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# Pro-arrhythmogenic Effects of the V141M KCNQ1 Mutation in Short QT Syndrome and Its Potential Therapeutic Targets: Insights from Modeling

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# Abstract

Gain-of-function mutations in the pore-forming subunit of  $I_{Ks}$  channels, KCNQ1, lead to short QT syndrome (SQTS) and lethal arrhythmias. However, how mutant  $I_{Ks}$  channels cause SQTS and the possibility of  $I_{Ks}$ -specific pharmacological treatment remain unclear. V141M KCNQ1 is a SQTS associated mutation. We studied its effect on  $I_{Ks}$  gating properties and changes in the action potentials (AP) of human ventricular myocytes. *Xenopus* oocytes were used to study the gating mechanisms of expressed V141M KCNQ1/KCNE1 channels. Computational models were used to simulate human APs in endocardial, mid-myocardial, and epicardial ventricular myocytes with and without  $\beta$ -adrenergic stimulation. V141M KCNQ1 caused a gain-of-function in  $I_{Ks}$  characterized by increased current density, faster activation, and slower deactivation leading to  $I_{Ks}$  accumulation. V141M KCNQ1 also caused a leftward shift of the conductance-voltage curve compared to wild type (WT)  $I_{Ks}$  ( $V_{1/2} = 33.6 \pm 4.0$  mV for WT, and  $24.0 \pm 1.3$  mV for heterozygous V141M). A Markov model of heterozygous V141M mutant  $I_{Ks}$  was developed and

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incorporated into the O'Hara–Rudy model. Compared to the WT, AP simulations demonstrated marked rate-dependent shortening of AP duration (APD) for V141M, predicting a SQTS phenotype. Transmural electrical heterogeneity was enhanced in heterozygous V141M AP simulations, especially under  $\beta$ -adrenergic stimulation. Computational simulations identified specific I<sub>K1</sub> blockade as a beneficial pharmacologic target for reducing the transmural APD heterogeneity associated with V141M KCNQ1 mutation. V141M KCNQ1 mutation shortens ventricular APs and enhances transmural APD heterogeneity under  $\beta$ -adrenergic stimulation. Computational simulations identified Specific I<sub>K1</sub> blockade as a beneficial pharmacologic target for reducing the transmural APD heterogeneity associated with V141M KCNQ1 mutation. V141M KCNQ1 mutation shortens ventricular APs and enhances transmural APD heterogeneity under  $\beta$ -adrenergic stimulation. Computational simulations identified I<sub>K1</sub> blockers as a potential antiarrhythmic drug of choice for SQTS.

#### Keywords

Arrhythmia; Anti-arrhythmic; I<sub>Ks</sub>; KCNQ1; Short QT syndrome

# **1** Introduction

Short QT Syndrome (SQTS) is an inherited channelopathy associated with marked shortening of QT intervals on the ECG and sudden cardiac death in individuals with structurally normal hearts [1–4]. Hereditary SQTS is genetically heterogeneous with six currently identified forms, SQT1 to SQT6, based on the chronology of their discovery [5–11]. The mutation V141M KCNQ1 causes a gain-of-function of the slow delayed rectifier potassium current ( $I_{Ks}$ ) and is one of the mutations that give rise to SQT2 [12, 13].

Shortening of the QT interval is a normal physiological response to an increase in heart rate. In patients with SQTS, the QT interval is relatively normal at fast rates, but abnormally short at slow heart rates [14]. Transmural dispersion of repolarization (TDR) has been suggested to correlate to ventricular arrhythmias in an experimental SQTS model that was generated by application of an  $I_{K,ATP}$  opener, pinacidil, and in patients with SQTS [15, 16]. Reducing TDR has been suggested as an important antiarrhythmic property of quinidine in a SQTS model [17] and in patients exhibiting the SQT1 variant [14]. In other forms of SQTS, data regarding pharmacological therapy remain too limited to permit specific suggestions or recommendations.

This study evaluated the effect of V141M KCNQ1 mutation on TDR and the drug effects on TDR of different anti-arrhythmic agents. First, we determined the kinetic changes relative to the wild type of V141M mutant KCNQ1 + KCNE1 channel expressed in *Xenopus* oocytes. Then we used computer simulations in the O'Hara–Rudy (ORd) human ventricular cell model to study the electrophysiological consequences of V141M KCNQ1 in ventricular myocytes in terms of its effects on  $I_{Ks}$  kinetics, action potential (AP) with and without isoproterenol (ISO) challenge, AP rate adaptation, and transmural AP duration (APD) heterogeneity. We also examined the effects of various anti-arrhythmic drugs on V141M KCNQ1-augmented transmural APD heterogeneity and identified a potential target for suppressing TDR and consequently reducing arrhythmic risk in SQT2.

