coefficients were used to simultaneously analyze the gains and phases for the following transfer functions:

$$G_{ABP \rightarrow RRI}(f) = \frac{A_{12}(f)}{1 - A_{11}(f)}$$

the heart rate baroreflex feedback (SBP \rightarrow RRI and DBP \rightarrow RRI, or alpha), and

$$G_{RR \rightarrow ABP}(f) = \frac{A_{21}(f)}{1 - A_{22}(f)}$$

the feed-forward from RRI to ABP (RRI \rightarrow SBP and RRI \rightarrow DBP, or beta), where

$$A_{ij}(f) = \sum_{k=1}^p a_{ij}[k] \cdot e^{-j2\pi fk}.$$

The feedback SBP \rightarrow RRI gain was taken as a measure of the sensitivity of closed loop baroreflex modulation of RRI, while the feedforward RRI \rightarrow DBP gain was taken as the measure of the sensitivity of the closed-loop mechanical coupling between RRI and DBP fluctuations. Phase relationships were also assessed to investigate the delays in the SBP-RRI and RRI-DBP interactions.

Gain and phase values were extracted in the low-frequency (LF) band (0.04–0.15 Hz) and the high-frequency (HF) band (0.15–0.5 Hz), anywhere the coherence between RRI and SBP signals reached its maximum inside each frequency band (Figure 1). As previously suggested, the α -gain for baroreflex feedback was characterized between SBP and RR, and the β -gain feedforward was characterized between RR and DBP because of the direct effects of changes in the RR interval on DBP (Barbieri et al. 2001). For subjects with two experimental recordings, the arithmetical mean for each variable was computed from corresponding experimental epochs.

Statistical analyses

Statistical analyses were carried out using SPSS statistical software. Based upon inspection of plots, most variables were appraised not to follow a normal distribution. Thus, results are expressed as median with non-parametric 95 % confidence intervals. The non-parametric Wilcoxon-Mann-Whitney's test (2-sided) was used to explore differences between the two groups. Since the research questions did not concern within group differences, statistical tests for repeated measurements were not applied. A p-value of ≤ 0.05 was considered statistically significant. In order to reduce the methodological problem of multiple comparisons, statistical tests were only performed for the cardiovascular variables considered to be most relevant to our hypothesis.

Results

A total of 14 CFS patients and 56 healthy controls were included in the study (Table 1). The two groups were comparable regarding sex, age, weight and height. All were of Caucasian ethnicity, except one control.

Mean duration of fatigue among the patients was 31 months. Their functional impairments were severe. They were physically inactive, did not participate in leisure activities and had a high level of school absenteeism. However, no one was permanently bedridden. HR and DBP were increased and RRI was decreased both at rest and during LBNP compared to controls (Table 2).

Results from the univariate spectral analyses of blood pressure signals are shown in Tables 3 and 4 and Figure 1. For SBP, HF_{abs} at baseline was significantly lower among CFS patients than controls. These differences persisted during LBNP. DBP variability indices did not differ among the two groups.

Results from bivariate spectral analyses are shown in Tables 5 and 6 and Figure 1. At rest, the α -phase HF for the SBP-RR spectrum was more negative among CFS patients than controls. Otherwise, no significant differences were identified among the two groups at rest. However, during LBNP, α -gain HF tended to decrease more and α -gain LF tended to increase more among CFS patients than controls, leading to a marked increase in the ratio of α -gain LF/ α -gain HF in the CFS-patients which was not present in the controls. Also during LBNP, α -phase LF was less negative in CFS patients than in controls. For feedforward β -gain, no significant differences were seen between CFS patients and controls for any of the parameters measured. For all computed bivariate spectra, median coherence values were acceptable in the range of 0.66 to 0.83.

Discussion

The most important finding of this study is that the ratio of LF to HF gain for baroreflex feedback increases markedly in CFS patients in response to orthostatic stress, compared to virtually no change in normal controls. The significant increase in the gain ratio was due to a combination of increased LF gain and decreased HF gain in the CFS group, while the controls only had a reduction in HF gain. These findings indicate that mild orthostatic stress leads to a small reduction of parasympathetically mediated heart rate control in both CFS patients and controls (decreased HF gain), but a significant increase in sympathetically mediated baroreflex gain in CFS patients (increased LF gain) which is not observed in controls.