### 2 Methods

#### 2.1 Mutagenesis and Oocyte Preparation

Xenopus oocytes that expressed human wild type (WT) KCNQ1 or V141M KCNQ1 and WT KCNE1 were used to record WT IKCN01+KCNE1 (WT IKs) and V141M IKCN01+KCNE1 (V141M  $I_{Ks}$ ). KCNQ1 (provided by S. Goldstein, University of Chicago, Chicago, IL) and KCNE1 (provided by S. Nakanishi, Osaka Bioscience Institute, Osaka, Japan) were subcloned into the HindIII/XbaI cloning sites of pcDNA3.1+ vectors (Invitrogen, Grand Island, NY). The V141M KCNQ1 mutation was generated by using overlap extension amplification with high-fidelity polymerase chain reaction (PCR), verified by DNA sequencing (IDT technology, Coralville, IW). Messenger RNA was transcribed in vitro using the mMessage mMachine T7 polymerase kit (Applied Biosystems, Oyster Bay, NY). The follicle layer of oocytes was digested using type 1A collagenase (Sigma-Aldrich, Saint Louis, MO). Stage IV-V Xenopus oocytes were selected and injected with 4.6 ng mRNA per oocyte. For implementing a heterozygous genotype, we expressed heterozygous V141M IKs channels in oocytes that RNAs of WT KCNQ1 and V141M KCNQ1 at 1:1 ratio were injected. Total KCNQ1 and KCNE1 injection ratios for WT and V141M were the same at 6:1. Injected oocytes were incubated in ND96 solution (in mM: 96 NaCl, 2 KCl, 1.8 CaCl2, 1 MgCl2, and 5 Hepes, pH 7.60) at 18 °C for 3-5 days before recording.

### 2.2 Electrophysiology

Whole cell current recordings were obtained with the two-microelectrode voltage clamp technique. Microelectrodes were pulled from glass capillary tubes and filled with 3 M KCl. Oocytes were constantly superfused with ND96 at room temperature (~22 °C). The membrane potential was clamped using a GENECLAMP 500B amplifier (Axon Instruments, New York, NY). Data acquisition was controlled using PULSE/PULSEFIT software (HEKA, Farmingdale, NY).

#### 2.3 Data Analysis

The electrophysiology data was analysed with Igor 4.09 (WaveMetrics, Lake Oswego, OR), and plotted with Prism 6 software (GraphPad, La Jolla, CA). Statistical evaluation was performed using the SAS program (JMP software, Version 9, Cary, NC). Where not otherwise specified, numerical variants were mean  $\pm$  SD. Two-way ANOVA analysis was used, followed by Ryan-Einot-Gabriel-Welsch Multiple Range Test. A value of p < 0.05 was considered statistically significant.

#### 2.4 Computational Model Simulations

Simulations of the ventricular myocyte AP were based on a modified ORd model of the human ventricular cardiomyocyte, in which the signaling cascade from ISO application to PKA phosphorylation of target proteins was incorporated [18–20]. Parameters affected by PKA phosphorylation were computed by the Heijman et al. model of the  $\beta$ -adrenergic signaling pathway [21]. In the simulations, 1 µmol/L ISO was applied starting from steady state after pacing at a cycle length of 1000 ms for 1000 beats. The original ORd model used data from measurements in isolated undiseased human ventricular myocytes at 37 °C to

formulate  $I_{Ks}$  [20, 22]. In this model, the Ca<sup>2+</sup> dependence of  $I_{Ks}$  was also taken into consideration. The transition rates in the  $I_{Ks}$  Markov model used here were corrected based on recordings obtained at room temperature (provided in the Supplemental Information). Simulation of  $I_{Ks}$  activation was constrained with the G–V curves and the deactivation was constrained with experimental values of Tau (see Fig. 1). The scaling factors of  $I_{Ks}$  conductance without any drug effects for Endo/Epi and Mid cells were taken from the ORd human model in which GKs for Endo and Epi were both 1.4 and for Mid was 1.0 [20].

AP durations (APD) at 95% repolarization (APD95) for endocardial (Endo), mid-myocardial (Mid), and epicardial (Epi) myocytes were measured. APD95 was measured as the interval between the time of maximum AP upstroke velocity and the time at which the membrane voltage returned to 95% of its resting value. The largest difference among Endo, Mid, and Epi APD95 was normalized by the APD95 of Mid and the value in % was used to represent TDR.

To determine how V141M KCNQ1 affects repolarization in the context of heterogeneous heart tissue, simulations were performed on a 1-dimensional transmural fiber model. The fiber was composed of 60 Epi, 45 Mid, and 60 Endo myocytes. Gap junction conductance was homogenous throughout the fiber at  $1.73 \mu s$ , except for a fivefold decrease at the Mid-to-Epi transition region. A 0.5-ms current stimulus was applied to Endo cell 1 to initiate Endo-to-Epi AP propagation. The resulting conduction velocity was 44 cm/s. The QT interval on the pseudo-ECG generated by the fiber was computed as the interval between the maximum negative derivative on the QRS and the maximum positive derivative on the T-wave.

We simulated antiarrhythmic drug effects by introducing conductance changes for specific ionic currents. Using conductance scaling, Benson et al. reproduced AP changes caused by sotalol and amiodarone in canine left ventricle transmural strips [22, 23]. To simulate amiodarone application of 30–40 mg/kg/day, maximal conductance of the late sodium current ( $I_{NaL}$ ) was scaled by 0.2 in Mid, and maximal conductance of  $I_{Ks}$  was scaled by 0.2 in Endo and 0.7 in Epi [23]. To simulate 100  $\mu$ M/L sotalol, we scaled the rapid delayed rectifier potassium current ( $I_{Kr}$ ) maximal conductance by 0.5 in Endo, 0.3 in Mid, and 0.8 in Epi [23]. To simulate 6–10  $\mu$ M/L quinidine, we scaled maximal conductance of  $I_{NaL}$  by 0.6, of  $I_{CaL}$  by 0.75, of  $I_{Kr}$  by 0.6, of the inward rectifier current ( $I_{K1}$ ) by 0.6 [24–26], and of the transient outward current ( $I_{to}$ ) by 0.6 in Mid, by 0.46 in Endo, and by 0.6 in Epi based on experimental results from guinea-pig, rabbit, or canine ventricular myocyte studies [24–27].

### 3 Results

# 3.1 V141M Mutation Accelerates $I_{Ks}$ Activation, Decelerates Deactivation, and Causes a Negative Shift in $I_{Ks}$ Voltage-Dependence

The KCNQ1/KCNE1 channels that were expressed in *Xenopus* oocytes were activated every 100 s from a holding potential of -100 mV with 3 s depolarizing pulses ranging from -100 to +60 mV (Fig. 1a). We had noticed much larger instantaneous currents on shorter sweep intervals and therefore used a long sweep interval of 100 s. After each test pulse, the membrane was repolarized to -40 mV to record tail currents. Measured from the

conductance–voltage (G–V) relation curves, heterozygous V141M KCNQ1/KCNE1 channels were activated at more negative potentials compared to the WT ( $V_{1/2} = 33.6 \pm 4.0$  mV for WT, 24.0  $\pm$  1.3 mV for V141M; n = 5 for each) (Fig. 1b). The rates of I<sub>Ks</sub> activation were fitted with a double exponential function. The V141M caused faster activation of I<sub>Ks</sub> at depolarizing potentials ranging from 0 to +50 mV (Fig. 1c). The same oocytes used for the voltage-dependence of I<sub>Ks</sub> conductance were subjected to another pulse protocol where a depolarizing pulse was fixed at +40 mV followed by various repolarizing pulses ranging from –70 to –10 mV. The time required for tail currents to decay at different repolarizing potentials was also quantified by fitting the traces to a double exponential function. The heterozygous V141M KCNQ1 expression caused slower deactivation for I<sub>Ks</sub> (Fig. 1d).

# 3.2 Simulated Voltage-Dependent Activation of WT $I_{Ks}$ and Heterozygous V141M $I_{Ks}$ is Consistent with Experimental Results

WT  $I_{Ks}$  and heterozygous V141M  $I_{Ks}$  were simulated for the voltage protocol employed in the experiment (Fig. 1a). The acceleration in  $I_{Ks}$  activation caused by the mutation was simulated by adjusting transition rates in the  $I_{Ks}$  Markov model (see Supplementary Material). The conductance-voltage relations show good agreement between the experimental and simulation results (Fig. 1b).

# 3.3 Simulations of Changes to Action Potentials, $I_{\mbox{Ks}}$ , and $I_{\mbox{CaL}}$ in Endo, Mid, and Epi Myocytes

The Markov models for WT and V141M  $I_{Ks}$  were introduced in the ORd model to simulate the AP and corresponding time course of  $I_{Ks}$  and L-type calcium current ( $I_{CaL}$ ) in Endo, Mid, and Epi myocytes. Further, AP simulations were performed to evaluate the effects of  $\beta$ adrenergic stimulation by using the Heijman et al. model of the  $\beta$ -adrenergic cascade [21] at 1 µmol/L ISO application. With V141M mutation, APD95 was shortened for all three myocyte types. The APD shortening resulted from the rapid activation of  $I_{Ks}$  and larger  $I_{Ks}$ peak amplitude during the AP (Fig. 2; Table 1). The rapidly repolarizing potential causes augmentation of  $I_{CaL}$  amplitude, especially in the presence of ISO (Fig. 2). This, in turn, resulted in a "bump" during phase-3 repolarization of the AP which was most noticeable in Mid. The magnitude of V141M-induced APD shortening was further enhanced by the presence of ISO in all three myocyte types (Table 1). Consistent with the reported clinical presentation of SQTS [28], the rate-adaptation of APD was blunted by the V141M mutation (Fig. 3).