In addition, reduced HF SBP variability was observed in CFS patients compared to controls, possibly reflecting a reduced effect of respiration on RR or SBP in CFS patients.

Blood Pressure Variability in CFS

The mechanical effect of ventilation is a significant source of blood pressure variability in the HF range (Malpas 2002; Zhang et al. 2002). Thus, our findings of reduced HF variability of SBP, which has not been previously reported, suggest either an altered ventilatory pattern or an altered effect of respiratory activity on SBP among CFS patients. There are several reports of reduced heart rate variability in the HF range, both at rest (Stewart 2000) and during orthostatic challenge in CFS patients (Stewart 2000; Wyller et al. 2008a; Wyller et al. 2007c). Since respiratory activity is also the primary source of heart rate variability in the HF range (Saul 1990), the reduced HF variability of SBP observed here could be due to a reduced effect of respiration on heart rate (respiratory sinus arrhythmia). However, since respiratory patterns were not controlled and a quantitative respiratory signal was not measured in these studies, the precise origin of reduced SBP variability in the HF range cannot be determined. Future research could focus on possible alterations in CFS ventilatory patterns and the relationships between ventilation and both heart rate and blood pressure in these patients.

No differences between CFS patients and controls were observed for blood pressure variability in the LF range, either at rest or during LBNP. An important source of such variability is sympathetically controlled vasomotion (Malpas 2002), which consequently appears to be unaltered in CFS. Although these findings are consistent with previously reported data from our laboratory (Wyller et al. 2007c), they contrast with Stewart's (2000) study of adolescent CFS patients, where increased blood pressure variability was noted in the LF range during 70° head-up tilt. This apparent inconsistency could be entirely explained by different experimental protocols: Firstly, LBNP and upright tilt, although similar in terms of physiological stress, do not result in identical hemodynamic responses. Secondly, LBNP of -20 mmHg used in this study, corresponding to head-up tilt of 20°-30°,

represents a much milder orthostatic challenge than 70° head-up tilt and might have been insufficient to provoke a difference between the two groups.

Dynamic Closed-loop Baroreflex Assessment in CFS

The baroreflex feedback mechanism includes both sympathetic and parasympathetic neural connections emanating from the brain stem cardiovascular control center to the sinus node (Lanfranchi and Somers 2002; Saul 1990). Because sympathetic heart rate control is relatively slow it only controls heart rate changes in the LF range, whereas the parasympathetic system has broad-band characteristics, operating in the LF as well as the HF range. Previous studies applying the same bivariate technique used here have demonstrated that during upright posture the α -gain decreases in both LF and HF range (Barbieri et al. 2002), presumably secondary to parasympathetic withdrawal. With the milder orthostatic stress in this study, we observed a similar decrease for both controls and CFS patients but only in the HF range. Among CFS patients, α -gain LF actually increased during LBNP. The net result was a marked and significant increase in the ratio α -gain LF/ α -gain HF, strongly suggesting that in addition to the reduced parasympathetic heart rate control, there was enhanced sympathetic heart rate control mediated by the baroreflex.

The observed increase in the sympathetic component of the baroreceptor feedback with even mild orthostatic stress in CFS patients indicates *early* sympathetic activation and may reflect diminished *baroreflex reserve* for more severe stressors. These changes further suggest that the baroreflex may have a diminished ability to buffer a variety of internal and external influences on arterial pressure, but particularly those related to upright activity and ambulation, in line with our previous report on the combined effect of orthostatic stress and isometric exercise in CFS patients (Wyller et al. 2008b).

The function of the baroreceptor reflex has been addressed in two previous CFS studies. In a group of adolescent CFS patients and controls, Stewart (2000) reported significantly lower α -gain in the HF as well as the LF range among CFS patients, both during rest and during 70° head-up tilt. In adult CFS patients, Peckerman and co-workers (2003) reported enhanced decline in baroreceptor sensitivity upon standing as compared to controls. However, the sequential method adopted in the latter study does not allow separate estimation of LF and HF gain, making it most sensitive for parasympathetic heart rate control. Differences from the current study might be explained by different inclusion criteria, experimental protocols and mathematical algorithms. Taken together, however, like this study they indicate a sympathetic predominance of baroreflex heart rate control during orthostatic stress in CFS patients.