#### 3.4 V141M KCNQ1 Mutation Increases Transmural Heterogeneity of Repolarization

Increased transmural heterogeneity of repolarization has been suggested as a pro-arrhythmic substrate in SQTS [15]. We quantified the transmural heterogeneity of repolarization as described in the Methods section. At baseline, APD heterogeneity augmentation by the V141M mutation was most noticeable at a cycle length of 1000 ms (Fig. 3). However, in the presence of ISO, V141M-augmented APD heterogeneity was present at long and short cycle lengths as well. In WT, ISO induced less transmural APD heterogeneity at both rapid and slow cycle lengths. In contrast, with V141M KCNQ1 mutation, ISO induced more transmural heterogeneity at slow cycle lengths (Fig. 3).

#### 3.5 Specific I<sub>K1</sub> Blockade Reduces the Transmural APD Heterogenecity

The effects of different anti-arrhythmic drug actions and several specific channel blockers on the V141M-augmented transmural APD heterogeneity were examined by computer simulations. Amiodarone and sotalol are class III antiarrhythmic agents whose main electrophysiological effects include AP prolongation [23]. However, in our simulations of the cellular effects of 100  $\mu$ M/L sotalol or amiodarone (30 mg/kg/day), both drugs failed to reduce the transmural heterogeneity of APD. The next anti-arrhythmic drug we tested was quinidine, which has multiple depressing effects on sodium, calcium and potassium currents and generally prolongs the AP [24–26, 29]. Quinidine has shown promise in treating SQTS patients [30]. However, it did not reduce the transmural heterogeneity of APD in our simulations for the V141M mutation. Specific I<sub>Ks</sub> blockade also failed to reduce the transmural heterogeneity of APD at either 50 or 90% blockade. Finally, with 90% specific I<sub>K1</sub> blockade, the transmural heterogeneity of V141M APD was reduced below that of WT. The APD heterogeneity was reduced by specific I<sub>K1</sub> blockade at both long and short cycle lengths (Fig. 4).

#### 3.6 Specific I<sub>K1</sub> Blockade Abolishes V141M Mutation-Induced QT Interval Shortening

We examined effects of the V141M KCNQ1 mutation on QT intervals of a pseudo-ECG that was computed for a 1D transmural fiber at different pacing cycle lengths (Fig. 5a). The phenotype of QT shortening was reproduced by introducing a V141M I<sub>Ks</sub> Markov model into the Endo, Mid, and Epi myocytes of the fiber (Fig. 5b). The QT intervals for mutant V141M were shorter than WT at all (short and long) cycle lengths, especially with ISO challenge (Fig. 5c). V141M-induced QT shortening with ISO challenge was abolished by 90% specific I<sub>K1</sub> blockade (Fig. 5b, c).

### 4 Discussion

The results of the present study show that: (1) the V141M KCNQ1 mutation causes gain-offunction of  $I_{Ks}$  mainly by accelerating channel activation and decelerating deactivation; (2) V141M KCNQ1 mutation-induced shortening of APs is more prominent in the presence of  $\beta$ -adrenergic stimulation; (3) V141M KCNQ1 augments transmural heterogeneity of repolarization, a property that has been suggested as an arrhythmogenic mechanism in SQTS; and (4) specific  $I_{K1}$  blockade has a beneficial effect of reducing the transmural APD heterogeneity and normalizing the short QT interval associated with the V141M KCNQ1 mutation.

Hong et al. reported that the V141M KCNQ1 mutation only altered the gating of  $I_{Ks}$  channels in the presence of KCNE1 auxiliary subunits [12]. They also showed that coexpression of V141M and WT KCNQ1 with KCNE1 produced a current with intermediate biophysical properties between homozygous V141M and WT  $I_{Ks}$ . Consistent with their results, our heterozygous V141M  $I_{Ks}$  also demonstrated an instantaneous current. Notably, the magnitude of the instantaneous current became smaller as we prolonged the sweep interval from 40 to 100 s. With the longer sweep interval, tail currents were suitable for an accurate fitting analysis of the G-V relationship.