Cardiovascular Dysregulation in CFS

In agreement with past reports, the findings from this study confirm that CFS patients have functional disturbances of the autonomic nervous system affecting cardiovascular regulation. The underlying mechanism for this disturbance has been disputed.

One possibility would be that CFS patients suffer from absolute or relative hypovolemia, which has indeed been reported previously (Farquhar et al. 2002; Streeten 2001; Streeten et al. 2000; Hurwitz et al 2009). However, detailed studies of baroreflex function with techniques similar to ours have revealed a reduced LF baroreflex gain at rest following blood donation (Triedman et al. 1993) and furosemide treatment (Iwasaki et al. 2000), and a further attenuation of LF baroreflex gain in hypovolemic individuals during orthostatic stress (Triedman et al. 1993). Also, an attenuation of LF baroreflex gain has been demonstrated during experimentally induced hypovolemia by LBNP (Barbieri et al. 2002). Contrasting these results, we found equal LF baroreflex gain among controls and CFS

patients at rest and increased LF baroreflex gain in CFS patients during orthostatic stress, making hypovolemia an unlikely explanation.

A second possibility would be cardiovascular deconditioning due to physical inactivity in CFS patients (De Lorenzo et al. 1998). The deconditioning influence on cardiovascular control appears to be partly a consequence of concomitant hypovolemia (Iwasaki et al. 2000), adding to the relevance of the reasoning above. Furthermore, in adults, both sedentary and gravitational deconditioning seems to be associated with attenuated sympathetic responsiveness during orthostatic stress (Levine et al. 1991; Sun et al. 2003), and endurance training in sedentary individuals tends to increase LF baroreflex gain at rest (Iwasaki et al. 2003). In a previous study of healthy adolescents, the degree of aerobic fitness did not predict cardiac autonomic responses during head-up tilt (Brunetto et al. 2005). Finally, no one of the CFS patients in this study was permanently bedridden, and previous evidence suggests that intermittent exposure to gravity during a bed-rest period is sufficient to prevent gravitational deconditioning (Sun et al. 2003; Zhang et al. 2000). Taken together, cardiovascular deconditioning does not seem to explain the results reported in this study.

A third possible explanation is a discrete disturbance of CNS autonomic control, such as temporary central resetting, redefining the homeostatic range of the baroreflex (Goldstein 2001). The smaller negative value for α -phase LF among CFS patients as compared to controls during LBNP suggests a shortened response time within the sympathetic part of the baroreflex, possibly caused by central enhancement of neural transmission. Also, as orthostatic challenge neither altered feedforward β -gain nor DBP variability in the LF range differently among CFS patients, the sympathetic predominance does not seem to be a reflection of blood pressure buffering, further pointing towards a central mechanism. Central resetting is not a common feature of orthostatic challenge, but does occur during aerobic exercise, resulting in attenuation of parasympathetic and predominance of sympathetic heart rate control (Macor et al. 1996; Spadacini et al. 2006), analogous to what we report in this study.

Data Quality and Study Limitations

The responses among healthy adolescents to LBNP were similar in all respect to responses among healthy adults in previously reported LBNP experiments from our institutions, supporting the validity of this study (Barbieri et al. 2002). Furthermore, coherence values were well above 0.5 for all computed bivariate spectra, supporting the validity of the calculated gain and phase values.

Blood and/or plasma volume were not measured, leaving the question of hypovolemia unresolved. Finally, respiratory activity has been shown to change during orthostatic challenge, and could therefore influence cardiovascular variability (Cooke et al. 1999); however, ventilation was not controlled for in this study.