The V141M KCNQ1 mutation has been linked to SQTS2, with presentation including extremely short QT interval, fetal bradycardia, and atrial fibrillation [12, 13]. Heterogeneous AP shortening was shown to result in augmented dispersion of APD across the ventricular wall with another SQTS2 mutation [31]. Our simulations showed that the APD shortening resulting from the V141M KCNQ1 mutation is also heterogeneous (Table 1) and leads to an increase in transmural APD heterogeneity and dispersion of repolarization.

In long QT syndrome 1, which is also caused by KCNQ1 mutation affecting  $I_{Ks}$ , a greater reactivity of the sympathetic control of the QT interval has been recognized as a protective factor [32]. Similarly, it is crucial to determine the reactivity of the sympathetic control of the QT interval to evaluate the arrhythmic risk related to V141M KCNQ1 mutation. To our knowledge, there is no published report showing how the V141M mutant responds to  $\beta$ -adrenergic stimulation. Therefore we assumed that  $\beta$ -adrenergic targets are the same as in WT I<sub>Ks</sub> and respond similarly to adrenergic stimulation. Based on this assumption,  $\beta$ -adrenergic stimulation augments APD heterogeneity for V141M KCNQ1 mutation.

In the simulations,  $I_{CaL}$  is severely reduced by including V141M in the model (Fig. 2). The literature reports a phenotype of concurrent sinus bradycardia in patients with V141M mutation [12, 13]. Reduced  $I_{CaL}$  density was shown to contribute to slowing of diastolic depolarization of the sinoatrial AP, resulting in slowing of the intrinsic heart rate, even with preserved  $\beta$ -adrenergic response [33]. Reduced  $I_{CaL}$  may also affect contractility, but clinical reports did not mention abnormal ventricular function [12].

Notably different from wild type, the degree of APD heterogeneity in V141M KCNQ1 is greater at a long cycle length. Reduced rate-adaptation of the QT interval has been observed in SQTS [14, 28]. SQTS2 patients with the V141M KCNQ1 mutation have been reported to present with bradycardia resulting from sinus and atrioventricular node dysfunction in utero and after birth [4, 12, 13]. Our simulations suggest that in SQTS2 with V141M KCNQ1 mutation, arrhythmia vulnerability is higher at a slow heart rate. In the simulations, both amiodarone and sotalol failed to reduce V141M-augmented APD heterogeneity. Amiodarone and sotalol can inhibit sinus and atrioventricular nodal function but can potentially worsen the bradycardia observed in SQTS2 patients. Therefore we suggest that these drugs should probably be avoided for SQTS2 patients with the V141M KCNQ1 mutation.

There has been growing evidence that quinidine is effective in treating SQTS [14, 30, 34]. However, quinidine can cause serious side effects such as thrombocytopenia and agranulocytosis [35]. In the simulations, quinidine did not reduce APD heterogeneity during  $\beta$ -adrenergic stimulation. An important finding of this study is that I<sub>K1</sub> blockade markedly reduced APD heterogeneity in SQTS. Specific I<sub>K1</sub> blockade was shown to reduce the incidence of ventricular fibrillation and ischemia–reperfusion ventricular arrhythmias in rats, rabbits, and primates by prolonging APD. Based on pioneering efforts using a transmural ventricular wedge preparation to relate the AP to electrocardiographic waveforms in experiments and in silico [36, 37], we applied the pseudo-ECG modeling approach to provide QT interval changes in KCNQ1 V141M mutation under variable conditions. The specific I<sub>K1</sub> block was also effective in reducing TDR [38, 39]. Our simulations provide

support for specific  $I_{K1}$  blockade as a potential antiarrhythmic strategy in patients with SQTS. The results are relevant to a better understanding of SQTS2, offering a clue to more feasible risk stratification, and helping to dissect the mechanisms underlying the efficacy of pharmacologic interventions.

In this study, we used the ORd model without considering the possibility of mutation effects on the membrane expression levels of  $I_{Ks}$ . In addition to affecting  $I_{Ks}$  kinetics, it is possible that the V141M KCNQ1 mutation also changes  $I_{Ks}$  densities in a transmurally heterogeneous fashion, adding to TDR. The purpose of the channel expression system is to determine the WT and V141M  $I_{Ks}$  channel kinetics in order to perform the subsequent human AP simulations. The oocyte system provide large  $I_{Ks}$  therefore the endogenous KCNQ1 current can be ignored. There are other systems would offer different advantages. The mammalian heterologous expression systems such as HEK293 cells provide feasibility for applying a physiological temperature (37 °C), and for inducing cAMP as a PKA activation. The human cardiomyocytes that are generated from inducible pluripotent stem cells would allow us to precisely determine the sensitivity to channel inhibitors or drugs for V141M mutation. However there remains problems to reproduce a homogenous population of ventricular myocytes with typical and same phenotype in dishes [40].

In conclusion, we demonstrated shortening of APD and QT in V141M KCNQ1 mutation due to accelerated activation and decelerated deactivation kinetics of  $I_{Ks}$ . The APD shortening is transmurally heterogeneous and results in increased transmural dispersion. This effect can contribute to arrhythmia vulnerability in SQTS2 patients with the V141M mutation. Simulated application of  $I_{K1}$  blocker improved transmural APD heterogeneity and QT interval widening, suggesting specific  $I_{K1}$  blockade as a potential antiarrhythmic strategy in SQTS.

## **Supplementary Material**

Refer to Web version on PubMed Central for supplementary material.

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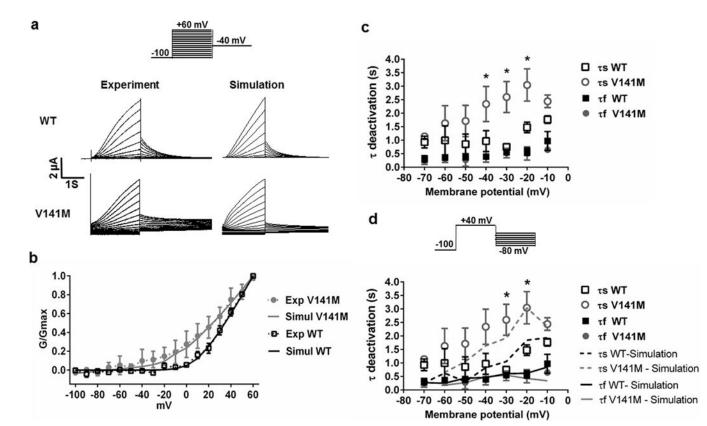
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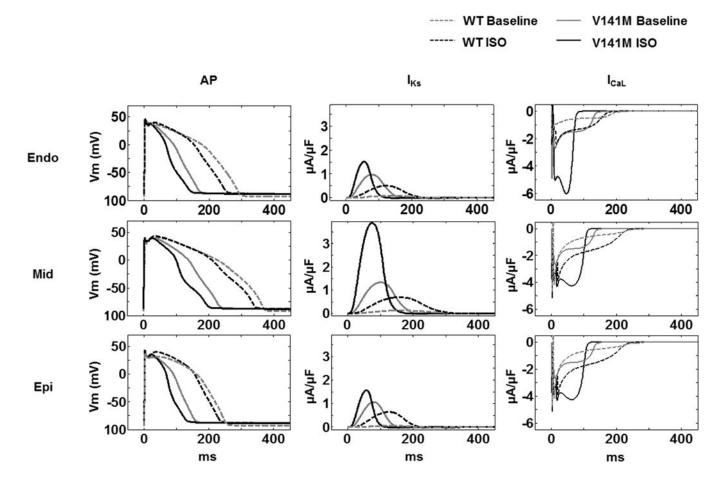
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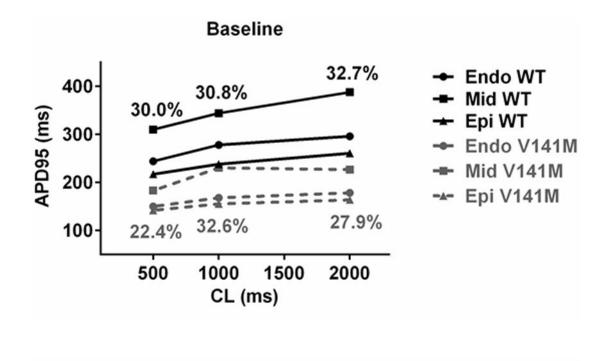
#### Fig. 1.