Concluding remarks

Our findings of cardiovascular dysregulation point towards a discrete disturbance of CNS autonomic control in CFS patients. This may represent a distinct pathophysiologic phenomenon possibly conceptualized as a mismatch-phenomenon, in which sensory input during orthostatic challenge evokes a disproportional or 'untuned' autonomic response. This concept is compliant with recently proposed theories of CFS pathophysiology, such as the theory of central sensitization (Yunus 2007) and our recently proposed theory of sustained arousal (Wyller et al. 2009). On a more general level, such a concept is in line with recent models on the mechanistic link between psychosocial stressors and cardiovascular morbidity

(Goldstein 2001; Lucini et al. 2008). Further research should aim at exploring these relations in more detail, both in CFS and other related disorders.

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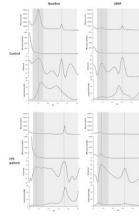


Figure 1.

Individual univariate and bivariate spectra from one healthy control (upper panels) and one CFS patient (lower panels) at baseline (left) and during LBNP (right). Dark shadowed areas indicate the low frequency range (0.04 – 0.15 Hz); light shadowed areas indicate the high frequency range (0.15 – 0.50 Hz). Vertical dotted lines mark the point of maximal coherence within each frequency band. Of note, in the healthy control, LBNP results in a reduction of α -gain in both frequency bands, whereas in the CFS patient, LBNP is associated with a decrease of HF α -gain and an increase in LF α -gain.

Table 1

Subject characteristics

	Control		CFS	
	n	%	n	%
Number	56		14	
Female gender	33	58.9	9	64.3
	Mean	(range)	Mean	(range)
Age (years)	15.6	(13–18)	15.2	(12–18)
Weight (kg)	61.6	(44–99)	59.5	(43–92)
Height (cm)	171.5	(149–195)	172.2	(160–192)
Body surface area (m ²)	1.7	(1.4–2.2)	1.7	(1.4–2.2)
Duration of fatigue (months)			31.3	(6–60)

Table 2

Standard hemodynamic variables at baseline and during LBNP -20 mmHg. Median (confidence interval)

	Baseline		LBNP	
	<i>Control</i> (n=56)	<i>CFS</i> (n=14)	<i>Control</i> (n=56)	<i>CFS</i> (n=14)
Heart rate (beats/min)	65.1 (62.0–67.6)	71.9 (66.1–81.5)	70.8 (67.6–75.7)	86.2 (80.6–93.0)
RR-interval (ms)	921 (887–968)	834 (736–908)	847 (793–887)	696 (645–744)
Systolic blood pressure (mmHg)	118.6 (113.5–123.9)	115.6 (110.5–130.3)	117.4 (112.9–122.1)	118.2 (110.7–133.1)
Diastolic blood pressure (mmHg)	63.8 (62.1–66.0)	69.4 (65.5–74.9)	66.3 (64.1–67.9)	73.8 (68.7–79.5)

Table 3
Systolic blood pressure variability at baseline and during LBNP -20 mmHg. Median (confidence interval)

	Baseline			LBNP			Δ (LBNP-Baseline)		
	Control (n=56)	CFS (n=14)	P- value*	Control (n=56)	CFS (n=14)	P- value*	Control (n=56)	CFS (n=14)	P- value*
Variance (mmHg ²)	37.2 (32.3-43.7)	41.7 (25.1-63.4)	0.509	35.0 (27.8-40.7)	38.0 (33.9-47.6)	0.883	-1.2 (-6.1-3.2)	1.5 (-12.3-10.3)	0.883
Total Power (mmHg ²)	48.4 (41.5-60.8)	51.1 (41.5-81.6)	0.472	40.2 (34.3-43.3)	43.0 (32.2-54.2)	0.481	-2.4 (-18.1-1.2)	-10.2 (-46.2-6.1)	0.481
HF absolute units (mmHg ²)	1.03 (0.89-1.25)	0.71 (0.33-1.22)	0.012	0.92 (0.77-1.19)	0.68 (0.43-0.93)	0.780	-0.14 (-0.27-0.02)	0.02 (-0.40-0.32)	0.780
LF absolute units (mmHg ²)	5.76 (4.44-6.95)	2.96 (1.87-8.58)	0.223	6.00 (5.11-8.74)	6.66 (3.98-11.52)	0.186	-0.04 (-1.73-1.83)	2.97 (-0.56-4.48)	0.186
HF normalized units (nu)	0.19 (0.15-0.25)	0.13 (0.07-0.49)	0.325	0.14 (0.10-0.21)	0.09 (0.08-0.14)	0.370	-0.03 (-0.07-0.03)	-0.03 (-0.09-0.02)	0.370
LF normalized units (nu)	0.81 (0.75-0.85)	0.87 (0.51-0.93)	0.325	0.86 (0.79-0.90)	0.91 (0.86-0.92)	0.370	0.03 (-0.03-0.07)	0.03 (-0.02-0.09)	0.370
LF/HF	6.24 (4.37-8.23)	8.23 (1.34-15.38)	0.528	7.64 (4.61-10.33)	12.21 (7.84-20.40)	0.386	-0.03 (-1.42-3.24)	2.52 (-1.53-8.68)	0.386

* Wilcoxon-Mann-Whitney's test. In order to reduce the methodological problem of multiple comparisons, statistical tests were only performed for the cardiovascular variable baseline and Δ (LBNP-Baseline)

Table 4
Diastolic blood pressure variability at baseline and during LBNP -20 mmHg. Median (confidence interval)

	Baseline			LBNP			Δ (LBNP-Baseline)		
	Control (n=56)	CFS (n=14)	P- value*	Control (n=56)	CFS (n=14)	P- value*	Control (n=56)	CFS (n=14)	P- value*
Variance (mmHg ²)	9.3 (8.4-12.4)	12.7 (7.9-17.4)	0.154	12.6 (10.2-13.7)	12.0 (10.0-14.6)	0.333	2.3 (0.4-4.7)	2.0 (-1.2-3.5)	0.333
Total Power (mmHg ²)	10.2 (8.9-11.5)	13.7 (9.4-18.3)	0.089	12.2 (10.5-14.7)	11.3 (10.7-17.4)	0.106	2.3 (0.4-4.5)	-0.4 (-3.1-2.4)	0.106
HF absolute units (mmHg ²)	0.35 (0.24-0.42)	0.31 (0.18-0.43)	0.883	0.30 (0.21-0.44)	0.26 (0.16-0.37)	0.340	0.03 (-0.06-0.06)	-0.06 (-0.14-0.09)	0.340
LF absolute units (mmHg ²)	1.86 (1.53-2.49)	2.52 (1.55-3.62)	0.403	3.41 (2.99-4.27)	3.44 (2.34-4.90)	0.557	1.50 (0.72-2.19)	0.74 (-0.37-2.61)	0.557
HF normalized units (nu)	0.17 (0.11-0.22)	0.14 (0.09-0.21)	0.638	0.07 (0.05-0.13)	0.08 (0.05-0.10)	0.454	-0.05 (-0.08-0.01)	-0.05 (-0.15-0.01)	0.454
LF normalized units (nu)	0.83 (0.78-0.89)	0.86 (0.79-0.91)	0.638	0.93 (0.87-0.95)	0.92 (0.90-0.95)	0.454	0.05 (0.01-0.08)	0.05 (0.01-0.15)	0.454
LF/HF	6.84 (4.20-9.97)	7.17 (4.62-16.82)	0.355	15.91 (8.02-19.79)	14.55 (9.77-20.10)	0.860	4.88 (2.21-7.55)	5.68 (1.47-11.48)	0.860

* Wilcoxon-Mann-Whitney's test. In order to reduce the methodological problem of multiple comparisons, statistical tests were only performed for the cardiovascular variable baseline and Δ (LBNP-Baseline)

Table 5

Bivariate spectral relation between RR and SBP at baseline and during LBNP -20 mmHg. Median (confidence interval)