V141M KCNQ1 affects activation kinetics and voltage dependence of IKs. a Currents of WT KCNQ1/KCNE1 channels (WT IKs) and heterozygous V141M KCNQ1/KCNE1 channels  $(V141M I_{Ks})$  expressed in *Xenopus* oocytes (*left panels*). The currents were elicited by test pulses to +60 mV from a holding potential of -100 mV. Tail currents were measured at -40 mV for WT and V141M  $I_{\text{Ks}}.$  The WT and V141M  $I_{\text{Ks}}$  were simulated using a Markov model (right panels; see supplementary materials). b V141M KCNQ1 mutation caused a leftward shift of the conductance–voltage curve ( $V_{1/2} = 33.6 \pm 4.0$  mV for WT,  $24.0 \pm 1.3$ mV for heterozygous V141M; n = 5 for each). Simulation results (solid lines) are consistent with the experimental data (dashed lines). c Voltage dependence of activation and deactivation time constants ( $\tau$ ) of WT and heterozygous V141M I<sub>Ks</sub> (n = 5 for each).  $\tau$ activation was obtained from fitting the activating current traces with a double exponential function. V141M KCNQ1 causes faster activation of  $I_{Ks}$  (\*p < 0.05 for  $\tau 1$  and <sup>#</sup>p < 0.05 for  $\tau$ 2; V141M vs WT; n = 3 for each). d V141M KCNQ1 causes slower deactivation of I<sub>Ks</sub> (\*p value <0.05 for  $\tau_s$ ; V141M (n = 5) versus WT (n = 3).  $\tau$  deactivation was obtained from fitting the deactivating current traces with a double exponential function. Lines indicate specific  $\tau$  values for simulations

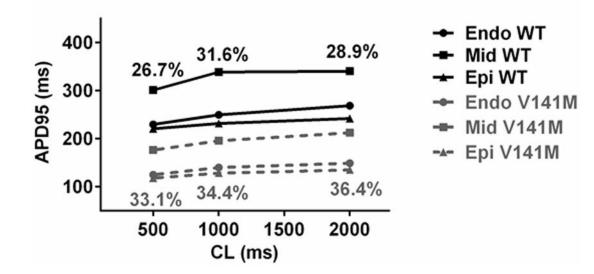


#### Fig. 2.

Simulated WT and heterozygous V141M KCNQ1 action potentials (AP) and the  $I_{Ks}$  and  $I_{CaL}$  during the AP in endocardial (Endo), epicardial (Epi) and midmyocardial (Mid) myocytes with and without isoproterenol (ISO). A modified O'Hara-Rudy (ORd) human ventricular myocyte model was used in the simulations. The cycle length was 1000 ms. Baseline APs (in *grey*) and APs with ISO challenge (in *black*) were simulated for WT (*dash lines*) and V141M KCNQ1 (*solid lines*) respectively. APs were shortened significantly by the V141M KCNQ1 mutation with and without ISO. In all V141M cases,  $I_{Ks}$  and  $I_{CaL}$  increased relative to WT during the AP



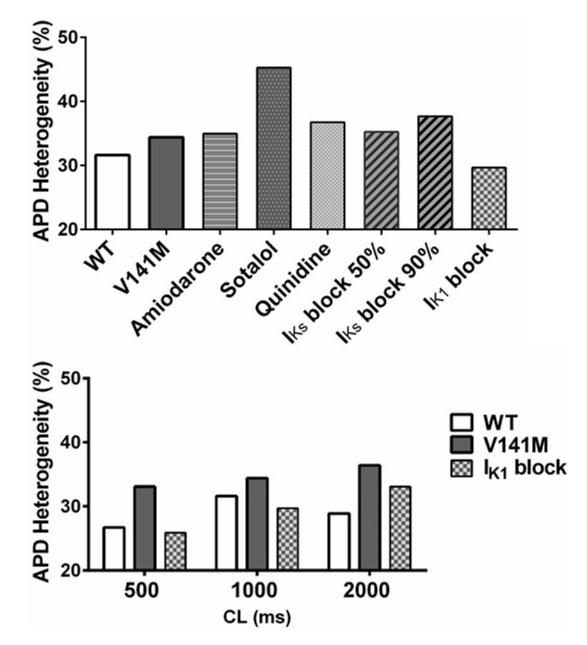
ISO



#### Fig. 3.

AP simulations show blunted APD rate adaptation and increased transmural heterogeneity of APD associated with the V141M KCNQ1 mutation. At fast cycle lengths of 500 ms and slow cycle lengths of 2000 ms, WT KCNQ1 APD increased 52.0, 77.6, and 43.5 ms in Endo, Mid and Epi, respectively, but V141M KCNQ1 mutation APD increased 28.3, 43.7, and 21.5 ms respectively (*upper panel*). At cycle lengths of 500 and 2000 ms, APD heterogeneity diminished from 30.0 to 26.7% and from 32.7 to 28.9% respectively in the presence of isoproterenol (ISO) challenge in WT. In contrast, the heterogeneity of APD was augmented with ISO in V141M KCNQ1. In the presence of ISO, APD heterogeneity increased from 22.4 to 33.1%, from 27.9 to 36.4%, and from 32.6 to 34.4%, at cycle lengths

of 500, 2000, or 1000 ms, respectively. The heterogeneity increase was due to preferential abbreviation of epicardial (Epi) and endocardial (Endo) cells as compared with mid-myocardial (Mid) cells

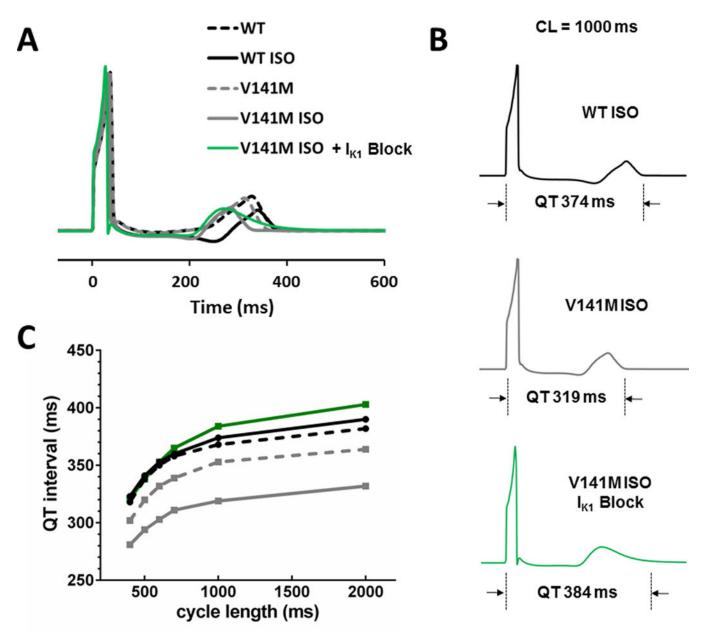


#### Fig. 4.

Effects of different anti-arrhythmic agents or channel blockers on the V141M KCNQ1augmented transmural heterogeneity of APD. At a cycle length of 1000 ms with isoproterenol (ISO) (*upper panel*), amiodarone, sotalol, quinidine and  $I_{Ks}$  block (either at 50 or 90% block) all failed to reduce the mutation-augmented transmural heterogeneity of APD (*upper panel*). Only the  $I_{K1}$  block (with 90% block) improved APD heterogeneity at both long and short cycle lengths under ISO challenge (*lower panel*)

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#### Fig. 5.

Effects of  $I_{K1}$  blockade on the pseudo-ECG and QT interval. **a** Pseudo-ECGs at a cycle length of 1000 ms for WT and V41M KCNQ1 mutation, at baseline and with isoproterenol, and with 90%  $I_{K1}$  block. **b** QT interval measurements for each pseudo-ECG are indicated. c QT intervals on the pseudo-ECG are plotted against the cycle length. In the case of V141M, the QT interval was abnormally shortened with ISO; the shortening of the QT interval was corrected by specific  $I_{K1}$  blockade. *ECG* electrocardiogram, *WT* wild type, *V141M* V141M KCNQ1 mutation Author Manuscript

# Table 1

Computed APD<sub>95</sub> and I<sub>Ks</sub> for WT and V141M KCNQ1 using the ORd human ventricular model for Endo, Mid, and Epi myocytes

| Myocytes | Condition       | ORd human              | Myocytes Condition ORd human ventricular myocyte model [20] |  |  |
|----------|-----------------|------------------------|---|--|--|
|          |                 | APD <sub>95</sub> (ms) | Peak I <sub>Ks</sub> amplitude (pA/pF)                      | PD <sub>95</sub> (ms) Peak I <sub>Ks</sub> amplitude (pA/pF) APD <sub>95</sub> shortening (ms%) (V141M V.S. WT) APD <sub>95</sub> shortening (ms%) (ISO V.S. baseline) | APD <sub>95</sub> shortening (ms/%) (ISO V.S. baseline |
| Endo     | WT              | 278.3                  | 0.086   |  |  |
|          | V141M           | 168.1                  | 0.973   | 110.2/39.6   |  |
|          | WT ISO          | 249.9                  | 0.507   |  | 28.4/10.2  |
|          | V141M ISO 140.1 | 140.1                  | 1.516   | 109.8/43.9   | 28.0/16.7  |
| Mid      | WT              | 344                    | 0.128   |  |  |
|          | V141M           | 230.6                  | 1.336   | 113.4/33.0   |  |
|          | WT ISO          | 338.9                  | 0.696   |  | 5.1/1.5  |
|          | V141M ISO       | 195.7                  | 3.898   | 143.2/42.3   | 34.9/15.1  |
| Epi      | WT              | 238.2                  | 0.0695  |  |  |
|          | V141M           | 155.5                  | 1.066   | 82.7/34.7  |  |
|          | WT ISO          | 231.8                  | 0.648   |  | 6.4/2.9  |
|          | V141M ISO 128.4 | 128.4                  | 1.565   | 103.4/44.6   | 27.1/17.4  |