	Baseline			LBNP			Δ (LBNP-Baseline)		
	Control (n=56)	CFS (n=14)	P- value*	Control (n=56)	CFS (n=14)	P- value*	Control (n=56)	CFS (n=14)	P- value*
Max. coherence, HF range	0.77 (0.75-0.83)	0.83 (0.74-0.85)		0.74 (0.68-0.79)	0.75 (0.56-0.86)		-0.04 (-0.09-0.02)	-0.03 (-0.18--0.02)	
Max. coherence, LF range	0.71 (0.69-0.76)	0.71 (0.55-0.76)		0.69 (0.65-0.73)	0.78 (0.71-0.84)		0.02 (-0.07-0.08)	0.11 (0.01-0.19)	
α -gain HF (ms/mmHg)	11.39 (8.25-13.18)	11.10 (7.99-17.09)	0.333	8.37 (6.66-10.27)	6.81 (5.41-9.04)	0.091	-2.39 (-4.05-0.06)	-3.67 (-10.41--1.31)	0.091
α -gain LF (ms/mmHg)	4.47 (3.18-5.34)	4.01 (3.38-5.27)	0.670	4.52 (4.15-5.21)	5.54 (3.85-7.19)	0.060	-0.38 (-0.86-0.15)	1.79 (-1.17-3.23)	0.060
α -gain LF/ α -gain HF	0.44 (0.38-0.65)	0.34 (0.16-0.62)	0.097	0.52 (0.38-0.66)	0.81 (0.51-1.12)	0.017	0.03 (-0.07-0.16)	0.47 (0.20-0.62)	0.017
α -phase HF (rad)	-0.15 (-0.51-0.22)	-0.72 (-0.83--0.35)	0.047	-0.83 (-1.01--0.57)	-1.21 (-1.33--0.84)	0.528	-0.46 (-0.80--0.07)	-0.51 (-0.61-0.38)	0.528
α -phase LF (rad)	-0.96 (-1.16--0.76)	-0.61 (-1.12--0.11)	0.150	-0.83 (-0.94--0.69)	-0.50 (-0.72--0.36)	0.872	0.12 (-0.15-0.19)	-0.03 (-0.56-0.76)	0.872

* Wilcoxon-Mann-Whitney's test. In order to reduce the methodological problem of multiple comparisons, statistical tests were only performed for the cardiovascular variable baseline and Δ (LBNP-Baseline)

Table 6

Bivariate spectral relation between RR and DBP at baseline and during LBNP -20 mmHg. Median (confidence interval)

	Baseline			LBNP			Δ (LBNP-Baseline)		
	Control (n=56)	CFS (n=14)	p- value*	Control (n=56)	CFS (n=14)	p- value*	Control (n=56)	CFS (n=14)	p- value*
Max. coherence, HF range	0.75 (0.65-0.83)	0.82 (0.73-0.89)		0.67 (0.59-0.71)	0.67 (0.58-0.80)		-0.08 (-0.10-0.004)	-0.16 (-0.25-0.07)	
Max. coherence, LF range	0.71 (0.66-0.77)	0.74 (0.60-0.78)		0.75 (0.73-0.78)q	0.79 (0.75-0.86)		0.02 (-0.02-0.09)	0.08 (0.02-0.11)	
β -gain HF (mmHg/ms)	0.017 (0.015-0.022)	0.020 (0.014-0.027)	0.577	0.021 (0.017-0.024)	0.028 (0.024-0.037)		0.002 (-0.0001-0.005)	0.005 (0.002-0.012)	0.058
β -gain LF (mmHg/ms)	0.040 (0.030-0.049)	0.045 (0.029-0.066)	0.386	0.050 (0.043-0.055)	0.058 (0.048-0.069)		0.014 (0.006-0.018)	0.016 (0.003-0.023)	0.587
β -phase HF (rad)	1.36 (1.20-1.57)	1.31 (0.97-2.00)	0.649	1.38 (1.00-1.50)	1.30 (1.05-1.63)		-0.08 (-0.35-0.20)	-0.13 (-1.00-0.17)	0.618
β -phase LF (rad)	1.79 (1.63-1.91)	1.67 (1.27-1.81)	0.172	1.68 (1.55-1.77)	1.45 (1.24-1.56)		-0.06 (-0.23-0.04)	-0.10 (-0.85-0.21)	0.826

* Wilcoxon-Mann-Whitney's test. In order to reduce the methodological problem of multiple comparisons, statistical tests were only performed for the cardiovascular variable baseline and Δ (LBNP-Baseline)